**Electronic Supplementary Information** 

## Synthesis of mucoadhesive thiol-bearing microgels from 2-(acetylthio)ethylacrylate and 2-hydroxyethylmethacrylate: towards novel drug delivery systems for chemotherapeutic agents to the bladder

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Fig. S1: Exemplar images showing wash-off of fluorescent microgels from porcine urinary bladder mucosa.



Fig. S2. IR spectra of ATEA:HEMA microgels: (a) 0, (b) 10, (c) 30, (d) 50, (e) 80 and (f) 100 mol% ATEA



Fig. S3: NMR of 80 mol% ATEA microgels, before (blue) and after (red) deprotection with sodium thiomethoxide. Note the disappearance of the thioacetyl  $CH_3$  peak at ~ 2.4 ppm and the appearance of an SH peak at ~1.25 ppm. This peak disappeared upon shaking with  $D_2O$ . During deprotection, the  $CH_2$  protons adjacent to sulphur are shifted upfield, to become a shoulder on the DMSO- $D_6$  solvent peak.



Figure S4: <sup>1</sup>H NMR spectra (DMSO-D<sub>6</sub>) of 10 (red), 30 (blue), 50 (green), and 80 (purple) mol% ATEA microgels. The peak discarded at 2.09 ppm is residual acetone. Not the decreasing intensity of HEMA's OH proton at 4.9 ppm with increasing ATEA content.



Fig. S5: Exemplar FTIR spectrum of 30% ATEA before (blue) and after (green) treatment with sodium thiomethoxide. Cleavage of acetate protecting group confirmed by loss of shoulder at 1690 cm<sup>-1</sup>, corresponding to C=O stretch (expanded in insert), CH<sub>3</sub> bends at 1520 and 1350 cm<sup>-1</sup>, and C-S stretch at 622 cm<sup>-1</sup>. Stretch at 1568 cm<sup>-1</sup> arises from thiolate anion, consistent with Montero-Rama et al.<sup>12</sup>



Fig. S6: Drug release from 30 mol% (blue) and 80 mol% ATEA (yellow) microgels, expressed as % drug release.



Fig. S7: Fitting of Higuchi equation to release data

Table ST Feed mixtures for each copolymer polymerization	Table S1 Feed	mixtures fo	r each co	polymer	polymerization
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ATEA content (mol%)	HEMA (mg)	ATEA (mg)	EGDMA (mg)
0	1000	0	100
10	870	130	100
30	634	366	100
50	428	572	100
80	157	843	100
100	0	1000	100

Table S2 Doxorubicin hydrochloride loading into microgels.

ATEA content (mol%)	Encapsulation efficiency (%)	Drug loading (%)	Equivalent therapeutic dose (mg/mL)
30	75 ± 15	37 ± 5	2.5 ± 1.0
80	86 ± 8	40 ± 4	2.7 ± 1.4

Equation S1:

Encapsulation efficiency = 
$$100 \times \frac{Cmax - Csup}{Cmax}$$

Where Cmax is the total mass of doxorubicin added to the microgel suspension, and Csup is the mass of doxorubicin in the supernatant after centrifugation (i.e. the unloaded doxorubicin).

**Equation S2** 

 $Drug \ loading = 100 \ \times \ \frac{Mass \ of \ doxorubicin \ in \ microgels}{Mass \ of \ doxorubicin \ in \ microgels + mass \ of \ microgels}$ 

Where the mass of doxorubicin can be calculated from the encapsulation efficiency multiplied by the Cmax. Cmax in these experiments was 780  $\mu$ g; and the mass of microgels used was 1 mg.