Supplementary Information

Deformability-induced lift force in spiral microchannels for cell

separation

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Supplementary Figures

Cell type/ process	Channel specifications	Process specifications	Ref.
Cell cycle synchronisation of several cell lines (HeLa, KKU-100, CHO-CD36 and hMSCs)Spiral channel (9 loops, 40cm long, 		Throughput: 15×10^6 cells/h Flow rate: 2.5ml/min Enrichments of cells at	1
	Height was fine funed for each cell type to satisfy $a/D_h>0.07$ Made of PDMS	G0/G1: >85% Viability: 95%	
Focusing and ordering of HL-60 and K562 cells to facilitate deterministic single cell encapsulation in droplets	Spiral channel (5 loops, 7.2cm long), 50µm wide, 29µm high, initial radius of 1500µm Made of PDMS	Flow rate: 15µl/min	2
Separation of tumour cells (MCF-7 and HeLa) from spiked blood sample	Double spiral channel (12 loops: 6 loops counter-clockwise & 6 loops clockwise, one inlet, three outlets), 300µm wide, 50µm deep Made of PDMS	Throughput: 3.33×10 ⁷ cells/min Flow rate: 350µl/min Recovery: 88.5%	3
Isolation of CTC from whole diluted blood (20- 25% hematocrit) from	Spiral channel (2 loops, 10cm long, 2 inlets, 2 outlets), 500µm wide, 160µm deep	Flow rate: 3ml/hr Efficiency: 88% Detection rate: 100% (cells	4

cancer patients.	Made of PDMS	detected in all cancer patients' blood samples, n=20)				
Separation of single cells	Spiral channel (5 loops, one inlet, 8	Efficiency: 75%	5			
from cell clumps for murine neurosphere assay	outlets), 500µm wide, 150µm deep, initial radius of curvature 1cm.	Flow rate: 3ml/min				
	Made of PDMS	Viability: >97%				
Separation of plasma from	Spiral channel (5 loops, 16cm long,	Throughput: 700µl/min	6			
whole blood sample ×20 diluted	one inlet, two outlets), 150μm wide, 50μm deep, the initial radius was	Efficiency: 38.5%				
	3500µm.	Plasma purity: 99.9%				
	Made of PDMS					
Separation of non-motile	Spiral channel (4 loops, 1 inlet, 4	Throughput: 520µl/min	7			
sperm cells from RBC in TESE/mTESE samples	outlets), 150µm wide, 50µm deep, the initial radius was 700µm	Efficiency: 81% for sperm cells, 99% for RBC				
	Made of PDMS	cens, 9970 101 KBC				
Separation of higher quality	Spiral channel (4 loops, 1 inlet, 4	Throughput: 550µl/min	8			
sperm from lower quality sperm without using sperm motility	outlets), 150µm wide, 50µm deep, initial radius 853µm.	Cell concentration:2×10 ⁷ cells/ml				
	Made of PDMS	Higher quality sperm was 4 times enriched in comparison to the input				
Separation and	Spiral channel (3 loops, 1 inlet, 2	Throughput: 2ml/min	9			
concentration of <i>Phytopthora ramorum</i> sporangia (fungal plant	outlets), 600µm wide, 200µm deep, the radius of curvature was 2cm on average	5.3-fold increase in pathogen content with 95%				
phatogen, Ø30µm)	Made of thermoplastic polymer	recovery				
Separation of algae (sub-	Spiral channel (3 loops, 1 inlet, 2	Flow rate: 3.2ml/min	10			
millimetre phytoplankton) of two specimens:	outlets), 350 μ m wide and 100 μ m deep, initial radius 5mm, total length ~14cm	Efficiency: 77%				
Monoraphium griffithii from Cyanothece aeruginosa.	Made of PDMS					
Isolation of blood plasma,	A cascade of two spiral channels, each	Flow rate: f 1.25ml/min	11			
blood sample diluted 1:20	with 1 inlet,3 outlets and 5 loops:	Efficiency:				
	1st: 500µm wide, 60µm deep	1 st : 55% of blood cells				
	2 nd : 250µm wide, 60µm deep	removed				
	Made of PDMS	2 nd : 99% of blood cells removed				
Concentration of <i>E.coli</i> and 1µm beads	Spiral channels (3 loops, 1 inlet and 2 outlets):	Flow rate:	12			
i µin ocaus	$1^{\text{st}} \text{ part}: 10 \times 24 \mu \text{m}^2 \text{ cross-section}$	50µl/min (generated 70 bars)				
		100µl/min (generated 150				

	2^{nd} part: $10 \times 60 \mu m^2$ cross-section	bars)	
	Made of glass to withstand high pressure (up to 200 bar)		
Separation of neural stem	Spiral channel (1 inlet, 8 outlets and 10	Flow rate: 3ml/min	13
cells derived from induced pluripotent stem cells from	loops), 500 μ m wide and 160 μ m deep, total length ~ 50cm	Efficiency: 2.5× enrichment of neural stem	
spontaneously differentiated non-neural cells	Made of PDMS	cells with 38% recovery	
Enrichment of mesenchymal stem cells from bone	Spiral channel (1 inlet, 8 outlets, 10	Flow rate: up to 3 ml/min	14
marrow	loops), 500 μ m wide and 160 μ m deep, total length ~50cm	Efficiency: the best performance at 1.6ml/min,	
		6× enriched, 73% recovery rate	

STable. 1

Examples of published data using IF in spiral channels with a symmetrical cross-section for size-based separating a wide range of biological samples.



Distance from the outer wall [µm]

SFig.1

Hydrodynamic behaviour of polystyrene beads with (a) 20, (b) 15 and (c) 10, μ m diameter in design I spiral microchannel with 360 × 60 μ m² cross-section at five different flow rates corresponding to Re=79, 119, 158, 198 and 237 and (d) 10 μ m diameter in design II spiral microchannel with 170 × 30 μ m² cross-section, at five different flow rates corresponding to Re=33, 66, 97, 132 and 168. The lateral equilibrium positions were measured as a distance from the outer wall (μ m) at the end of the spiral channel for at least 10000 events and there were generated by image analysis. Here, it is reported as mean (represented as the symbols) and standard deviation (indicated by the short vertical lines). Vertical dotted lines indicate four sections of the channel corresponding to four outlets of the channel (0-90 μ m- outlet A, 90-180 μ m- outlet B, etc.). Events belonging to a given section have the highest probability of being captured within the corresponding outlet. (e) Size measurement report generated for Jurkat cells using MoxiZ automated cell counter. The report is a histogram, where blue vertical lines

indicate number of cells measured within a given size range (bins), the red curve is a fit into the data generated automatically by the MoxiZ software and green color indicated area under the curve. (f) A histogram showing percentage of size ranges found within Jurkat cells population (red) in comparison to 10 (yellow) and 15 (green) μ m beads. Please note that there are discrepancies in sizes measured with the MoxiZ and by the image analysis. MoxiZ measures light scatter around the measured particles which is further converted by an algorithm into a numerical value, while size measured by image analysis is reported as a projected particle's area.



SFig. 3

Summary of operating conditions of spiral channels reported in the literature, up to end of 2018, in comparison to design I and II (pink). The scatter plot represents applied Re numbers versus hydraulic diameter (D_h). The grey dotted lines represent median Re number value (excluding design I and II) and lower and upper quartile as labelled on the graph. The pink dotted line represents the Re number applied in design II at which the effect of F_D was significant.



SFig. 4

(A) Schematic of the spiral channel with six loops, one inlet and four outlets for size and deformability-based separation. Scale bar corresponds to 1 cm.

	Flow rate [ml/min]	Velocity [m/s]	Re [-]	De
	1	0.8	79	18
n I	1.5	1.2	119	27
Design	2	1.5	158	35
De	2.5	1.9	198	44
	3	2.3	237	53
	0.2	0.65	33	5
Πu	0.4	1.3	66	10
Design	0.6	1.9	97	15
De	0.8	2.6	132	21
	1	3.3	168	26

STable 2

Table summarising experimental conditions (applied flow rates and corresponding velocities, *Reynolds numbers (Re) and Dean numbers (De)) in design I (with 360 \times 60 \ \mu m^2 cross section)* and design II (with $170 \times 30 \ \mu m^2$ cross-section).

De is used to quantify the secondary flow within spiral microchannel, and it is defined as

 $De = Re \sqrt{\frac{D_h}{R}}$, where Dh is hydraulic diameter, for channles with rectangular cross section

defined as $D_h =$ H+W, where H- channel height and W- channel width.

Supplementary materials and methods

Real-time fluorescence and deformability cytometry

While there are many available well-established technologies for assessing cell mechanotype such as Atomic Force Microscopy (AFM)¹⁵, micropipette aspiration¹⁶, magnetic tweezers and optical stretchers ¹⁷, these methods suffer from low-throughput ¹⁸. To assess a high number of cells (thousands of events per minute), we used a microfluidic-based Real-Time Deformability Cytometer (RT-DC)¹⁹. RT-DC is a contactless technique, allowing gain of thousands of events per minute, which is convenient for the global characterisation of complex samples ²⁰. In the RT-DC set-up, a PDMS (Polydimethylsiloxane) channel consisting of three sections, two reservoir sections and one constriction channel (20 μ m × 20 μ m or 30 μ m \times 30 μ m cross section), where cells undergo deformation and measurements are undertaken. The microfluidic chip is mounted on a microscope. A syringe pump is used to pump cells suspension in the chip, pulsing LED light enables high-speed image acquisition (4000 fps), for a standard measurements, the images are acquired at 40x magnification. Cells are introduced in the chip through central reservoir channel and they are directed into the measurement channel by sheath flow (both flow liquid and cell carrier are viscous solution of methylcellulose). Measurement channel has a cross-section slightly bigger than the cell diameter, thus cells entering the channel experiences shear stress that causes cell deformation. The images are captured in the Region of Interest (ROI) at the end of the measurement channel and processed in real time.

The RT-DC system employs image processing algorithms which enable the measurement of cell area and deformation. Deformation (D) is expressed as a deviation from a perfect circle

$$D = 1 - c \tag{1}$$

where c is the circularity defined as

$$c = 2\sqrt{\pi A}/l \tag{2}$$

A being the projected cell area and l the cell perimeter

Deformation (D) in the channel is independently measured from the initial cell shape and therefore any treatment-induced morphological changes to shape. Consequently, when possible, a differential deformation DD parameter has been introduced ²¹.

DD includes morphological information acquired in the reservoir (D_{Res}) section of the RT-DC chip (where applied shear is negligible) by subtracting this value from the deformation measured in the channel (D_{Ch}). From each vector of deformations values with length n, sampling is done with replacement n-times and the resulting distribution is used to calculate a statistic like the median (M). A single DD value is computed using

$$DD_{j,CH} = D_{j,Ch} - D_{j,Res}$$
(3)

Subtraction is done by statistical representations of channel and reservoir measurements and using a bootstrapping approach. The process of sampling, calculation of M and DDj has to be repeated for a sufficient number of iterations (>1000) to obtain a bootstrap distribution follows a Gaussian distribution ^{21,22}.

RT-FDC is an enhanced high-throughput (thousands of events per minute) microfluidic platform that enables mechanotype analysis of cells within a heterogeneous sample with no necessity of pre-sorting into pure populations, due to the integration of fluorescent signal for confirmation of cell identity ²³. As in the conventional real-time deformability cytometry (RT-DC) ¹⁹, cells are deformed in a contactless manner by experiencing shear stress generated by flowing in a viscous buffer through the measurement channel which is only slightly larger than the actual cell dimensions. In RT-FDC (1) Immuno-labelled cells are introduced into the microfluidic chip mounted on a microscope and while passing through the measurement channel (2) in the ROI they are imaged by bright-field microscopy (3). Information about cells size (expressed as projected cell area [μ m²]) and induced by applied shear stress deformability (understood as 1- circularity) is generated by image processing in real time for each captured event and reported as a scatter plot. Additionally, cells passing through the ROI are illuminated by focused lasers (4) which excite signal detected and measured in the detector array. (5) The fluorescent signal is correlated with the acquired image, which allows cell identity confirmation.

Summary of Triplicate results

The hydrodynamic behaviour of cells was assessed in terms of lateral equilibrium position (measured as a distance from the particle centre to the outer wall [μ m]) obtained at the end of the spiral channel by monitoring the ROI, by high-speed microscopic imaging. For one replica of one condition at one flow rate we obtained at least 10000 events. As an example, we provide **SFig. 5** showing a single image extracted from a video recorded for soft cells at flow rate corresponding to Re=119 in the spiral channel with $360 \times 60 \ \mu$ m² cross-section. <u>All of the raw files can be accessed upon a request.</u>



SFig. 5

An exemplary image extracted from a video recorded for soft cells at flow rate corresponding to Re=119 in the spiral channel with $360 \times 60 \ \mu\text{m}^2$ cross-section. in comparison to the statistical summary of the lateral equilibrium position (expressed as distance from the pouter wall [µm]) reported as median (represented as the symbol) and the interquartile range (indicated by the short vertical lines). Vertical dotted lines indicate four sections of the channel corresponding to four outlets of the channel (0-90 µm- outlet A, etc.).

Design I: Hydrodynamic behaviour of cells of cellular deformability model

Hydrodynamic behaviour of cells (10000 per condition) of five different deformabilities (soft max, soft half-max, soft, stiff half-max and stiff) (A) in comparison to reference 15 μ m beads in design I spiral microchannele with 360 × 60 μ m² cross-section at five different flow rates corresponding to Re=79, 119, 158, 198 and 237 The lateral equilibrium positions were measured as a distance from the outer wall (μ m) at the end of the spiral channel and there were generated by image analysis. Here, it is reported as median (represented as the symbols) and the interquartile range (indicated by the short vertical lines). Vertical dotted lines indicate four sections of the channel corresponding to four outlets of the channel (0-90. μ m- outlet A, 90-180 μ m- outlet B, etc.). Events belonging to a given section have the highest probability of being captured within the corresponding outlet **and** tables showing statistical summary (mean and standard deviation from the mean (SD), median, 25th (Qi) and 75th (Q3) percentile as well as minimal (min) and maximal (max) measured value) of latera equilibrium positions obtained for at least 10000 events.

Design I: Hydrodynamic behaviour of cells of cellular deformability model

Replica I

	Re=237	Mean	SD	Min	Q1	Median	Q3	Max
	Soft max	122	49	37	86	112	144	328
č	Soft half-max	110	44	33	79	101	131	334
Re=237	Soft	132	50	38	98	124	156	335
e.	Stiff half-max	251	77	34	191	289	308	338
	Stiff max	305	45	33	304	316	331	341
	15µm beads	318	26	43	308	328	335	339
	Re=198	Mean	SD	Min	Q1	Median	Q3	Max
\sim	Soft max	201	66	46	150	198	261	335
6	Soft half-max	169	59	36	127	161	205	335
Π	Soft	203	62	46	155	201	256	337
Re=198	Stiff half-max	270	62	20	254	294	308	338
	Stiff max	310	29	63	303	313	327	339
	15µm beads	328	21	34	325	337	337	340
	Re=158	Mean	SD	Min	Q1	Median	Q3	Max
∞	Soft max	265	51	48	248	285	298	336
Ñ	Soft half-max	242	57	43	206	262	286	335
Ī	Soft	265	46	47	251	282	295	337
Re=158	Stiff half-max	273	51	49	263	289	302	338
	Stiff max	306	24	61	299	308	318	338
	15µm beads	333	15	80	337	338	338	341
	Re=119	Mean	SD	Min	Q1	Median	Q3	Max
6	Soft max	281	34	69	276	291	301	335
Re=11	Soft half-max	269	39	16	259	281	292	334
	Soft	273	33	40	266	283	293	335
ž	Stiff half-max	268	42	71	259	281	292	336
	Stiff max	294	24	67	287	297	306	337
	15µm beads	332	17	46	336	337	338	341
	Re=79	Mean	SD	Min	Q1	Median	Q3	Max
-	15µm beads	302	30	8	295	303	317	337
79	Stiff max	270	27	35	264	277	286	334
Ĭ,	Stiff half-max	259	36	49	249	270	281	332
Ř	Soft	265	29	90	259	274	283	335
	Soft half-max	263	34	18	255	273	283	332
	Soft max	273	32	20	265	282	292	334
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Design I: Hydrodynamic behaviour of cells of cellular deformability model

Replica II



Design I: Hydrodynamic behaviour of cells of cellular deformability model Replica III

	Re=237	Mean	SD	Min	Q1	Median	Q3	Max
	15µm beads	318	26	43	308	328	335	339
H H	Stiff max	304	47	49	303	316	332	341
► -	Stiff half-max	246	79	30	180	284	308	339
	Soft	131	51	43	95	122	154	336
	Soft half-max	105	45	36	74	94	122	335
	Soft max	119	49	35	83	109	139	332
H	Re=198	Mean	SD	Min	Q1	Median	Q3	Max
H o -H	15µm beads	328	21	34	325	337	337	340
	Stiff max	310	30	12	303	313	328	340
	Stiff half-max	269	64	34	250	295	308	338
	Soft	194	63	47	146	189	244	337
	Soft half-max	161	61	18	118	152	195	334
	Soft max	198	66	41	147	195	259	336
	Re=158	Mean	SD	Min	Q1	Median	Q3	Max
	15µm beads	333	15	80	337	338	338	341
	Stiff max	307	23	79	299	308	318	338
	Stiff half-max	273	50	59	262	288	301	337
⊢ ● I	Soft	264	47	51	247	281	294	337
	Soft half-max	242	58	18	204	262	287	336
	Soft max	264	52	43	247	285	298	335
H	Re=119	Mean	SD	Min	Q1	Median	Q3	Max
H	15µm beads	332	17	46	336	337	338	341
⊢✦┤	Stiff max	295	25	75	287	298	307	337
	Stiff half-max	267	43	53	258	280	293	336
	Soft	272	34	82	265	283	293	337
	Soft half-max	266	42	18	254	281	293	334
	Soft max	277	40	21	271	290	300	335
	Re=79	Mean	SD	Min	Q1	Median	Q3	Max
	15µm beads	302	30	8	295	303	317	337
	Stiff max	271	27	52	264	277	286	333
	Stiff half-max	259	35	60	250	270	281	332
	Soft	265	29	94	258	274	283	334
	Soft half-max	262	34	19	255	273	283	330
H	Soft max	274	32	22	266	282	292	335
90 180 270 360)							
Distance from the outer wall								
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[um] → Stiff max ● Soft ▲ Soft max → Stiff half-max ■ Soft half-max ● Reference 1	5 h1.							

Design II: Hydrodynamic behaviour of cells of cellular deformability model

Hydrodynamic behaviour of cells of five different degrees of deformability (Soft max, soft half-max, soft, stiff half-max and stiff) in comparison to reference 15 μ m beads, in design II spiral channel with 170 × 30 μ m cross-section at five different flow rates corresponding to Re=33, 66, 97, 132 and 168 (as outlined in the tables on the right). The lateral equilibrium positions were measured as a distance from the outer wall (μ m) at the end of the spiral channel and there were generated by image analysis. Here, it is reported as median (represented as the symbols) and the interquartile range (indicated by the short vertical lines). Vertical dotted lines indicate four sections of the channel corresponding to four outlets of the channel (0-90. μ m-outlet A, 90-180 μ m- outlet B, etc.). Events belonging to a given section have the highest probability of being captured within the corresponding outlet **and** tables showing statistical summary (mean and standard deviation from the mean (SD), median, 25th (Qi) and 75th (Q3) percentile as well as minimal (min) and maximal (max) measured value) of latera equilibrium positions obtained for at least 10000 events

Design II: Hydrodynamic behaviour of cells of cellular deformability model

Replica I

	Re=168	Mean	SD	Min	Q1	Median	Q3	Max
8	10µm beads	119	23	7	95	136	139	155
16	Stiff max	113	21	34	102	121	128	143
Re=168	Stiff half-max	100	27	21	78	109	124	143
R	Soft	68	21	20	54	62	79	161
	Soft half-max	80	26	20	59	74	96	142
	Soft max	75	24	19	57	70	92	142
	Re=132	Mean	SD	Min	Q1	Median	Q3	Max
2	10µm beads	128	11	28	121	132	137	161
13	Stiff max	101	25	29	84	107	123	147
	Stiff half-max	88	29	26	67	85	119	143
Re=132	Soft	75	18	23	63	74	86	141
	Soft half-max	84	23	20	66	83	102	143
	Soft max	80	23	15	62	77	97	162
	Re=97	Mean	SD	Min	Q1	Median	Q3	Max
	10µm beads	108	20	29	91	97	131	158
) Ô	Stiff max	89	25	25	76	87	107	144
Re=97	Stiff half-max	79	24	21	64	79	92	148
X	Soft	85	20	24	70	85	99	141
	Soft half-max	85	20	24	70	85	99	141
	Soft max	82	21	20	66	81	97	141
	Re=66	Mean	SD	Min	Q1	Median	Q3	Max
9	10µm beads	99	17	60	80	107	115	150
9=	Stiff max	82	26	18	70	84	94	145
Re=66	Stiff half-max	80	21	18	75	83	89	148
Y	Soft	78	18	21	69	80	87	149
	Soft half-max	84	18	19	74	85	96	144
	Soft max	82	18	21	71	83	93	138
	Re=33	Mean	SD	Min	Q1	Median	Q3	Max
\mathbf{c}	10µm beads	102	8	40	97	102	105	152
Re=33	Stiff max	87	19	18	80	90	97	150
e	Stiff half-max	84	18	17	78	87	94	150
\mathbf{X}	Soft	82	17	19	74	83	90	149
	Soft half-max	86	19	18	77	89	98	148
	Soft max	84	20	17	73	86	96	150
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Distance from the outer wall [um]

Design II: Hydrodynamic behaviour of cells of cellular deformability model

	_							
	Re=168	Mean	SD	Min	Q1	Median	Q3	Max
	10µm beads	119	23	7	95	136	139	155
	Stiff max	101	26	21	83	106	123	142
	Stiff half-max		27	30	85	116	126	143
	Soft	75	23	15	59	72	88	145
	Soft half-max	80	26	19	61	76	100	142
	Soft max	78	28	25	55	71	102	138
	Re=132	Mean	SD	Min	Q1	Median	Q3	Max
	10µm beads	128	11	28	121	132	137	161
	Stiff max	100	27	21	78	109	124	143
	Stiff half-max	94	28	22	74	94	122	146
	Soft	76	20	17	62	75	88	144
	Soft half-max	82	20	17	67	81	95	137
	Soft max	86	24	31	66	84	108	135
	-							
i i i	Re=97	Mean	SD	Min	Q1	Median	Q3	Max
	10µm beads	108	20	29	91	97	131	158
	Stiff max	94	26 26	21	79	91	120	155
├──�───┤	Stiff half-max	90	28	21	72	89	116	144
	Soft	80	15	21	70	80	88	144
	Soft half-max	80	18	21	69	80	90	133
	Soft max	85	19	30	71	85	90 98	133
	Soft max	85	19	50	/1	65	90	141
	Re=66	Mean	SD	Min	Q1	Median	Q3	Max
	10µm beads	99	17	60	80	107	115	150
	Stiff max	86	27	23	74	88	99	155
	Stiff half-max	84	27	20	67	85	100	151
	Soft	77	18	18	68	79	86	143
	Soft half-max	82	19	27	71	83	92	142
	Soft max	83	20	17	73	84	94	141
	·							
	Re=33	Mean	SD	Min	Q1	Median	Q3	Max
	10µm beads	102	8	40	97	102	105	152
	Stiff max	86	22	20	76	89	98	155
	Stiff half-max	86	21	18	74	87	99	150
	Soft	80	16	16	73	81	88	149
	Soft half-max	84	19	18	73	85	95	149
	Soft max	83	21	16	72	85	95	152
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Replica II

Design II: Hydrodynamic behaviour of cells of cellular deformability model Replica III

Re-168 Mean SD Min QI Median Q3 Maxim Jumbada Stiff max 119 23 7 95 136 139 155 Stiff max 115 21 31 110 123 54 63 97 123 143 Soft max 77 25 17 57 69 90 140 Mema SD Min Q1 Median Q3 Maxim 71 45 73 95 140 Soft max 77 25 17 57 69 90 140 Mema SD Min Q1 Median Q3 Maxim 74 23 19 57 69 90 140 Min Particit Partit Partit Partit Pari									
Stiff max 115 21 31 110 123 129 155 Soft Soft Soft 28 28 74 97 123 143 Soft Soft Soft Soft Soft 31 100 123 143 Soft Soft Soft Soft Soft 31 110 123 129 155 Soft						-		-	
Stiff half-max 96 28 28 74 97 123 143 Soft latemax 77 25 17 57 73 95 140 Soft max 74 23 19 57 69 90 140 Soft max 74 23 19 57 69 90 140 Soft max 74 23 19 57 69 90 140 Soft max 74 23 19 57 69 90 140 Soft max 74 23 19 57 69 90 140 Soft max 74 23 19 57 69 90 140 Soft max 74 23 19 57 69 90 140 Soft max 75 73 73 13 158 107 142 Soft max 86 22 28 18 61 66 80 92 143 Soft max Soft max Soft max 18 10 <th></th> <th></th> <th></th> <th></th> <th></th> <th></th> <th></th> <th></th> <th></th>									
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Summary of flow cytometric viability assay. On the top- an exemplary scatter plot showing gating strategy for live cell (green, negative for both Alexa Fluor 488-annexin V and propidium iodide (PI) fluorescence), apoptotic cells (orange, annexin V-positive and PI-negative) and necrotic (red, annexin V-positive and PI-positive). Summary of flow cytometric assessment of the presence of live, apoptotic and necrotic Jurkat cells before (stained control and after processing (stained test).

Design I spiral channel with $360 \times 60 \ \mu m$ cross-section at highest applied flow rate (Re=237) for three replicas.



Propidium iodide fluorescence



Design II spiral channel with 170 \times 30 μm cross-section at highest applied flow rate (Re=168) for three replicas.

Propidium iodide fluorescence

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