

Supplementary Information

Deformability-induced lift force in spiral microchannels for cell separation

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Supplementary Figures

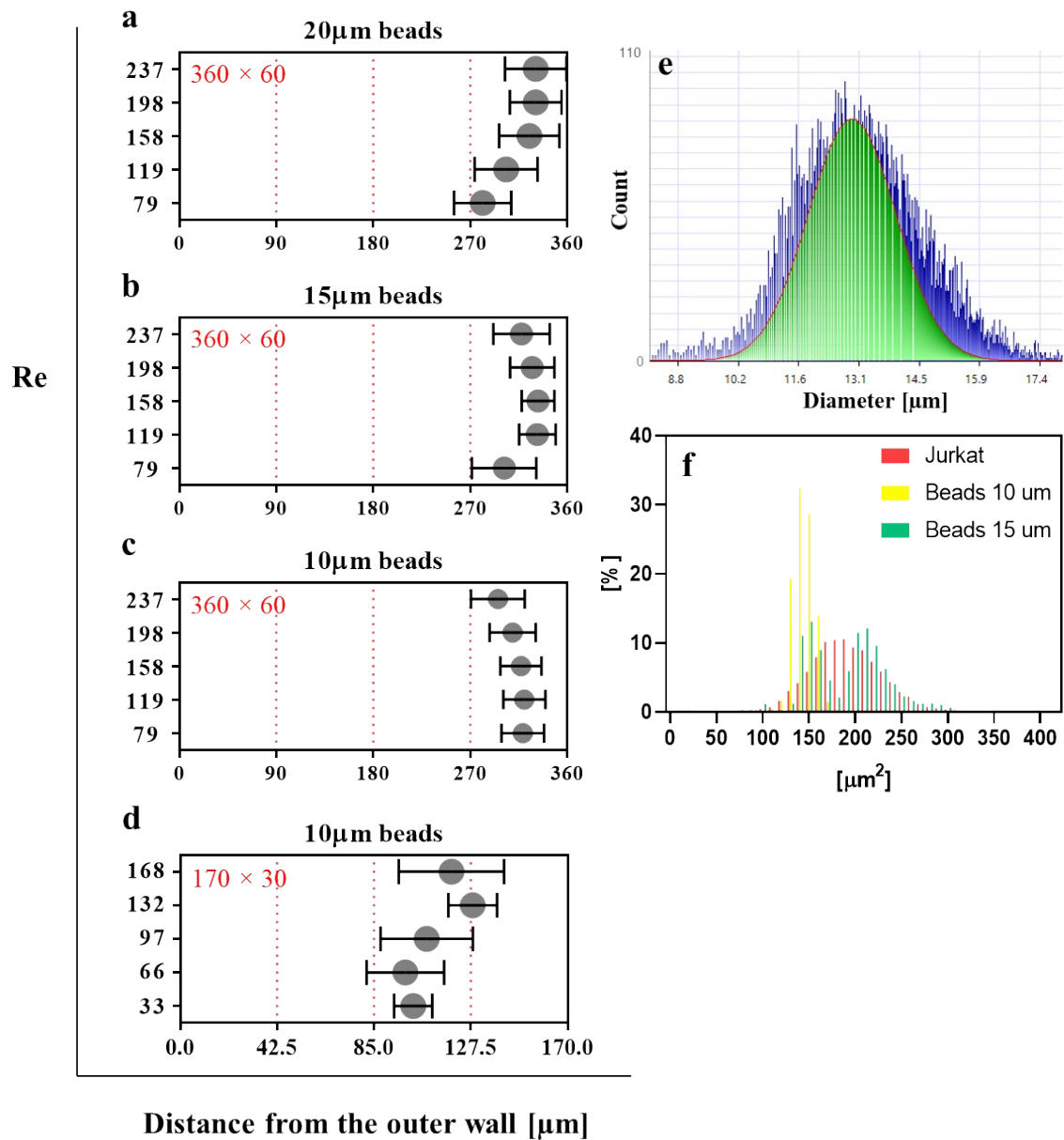
Cell type/ process	Channel specifications	Process specifications	Ref.
Cell cycle synchronisation of several cell lines (HeLa, K562, CHO-CD36 and hMSCs)	Spiral channel (9 loops, 40cm long, single inlet, 8 outlets) 500µm wide Height was fine tuned for each cell type to satisfy $a/D_h > 0.07$ Made of PDMS	Throughput: 15×10^6 cells/h Flow rate: 2.5ml/min Enrichments of cells at G0/G1: >85% Viability: 95%	¹
Focusing and ordering of HL-60 and K562 cells to facilitate deterministic single cell encapsulation in droplets	Spiral channel (5 loops, 7.2cm long), 50µm wide, 29µm high, initial radius of 1500µm Made of PDMS	Flow rate: 15µl/min	²
Separation of tumour cells (MCF-7 and HeLa) from spiked blood sample	Double spiral channel (12 loops: 6 loops counter-clockwise & 6 loops clockwise, one inlet, three outlets), 300µm wide, 50µm deep Made of PDMS	Throughput: 3.33×10^7 cells/min Flow rate: 350µl/min Recovery: 88.5%	³
Isolation of CTC from whole diluted blood (20-25% hematocrit) from	Spiral channel (2 loops, 10cm long, 2 inlets, 2 outlets), 500µm wide, 160µm deep	Flow rate: 3ml/hr Efficiency: 88% Detection rate: 100% (cells	⁴

cancer patients.	Made of PDMS	detected in all cancer patients' blood samples, n=20)	
Separation of single cells from cell clumps for murine neurosphere assay	Spiral channel (5 loops, one inlet, 8 outlets), 500µm wide, 150µm deep, initial radius of curvature 1cm. Made of PDMS	Efficiency: 75% Flow rate: 3ml/min Viability: >97%	5
Separation of plasma from whole blood sample ×20 diluted	Spiral channel (5 loops, 16cm long, one inlet, two outlets), 150µm wide, 50µm deep, the initial radius was 3500µm. Made of PDMS	Throughput: 700µl/min Efficiency: 38.5% Plasma purity: 99.9%	6
Separation of non-motile sperm cells from RBC in TESE/mTESE samples	Spiral channel (4 loops, 1 inlet, 4 outlets), 150µm wide, 50µm deep, the initial radius was 700µm Made of PDMS	Throughput: 520µl/min Efficiency: 81% for sperm cells, 99% for RBC	7
Separation of higher quality sperm from lower quality sperm without using sperm motility	Spiral channel (4 loops, 1 inlet, 4 outlets), 150µm wide, 50µm deep, initial radius 853µm. Made of PDMS	Throughput: 550µl/min Cell concentration: 2×10 ⁷ cells/ml Higher quality sperm was 4 times enriched in comparison to the input	8
Separation and concentration of <i>Phytophthora ramorum</i> sporangia (fungal plant pathogen, Ø30µm)	Spiral channel (3 loops, 1 inlet, 2 outlets), 600µm wide, 200µm deep, the radius of curvature was 2cm on average Made of thermoplastic polymer	Throughput: 2ml/min 5.3-fold increase in pathogen content with 95% recovery	9
Separation of algae (sub-millimetre phytoplankton) of two specimens: <i>Monoraphium griffithii</i> from <i>Cyanobacteria aeruginosa</i> .	Spiral channel (3 loops, 1 inlet, 2 outlets), 350µm wide and 100µm deep, initial radius 5mm, total length ~14cm Made of PDMS	Flow rate: 3.2ml/min Efficiency: 77%	10
Isolation of blood plasma, blood sample diluted 1:20	A cascade of two spiral channels, each with 1 inlet, 3 outlets and 5 loops: 1 st : 500µm wide, 60µm deep 2 nd : 250µm wide, 60µm deep Made of PDMS	Flow rate: f 1.25ml/min Efficiency: 1 st : 55% of blood cells removed 2 nd : 99% of blood cells removed	11
Concentration of <i>E.coli</i> and 1µm beads	Spiral channels (3 loops, 1 inlet and 2 outlets): 1 st part: 10 × 24µm ² cross-section	Flow rate: 50µl/min (generated 70 bars) 100µl/min (generated 150	12

	2 nd part: $10 \times 60\mu\text{m}^2$ cross-section	bars)	
	Made of glass to withstand high pressure (up to 200 bar)		
Separation of neural stem cells derived from induced pluripotent stem cells from spontaneously differentiated non-neural cells	Spiral channel (1 inlet, 8 outlets and 10 loops), $500\mu\text{m}$ wide and $160\mu\text{m}$ deep, total length $\sim 50\text{cm}$ Made of PDMS	Flow rate: 3ml/min Efficiency: $2.5\times$ enrichment of neural stem cells with 38% recovery	13
Enrichment of mesenchymal stem cells from bone marrow	Spiral channel (1 inlet, 8 outlets, 10 loops), $500\mu\text{m}$ wide and $160\mu\text{m}$ deep, total length $\sim 50\text{cm}$	Flow rate: up to 3 ml/min Efficiency: the best performance at 1.6ml/min, $6\times$ enriched, 73% recovery rate	14

STable. 1

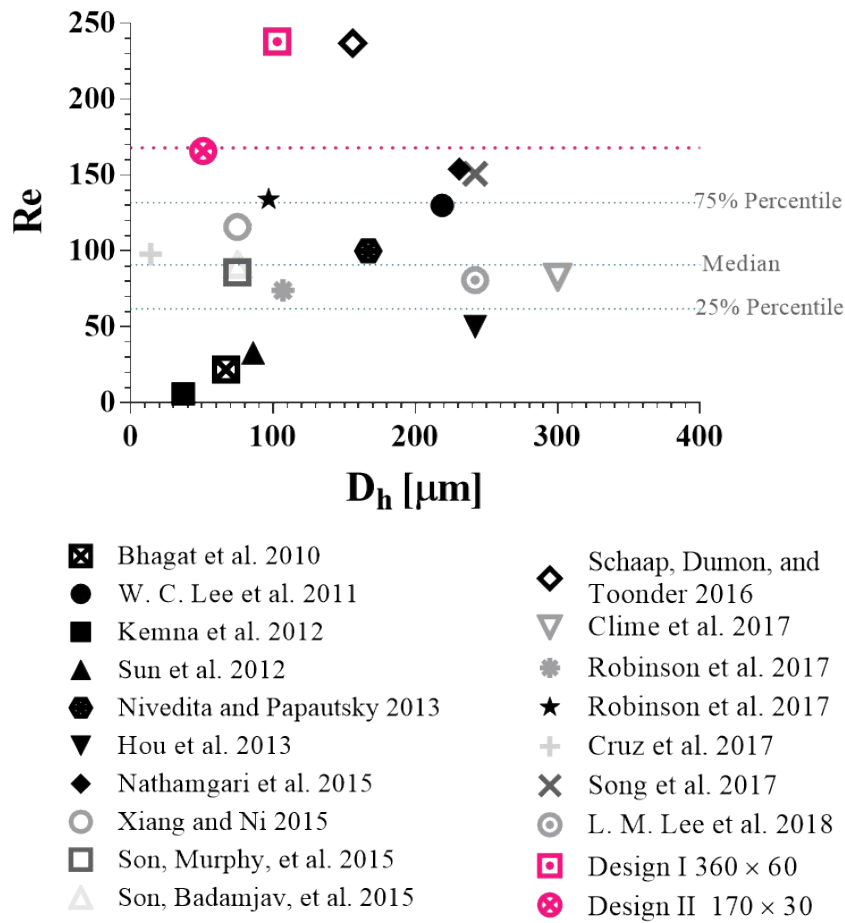
Examples of published data using IF in spiral channels with a symmetrical cross-section for size-based separating a wide range of biological samples.



SFig.1

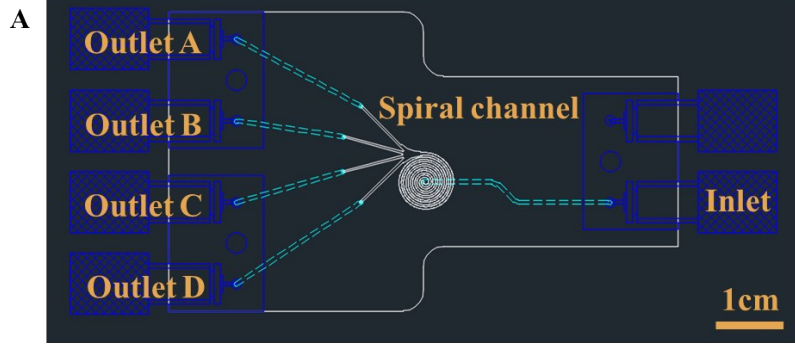
Hydrodynamic behaviour of polystyrene beads with (a) 20, (b) 15 and (c) 10, μm diameter in design I spiral microchannel with $360 \times 60 \mu\text{m}^2$ cross-section at five different flow rates corresponding to $\text{Re}=79, 119, 158, 198$ and 237 and (d) 10 μm diameter in design II spiral microchannel with $170 \times 30 \mu\text{m}^2$ cross-section, at five different flow rates corresponding to $\text{Re}=33, 66, 97, 132$ and 168 . The lateral equilibrium positions were measured as a distance from the outer wall (μm) at the end of the spiral channel for at least 10000 events and there were generated by image analysis. Here, it is reported as mean (represented as the symbols) and standard deviation (indicated by the short vertical lines). Vertical dotted lines indicate four sections of the channel corresponding to four outlets of the channel (0-90 μm - outlet A, 90-180 μm - outlet B, etc.). Events belonging to a given section have the highest probability of being captured within the corresponding outlet. (e) Size measurement report generated for Jurkat cells using MoxiZ automated cell counter. The report is a histogram, where blue vertical lines

indicate number of cells measured within a given size range (bins), the red curve is a fit into the data generated automatically by the MoxiZ software and green color indicated area under the curve. **(f)** A histogram showing percentage of size ranges found within Jurkat cells population (red) in comparison to 10 (yellow) and 15 (green) μm beads. Please note that there are discrepancies in sizes measured with the MoxiZ and by the image analysis. MoxiZ measures light scatter around the measured particles which is further converted by an algorithm into a numerical value, while size measured by image analysis is reported as a projected particle's area.



SFig. 3

Summary of operating conditions of spiral channels reported in the literature, up to end of 2018, in comparison to design I and II (pink). The scatter plot represents applied Re numbers versus hydraulic diameter (D_h). The grey dotted lines represent median Re number value (excluding design I and II) and lower and upper quartile as labelled on the graph. The pink dotted line represents the Re number applied in design II at which the effect of F_D was significant.



SFig. 4

(A) Schematic of the spiral channel with six loops, one inlet and four outlets for size and deformability-based separation. Scale bar corresponds to 1 cm.

	Flow rate [ml/min]	Velocity [m/s]	Re [-]	De
Design I	1	0.8	79	18
	1.5	1.2	119	27
	2	1.5	158	35
	2.5	1.9	198	44
	3	2.3	237	53
Design II	0.2	0.65	33	5
	0.4	1.3	66	10
	0.6	1.9	97	15
	0.8	2.6	132	21
	1	3.3	168	26

STable 2

Table summarising experimental conditions (applied flow rates and corresponding velocities, Reynolds numbers (Re) and Dean numbers (De)) in design I (with $360 \times 60 \mu\text{m}^2$ cross section) and design II (with $170 \times 30 \mu\text{m}^2$ cross-section).

De is used to quantify the secondary flow within spiral microchannel, and it is defined as

$$De = Re \sqrt{\frac{D_h}{R}}, \text{ where } D_h \text{ is hydraulic diameter, for channles with rectangular cross section defined as } D_h = \frac{2 \times H \times W}{H + W}, \text{ where } H\text{- channel height and } W\text{- channel width.}$$

Supplementary materials and methods

Real-time fluorescence and deformability cytometry

While there are many available well-established technologies for assessing cell mechanotype such as Atomic Force Microscopy (AFM) ¹⁵, micropipette aspiration ¹⁶, magnetic tweezers and optical stretchers ¹⁷, these methods suffer from low-throughput ¹⁸. To assess a high number of cells (thousands of events per minute), we used a microfluidic-based Real-Time Deformability Cytometer (RT-DC) ¹⁹. RT-DC is a contactless technique, allowing gain of thousands of events per minute, which is convenient for the global characterisation of complex samples ²⁰. In the RT-DC set-up, a PDMS (Polydimethylsiloxane) channel consisting of three sections, two reservoir sections and one constriction channel (20 $\mu\text{m} \times 20 \mu\text{m}$ or 30 $\mu\text{m} \times 30 \mu\text{m}$ cross section), where cells undergo deformation and measurements are undertaken. The microfluidic chip is mounted on a microscope. A syringe pump is used to pump cells suspension in the chip, pulsing LED light enables high-speed image acquisition (4000 fps), for a standard measurements, the images are acquired at 40x magnification. Cells are introduced in the chip through central reservoir channel and they are directed into the measurement channel by sheath flow (both flow liquid and cell carrier are viscous solution of methylcellulose). Measurement channel has a cross-section slightly bigger than the cell diameter, thus cells entering the channel experiences shear stress that causes cell deformation. The images are captured in the Region of Interest (ROI) at the end of the measurement channel and processed in real time.

The RT-DC system employs image processing algorithms which enable the measurement of cell area and deformation. Deformation (D) is expressed as a deviation from a perfect circle

$$D = 1 - c \quad (1)$$

where c is the circularity defined as

$$c = 2\sqrt{\pi A}/l \quad (2)$$

A being the projected cell area and l the cell perimeter

Deformation (D) in the channel is independently measured from the initial cell shape and therefore any treatment-induced morphological changes to shape. Consequently, when possible, a differential deformation DD parameter has been introduced ²¹.

DD includes morphological information acquired in the reservoir (D_{Res}) section of the RT-DC chip (where applied shear is negligible) by subtracting this value from the deformation measured in the channel (D_{Ch}). From each vector of deformations values with length n , sampling is done with replacement n -times and the resulting distribution is used to calculate a statistic like the median (M). A single DD value is computed using

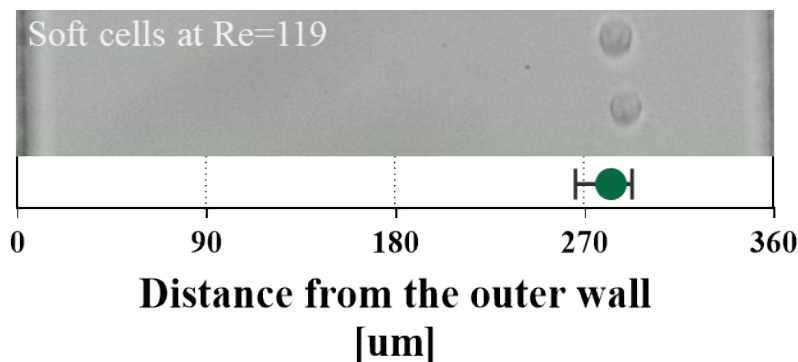
$$DD_{j,CH} = D_{j,Ch} - D_{j,Res} \quad (3)$$

Subtraction is done by statistical representations of channel and reservoir measurements and using a bootstrapping approach. The process of sampling, calculation of M and DDj has to be repeated for a sufficient number of iterations (>1000) to obtain a bootstrap distribution follows a Gaussian distribution ^{21,22}.

RT-FDC is an enhanced high-throughput (thousands of events per minute) microfluidic platform that enables mechanotype analysis of cells within a heterogeneous sample with no necessity of pre-sorting into pure populations, due to the integration of fluorescent signal for confirmation of cell identity ²³. As in the conventional real-time deformability cytometry (RT-DC) ¹⁹, cells are deformed in a contactless manner by experiencing shear stress generated by flowing in a viscous buffer through the measurement channel which is only slightly larger than the actual cell dimensions. In RT-FDC **(1)** Immuno-labelled cells are introduced into the microfluidic chip mounted on a microscope and while passing through the measurement channel **(2)** in the ROI they are imaged by bright-field microscopy **(3)**. Information about cells size (expressed as projected cell area [μm^2]) and induced by applied shear stress deformability (understood as 1- circularity) is generated by image processing in real time for each captured event and reported as a scatter plot. Additionally, cells passing through the ROI are illuminated by focused lasers **(4)** which excite signal detected and measured in the detector array. **(5)** The fluorescent signal is correlated with the acquired image, which allows cell identity confirmation.

Summary of Triplicate results

The hydrodynamic behaviour of cells was assessed in terms of lateral equilibrium position (measured as a distance from the particle centre to the outer wall [μm]) obtained at the end of the spiral channel by monitoring the ROI, by high-speed microscopic imaging. For one replica of one condition at one flow rate we obtained at least 10000 events. As an example, we provide **SFig. 5** showing a single image extracted from a video recorded for soft cells at flow rate corresponding to $\text{Re}=119$ in the spiral channel with $360 \times 60 \mu\text{m}^2$ cross-section. All of the raw files can be accessed upon a request.



SFig. 5

An exemplary image extracted from a video recorded for soft cells at flow rate corresponding to $\text{Re}=119$ in the spiral channel with $360 \times 60 \mu\text{m}^2$ cross-section. in comparison to the statistical summary of the lateral equilibrium position (expressed as distance from the outer wall [μm]) reported as median (represented as the symbol) and the interquartile range (indicated by the short vertical lines). Vertical dotted lines indicate four sections of the channel corresponding to four outlets of the channel (0-90 μm - outlet A, etc.).

Design I: Hydrodynamic behaviour of cells of cellular deformability model

Hydrodynamic behaviour of cells (10000 per condition) of five different deformabilities (soft max, soft half-max, soft, stiff half-max and stiff) (A) in comparison to reference 15 μm beads in design I spiral microchannel with $360 \times 60 \mu\text{m}^2$ cross-section at five different flow rates corresponding to $\text{Re}=79, 119, 158, 198$ and 237 . The lateral equilibrium positions were measured as a distance from the outer wall (μm) at the end of the spiral channel and there were generated by image analysis. Here, it is reported as median (represented as the symbols) and the interquartile range (indicated by the short vertical lines). Vertical dotted lines indicate four sections of the channel corresponding to four outlets of the channel (0-90 μm - outlet A, 90-180 μm - outlet B, etc.). Events belonging to a given section have the highest probability of being captured within the corresponding outlet **and** tables showing statistical summary (mean and standard deviation from the mean (SD), median, 25th (Qi) and 75th (Q3) percentile as well as minimal (min) and maximal (max) measured value) of lateral equilibrium positions obtained for at least 10000 events.

Design I: Hydrodynamic behaviour of cells of cellular deformability model

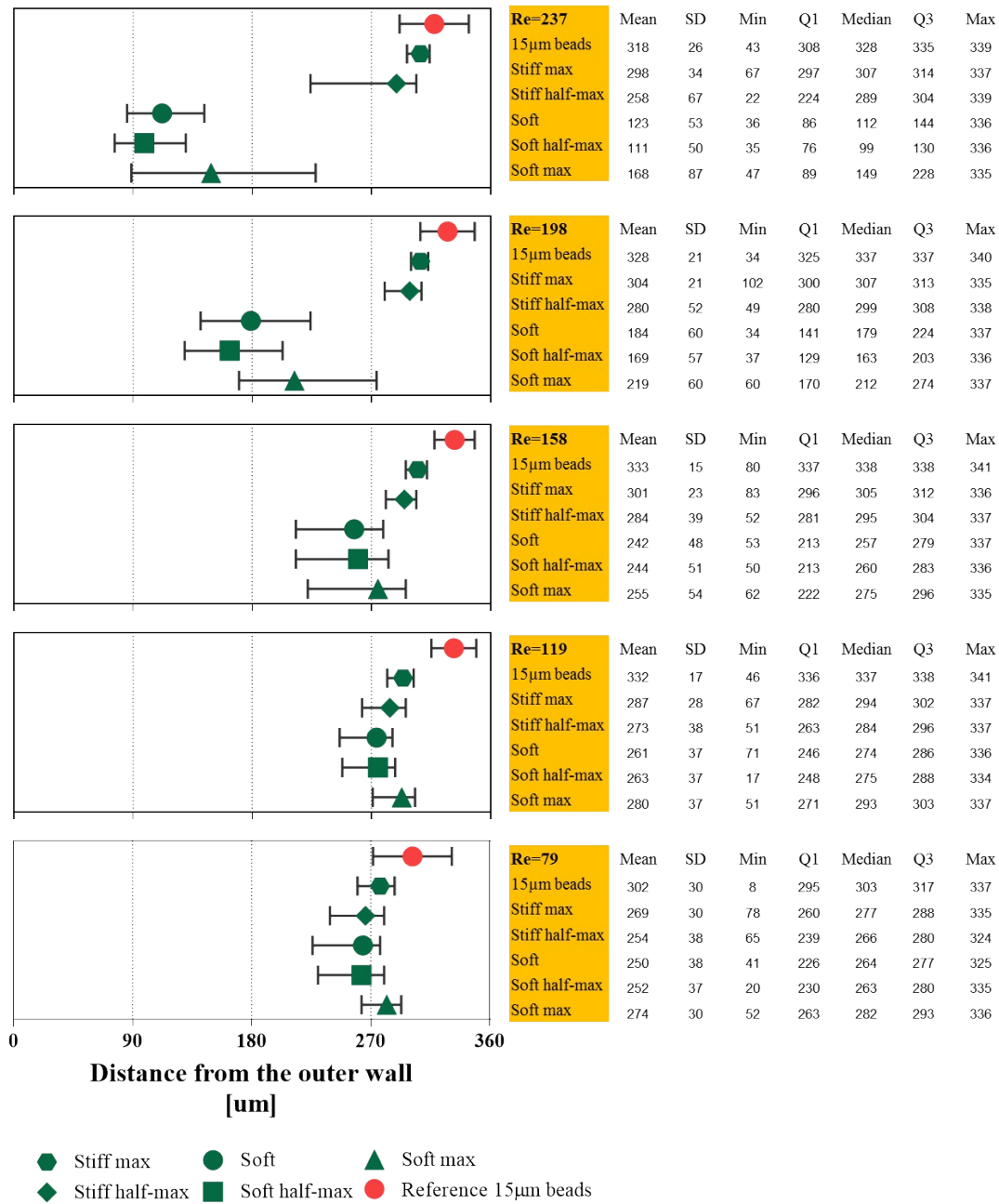
Replica I

Re=237	Re=237	Mean	SD	Min	Q1	Median	Q3	Max
	Soft max	122	49	37	86	112	144	328
	Soft half-max	110	44	33	79	101	131	334
	Soft	132	50	38	98	124	156	335
	Stiff half-max	251	77	34	191	289	308	338
	Stiff max	305	45	33	304	316	331	341
	15µm beads	318	26	43	308	328	335	339
Re=198	Re=198	Mean	SD	Min	Q1	Median	Q3	Max
	Soft max	201	66	46	150	198	261	335
	Soft half-max	169	59	36	127	161	205	335
	Soft	203	62	46	155	201	256	337
	Stiff half-max	270	62	20	254	294	308	338
	Stiff max	310	29	63	303	313	327	339
	15µm beads	328	21	34	325	337	337	340
Re=158	Re=158	Mean	SD	Min	Q1	Median	Q3	Max
	Soft max	265	51	48	248	285	298	336
	Soft half-max	242	57	43	206	262	286	335
	Soft	265	46	47	251	282	295	337
	Stiff half-max	273	51	49	263	289	302	338
	Stiff max	306	24	61	299	308	318	338
	15µm beads	333	15	80	337	338	338	341
Re=119	Re=119	Mean	SD	Min	Q1	Median	Q3	Max
	Soft max	281	34	69	276	291	301	335
	Soft half-max	269	39	16	259	281	292	334
	Soft	273	33	40	266	283	293	335
	Stiff half-max	268	42	71	259	281	292	336
	Stiff max	294	24	67	287	297	306	337
	15µm beads	332	17	46	336	337	338	341
Re=79	Re=79	Mean	SD	Min	Q1	Median	Q3	Max
	15µm beads	302	30	8	295	303	317	337
	Stiff max	270	27	35	264	277	286	334
	Stiff half-max	259	36	49	249	270	281	332
	Soft	265	29	90	259	274	283	335
	Soft half-max	263	34	18	255	273	283	332
	Soft max	273	32	20	265	282	292	334

**Distance from the outer wall
[µm]**

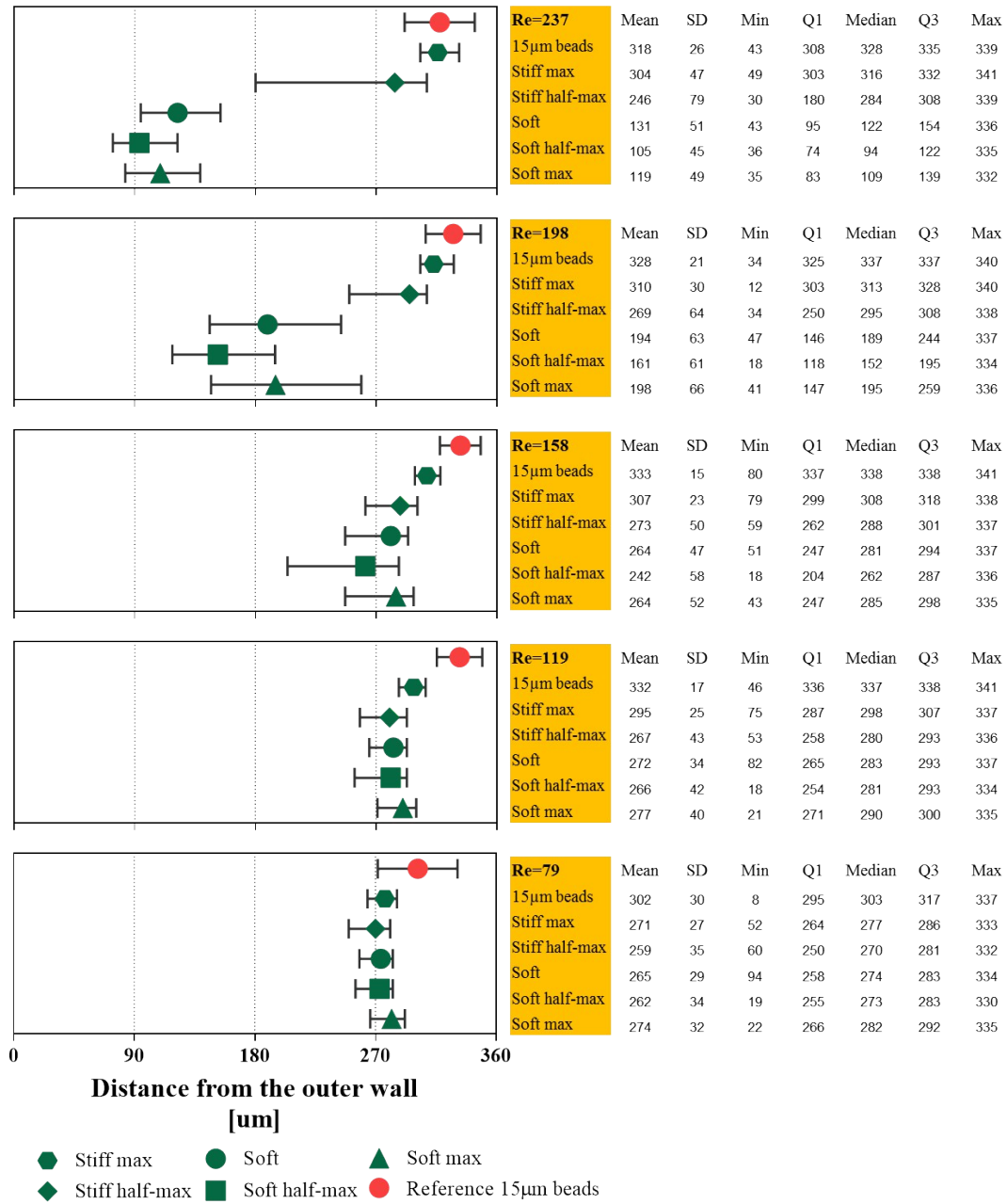
Design I: Hydrodynamic behaviour of cells of cellular deformability model

Replica II



Design I: Hydrodynamic behaviour of cells of cellular deformability model

Replica III



Design II: Hydrodynamic behaviour of cells of cellular deformability model

Hydrodynamic behaviour of cells of five different degrees of deformability (Soft max, soft half-max, soft, stiff half-max and stiff) in comparison to reference 15 μm beads, in design II spiral channel with $170 \times 30 \mu\text{m}$ cross-section at five different flow rates corresponding to $\text{Re}=33, 66, 97, 132$ and 168 (as outlined in the tables on the right) . The lateral equilibrium positions were measured as a distance from the outer wall (μm) at the end of the spiral channel and there were generated by image analysis. Here, it is reported as median (represented as the symbols) and the interquartile range (indicated by the short vertical lines). Vertical dotted lines indicate four sections of the channel corresponding to four outlets of the channel (0-90. μm -outlet A, 90-180 μm - outlet B, etc.). Events belonging to a given section have the highest probability of being captured within the corresponding outlet **and** tables showing statistical summary (mean and standard deviation from the mean (SD), median, 25th (Q_i) and 75th (Q₃) percentile as well as minimal (min) and maximal (max) measured value) of latera equilibrium positions obtained for at least 10000 events

Design II: Hydrodynamic behaviour of cells of cellular deformability model

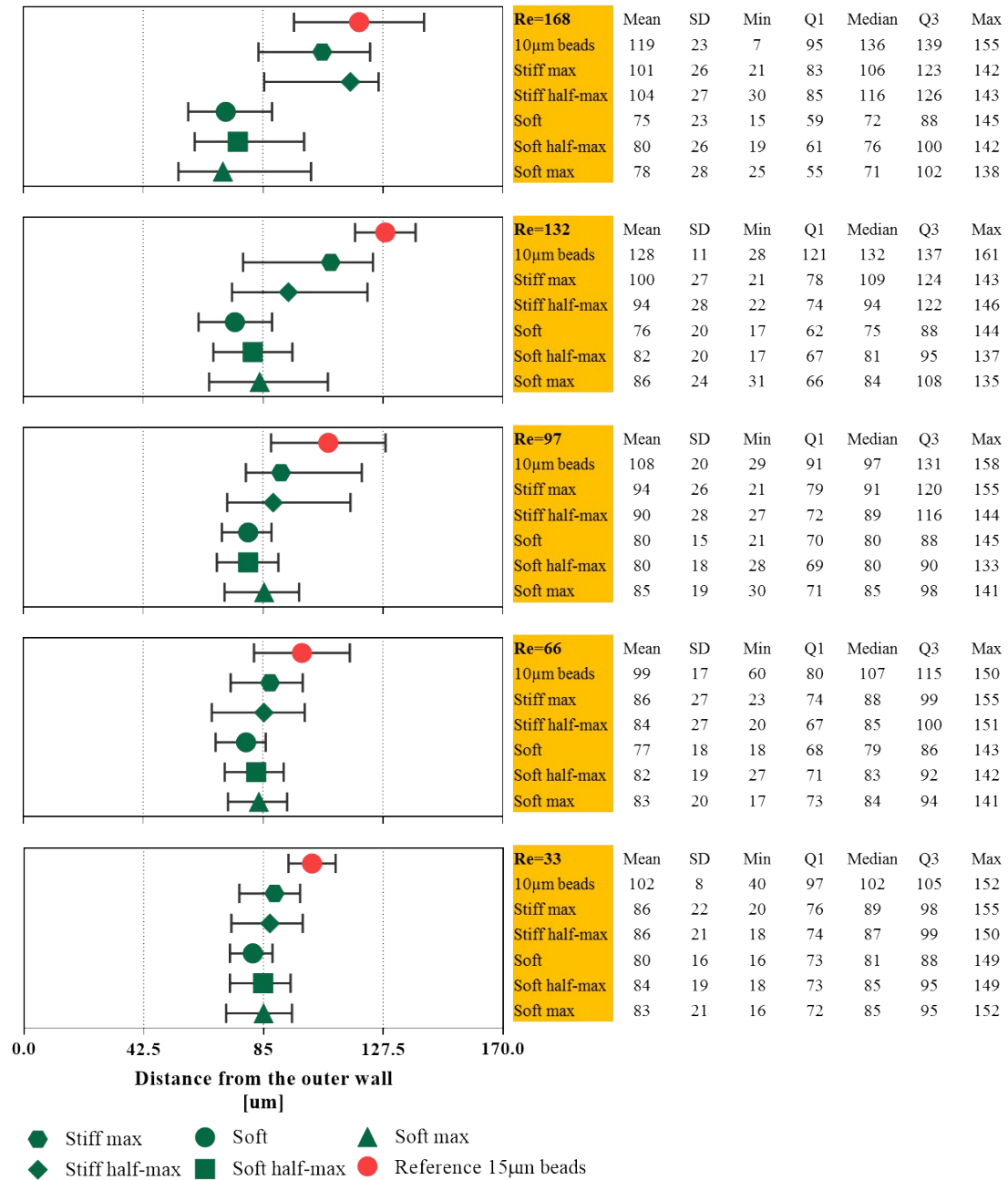
Replica I

Re=168	Re=168	Mean	SD	Min	Q1	Median	Q3	Max
	10µm beads	119	23	7	95	136	139	155
	Stiff max	113	21	34	102	121	128	143
	Stiff half-max	100	27	21	78	109	124	143
	Soft	68	21	20	54	62	79	161
	Soft half-max	80	26	20	59	74	96	142
	Soft max	75	24	19	57	70	92	142
Re=132	Re=132	Mean	SD	Min	Q1	Median	Q3	Max
	10µm beads	128	11	28	121	132	137	161
	Stiff max	101	25	29	84	107	123	147
	Stiff half-max	88	29	26	67	85	119	143
	Soft	75	18	23	63	74	86	141
	Soft half-max	84	23	20	66	83	102	143
	Soft max	80	23	15	62	77	97	162
Re=97	Re=97	Mean	SD	Min	Q1	Median	Q3	Max
	10µm beads	108	20	29	91	97	131	158
	Stiff max	89	25	25	76	87	107	144
	Stiff half-max	79	24	21	64	79	92	148
	Soft	85	20	24	70	85	99	141
	Soft half-max	85	20	24	70	85	99	141
	Soft max	82	21	20	66	81	97	141
Re=66	Re=66	Mean	SD	Min	Q1	Median	Q3	Max
	10µm beads	99	17	60	80	107	115	150
	Stiff max	82	26	18	70	84	94	145
	Stiff half-max	80	21	18	75	83	89	148
	Soft	78	18	21	69	80	87	149
	Soft half-max	84	18	19	74	85	96	144
	Soft max	82	18	21	71	83	93	138
Re=33	Re=33	Mean	SD	Min	Q1	Median	Q3	Max
	10µm beads	102	8	40	97	102	105	152
	Stiff max	87	19	18	80	90	97	150
	Stiff half-max	84	18	17	78	87	94	150
	Soft	82	17	19	74	83	90	149
	Soft half-max	86	19	18	77	89	98	148
	Soft max	84	20	17	73	86	96	150

**Distance from the outer wall
[µm]**

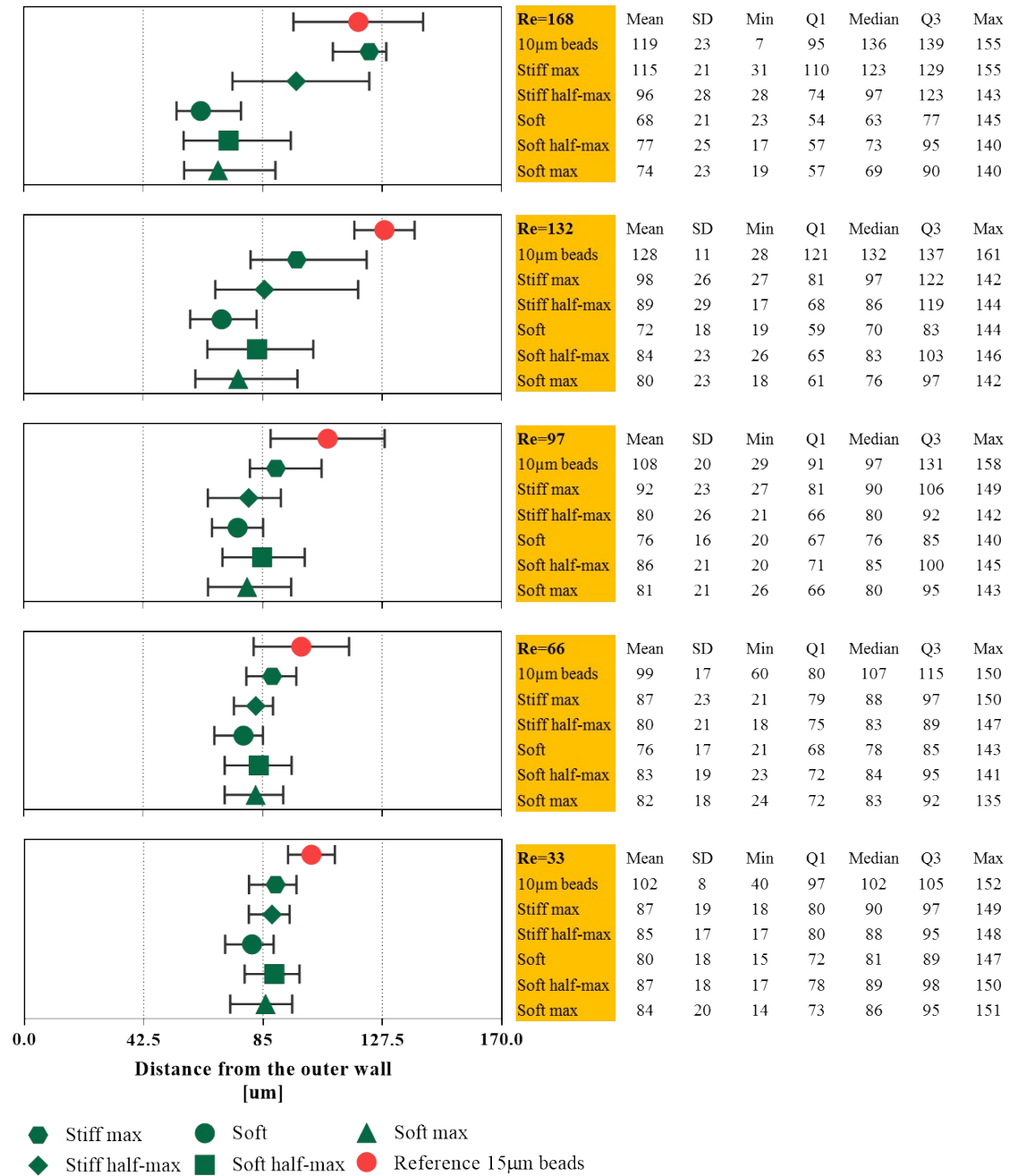
Design II: Hydrodynamic behaviour of cells of cellular deformability model

Replica II



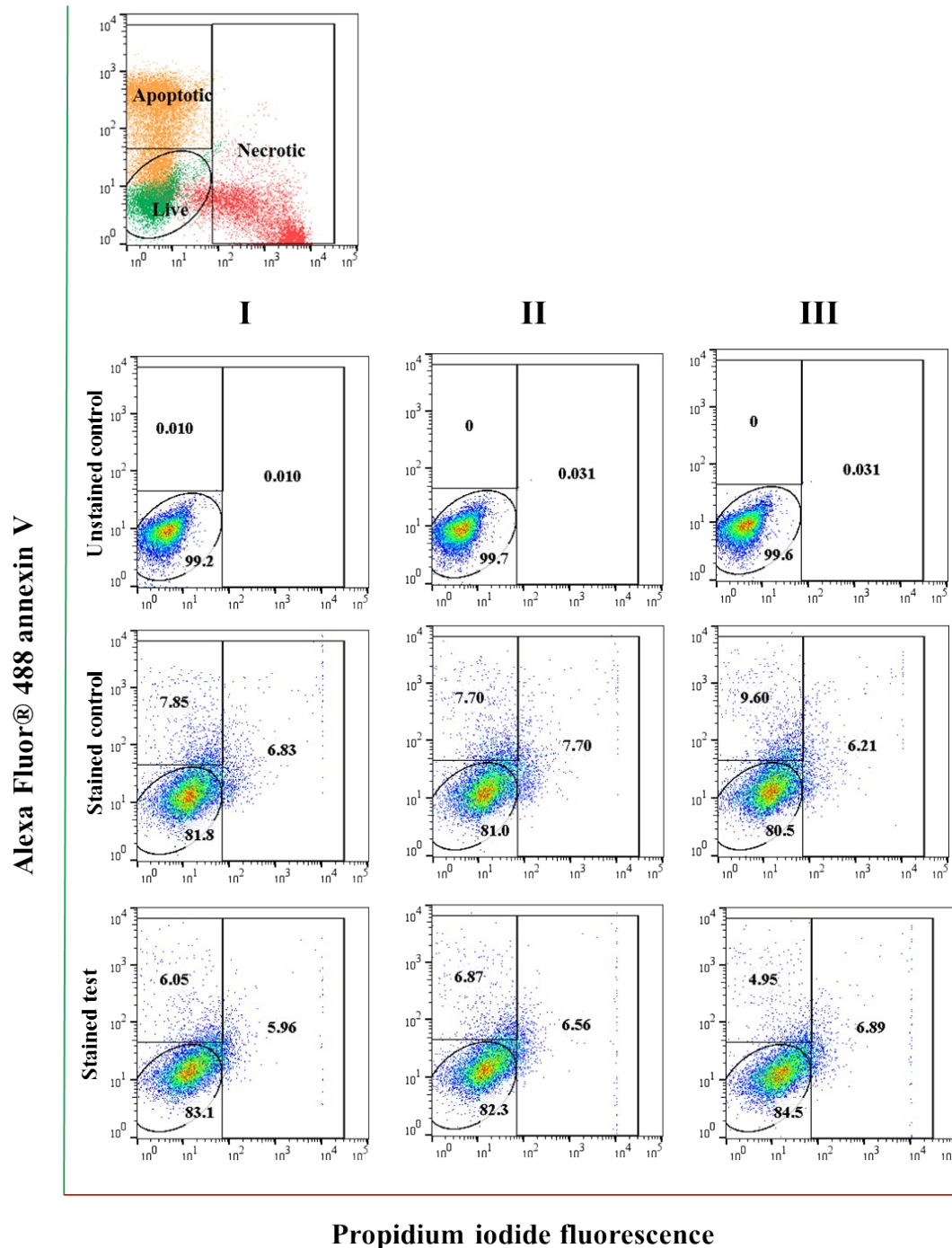
Design II: Hydrodynamic behaviour of cells of cellular deformability model

Replica III



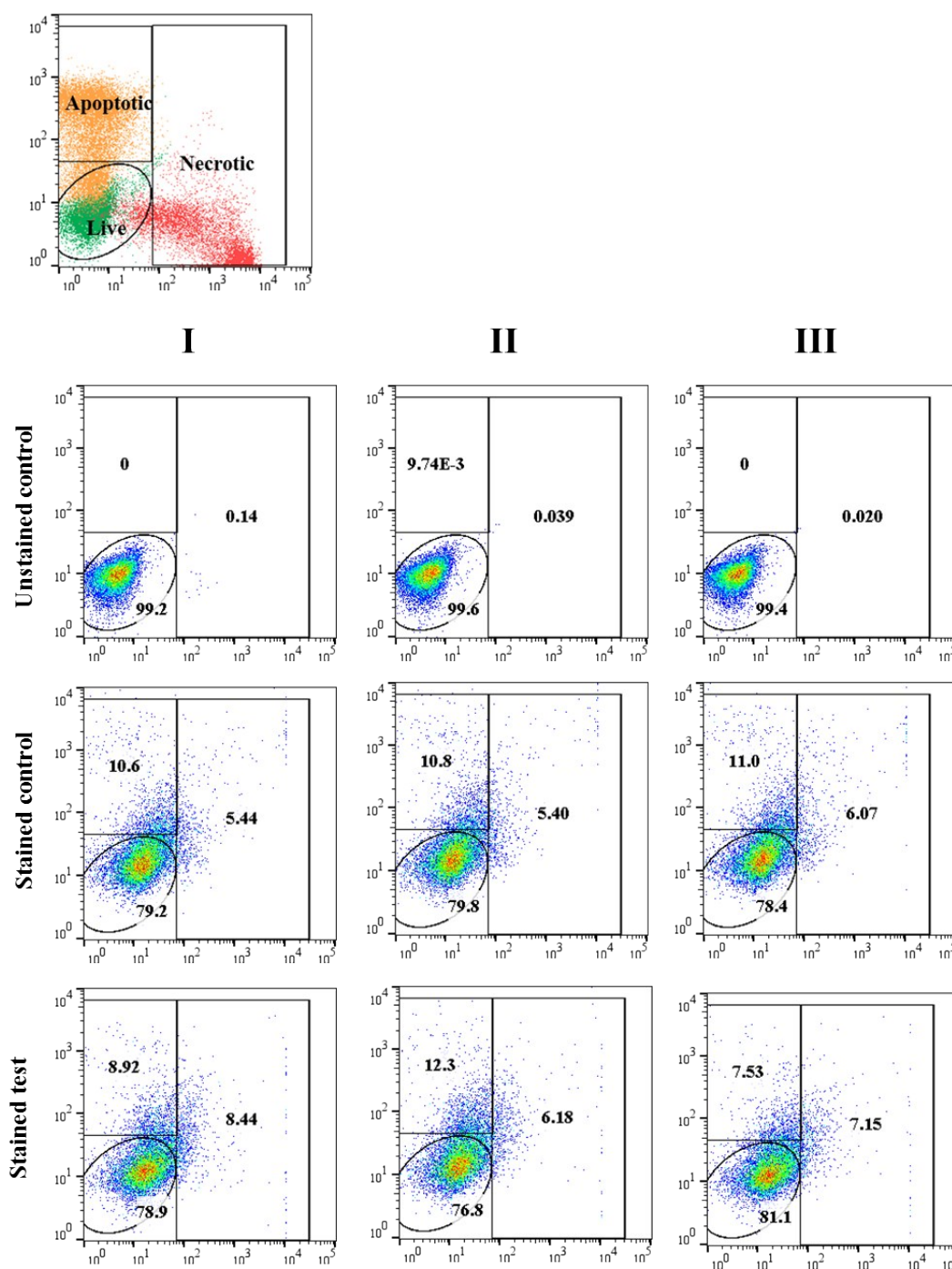
Summary of flow cytometric viability assay. On the top- an exemplary scatter plot showing gating strategy for live cell (green, negative for both Alexa Fluor 488-annexin V and propidium iodide (PI) fluorescence), apoptotic cells (orange, annexin V-positive and PI-negative) and necrotic (red, annexin V-positive and PI-positive). Summary of flow cytometric assessment of the presence of live, apoptotic and necrotic Jurkat cells before (stained control and after processing (stained test).

Design I spiral channel with $360 \times 60 \mu\text{m}$ cross-section at highest applied flow rate ($Re=237$) for three replicas.



Design II spiral channel with $170 \times 30 \mu\text{m}$ cross-section at highest applied flow rate ($\text{Re}=168$) for three replicas.

Alexa Fluor® 488 annexin V



Propidium iodide fluorescence

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