Supplemental Information

A microfluidic cardiac flow profile generator for studying the effect of shear stress on the valvular endothelial cell

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Figure SI 1. Schematic drawing of the entire system for microfluidic cardiac flow profile generator. (A) An integrated form of cardiac flow profile generator is divided by two layers including pneumatic and fluidic layers and bonded with glass substrate. (B) The generator is operated by applying a positive or negative pressure, and each pressure source is connected to solenoid valves and actuated by a programmed computer. A programmed cardiac sequence makes a cardiac-like shear stress pattern in on-chip generator to make a widely adjustable physiological range within a cell culturing bifurcating channel.



Figure SI 2. The figures represent (A) the pumping actuation sequence and (B) maximum shear stress per pump stroke graphs for characterization of PV1, PV2, PV3, and PV4 at 350 μ m channel width. The maximum shear stresses are shown as functions of closing pressure (40, 60 and 80 kPa) and actuation time (50-1000 ms). Measured volumetric flow rate (Q) from each pump was plugged into the shear stress equation ($\tau = 6Q\mu/h^2w$) for a rectangular channel and generates various max shear stress ranges at 350 μ m channel width (PV1: 7-11 dyne/cm², PV2: 9-17 dyne/cm², PV3: 13-27 dyne/cm², PV4: 26-56 dyne/cm²).



Figure SI 3. Validation of controlling (A) magnitude and (B) frequency levels for both aortic and mitral inflows. By selecting proper sets of pumps, a wide range of the shear stress magnitude can be reconstructed. In addition, by selecting actuation times, different heart rhythms can be demonstrated at 0.8Hz (t_{m1} =700, t_{m2} =400, t_{m3} =100, t_{m4} =100 ms/ t_a =1200ms), 1.2Hz (t_{m1} =300ms, t_{m2} =400, t_{m3} =100, t_{m4} =100 ms/ t_a =200, t_{m3} =50, t_{m4} =50 ms/ t_a =250ms). All the flows were generated by programmed actuation sequence as shown in each table.



Figure SI 4. Initial assessment of PEVEC culture in a microfluidic channel. Among three different width microfluidic channels, 350 μ m in width shows the best loading conditions for culturing the PAVECs.

Reynolds number, Womersley number, and Oscillatory Shear Index: Reynolds number was calculated using the normal definition: $Re = \frac{uL}{v}$ with u as the flow velocity, L as the characteristic length, and v as the kinematic viscosity of the media. The height of the fluidic channel was used as the characteristic length and the kinematic viscosity of water at 20 Celsius were used for calculations in our fluidic channels. Womersley number was calculated as usually defined: $W = L\sqrt{\frac{\omega}{v}}$ with L again as the characteristic length, ω as the frequency, and v again as the kinematic viscosity. Lastly, OSI was calculated as: $OSI = 0.5 \left(1 - \frac{\left|\int_{0}^{T} WSS \ dT\right|}{\int_{0}^{T} |WSS| \ dT}\right)$ and the values referenced in the plain texted are calculated based on the shear stress presented in **Figure 3**. The dynamic viscosities used in these calculations are $1.00*10^{-6}$ m²/s for water and media and $1.32*10^{-6}$ m²/s for blood.

Sources	Re	W	OSI	L
In-Vivo Aortic inflow	~849-4,100 [1]	21.15 [2] ^{\$}	0.13-0.47 [3-4]	~22.5 mm [5]
In-Vivo Mitral inflow	~2,053 [2] #	~29.42 [2] ^{\$}	0.051 [2]*	~31.3 mm [6]
Butcher & Nerem [6]	~2200	-	0	~3 mm
Mahler et al. [7]	~113-321	~1.12- 5.64	0.5	~5 mm
Young et al. [8]	~6-129 ^x	-	0	59 µm
Aortic inflow in this work	0.22-4.16	0.14-0.6	0.2-0.32	80 µm
Mitral inflow in this work	0.22-4.16	0.14-0.6	0.1928	80 µm

Table SI1: Various flow characteristic values (Re, W, OSI) with respect to characteristic length from previous valve studies.

Max values based on overall flow rate of the profile (4 L/min). Based on a 1.7 Hz frequency * Estimated using Figure 5-1 of reference 1. ^x Experiments ran for 12 minutes only at high shear levels.

References

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