Supporting Information

Intracellular Thiol-Responsive Nanosized Drug Carriers Self-assembled by Poly(ethylene glycol)-b-Poly(ε-caprolactone)-b-Poly(ethylene glycol) Having Multiple

Bioreducible Disulfide Linkages in Hydrophobic Block

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(b)



(a)



Figure S1. ¹H-NMR spectra of (a) the synthesized RSPCL_{1.2} polymers and mPEG-RSPCL_{1.2} copolymers, (b) the commercially-available PCL₅-COOH polymers and the synthesized mPEG-PCL₅ copolymers, and (c) the synthesized ssPCLss polymers and mPEG-ssPCL₅ copolymers in CDCl₃.



Figure S2. GPC chromatograms of (a) the synthesized RSPCL_{1.2} polymers and mPEG-RSPCL_{1.2} copolymers, (b) the commercially-available PCL₅-COOH polymers and the synthesized mPEG-PCL₅ copolymers, and (c) the synthesized ssPCL₅ss polymers and mPEG-ssPCL₅ copolymers in THF.

(a)



Figure S3. Thiol-induced MW change of mPEG-RSPCL_{1.2} copolymers in drug-free mPEG-RSPCL_{1.2} NPs. The degradation experiment was carried out at 37 °C and was analyzed by GPC chromatograms. ($[mPEG-RSPCL_{1.2} NP] = 0.25 mg/mL$, [DTT] = 10 mM)



Figure S4. Thiol-induced size (intensity average) change of various NPs such as mPEG-PCL₅ NPs, mPEG-ssPCL₅ NPs, mPEG-RSPCL_{0.5} NPs and mPEG-RSPCL_{1.2} NPs in DTT-containing DPBS (50 mM, pH 7.4). The degradation experiment was performed at 37 °C for 2 hrs. ([Polymer] = 0.25 mg/mL, [DTT] = 10 mM)



Figure S5. Size change of mPEG-RSPCL_{0.5} NPs was monitored as a function of DTT concentration (1 μ M-100 mM) for 2 hr at RT (n=3).



Figure S6. In vitro cytotoxicity of drug-free mPEG-PCL₅ NPs and mPEG-ssPCL₅ NPs in HeLa and HepG2 cells 48 hr post-treatment. Various concentrations of NPs were used to treat the cells for 48 hr, and the data are expressed as the mean \pm standard error of the mean (SEM) (n=12).



Figure S7. CryoTEM images of drug-free mPEG-RSPCL_{1.2} NPs and drug-loaded mPEG-RSPCL_{1.2} NPs.



Figure S8. Drug loading content (DLC, %) and efficiency (DLE, %) of DOX·HCl-mPEG-RSPCL_{0.5} NPs as a function of temperature (n=3).