# CONTRACTILE SKELETAL MUSCLE MICROTISSUES IN MICROCHANNEL

Kazunori Shimizu<sup>1,2\*</sup>, Hiroyuki Araki<sup>2</sup>, Wataru Tonomura<sup>2</sup>, Mitsuru Hashida<sup>2</sup>, Satoshi Konishi<sup>1</sup>

<sup>1</sup>Kyoto University, Japan, <sup>2</sup>Ritsumeikan University, Japan

### ABSTRACT

This paper reports a development of the microfluidic device for fabrication and cultivation of contractile skeletal muscle tissue in microchannels. Microfluidic processes were only used to develop contractile skeletal muscle microtissues in microchannels. Thus, the volume of the collagen gel used to fabricate the microtissues can be defined precisely. The fabricated microtissues can be cultured under a more *in vivo*-like environment and used for higher throughput applications. Tunnel-like microchannels connecting 2 microchannels realized to pattern the collagen gel with cells and supply the medium to the cells (Fig.1). The developed microtissues in microchannels may be powerful tools for drug development and biological research.

#### **KEYWORDS**

Cells, 3D-Cell culture, Skeletal muscle, Muscle on a chip, Electrical stimulation, Force



Figure 1: Conceptual illustrations of the device.

# INTRODUCTION

Skeletal muscle possesses the physiological significance and outstanding characteristics. So far, some groups including our group have fabricated 3-dimensional (3D) cultured skeletal muscle microtissues in vitro and utilized them for drug screening and biological research [1-3]. Although the microfluidic devices for 3D cell culture have been developed for some cell types (endothelial cells, neural cells, etc), the devices for skeletal muscle cells have not been reported to the best of our knowledge. Previously, the skeletal muscle microtissues were fabricated by using microfabrication techniques and cultured in micro-wells or dishes filled with medium [3-6]. In contrast, in the present study, microfluidic technologies were used to both fabricate and culture the skeletal muscle microtissues.

# EXPERIMENT

As shown in Fig.1, the device consists of 2 microchannels for cells ( $\mu$ Ce) and medium ( $\mu$ Me). They are connected each other by tunnel-like microchannels. Collagen solution mixed with cells are introduced into the  $\mu$ Ce and solidified at 37°C. After that, medium is introduced into the  $\mu$ Me and cells in the collagen gel are cultured. In this process, tunnels play 2 roles. One is that they prevent the collagen solution from leaking into the  $\mu$ Me. The other is that they allow the medium diffuse into the gel in the  $\mu$ Ce for cell culture. The device was made of 2 layers of PDMS. Micropatterned slabs were bonded to slabs without patterns (Fig.2).



Figure 2. Top and cross-sectional views of the developed microdevice.

The performance of the tunnels was investigated (Figs.3 and 4). When the colored solution was introduced into  $\mu$ Ce, no leakage of the solution into  $\mu$ Me was observed (Fig.3). To confirm the diffusion of the medium, FITC-labeled albumin solution was introduced into the  $\mu$ Me after the collagen solution was solidified in the  $\mu$ Ce. The albumin diffused throughout the collagen gel within 120 min (Fig.4).



Figure 3. Introduction of the colored solution into the  $\mu$ Ce. No leakage was observed to the  $\mu$ Me.



Figure 4. Introduction of the FITC labeled albumin solution into the  $\mu$ Me of the device with collagen gel in the  $\mu$ Ce. The albumin was diffused throughout the gel within 120 min (A and B).

Mice skeletal myoblasts (C2C12) was cultured in the device (Fig.5). Myoblasts need to differentiate to myotubes to obtain contractility. The medium containing 2% horse serum was used for inducing differentiation. The collagen solution containing myoblasts (10^7 cells/ml) was introduced and solidified in the  $\mu$ Ce. Then, the medium was introduced into the  $\mu$ Me. The gel started to dissociate from the inner surface of the  $\mu$ Ce after 4 days and cylindrical 3D micro-tissue was formed after 6 days (Fig.5A). Aligned myotubes ( $\alpha$ -actinin positive cells) were observed in the microtissue (Fig.5B) and the cultured tissue in the  $\mu$ Ce contracted in response to the applied electric stimulation (Fig.6).



*Figure 5. Results of cell culture in the device. A: Process of differentiation. B: Myotubes were visualized* (*Green: α-Actinin*).



Figure 6. Cultured skeletal muscle microtissues (day6) were contracted in response to the applied electrical stimulation (1 and 0.5 Hz). Scale bar: 50 µm.

#### ACKNOWLEDGEMENTS

This study was partly supported by the Ritsumeikan Global Innovation Research Organization (R-GIRO).

#### REFERENCES

[1] H. Vandenburgh, J. Shansky, F. Benesch-Lee, V. Barbata, J. Reid, L. Thorrez, R. Valentini, and G. Crawford, *Drug-screening platform based on the contractility of tissue-engineered muscle*, Muscle Nerve, 37, 438 (2008).

[2] A. Khodabukus, K. Baar, *Defined Electrical Stimulation Emphasizing Excitability for the Development and Testing of Engineered Skeletal Muscle*. Tissue Engineering Part C-Methods 18, 349 (2012).

[3] H. Fujita, K. Shimizu, E. Nagamori, *Novel Method for Measuring Active Tension Generation by C2C12 Myotube Using UV-Crosslinked Collagen Film.* Biotechnol. Bioeng. 106, 482 (2010).

[4] K. Shimizu, H. Sasaki, H. Hida, H. Fujita, K. Obinata, M. Shikida, E. Nagamori, Assembly of skeletal muscle cells on a Si-MEMS device and their generative force measurement, Biomedical Microdevices, 12, 247 (2010).

[5] K. Nagamine, H. Kaji, M. Kanzaki, and M. Nishizawa, Gel sheet based skeletal muscle cell culture system integrated with the microelectrode array device, Proceedings of MicroTAS 2010, 175. (2010)

[6] Y. Morimoto, M. Kato-Negishi, H. Onoe, and S. Takeuchi, *Aligned free-standing muscle fibers connected with neurons*, Proceedings of MicroTAS 2011, 789. (2011)

#### CONTACT

\*Kazunori Shimizu tel: +81-75-753-9568; kshimizu@pharm.kyoto-u.ac.jp