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Electronic Supplementary Information (ESI)

Rapid sub-micromolar amperometric enzyme biosensing with free substrate access but without nanomaterial signalling support: Oxidase-based glucose detection as proof-of-principle case

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Table S1: Summary of analytical figures of merit for published biosensors that use nanomaterials of various types as components of the immobilization matrix to establish μM limits of detection. (Source of the reference collection: Web of Science).

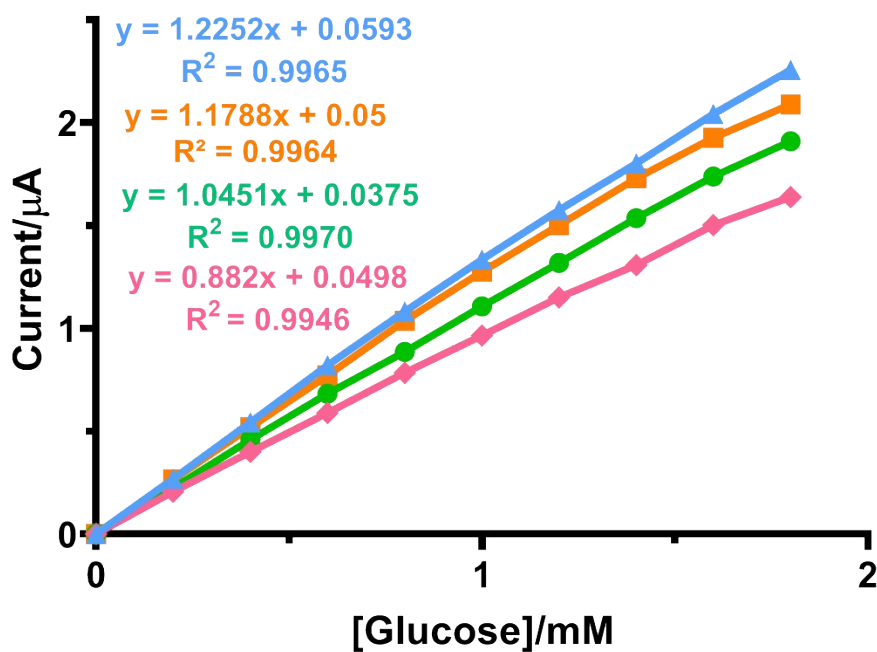
Nanomaterial in enzyme immobilization matrix	Study	Year	Linear Range	Sensitivity	LOD (μM)	Response time (s)
Carbon Nanotubes	Ref. 1	2013	0.42 μM - 8.0mM	52.0 $\mu\text{AmM}^{-1}\text{cm}^{-2}$	-	-
	Ref. 2	2016	0.01mM - 4.7mM	2860.3 $\mu\text{AmM}^{-1}\text{cm}^{-2}$	5	3
	Ref. 3	2017	6 μM – 2mM 10 μM – 1mM	-	2.12 3.8	-
	Ref. 4	2018	Up to 1.0mM	0.44 \pm 0.01 mA M ⁻¹	3	28 \pm 2
	Ref. 5	2019	50 – 500 μM	4.83 μAmM^{-1}	1.2	-
Graphene	Ref. 6	2015	10 μM – 12.55mM	6.36 μAmM^{-1}	1	-
	Ref. 7	2015	0.14 – 4.0 μM	15.04 mAmM ⁻¹	0.06	-
	Ref. 8	2015	-	221.0 mAmM ⁻¹ cm ⁻²	-	-
	Ref. 9	2019	0.1mM – 11mM	15.85 $\mu\text{AmM}^{-1}\text{cm}^{-2}$	20	-
	Ref. 10	2020	0.001 – 0.1mM	-	0.018	-
	Ref. 11	2020	0 – 1.2mg/mL	0.77 nm/(mg/mL)	-	2.16
Mesoporous carbon and carbon nanodots	Ref. 12	2020	0.006 – 6mM	64.51 $\mu\text{AmM}^{-1}\text{cm}^{-2}$	1.8	-
	Ref. 13	2015	48.6 – 12500 μM	6.9 $\mu\text{AmM}^{-1}\text{cm}^{-2}$	2.7	-
	Ref. 14	2015	1 – 16mM	0.31 μAmM^{-1}	88	-
	Ref. 15	2015	0 – 0.64mM	6.1 μAmM^{-1}	1.07	-
	Ref. 16	2019	0.0002 – 0.1mM	123.28 $\mu\text{AmM}^{-1}\text{cm}^{-2}$	0.023	3.7
Metal Organic Framework	Ref. 17	2019	250 μM – 3mM	56.12 $\mu\text{AmM}^{-1}\text{cm}^{-2}$	4.1	-
	Ref. 18	2017	25 μM – 17mM	25.1 μAmM^{-1}	8	-
	Ref. 19	2018	0.51 μM – 5.62mM	28.67 $\mu\text{AmM}^{-1}\text{cm}^{-2}$	0.48	-
Prussian blue nanoparticles	Ref. 20	2018	1 μM – 2mM	-	0.333	-
	Ref. 21	2000	-	3 μAcM^{-2}	-	-
	Ref. 22	2016	5 μM – 1.2mM	32 $\mu\text{AmM}^{-1}\text{cm}^{-2}$	0.5	3-4
Redox polymer and polymer nanoparticles	Ref. 23	2017	2 – 68mM	0.19 – 3.87 $\mu\text{AmM}^{-1}\text{cm}^{-2}$	-	-
	Ref. 24	2015	0.3 – 17mM	-	2.7	1
	Ref. 25	2015	-	120.87 mAm ⁻¹ cm ⁻²	37.6	-
	Ref. 26	2015	200 μM – 3.4mM	1.59 nA μM^{-1}	46.2	15
	Ref. 27	2016	1 – 10mM	16.04 $\mu\text{AmM}^{-1}\text{cm}^{-2}$	820	10
	Ref. 28	2016	Up to 1.5mM	176 mAmM ⁻¹ cm ⁻² U ⁻¹	9	<4
	Ref. 29	2016	9.0 μM – 8.26mM	11.98 mAm ⁻¹ cm ⁻²	10	-
	Ref. 30	2018	0.1 – 0.8mM 0.1 – 10mM 0.1 – 10mM	- - -	2.9 3.2 3.4	- - -
	Ref. 31	2018	5 – 30mM	-	550	< 3
	Ref. 32	2018	0.01 – 0.8mM	74.22 $\mu\text{AmM}^{-1}\text{cm}^{-2}$	2.9	2-3
	Ref. 33	2019	500nM – 10nM	-	0.01	-
Ref. 34	2020	10 μM – 1.94mM	35.56 $\mu\text{AmM}^{-1}\text{cm}^{-2}$	0.1	-	
	Ref. 35	2015	0.005 – 10mM	175.49 $\mu\text{AmM}^{-1}\text{cm}^{-2}$	50	<2
	Ref. 36	2015	0.1 – 10.0mM	52.1 $\mu\text{AmM}^{-1}\text{cm}^{-2}$	24	-
	Ref. 37	2015	55.1 μM – 16.53mM	390.5 $\mu\text{AmM}^{-1}\text{cm}^{-2}$	11	-
	Ref. 38	2015	0.05 – 2.25mM	9.62 $\mu\text{AmM}^{-1}\text{cm}^{-2}$	10	-

Metal, metal oxide and semiconductor nanoparticles	Ref. 39	2015	1 – 20mM	0.58 μAmM^{-1}	68	4
	Ref. 40	2015	0.02 – 6.0mM	6.31 $\mu\text{AmM}^{-1}\text{cm}^{-2}$	18	10
	Ref. 41	2015	50 μM – 10mM	12.1 $\mu\text{AmM}^{-1}\text{cm}^{-2}$	1.02	-
	Ref. 42	2015	2.0 – 52 μM 0.052 – 2.3mM	68.58 $\text{mAmM}^{-1}\text{cm}^{-2}$	0.5	-
	Ref. 43	2015	0.05 – 2.5mM	24.65 $\mu\text{AmM}^{-1}\text{cm}^{-2}$	20	-
	Ref. 44	2015	0.2 – 9.0mM	2.52 $\mu\text{AmM}^{-1}\text{cm}^{-2}$	100	-
	Ref. 45	2016	-	-	40	-
	Ref. 46	2016	5 μM – 2mM	-	1.8	5
	Ref. 47	2016	0.1 – 2.7mM	6.37 $\text{mAmM}^{-1}\text{cm}^{-2}$	14.1	5
	Ref. 48	2016	0.1 – 18mM	4.2 $\mu\text{AmM}^{-1}\text{cm}^{-2}$	5.9	-
	Ref. 49	2016	-	18.6 $\text{mAmM}^{-1}\text{cm}^{-2}$	2.2	-
	Ref. 50	2017	1 – 6mM	6.82 $\mu\text{AmM}^{-1}\text{cm}^{-2}$	0.2	< 5
	Ref. 51	2017	0.025 – 2.20mM	3.19 μAmM^{-1}	0.2	-
	Ref. 52	2018	0.2 – 12mM	231.7 $\mu\text{AmM}^{-1}\text{cm}^{-2}$	6.3	3
	Metal, metal oxide and semiconductor nanoparticles	Ref. 53	2018	5 - 100 μM	-	1.8
Ref. 54		2019	0.02 – 2.5mM	42.8 $\mu\text{AmM}^{-1}\text{cm}^{-2}$	10	5
Ref. 55		2019	0.008 – 1.13mM 1.13 – 5.53mM	18.9 $\text{mAmM}^{-1}\text{cm}^{-2}$	1.8	< 8
Ref. 56		2019	0.005 – 3.3mM	12.5 $\mu\text{AmM}^{-1}\text{cm}^{-2}$	0.9	< 3
Ref. 57		2019	-	8.5 $\mu\text{AmM}^{-1}\text{cm}^{-2}$	3.2	< 10
Ref. 58		2019	1 – 14mM	12.99 $\text{mAmM}^{-1}\text{cm}^{-2}$	300	-
Ref. 59		2019	0.003 – 3.43 mM	35.4 $\mu\text{AmM}^{-1}\text{cm}^{-2}$	1.34	< 3
Ref. 60		2019	-	3.7277 $\text{mAmM}^{-1}\text{cm}^{-2}$	3	-
Ref. 61		2019	0.1 – 2.6 mM	25.9 $\text{mAmM}^{-1}\text{cm}^{-2}$	-	30
Nanomaterial-Free		This work	2020	Up to 1.8 mM	158 $\mu\text{AmM}^{-1}\text{cm}^{-2}$	0.5

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Supplementary Figure S1: Response linearity of four gelatin/GOx biosensors, prepared identically on different days. The calibrations were carried out at day 1, after one-night storage in a refrigerator in 0.1 M Na-PB/0.1 M KCl. The electrolyte for all trials was 0.1 M Na-PB/0.1 M KCl, and amperometry was at 25° C, with a H₂O₂ detection potential of + 0.6 V vs. Ag/AgCl.

Experimental Section

Chemicals, materials, solutions. Anhydrous β -D (+) glucose, monobasic (NaH_2PO_4) and dibasic (Na_2HPO_4) sodium phosphate for buffer preparation and ascorbic acid, uric acid, dopamine and paracetamol for the interference tests were from Italmar (Thailand) Co., Ltd., Bangkok, Thailand. GOx (source: *Aspergillus Niger*, #G7141, 228,253 U/g) and glutaraldehyde (Grade I, 25 % in H_2O) were from S.M. Chemical Supplies Co., Ltd., Bangkok, Thailand. Food-grade 'McGarret' gelatin powder was from a local store. Ultrapure de-ionized water was used for solution preparation. The biosensor storage solution and supporting electrolyte for all biosensor tests was 0.1 M Na phosphate buffer pH 7.4 containing 0.1 M KCl.

Human serum samples. The serum glucose analysis with gelatin/GOx biosensors was conducted on aliquots of one particular whole-blood sample, which was an agreed donation of the principal investigator (PI) of the study (AS). Blood sampling from others, typical of large-scale clinical trials on many patients, was not part of this study, so institutional approval was not required. The blood sample from the PI was converted to serum by a standard procedure.¹ The glucose content of stockpiled serum samples was measured according to instructions with an Accu-Chek® Active blood glucose meter, a commercial hand-held device normally used by diabetic patients for blood tests. The mean of triplicate glucose meter assessments was used as the reference value for the data obtained with gelatin/GOx-based biosensors.

Biosensor fabrication. First, a 1-mm diameter platinum (Pt) disk electrode encased in a PEEK (polyether-ether-ketone) body of 3 mm outer diameter diameter from eDAQ Pty Ltd (Denistone East, Australia) was polished and cleaned, as usual for voltammetry, then 2 μL gelatin solution (5 mg mL^{-1} in H_2O) was placed on the Pt disk and an even gelatin film formed on the smooth metal surface by solvent evaporation for 10-15 min at room temperature, 25°C. Next, 2 μL of GOx solution (10 mg mL^{-1} in Na phosphate buffer) was dropped onto the gelatin-coated Pt disk and air-dried at room temperature for 10-15 min. Finally, the gelatin/GOx-covered electrode was pushed in an inverted position through a suitably-sized hole in the cap of an Eppendorf tube containing 200 μL of 10 % glutaraldehyde solution. Care was taken not to touch the central biolayer and a Parafilm® M wrap was then applied, to seal the tube cap to the electrode stem. The Pt disk coating was thus exposed to glutaraldehyde vapor in the tube, causing chemical crosslinking of NH_2 -groups. The glutaraldehyde treatment was routinely continued for 6 h at 4°C to complete the desired gelatin/GOx-Pt sensors. Finished sensors were stored overnight in phosphate buffer, pH 7.4 at 4°C before performing calibrations or glucose measurements with model or real samples.

The 1-mm diameter copper (Cu) disk electrodes were home-made. In course of the procedure a 1-mm diameter electrical cable copper wire was placed in a tapered glass tube and the tube then filled with liquid superglue. After overnight superglue hardening the desired Cu disk was exposed by careful grinding of the tip of the assembly on emery paper. Polishing on progressively finer emery paper and finally on a soft polishing pad soaked with alumina paste of small grade created the circular and smooth Cu electrode, surrounded by a layer of insulating

resin in the glass case. The gelatin modification of the Cu disk followed the procedure used for the Pt disks, but with 1.5 μL instead of the 2 μL of the gelatin and GOx solution used in the drop-and-dry coating procedure.

Biosensor amperometry. Electrochemical measurements with the developed gelatin/GOx-Pt and gelatin/GOx-Cu biosensors were performed with a PalmSens4 potentiostat (PalmSens BV, GA Houten, The Netherlands). The instrument was connected to a three-electrode electrochemical cell and controlled by the latest version of the PalmSens software. All amperometric trials took place at room temperature of 25°C in 5 mL of stirred Na phosphate buffer, pH 7.4. The biosensor of choice, an AgCl-coated silver wire and a Pt foil were the working-, pseudo-reference- and counter-electrodes, respectively. H_2O_2 currents on glucose addition to electrolyte were recorded at an anodic working electrode potential of + 0.6 V vs. Ag/AgCl for the Pt biosensor version and at a cathodic working electrode potential of – 0.25 V vs. Ag/AgCl for the Cu-based version.

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