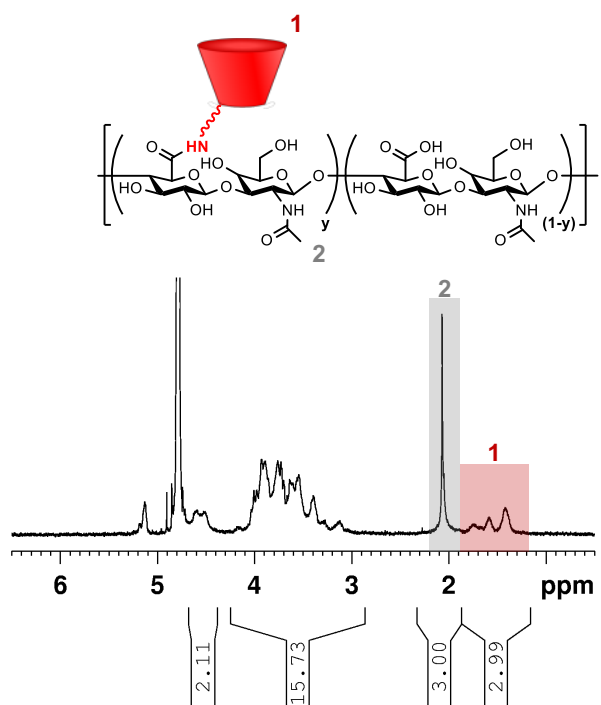


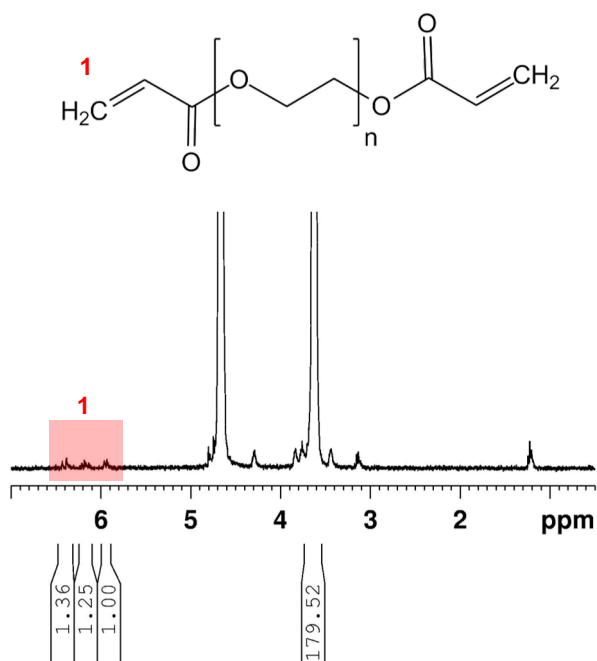
**Supplementary Figure 1 <sup>1</sup>H NMR spectrum of adamantane-functionalized hyaluronic acid (Ad-HA) in D<sub>2</sub>O.**

Modification of HA with pendant Ad (23%) determined by integration of the ethyl multiplet (12H, shaded blue) relative to the sugar ring of HA (10H, shaded grey).



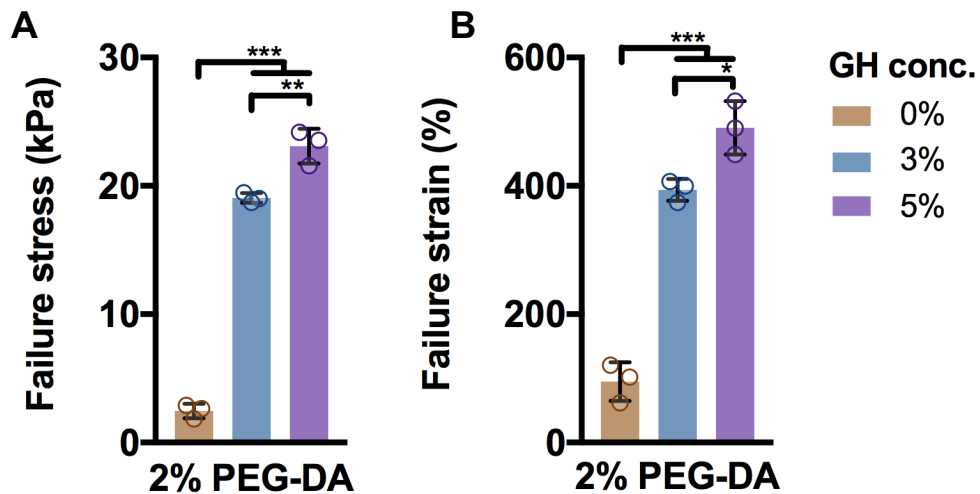
**Supplementary Figure 2**  $^1\text{H}$  NMR spectrum of  $\beta$ -cyclodextrin-functionalized hyaluronic acid (CD-HA) in  $\text{D}_2\text{O}$ .

Modification of HA with pendant CD (24.9%) determined by integration of the hexane linkers (12H, shaded red) relative to the N-acetyl singlet of HA (3H, shaded grey).



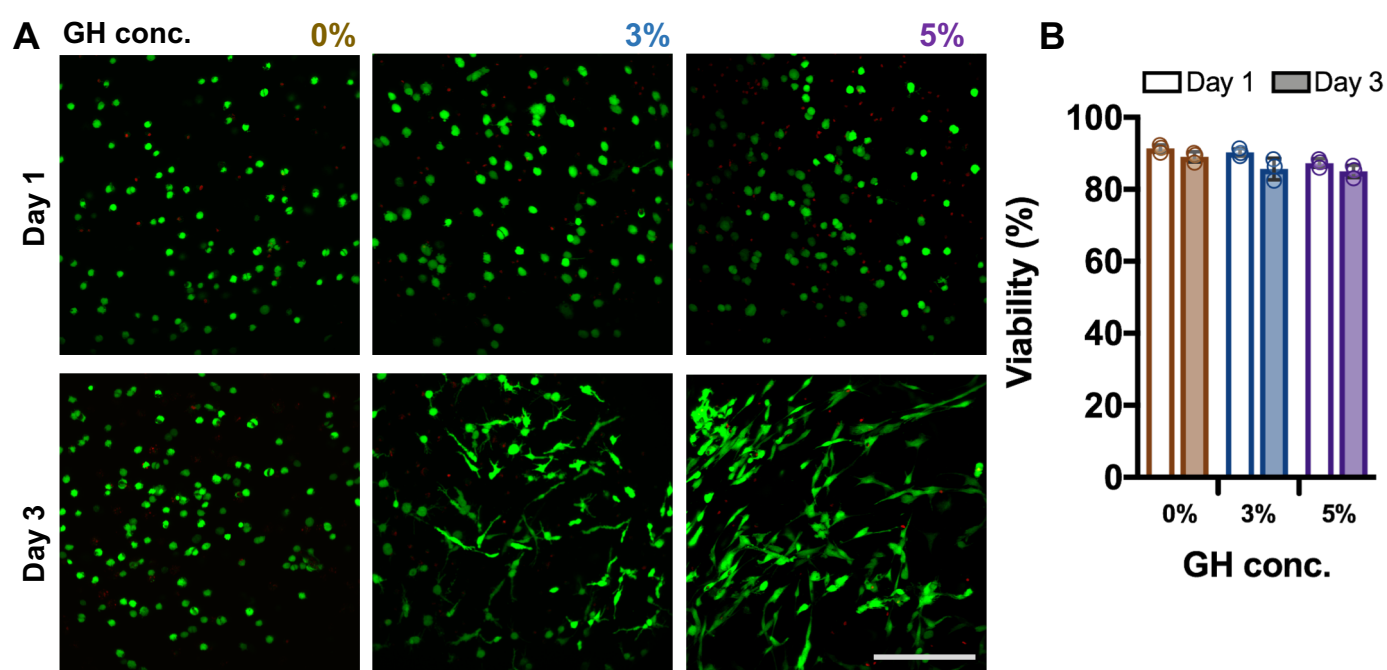
**Supplementary Figure 3 <sup>1</sup>H NMR spectrum of poly(ethylene glycol) (PEG-DA) in D<sub>2</sub>O.**

Modification of PEG (10 kDa) with diacrylate determined by integration of the acrylate groups (each 1H, shaded red).



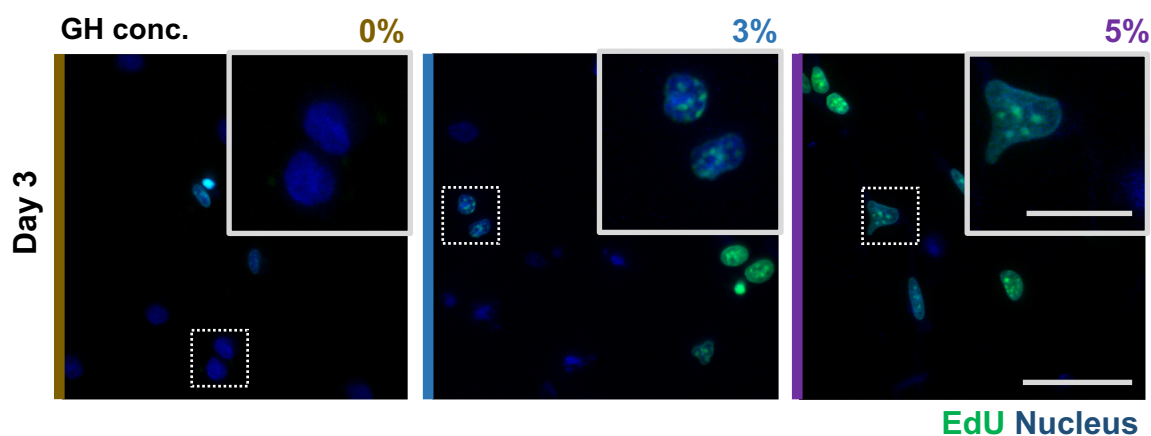
#### Supplementary Figure 4 Characterization of tensile hydrogel properties.

Influence of GH concentration on tensile ( $5.0 \text{ mm sec}^{-1}$  elongation) **A** failure stress and **B** failure strain of GH-DN hydrogels including PEG-fibrinogen (8 mg/mL plus 2% PEG-DA) and varying GH concentrations (conc.) of 0%, 3% and 5% ( $n = 3$  replicates per group, mean  $\pm$  SD,  $*p \leq 0.05$ ,  $***p \leq 0.001$  by one-way ANOVA with Bonferroni *post hoc*).



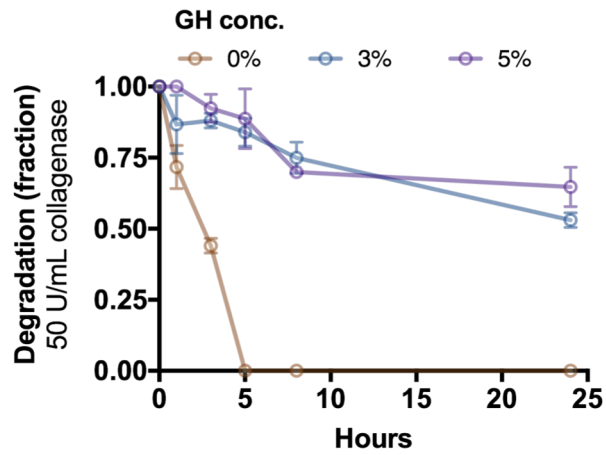
**Supplementary Figure 5 Cell viability in GH-DN hydrogels.**

A Representative images of MSCs stained with Calcein-AM (green, live) and Ethidium homodimer-1 (red, dead) after one and three days in GH-DN hydrogels including PEG-fibrinogen (8 mg/mL plus 2% PEG-DA) and varying GH concentrations (conc.) of 0%, 3% and 5% (scale bar = 200  $\mu$ m). B Quantification of cell viability after one and three days of culture (n = 3 replicates per group, mean  $\pm$  SD).



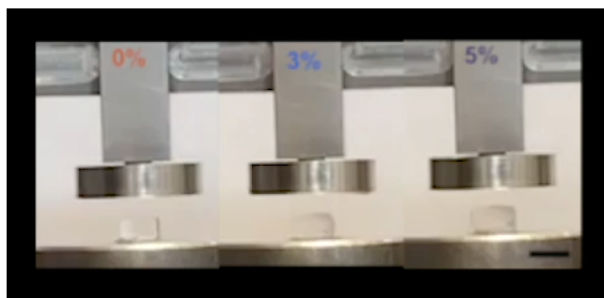
#### Supplementary Figure 6 Detection of cell proliferation in GH-DN hydrogels.

Representative images of 5-ethynyl-2'-deoxyuridine (EdU) incorporation into newly synthesized DNA over three days of MSCs in GH-DN hydrogels including PEG-fibrinogen (8 mg/mL plus 2% PEG-DA) and varying GH concentrations (conc.) of 0%, 3% and 5%, visualized with a fluorescent azide using click chemistry (scale bar 50 μm, inset 20 μm).



**Supplementary Figure 7 Enzymatic degradation of GH-DN hydrogel properties.**

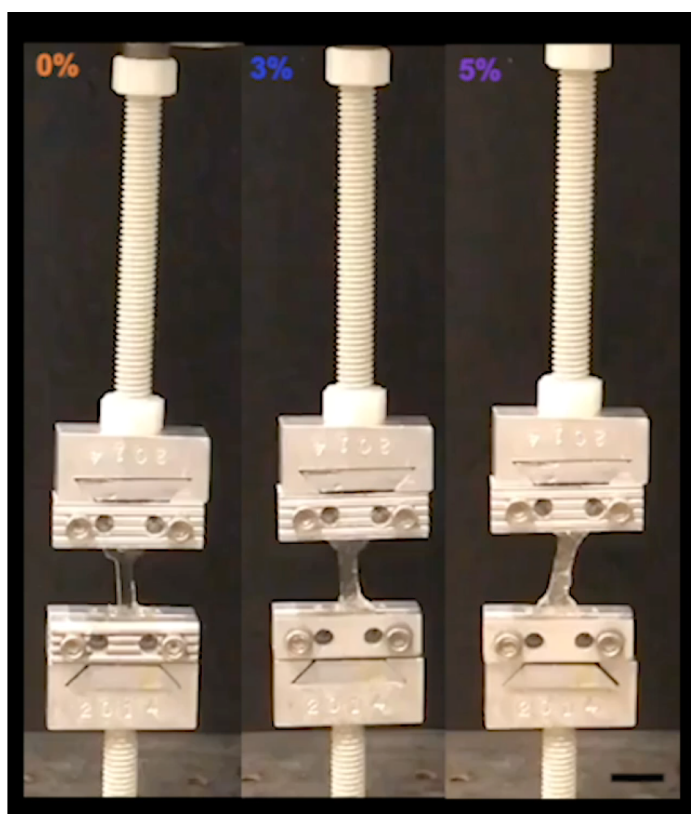
**A** Proteolytic degradation over the time course of 24 hours in 50 Units/mL collagenase in PBS at 37° C of hydrogels including PEG-fibrinogen (8 mg/mL plus 2% PEG-DA) and varying GH concentrations (conc.) of 0%, 3% and 5% (n = 3 replicates per group, mean  $\pm$  SD).



**Supplementary Video 1 Compressive failure of GH-DN hydrogels.**

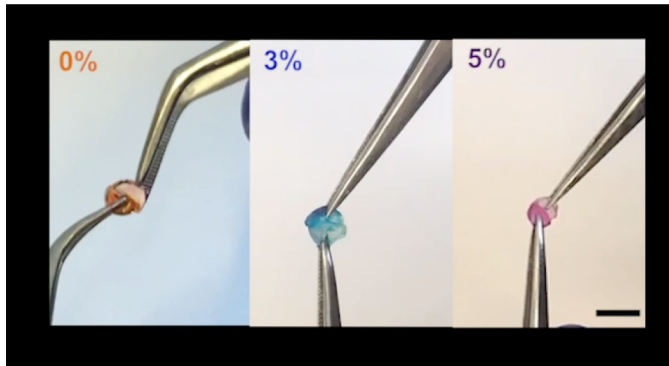
GH-DN hydrogels including PEG-fibrinogen (8 mg/mL plus 2% PEG-DA) and varying GH concentrations of 0% (left), 3% (middle) and 5% (right) were compressed to 90% strain (strain rate  $0.5 \text{ N/min}^{-1}$ , scale bar 5 mm).





**Supplementary Video 2 Tensile failure of GH-DN hydrogels.**

GH-DN hydrogels including PEG-fibrinogen (8 mg/mL plus 2% PEG-DA) and varying GH concentrations of 0% (left), 3% (middle) and 5% (right) were elongated ( $5 \text{ mm/sec}^{-1}$ ) until failure was observed (scale bar 5 mm).



**Supplementary Video 3 Self-healing and mechanical loading of GH-DN hydrogels.**

GH-DN hydrogel fragments including PEG-fibrinogen (8 mg/mL plus 2% PEG-DA) and varying GH concentrations of 0% (left), 3% (middle) and 5% (right) were subjected to repeated application of tension upon contact (scale bar 5 mm).