Retraction for Analyst:

Retracted article: A new sensor for the assay of breast cancer antigen

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We, the authors Raluca-Ioana Stefan-van Staden, Ileana Stefanescu, Jacobus F. van Staden and Marius Enachescu, hereby wholly retract this *Analyst* article. Due to confidentiality reasons and possible conflict of interest we cannot provide at this stage more data to support the conclusions of the article.

Signed: R. I. Stefan-van Staden, J. F. van Staden, National Institute of Electrochemistry and Condensed Matter, Bucharest, Romania, and I. Stefanescu, M. Enachescu, University "Politehnica" Bucharest, Romania.

This retraction is endorsed by May Copsey, Editor. Retraction published 6th September 2012.

Editor's Note: Significant concerns have been received from members of the community regarding the extent of the conclusions that have been drawn in the above *Analyst* article based on the data presented in the article. May Copsey, Editor.

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ARTICLE TYPE

A new sensor for the assay of breast cancer antigen

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⁵ A stochastic sensor based on maltodextrin (dextrose equivalent between 4 and 7), and diamond paste was designed and used for the screening of whole blood for a specific breast cancer biomarker. The sensor can be used for the assay of the breast cancer antigen in the linear concentration range: 5.0-10 500.0U/mL.

Early diagnosis of cancer is a priority in the medical world because patients detected at an early stage have the highest rate (80 to 100%) of survival if treated with correct medication. ¹⁵ Screening is an option for this purpose, and can be performed using stochastic sensors, because this type of sensors can show the "signature" of the analyte (t_{off}) as well as the amount of the

analyte in the sample (t_{on}).¹⁻³ Studies were conducted by different scientists in order ²⁰ to identify the biomarkers for breast cancer with the highest incidents in patients.^{4,5} Tests performed on human mammary cells reveals that these cells expressed at their surfaces polymorphic epithelial mucin (PEM) which was named breast cancer antigen and CA15-3.^{4,5} Accordingly this was the substance

- ²⁵ to identify and quantify in the biological fluids in order to have the correct diagnosis of breast cancer. To date, different methods were proposed for detection of cancer, based on cancer cell detection using impedimetric transducers,⁶ biosensors based on gold nanoparticles,⁷ Raman maps,⁸ fluorescence,⁹ and detection ³⁰ of the specific biomarkers using calorimetry,¹⁰ suspended
- ³⁰ of the specific biomarkers using calorimetry,¹⁰ suspended microchannel resonators¹¹ and opto-fluidic ring resonator biosensors.¹²

In this article we propose a stochastic sensor based on maltodextrin with dextrose equivalent between 4 and 7 (this is the

³⁵ first dextrin used to develop a stochastic sensor), having a compact helix structure – as electrochemical active material. The maltrodextrin was physically immobilized on a diamond paste matrix. We chose the natural diamond powder having a particle size of 1µm, because in previous experiments it gave the best
⁴⁰ sensitivity, selectivity and S/N ratio for amperometric

measurements.¹³ The choice of stochastic sensors for this type of determination was done because one can determine if the biomarker is in the biological fluid, and in which quantity, the values of t_{off} and t_{on} being independent on the matrix from where ⁴⁵ the biomarker is determined.¹⁴

Experimental

Natural diamond powder having a particle size of 1µm (99.9%), maltodextrin (dextrose equivalent 4-7) and breast tumor antigen (0.1mol/L solution in phosphate buffer, pH=7.4 ⁵⁰ containing 0.1% NaN₃) were purchased from Aldrich

(Milwaukee, USA); paraffin oil was purchased from Fluka (Buchs, Switzerland). 0.1mol/L Phosphate buffer solution (pH=7.4), and NaN₃ were purchased from Merck. Deionised water obtained from a Millipore Direct-Q 3 System (Molsheim, Experimentation of 0.025 S/

⁵⁵ France) having a conductivity of 0.05µS/cm, was used for the preparation of all solutions. The solutions of biomarkers were all made in 0.1 mol/L phosphate buffer (pH=7.4) containing 0.1% NaN₃ in order to have the medium from the vials on which the antigen was purchased. The range of concentrations for sensors'
⁶⁰ evaluation was obtained using serial dilution technique, from 0.005 to 5000U/mL.

Maltodextrin was physically immobilized in the diamond paste. The modified diamond paste was prepared as follows: 200 mg of natural monocrystalline diamond powder was ⁶⁵ mixed with 20 μ L paraffin oil to form a diamond paste. 100 μ L from the solution of maltodextrin with dextrose equivalent 4-7 (10⁻³mol/L) was added to the diamond paste. The modified paste was placed into a plastic tube (Fig.1). The diameter of the sensor was about 300 μ m. Electric contact was obtained by inserting an A (C) sensor was about 300 μ m.

70 Ag/AgCl wire into the modified diamond paste. The surface of the sensor was wetted with deionised water and polished with alumina paper (polishing strips 30144-001, Orion) before using. When not in use, the sensor was stored in a dry state at room temperature.



Fig. 1 Stochastic sensor based on maltodextrin.

A PGSTAT 12 and software Ecochemie (version 4.9) ⁸⁰ were used for all chronoamperometric measurements. A Pt electrode and an Ag/AgCl electrode served as the counter and reference electrodes in the cell. A Cyberscan PCD 6500 pH/mVmeter from Eutech Instruments was employed for all pH measurements.

A chronoamperometric technique was used for the measurements of t_{on} and t_{off} at 125mV. At this value of potential the sensor had a stochastic behavior. The electrodes were dipped into a cell containing solutions of biomarker (buffered with a

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solution containing 0.1 mol/L phosphate buffer (pH=7.4) and 0.1% NaN₃) of different concentrations. Equations of calibration $1/t_{on} = f(\text{Conc.})$ are determined using statistics. The unknown concentrations of biomarker in blood samples were determined s from the calibration equations.

Results and discussions

High-resolution imaging using atomic force microscopy (AFM) has been applied to observe the differences of surface structures between unmodified diamond paste and ¹⁰ modified diamond paste with maltodextrin. The topography of the surfaces was investigated by AFM in tapping mode in a range of scan lengths from 50µm to 1µm. These measurements were carried out with an Agilent 5500 SPM system, described by PicoSPM controlled by a MAC Mode module and interfaced with

- ¹⁵ a PicoScan controller from Agilent Technologies, Tempe, AZ, USA (formally Molecular Imaging). A multipurpose large scanner and Point Probe Plus Silicon SPM Sensor cantilevers (PPP-FM cantilevers), n⁺- silicon material with no coating, of about 227 μ m length, 1.8 N m⁻¹ spring constants, with the tips
- 20 oscillated near their resonant frequencies in air, of about 64 kHz were used for all measurements. Scanning of the surface was done at a rate of 0.8-1.2 lines per second, at room temperature in the tapping mode.
- Table 1 shows the AFM topographical images of plane ²⁵ and modified diamond paste based sensor. The surface roughness analysis was performed for both modified and unmodified diamond pastes. Because the roughness can be defined by either S_q (root mean square height) or S_a (arithmetical mean height) value, we determine these parameters using the PicoImage tool
- ³⁰ and accordingly with ISO25178, these values were automatically calculated. The values obtained for the unmodified diamond paste were S_q =13.6nm, and S_a =10.8nm, while for the diamond paste modified with maltodextrin were S_q =119nm, and S_a =88.2nm. The significant difference between roughness of plane and modified ³⁵ pastes as well as of images obtained proved that the maltodextrin
- was physically immobilized into the diamond paste.

Table 1 AFM topographical	images	of plane	and	modified
diamond paste based sensor				



No structural changes (for maltodextrin or diamond) are expected from this type of immobilization. The presence of

the round channel in the modified paste justified the stochastic behavior of the sensor when a constant value of potential 45 (125mVvs Ag/AgCl) was applied and the current value vs. time was recorded.

Breast cancer antigen is a transmembrane protein which contains two subunits that form a stable dimer. The signature of breast tumor antigen is given by the value of t_{off} which is 3.3s ⁵⁰ when both standard biomarker solutions and whole blood samples were measured. This value can be used for the qualitative analysis of the antigen in whole blood, because it did not change when the biomarker was assayed from whole blood samples (Table 2).

For the quantitative analysis, the measurements were performed for 6 months in order to determine the stability as well as the sensitivity of the sensor. The equation of calibration for the stochastic sensor was determined using the values of t_{on} - defined as the binding time¹ (binding constant (determined from the 60 experimental data) between maltodextrin and breast tumor antigen on the channel being $0.011U^{-1}/mL^{-1}$), measured in sec. obtained for different concentrations of the breast tumor antigen, measured in U/mL: $1/t_{on} = 20.11 + 0.044 \times C$

The correlation coefficient, r for this equation was 65 0.9608. Calibration graph is shown in Fig.2.



Fig. 2 Calibration graph of maltodextrin based stochastic sensor.

The linear concentration range was between 5.0 and 500U/mL, covering patients who are on an early stage as well as patients on late stages of breast cancer. The sensitivity was 0.044mol s/mL, with a limit of detection of 0.25U/mL. The relative standard deviation (RSD%) per sensor was less than 75 0.1% for the response/sensitivity of the sensor, values being recorded for the 6 months. Ten sensors were designed and tested during this period; while the results obtained in terms of sensitivity for 6 months had a RSD value less than 0.1%, proving the reliability of the design proposed.

⁸⁰ Other biomarkers such as ovarian cancer antigen, gastrointestinal cancer antigen, and hepatitis B virus antigen were tested as possible interferences using separate solution method and mixed solution method. On both separate and mixed solution methods the tests have shown that each of the biomarkers ⁸⁵ mentioned had a specific signature given by the t_{off} value, which is different from the one recorded for breast cancer antigen. Accordingly, no interference was recorded. Furthermore, the biggest advantages of stochastic sensors is that the signature of the analytes (t_{off} values) are independent on the matrix from ⁹⁰ where the analytes are determined.

The proposed stochastic sensor was used for qualitative and quantitative analysis of the breast tumor antigen from whole

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blood samples. The results obtained were compared with those provided by the clinical laboratories that used for the analysis of breast tumor antigen in serum samples ELISA technique (used in clinical laboratory as standard method for the assay of CA15-3).

- Qualitative assay of the breast tumor antigen was done in whole blood samples using the value of $t_{\rm off}$. Accordingly, $t_{\rm off}$ values specific for the breast cancer antigen were found in four out of five diagrams obtained for real whole blood samples. As a result, there were four positive results and one negative result for
- 10 the screening test performed with the proposed stochastic sensor. The results obtained for qualitative assay are shown in Table 2. A very good correlation between the proposed method (based on stochastic sensor) and standard method (ELISA) was obtained.

15 **Table 2** Qualitative analysis of breast tumor antigen

Tuble 2 Quantative analysis of breast funior analgen					
Sample Nr.	Stochastic sensor based on	ELISA			
	maltodextrin	(standard method,			
	(whole blood samples)	serum samples)			
1	+	+			
2	+	+			
3	+	+			
4	+	+			
5	-	-			

The results obtained for the quantitative assay of breast tumor antigen performed for samples 1-4 are shown in Table 3. The lowest values obtained when ELISA method was used are 20 due to the fact that ELISA is using serum samples - separated

from whole blood samples. Each separation process will induce a decrease of concentration of the analyte determined. The correlation between the values is good, proving that the stochastic sensor can be used for the quantification of the antigen in whole 25 blood.

Table 5 Qualitative analysis of breast funior antigen					
Stochastic sensor based on					
	maltodextrin		ELISA		
Sample	(U/mL)		(standard method,		
Nr.	Whole	Serum	serum samples)		
	blood		(U/mL)		
	samples	samples			
1	98.0	96.2	96.0		
2	69.5	67.7	68.0		
3	45.2	42.8	43.0		
4	56.3	53.5	54.0		

Table 3 Quantitative analysis of breast tumor antigen

The proposed method comparing with ELISA is faster, more selective and reliable, as well as cost effective (more than 100 30 determinations of the breast cancer antigen from whole blood samples can be performed continuously with the same sensor in the same day). A major advantage is also its possibility to determine directly from the whole blood samples the breast cancer specific antigen, while for ELISA, a separation of serum is

³⁵ needed in order to perform the analysis.

The results obtained proved that the sensor is a good screening tool for breast cancer antigen. Its utilization can solve a major problem for breast cancer: early detection. Early detection of breast cancer can avoid the cancer evolution by treating the

⁴⁰ patient immediately with available medication, making possible in most of the cases the 100% recovery of the patient; at the moment treatment at a very early stage is the only way to cure the patients.

Conclusions

- 45 This article opens a new and very important field in the use of stochastic sensors in clinical analyses. The possibility of determining the quality as well as the quantity of the analyte in one run made the method comparable with the best existing chromatographic methods, but at higher precision and lower 50 quantification values. The proposed stochastic sensor was
- reproducible as design and response characteristics.

Notes and references

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