

## Electronic Supplementary Information

### **Cyclodextrin-based superparamagnetic host vesicles as ultra-sensitive nanobiocarriers for electroensing**

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## **Experimental Procedures**

### ***Chemicals and reagents***

All commercially available chemicals were used as received and were purchased from Sigma-Aldrich (St. Louis, Missouri, USA).

### ***Synthesis of oleic acid capped iron oxide nanoparticles***

Oleic acid coated magnetic nanoparticles were synthesized by co-precipitation of ferric and ferrous salts in alkaline medium as described in the literature.<sup>[1]</sup> To this end, 2 g of  $\text{FeSO}_4 \cdot 7\text{H}_2\text{O}$  and 3.5 g of  $\text{FeCl}_3 \cdot 6\text{H}_2\text{O}$  were dissolved in 100 mL Milli-Q water. Next, 25 mL of an aqueous  $\text{NH}_3$  solution (25%, w/w) was added to the mixture and the solution was kept stirring at RT. Once the solution turned black, 1 mL of oleic acid was added dropwise and aged at 80 °C under Ar atmosphere. Finally, the product was well dispersed into water and transferred into a toluene phase.

DLS (diameter number mean):  $37.0 \pm 0.7$  nm

### ***mCDV preparation***

mCDVs were synthesized following the method presented by Ravoo and co-workers.<sup>[2]</sup> 0.1 mg of oleic acid capped iron oxide nanoparticles and 6.5 mg of amphiphilic  $\beta$ -CD were dissolved in 100  $\mu\text{L}$  of  $\text{CHCl}_3$ . The solvent was slowly evaporated from the solution in Ar stream while continually rotating the flask. The residual solvent was removed from the film in strong vacuum. Then, the film was hydrated by adding 2 mL of PBS (pH 7.2) and vigorous stirring overnight. Then, the solution was sonicated for 10 s and extruded through a 100 nm pore size polycarbonate membrane in a Liposofast manual extruder. mCDVs were stored in the fridge after use. A fresh batch of mCDVs was synthesized every week.

DLS (diameter number mean):  $100 \pm 3$  nm

### ***mNC–CPE fabrication***

mNC–CPEs were fabricated by following the methodology employed by Muñoz and co-workers.<sup>[3]</sup> Graphite powder was hand-mixing dispersed within an insulating epoxy in a 1:4 (w/w) ratio. Then, a PVC tube (i.d.: 6 mm, length: 20 mm) containing a copper disk as electrical contact (body electrode) was tightly packed, where a small cylindrical neodymium magnet (3 mm diameter, N35) was placed into the center of this electrode. Finally, the electrode was cured at 80 °C for 24 h and polished with different sandpapers of decreasing grain size. After each electrochemical measurement, the electrode surface was reset by a simple polishing step.

### ***Apparatus and procedures***

*Dynamic light scattering (DLS):* DLS measurements were recorded using a Nano-ZS Zetasizer (Malvern Instruments, Malvern, UK). While mCDVs were measured in PBS (pH 7.2), oleic acid coated magnetic nanoparticles were measured in ethanol. Samples were measured in disposable 1 mL semi-micro PMMA cuvettes (Brand GmbH & Co. KG, Wertheim, Germany). Data analysis was realized with Malvern Zetasizer software 7.12 (Malvern Instruments, Malvern, UK).

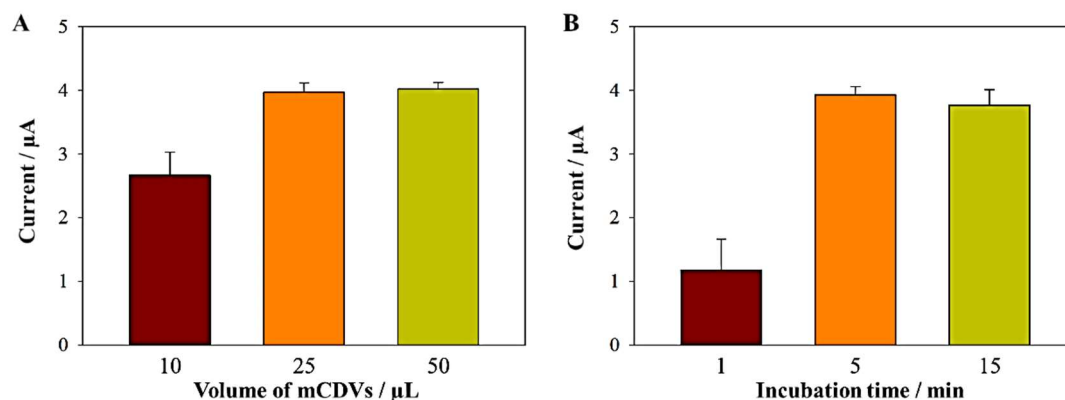
*Transmission electron microscopy (TEM):* Samples were deposited on a covered holey copper grid, by applying a drop of either mCDVs or oleic acid coated magnetic nanoparticles (blank). TEM images were acquired by using a Zeiss 200 FE electron microscope with schottky emitter and energy  $\Omega$  filter operating at 200 kV.

*Electrochemical measurements:* Electrochemical measurements were performed by Linear Sweep Voltammetry (LSV) and Electrochemical Impedance Spectroscopy (EIS) means employing an AutoLab Metrohm PGSTAT128N potentiostat/galvanostat equipped with NOVA 2.1.2 software, coupled with a conventional three-electrode configuration cell. The electrode configuration consists of: mNC–CPE as the working electrode, an Ag/AgCl wire as the reference electrode, and a Pt wire as the counter electrode. A 0.1 M KCl solution

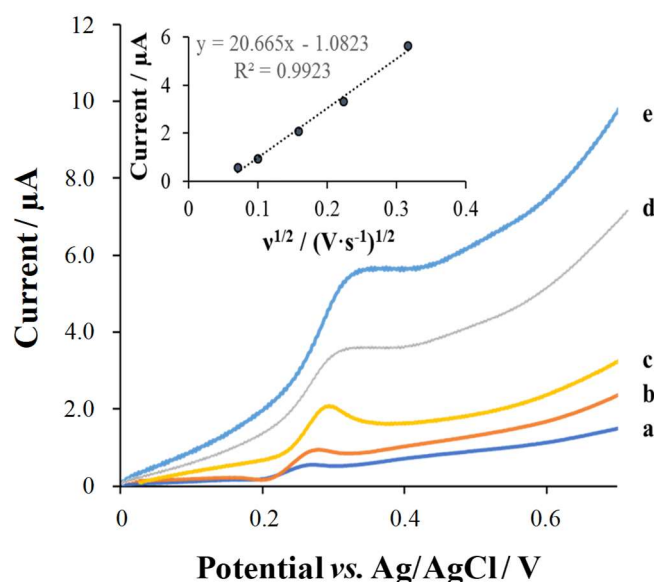
containing 10 mM  $[\text{Fe}(\text{CN})_6]^{3-/4-}$  was utilized as the redox marker for EIS characterization. A phosphate-buffered saline (PBS) solution at pH 7.2 was the electrolyte employed for DLS electroanalysis.

*Electroanalytical assay:* The developed methodology is similar to a conventional antigen-antibody immunoassay, following the three sequential steps: 1) 25  $\mu\text{L}$  of the synthesized mCDVs were incorporated into a vial containing 1.0 mL of a desired concentration of  $\text{T}_4$ . The vial was aged for 5 min to promote the supramolecular  $\beta\text{-CD-T}_4$  interactions. 2) The loaded-mCDVs were captured by dipping the mNC-CPE into the vial and washed twice with a PBS solution (pH 7.2). 3) The mNC-CPE containing the loaded-mCDVs was transferred into the three-electrode configuration cell filled with the electrolyte (PBS at pH 7.2) for LSV analysis. After each measurement, mCDVs were removed from the mNC-CPE by a simple polishing step, obtaining a reset electrode surface. For the control experiment, the same protocol was carried out using oleic acid coated magnetic nanoparticles.

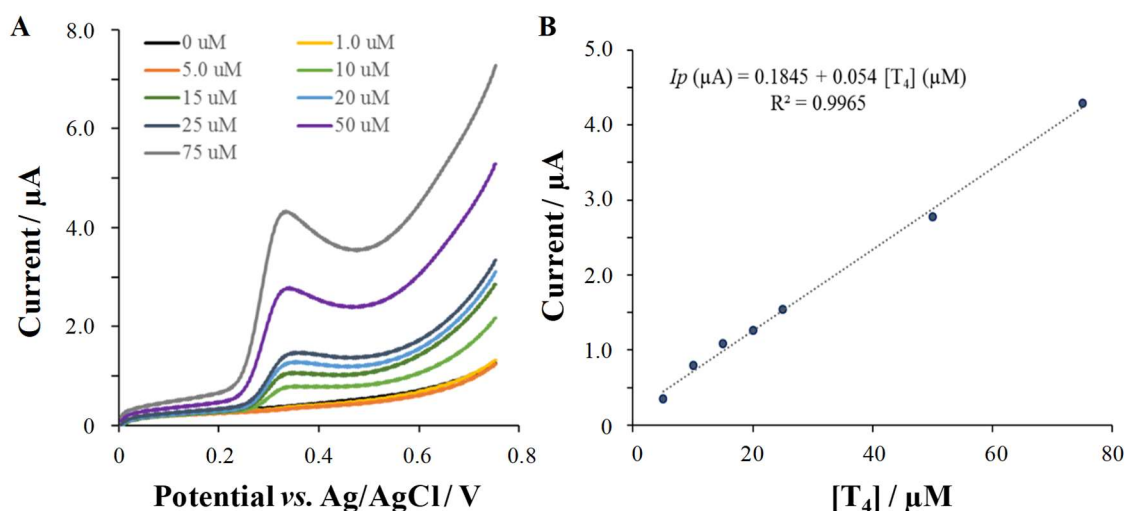
## Supplementary Information Figures



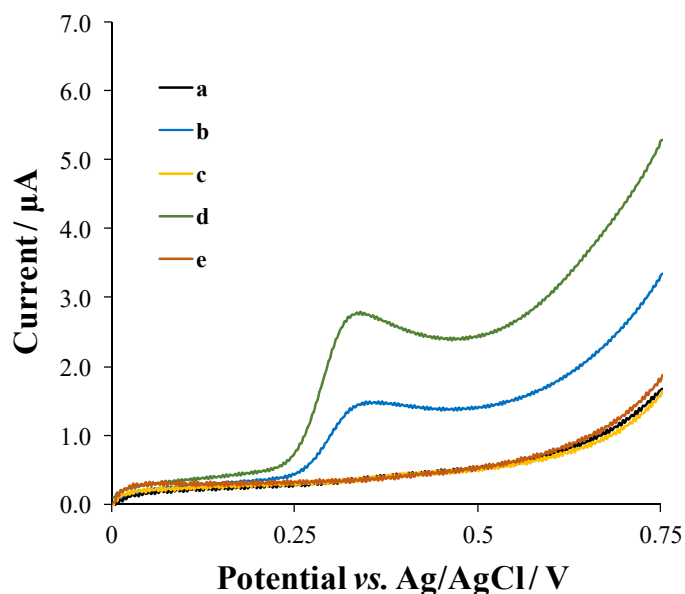
**Figure S1.** Optimization of some pivotal parameters for the electroanalytical assay. A) Study of the volume of mCDVs (10, 25 and 50  $\mu\text{L}$ ) for a fix  $\text{T}_4$  concentration (60 pM); incubation time: 15 min. B) Determination of the optimum incubation time for the supramolecular CD- $\text{T}_4$  binding formation (1, 5 and 15 min) for a mix  $\text{T}_4$  concentration (60 pM); volume of mCDVs: 25  $\mu\text{L}$ . LSV analyses were run in a three-electrode configuration cell filled with 10 mL of electrolyte (PBS at pH 7.2), employing a scan rate of  $25 \text{ mV}\cdot\text{s}^{-1}$ .



**Figure S2.** Influence of scan rate ( $v$ ) from 5 to  $100 \text{ mV}\cdot\text{s}^{-1}$  (a to e) in the presence of  $5.0 \mu\text{M}$   $\text{T}_4$  at the bio-recognition sensing system. Inset: lineal  $I_{pa}$  vs.  $v^{1/2}$  dependence. Experiments were run in a PBS electrolyte at pH 7.2.



**Figure S3.** A) LSV response at the naked NC-CPE (blank experiment) with increasing the [T<sub>4</sub>] from 1.0 to 75 μM. B) Linear response with a LOD of 5.0 μM. Experiments were carried out in a PBS electrolyte at pH 7.2 (scan rate: 25 mV·s<sup>-1</sup>).



**Figure S4.** Regeneration capability of the mNC-CPE surface before (a, c) and after sensing different [T<sub>4</sub>] (*i.e.*, (b) 10 pM and (d) 25 pM T<sub>4</sub>). After the polishing procedure (c, e), the electrode recovers its initial electrochemical performance. Experiments were carried out in a PBS electrolyte at pH 7.2 (scan rate: 25 mV·s<sup>-1</sup>).

## Supplementary Information Tables

**Table S1.** Study of four potentially interfering biomolecules on the  $R_{CT}$  signal of 5.0  $\mu\text{M}$   $\text{T}_4$ . The selectivity EIS test was carried out by incubating the mCDVs with a  $\text{T}_4$  solution doped with tyrosine (Tyr), ascorbic acid (AA), uric acid (UA) and dopamine (DA) in a 1:1 ratio.

Compounds	Concentration ( $\mu\text{M}$ )	$R_{CT}$ change (%)
$\text{T}_4$	5.0	100
Tyr	5.0	+2.57
AA	5.0	+1.28
UA	5.0	+0.97
DA	5.0	+0.99

## References

- [1] Sun, Y.; Ding, X.; Zheng, Z.; Cheng, X.; Hu, X.; Peng, Y., *European Polymer Journal* 2007, **43** (3), 762-772.
- [2] Schenkel, J. H.; Samanta, A.; Ravoo, B. J., *Advanced Materials* 2014, **26** (7), 1076-1080.
- [3] Muñoz, J.; González-Campo, A.; Riba-Moliner, M.; Baeza, M.; Mas-Torrent, M., *Biosensors and Bioelectronics* 2018, **105**, 95-102.