## **Biomaterials Science**



## Electronic Supplementary Information

## Dual-component Collagenous Peptide/ Reactive Oligomer Hydrogels as Potential Nerve Guidance Materials - from Characterization to Functionalization

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oPNMA- x				COL	base			
		derivatization					figure	description
- <i>x</i>	[%]	DEED	6-AF	[%]	type	[%]	Ū	·
7.5	3.5	-		15	ΝΜΡΟ	10, 8, 6, 4, 2	1 (S 2, S 3)	<ol> <li>storage modulus G´ of cGEL<sub>monolith</sub> of independent oPNMA batches and varying base concentration;</li> <li>S 2: gelation profile of cGEL dual component mixture;</li> <li>S 3: quantification of gelation profile S2</li> </ol>
		-		15	NMPO	2	4 (S 6)	<ul> <li>4: in vitro cell seeding on cGEL<sub>disc</sub></li> <li>S 6: storage modulus of cGEL<sub>disc</sub></li> </ul>
10	 3.5 	- x □		7.5, 10, 12.5, 15	TEA NMPO NMPO	10, 2 2 2	2A	quantification of leachable components from <b>cGEL<sub>disc</sub></b>
		- x		7.5, 10, 12.5, 15	TEA NMPO NMPO	2 2 2	2B 3C	storage modulus G' of <b>cGEL<sub>disc</sub></b>
		- x 🗆		15	NMPO	6, 4, 2	2C	leachables and cross-linking degree of cGEL <sub>disc</sub> and cGEL <sub>monolith</sub>
		- x 🗆		15	NMPO	6, 4, 2	2D (S 4) 3D	2D, 3D: storage modulus G' of cGEL <sub>monolith</sub> ; S 4: compression test of cGEL <sub>monolith</sub>
		- x		15	ΝΜΡΟ	2	3B (S 5)	<b>3B:</b> gelation profile of <b>cGEL</b> dual- component mixture with oPNMA derivatized for 0 h, 1 h and 4h;
		- x 🗆		15	ΝΜΡΟ	2	4 (S 6)	<ul> <li>S 5: storage modulus G' of cGEL<sub>disc</sub></li> <li>4: in vitro cell seeding (hSGSCs) and cytotoxicity testing (L929) on cGEL<sub>disc</sub>;</li> <li>S 6: storage modulus of cGEL<sub>disc</sub></li> </ul>
			x	15	NMPO	2	5C	derivatization pattern of cGEL <sub>conduit</sub>
12.5	3.5	- - x □		7.5, 10, 12.5, 15	TEA NMPO NMPO	10, 2 2 2	2A	quantification of leachable components from <b>cGEL<sub>disc</sub></b>
		- -		7.5, 10, 12.5, 15	TEA NMPO	2	2B	storage modulus G´ of <b>cGEL<sub>disc</sub></b>
		- x		15	NMPO	6, 4, 2	2C	leachables and cross-linking degree of cGEL <sub>disc</sub> and cGEL <sub>monolith</sub>
		- x		15	NMPO	6, 4, 2	2D 3D	storage modulus G´ of <b>cGEL<sub>monolith</sub></b>
		x		15	NMPO	2	5A, 5B ( S 6)	characterization of <b>cGEL<sub>conduit</sub> 5A:</b> conduit dimensions; 5B: leachables and water content; 5 6: conduit dimensions after rehydration

**S 1** Cross-linked hydrogel cGEL composition as used in this study. Concentrations %(w/v) are given as values during gelation; Abbreviations: oligo(PEDAS-co-NiPAAm-co-MA) (oPNMA), Collagel® (collagen hydrolysate) (COL), triethylamine (TEA), *N*-methylpiperidin-3-ol (NMPO), *N*,*N*-diethylethylendiamine (DEED), 6-Aminoflourescein (6-AF), human sweat gland derived stem cells (hSGSCs), L929 mouse fibroblasts (L929).

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**S 2** Kinetics of cGEL cross-linking. Storage moduli monitored over time for oPNMA-7.5 (3.5% in gelation mix), COL (15% in gelation mix), two base types and five base concentrations (base%). Data points are averaged (n = 5). Graphs are coded as follows: TEA (solid line), NMPO (dashed line), base%: 10% (x), 8% ( $\Box$ ), 6% ( $\Box$ ), 6% ( $\Box$ ), 6% ( $\Box$ ), 2% ( $\blacklozenge$ ). Base type and base% strongly affected gelation speed. Gelation decelerated at 4% and 2% NMPO. With TEA gelation was faster than with NMPO. Slowest gelation was found for 2% NMPO. Formulations with slower gelation kinetics resulted in increased storage moduli ( $G'_{max}$ ) at the end of measurement.



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S 3 Analysis of cGEL gelatior derived from the curves show NMPO (☐) (bars). Diamonds and means with different lett the parameter t<sub>0.25\*G'max</sub> wa accelerated for TEA 4%. In ac reduced TEA%. Thus, TEA di extracted for NMPO. The ge t<sub>0.25\*G'max</sub> was significantly init the gelation speed. Based on



e gelation mix). Data were d for 10%-2% TEA ( $\Box$ ) and standard deviation (n = 5) pendent of absolute G'<sub>max</sub>, lation speed and was also it change significantly with elation profiles were also Compared to NMPO 10%, lid not directly correlate to ces.

**S** 4 Compression test of cGEL<sub>monolith</sub>. Young's moduli were measured on distinct 17 mm thick cGEL<sub>monolith</sub> using a Sintech 5/D mechanical tester (MTS, Eden Prairie, Minnesota, USA) and 100 N load cell. Tests were carried out at a crosshead speed of 0.5 mm/min until 50% strain was reached. The force-elongation curves were converted into engineering stress-strain from which the compressive moduli were calculated. Columns represent means  $\pm$  standard deviations (n = 5). Means with different letters are statistically significantly different (p < 0.05). The compression for cGEL cylinders from oPNMA-10 and -12.5 (3.5% in gelation mix) with COL (15% in gelation mix) and NMPO 6% ( $\Box$ ), 4% ( $\Box$ ), or 2% ( $\Box$ ) in gelation mix was measured. Results reflect increase of mechanical stiffness with decreased base%. Moduli were approximately one order of magnitude higher than G' for identical formulations. Differences between oPNMA-10 and -12.5 were only statistically significant for NMPO 6%.



**S 5** Storage moduli of pristine and derivatized  $CGEL_{disc}$ . Discs derived from COL (15% in gelation mix) and oPNMA-10 or oPNMA-10<sup>+DEED</sup> (3.5% in gelation mix) with NMPO (2% in gelation mix). For measurement of moduli for pristine  $cGEL_{disc}(\Box)$ , two oPNMA-10 solutions (*i* and *ii*) were used for fabrication. Afterwards, DEED was added to solution *ii*, derivatized to oPNMA-10<sup>+DEED</sup> for 1 h and 4 h and  $cGEL_{disc}^{+DEED}$  (striped ) were fabricated. In parallel, solution *i* was stirred for 1 h and 4 h without DEED and control  $cGEL_{disc}$  ( $\Box$ ) were fabricated. G' was irrespective of functionalization and incubation time as no significant differences between pristine and derivatized  $cGEL_{disc}$  were detected. Any incorporation between 1 h and 4 h can be considered without negative impact on mechanical attributes of resulting gel matrices.



**S 6** Storage moduli G' of pristine and DEED-derivatized cGEL<sub>disc</sub> with COL (15% in gelation mix), NMPO (2% in gelation mix) and oPNMA-7.5, -10 or  $-10^{+DEED}$  (3.5% in gelation mix) as used for cell culture experiment with hSGSCs. Data is presented as means ± standard deviations (n = 5). No statistically significant differences between groups were observed. Thus, differences in cell attachment and spreading on cGEL and cGEL<sup>+DEED</sup> were triggered by chemical modification and focal adhesion sites and not by differences in hydrogel stiffness.

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**S 7** Dimensional parameters of cGEL<sub>conduit</sub> fabricated from different mold assemblies. Formulations were derived from oPNMA-12.5<sup>+DEED</sup> (3.5% in gelation mix), COL (15% in gelation mix) and NMPO (2% in gelation mix). Outer diameter (OD), inner diameter (ID) and wall thickness (WT) in hydrated ( $\Box$ ), freeze-dried ( $\Box$ ) and rehydrated ( $\Box$ ) state for four different conduit-molding geometries (g). Molds were assembled from silicone tubes and stainless steel cannula (inner diameter of silicon tubes:  $g_1$ ,  $g_2 = 4$  mm;  $g_3$ ,  $g_4 = 2.5$  mm; outer diameter of dispensing cannulas:  $g_1 = 1.9$  mm,  $g_2 = 0.8$  mm,  $g_3 = 1.65$  mm,  $g_4 = 0.7$  mm). Means with different letters are statistically significantly different (p < 0.01). Conduit dimensions were predefined by the mold geometry and initial dimensions were almost perfectly recovered after freeze-drying and rehydration. At the same time, conduits showed sufficient robustness during processing and predictable dimensional reconstitution after rehydration.