1 Toxicity and oxidative stress response induced by nano- and micro-CoCrMo 2 particles 3 4 5 6 Andrea L. Armstead^{a,b}, Thiago A. Simoes, ^c Xianfeng Wang^{a,d}, Rik Brydson, ^c Andy Brown, ^c Bing-7 8 Hua Jiang,^e Yon Rojanasakul,^{b,f} and Bingyun Li^{a,b,f,*} 9 ^aBiomaterials, Bioengineering & Nanotechnology Laboratory, Department of Orthopaedics, School of Medicine, West Virginia University, Morgantown, WV 26506, USA 10 11 12 ^bDepartment of Basic Pharmaceutical Sciences, School of Pharmacy, West Virginia University, Morgantown, WV 26506, USA 13 14 15 ^cInstitute for Materials Research, School of Chemical and Process Engineering, University of 16 Leeds, LS2 9JT, UK 17 ^dState Key Laboratory for Modification of Chemical Fibers and Polymer Materials, College of 18 Materials Science and Engineering, and Key Laboratory of Textile Science and Technology, 19 20 Ministry of Education, College of Textiles, Donghua University, Shanghai 201620, China 21 ^eDepartment of Pathology, Anatomy and Cell Biology, Thomas Jefferson University, Philadelphia, 22 PA 19107, USA 23 24 25 ^fMary Babb Randolph Cancer Center, Morgantown, WV 26506, USA 26 27 28 *Correspondence to: 29 30 31 Bingyun Li, PhD, Professor Director, Biomaterials, Bioengineering & Nanotechnology Laboratory 32 Department of Orthopaedics 33 School of Medicine, West Virginia University 34 1 Medical Center Drive 35 Morgantown, WV 26506-9196, USA 36 37 Tel: 1-304-293-1075, Fax: 1-304-293-7070, Email: bili@hsc.wvu.edu 38 URL: http://medicine.hsc.wvu.edu/ortho-bli/

40 SUPPLEMENTAL MATERIALS

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42 **1. Materials and Methods**

43 Particle Preparation and Characterization: CoCrMo nanoparticles (nano-CoCrMo) were 44 obtained via mechanical milling of the micro-CoCrMo particles. In brief, micro-CoCrMo particles were milled in 20 g/L of a heat shocked fetal bovine serum (FBS) solution (pH 7.0). The powders 45 were ball milled for 2.5 hr at a ball-to-powder weight ratio of 3:2 in a high energy Spex 8000M 46 mill (Metuchen, NJ) using zirconium oxide ceramic vials and balls. Before milling, the vial was 47 fully filled with an inert gas (Argon) to avoid atmospheric contamination. After collection, samples 48 were centrifuged in a Heraeus Megafuge at 25°C for 10 min with a centrifugal force of 8000G to 49 50 remove most of the FBS and coarse particles. Fine particles in the dispersion were collected for this study. For cell culture studies, both nano- and micro-CoCrMo particles were prepared using 51 our previous protocol [1] in a phosphate buffered saline (PBS) solution containing 10% FBS as a 52 stabilization agent and sonicated using an Omni International Sonic Ruptor 250 Ultrasonic 53 Homogenizer (Kennesaw, GA). A stock concentration of 5 mg/mL CoCrMo particles was 54 prepared by sonication (2 min, 120 watts power output, frequency 20 kHz) in an ice bath, to 55 minimize heating of the sample during particle dispersion. Dilute particle suspensions, ranging 56 57 from 0.1 to 1000 µg/mL, were prepared in DMEM containing 10% FBS and used immediately on the day of each experiment. Note that from an occupational standpoint, exposure limits have been 58 set for cobalt particles alone, but limits have yet to be defined for cobalt-containing alloys such as 59 CoCrMo or WC-Co, which have been reported to cause similar types of pneumoconiosis following 60 pulmonary exposure. Further, it is difficult to define an exact in vitro dosage parameter due to the 61 variability and extent of MoM orthopaedic implant wear on an individual patient basis. Therefore, 62 in this study, we intentionally encompassed a range of particle exposures, from 0.1 to $1000 \,\mu g/mL$, 63 to represent the potential range in CoCrMo exposure which may occur in occupational implant 64 manufacturing settings and in orthopaedic patient implant wear particle exposures. 65

The particle size of nano-CoCrMo was analyzed using transmission electron microscopy 66 (TEM) with a FEI Tecnai F20 field emission gun TEM operated at 200 kV and fitted with an 67 Oxford Instruments ultrathin window ISIS energy dispersive X-ray (EDX) system. A 3.5 µL 68 droplet of particle dispersion in 10% FBS was placed on a glow discharge-treated carbon support 69 70 film (R1.2/1.3 Quantifoil MicroTools GmBH; measured hole diameter of 1.65 µm), blotted and plunge frozen in liquid ethane [2]. The particle size of micro-CoCrMo particles was characterized 71 using scanning electron microscope (SEM). Secondary electron images were taken using a Hitachi 72 SU8230 Ultimate Cold Field Emission operated at 2 keV, 8.2 mm working distance and employing 73 an in-lens electron detector. Elemental composition was determined via EDX. 74

75 **CoCrMo Particle Assay Interference:** Prior to execution of the cell viability and oxidative stress 76 assays, the potential interference of CoCrMo particles was examined under the experimental conditions. To test compatibility with the MTT-based cell viability assay, 200 µL of CoCrMo 77 suspensions (0.1 to 1000 µg/mL in DMEM) was added to duplicate wells in a 96-well plate. The 78 plate was briefly centrifuged ($500 \times g$, 5 min) to pellet the particles at the bottom of the wells. The 79 supernatant was then aspirated and 100 µL of plain (un-supplemented) DMEM was added to each 80 well containing CoCrMo particles, along with 10 µL of MTT reagent. After 2 hr incubation at 81 37°C, 100 µL of solubilization solution was added to each well and the absorbance was determined 82 83 at 570 nm. Any auto-reduction of the MTT dye reagent to formazan by the CoCrMo particles

84 themselves would have been detected as an increase in absorbance compared to the blank wells, 85 containing only media, MTT dye reagent and solubilization solution. Similarly, for the oxidative stress assay, we tested whether the CoCrMo particles caused increased fluorescence of either DCF 86 87 or DHE under our assay conditions. CoCrMo particle suspensions were plated and centrifuged in duplicate wells of a 96-well plate as described above. The supernatant was then aspirated and 88 replaced with 100 µL of 10 µM DCF or DHE working solution prepared in PBS. Plates were 89 incubated for 15 min in the dark and then the fluorescence intensity of each well was quantified 90 every 5 min, up to one hour, at 520 nm for DCF or 620 nm for DHE, to identify any potential 91

92 particle/dye interference compared to the blank (dye solution only) wells.

93 Cell Culture and THP-1 Macrophage Differentiation: BEAS-2B lung epithelial cells were 94 cultured in DMEM supplemented with 10% FBS and 1% penicillin-streptomycin and maintained at 37°C and 5% CO₂. Human osteoblasts (h.FOB 1.19) were cultured in 1:1 Ham's F12/DMEM 95 supplemented with 10% FBS, 1% penicillin-streptomycin and 0.3 mg/mL G418 and maintained at 96 37°C and 5% CO₂. Upon confluency, BEAS-2B and osteoblasts (OB) were rinsed with PBS and 97 trypsinized, transferred to 15 mL tubes and centrifuged at 1200 rpm for 7 min to pellet. Cell pellets 98 were re-suspended in appropriate media at the desired plating density of 1.5×10^5 cells/mL, 99 100 transferred to a 96-well tissue culture plate and allowed to adhere overnight prior to the assay(s).

THP-1 monocytes were maintained in suspension culture in RPMI-1640 supplemented 101 102 with 10% FBS, 1% penicillin-streptomycin and 0.05 mM beta-mercaptoethanol and maintained at 37°C and 5% CO₂. Upon confluency, THP-1 cells were transferred to 15 mL tubes and centrifuged 103 at $125 \times g$ for 5 min to pellet. The cell pellet was re-suspended in RPMI-1640 containing 10 ng/mL 104 PMA, which induces THP-1 monocytes to undergo macrophage (M0) differentiation, and plated 105 in a 96-well culture plate at the desired density of 1.5×10^5 cells/mL. After 24 hr, THP-1 to M0 106 differentiation was confirmed via examination of cell morphology using a light microscope [3, 4], 107 108 where M0 cells underwent a signature change in morphology and became adherent to the culture 109 dish.











Figure S3. (A) DCF and (B) DHE assay interference tests in the presence of CoCrMo particles.

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