## **Supporting Information**

# Longitudinally Expanded Ni-Based Metal-Organic Framework with Enhanced Double Nickel Cation Catalysis Reaction Channels for Non-Enzymatic Sweat Glucose Biosensor

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## S1. Current Response and Scan Rate for Glucose Detection

CV curves of 0, 60, and 120 min Ni-MOFs in 0.1 M NaOH solutions with 0 or 100  $\mu$ M glucose at various potential scan rates from 10 to 100 mV s<sup>-1</sup> are shown in Fig. S1a and b, Fig. S1d and e, Fig. S1g and h, respectively. As shown in Fig. S1a, d and g, the well-defined oxidation peaks near 0.50 V and reduction peaks near 0.30 V in CV curves are ascribed to typical redox reactions between Ni ions and OH<sup>-</sup> in alkaline solution. With increasing potential scan rate, the oxidation peak moves toward larger potential value, while the reduction peak shifts toward smaller potential value, which is ascribed to the hindered electron transfer process at electrode/electrolyte interface.<sup>1</sup> Similar phenomenon has also been observed in 0.1 M NaOH solution with 100  $\mu$ M glucose for each sample, as shown in Fig. S1b, e and (h). The 60 min Ni-MOF exhibits the highest current densities both in 0.1 M NaOH solutions with 0 and 100  $\mu$ M glucose as shown in Fig. S1d and e, in comparison with those of 0 and 120 min Ni-MOFs as shown in Fig. S1a and b, Fig. S1g and h.

The data in Fig. S1 has been further analyzed according to equation (S1), with derived results illustrated in Fig. S1c, f and i.

$$t = a v^b \tag{S1}$$

where i is current density at a specific potential scan rate v obtained from CV curves, a and b are adjustable parameters. The dependence of increasing current density on increasing scan rate is presented by the b value according to equation (S1), and explained by the balance between diffusion and adsorption processes.<sup>2</sup> For reversible processes, b = 0.5 represents a diffusion-dominated electrochemical process, and b = 1 indicates an adsorption-dominated electrochemical process.<sup>3,4</sup> As shown in Fig. S1c, f and i, without glucose, the b values of 0, 60, and 120 min Ni-MOFs are all close to 0.5, indicating that the oxidation process of Ni-MOF is based on the diffusion of OH<sup>-</sup>, while with 100  $\mu$ M glucose, the b values of 0, 60, and 120 min Ni-MOFs are all less than 0.5, which is related to a restricted kinetics process.<sup>5</sup> The slopes of log(scan rate) versus log (current density) with and without glucose are different in Fig. S1c, f and i, where the two linear fitting lines intersects at a certain high scan rate between 60 and 100 mV s<sup>-1</sup>, which means that a current gain can be obtained at lower sweep speeds (< ~ 60 mV s<sup>-1</sup>) while a current loss can be caused at higher sweep speeds in glucose solution, different with those in non-glucose solution. For this reason, we choose the potential scan rate of 20 mV s<sup>-1</sup> in the following CV test.



Fig. S1 CV curves of 0 min Ni-MOF in 0.1 M NaOH solutions (a) without glucose

and b with 100  $\mu$ M glucose at various potential scan rates from 10 to 100 mV s<sup>-1</sup>. (c) Linear analysis of peak current density and potential scan rate for 0 min Ni-MOF. CV curves of 60 min Ni-MOF in 0.1 M NaOH (d) without glucose and (e) with 100  $\mu$ M glucose at various potential scan rates from 10 to 100 mV s<sup>-1</sup>. (f) Linear analysis of peak current density and potential scan rate for 60 min Ni-MOF. CV curves of 120 min Ni-MOF in 0.1 M NaOH (g) without glucose and (h) with 100  $\mu$ M glucose at various potential scan rates from 10 to 100 mV s<sup>-1</sup>. (i) Linear analysis of peak current density and potential scan rate for 60 min Ni-MOF. CV curves of 120 min Ni-MOF in 0.1 M NaOH (g) without glucose and (h) with 100  $\mu$ M glucose at various potential scan rates from 10 to 100 mV s<sup>-1</sup>. (i) Linear analysis of peak current density and potential scan rate for 120 min Ni-MOF.



**Fig. S2** CV peak separation of (a) 0 min, (b) 30 min, (c) 60 min, and (d) 120 min Ni MOF at 20 mV s<sup>-1</sup> in 0.1 M NaOH solution without glucose.

#### S2. Calculation of Diffusion Coefficient D

The slopes of the fitted linear curves in Fig. 8b are proportional to the diffusion coefficients D. The diffusion coefficients can be obtained by simplifying equation (7)

into equation (S2).

$$\frac{I_t}{A} = n F D^{1/2} C \pi^{-1/2} t^{-1/2}$$
(S2)

where the ordinate is the current density (A cm<sup>-2</sup>), the slope S can be expressed as equation (S3), and the diffusion coefficient D can be obtained by simplifying equation (S3) into equation (S4).

$$S = n F D^{1/2} C \pi^{-1/2}$$
(S3)  
$$D = \frac{\pi S^2}{C^2 F^2 n^2}$$
(S4)

(S4)

where n is the number of electrons in the redox process (n = 1), F is 96485 C mol<sup>-1</sup>. The bulk concentration C (0.1M + 100  $\mu$ M) is 10.01 × 10<sup>-5</sup> mol cm<sup>-3</sup>. Slope S is 4.92×  $10^{-3}$ , 6.69  $\times$  10<sup>-3</sup> and 5.59  $\times$  10<sup>-3</sup> A cm<sup>-2</sup> s<sup>-1</sup> for 0, 60 and 120 min Ni-MOFs, respectively. The diffusion coefficient D of catalytic process can be calculated to be  $8.15 \times 10^{-7}$ ,  $1.51 \times 10^{-6}$  and  $1.04 \times 10^{-6}$  cm<sup>2</sup> s<sup>-1</sup> for 0, 60 and 120 min Ni-MOFs, respectively.

### **S3.** Calculation of Active Surface Area

The active surface area can be can be obtained by simplifying equation (8) into equation (S5).

$$A = \frac{Ip}{0.4463 \sqrt{\frac{C^2 D n^3 F^3 v}{RT}}}$$
(S5)

In Fig. S1b, e and (h), the current density (electrode area =  $0.07 \text{ cm}^2$ ) in 0.1 M NaOH and 100  $\mu$ M glucose solution are 4.13, 10.51 and 3.03 mA cm<sup>-2</sup> for 0, 60 and 120 min Ni-MOFs at 20 mV s<sup>-1</sup>, respectively. The values of current Ip are  $2.92 \times 10^{-4}$ ,  $7.43 \times$ 

 $10^{-4}$ ,  $2.14 \times 10^{-4}$  A for 0, 60, and 120 min Ni-MOFs. The bulk concentration (0.1 M + 100  $\mu$ M) equals to  $10.01 \times 10^{-5}$  mol cm<sup>-3</sup>. n is the number of electrons in the redox process (n = 1). F is 96485 C mol<sup>-1</sup>. R is 8.314 J mol<sup>-1</sup> K<sup>-1</sup>. T is 298.15 K. The CV scan rate  $\nu$  is 0.02 V s<sup>-1</sup>. D is 8.15 × 10<sup>-7</sup>, 1.51 × 10<sup>-6</sup> and 1.04 × 10<sup>-6</sup> cm<sup>2</sup> s<sup>-1</sup> for 0, 60 and 120 min Ni-MOFs, respectively.

Therefore, we can roughly estimate the active surface area related to glucose detection performance of Ni-MOF electrode in 0.1 M NaOH solution with 100  $\mu$ M glucose to be 0.09, 0.16, and 0.06 cm<sup>2</sup> for 0, 60, and 120 min Ni-MOFs, respectively.

**Table S1.** Comparison of current response and linear range in glucose detection using

 60 min Ni-MOF with other studies in the literatures.

Sample	Sweeping potential methods		Fixed potential		
	(such as cyclic		methods (such as		Deference
	voltammetry)		chronoamperometry)		
	Sensitivity /		Sensitivity		Kelefelice
	uA mM <sup>-1</sup> cm <sup>-</sup>	Linear	/ uA mM <sup>-1</sup>	Linear	
	2	Range/µM	cm <sup>-2</sup>	Range /µM	
Au nanowire	728	500-14000	309.0	1000-10000	6
array					
Au nano/Ti	1389	1000-15000			7
Ni-MOF			1.54	1 500	8
nanobelts			1.34	1-300	-

Ni <sup>II</sup> MOF			585	40-500	9
Ni-MOF/carbon			77.7	20-4400	10
nanotubes					10
NiFe-MOF/Ni			41950	2-1600	11
NiCo-MOF/Au			684	1-8000	12
60 min Ni-	3297.10	0-400	3.03	0-2000	This
MOF					work
60 min Ni-	2260.77	400-1000	0.95	2000-3500	This
MOF					work

## References

- M. S. Rahmanifar, H. Hesari, A. Noori, M. Y. Masoomi, A. Morsali and M. F. Mousavi, A dual Ni/Co-MOF-reduced graphene oxide nanocomposite as a high performance supercapacitor electrode material, *Electrochim. Acta*, 2018, 275, 76-86.
- S. K. Hassaninejaddarzi and M. Gholamiesfidvajani, Preparation of nanoporous nickel phosphate VSB-5 nanorods carbon paste electrode as glucose nonenzymatic sensor, *J. Porous Mater.*, 2017, 24, 85-95.
- Y. Shao, M. F. El-Kady, J. Sun, Y. Li, Q. Zhang, M. Zhu, H. Wang, B. Dunn and R. B. Kaner, Design and mechanisms of asymmetric supercapacitors, *Chem. Rev.*, 2018, **118**, 9233-9280.
- 4. S. K. Hassaninejaddarzi, Fabrication of a non-enzymatic Ni(II) loaded ZSM-5 nanozeolite and multi-walled carbon nanotubes paste electrode as a glucose

electrochemical sensor, RSC Adv., 2015, 5, 105707-105718.

- S. N. Azizi, S. Ghasemi and H. Yazdanisheldarrei, Synthesis of mesoporous silica (SBA-16) nanoparticles using silica extracted from stem cane ash and its application in electrocatalytic oxidation of methanol, *Int. J. Hydrogen Energy*, 2013, 38, 12774-12785.
- S. Cherevko and C. H. Chung, Gold nanowire array electrode for non-enzymatic voltammetric and amperometric glucose detection, *Sens. Actuators B Chem.*, 2009, 142, 216-223.
- Q. Yi and W. Yu, Electrocatalytic activity of a novel titanium-supported nanoporous gold catalyst for glucose oxidation, *Microchim. Acta*, 2009, 165, 381-386.
- X. Xiao, S. Zheng, X. Li, G. Zhang, X. Guo, H. Xue and H. Pang, Facile synthesis of ultrathin Ni-MOF nanobelts for high-efficiency determination of glucose in human serum, *J. Mater. Chem. B*, 2017, 5, 5234-5239.
- N. S. Lopa, M. M. Rahman, F. Ahmed, S. C. Sutradhar, T. Ryu and W. Kim, A Ni-based redox-active metal-organic framework for sensitive and non-enzymatic detection of glucose, *J. Electroanal. Chem.*, 2018, 822, 43-49.
- F. Wang, X. Chen, L. Chen, J. Yang and Q. Wang, High-performance nonenzymatic glucose sensor by hierarchical flower-like nickel(II)-based MOF/carbon nanotubes composite, *Mater. Sci. Eng. C Mater. Biol. Appl.*, 2019, 96, 41-50.
- 11. L. Zhang, X. Ma, H. Liang, H. Lin and G. Zhao, A non-enzymatic glucose

sensor with enhanced anti-interference ability based on a MIL-53(NiFe) metalorganic framework, *J. Mater. Chem. B*, 2019, **7**, 7006-7013.

 W. Li, S. Lv, Y. Wang, L. Zhang and X. Cui, Nanoporous gold induced vertically standing 2D NiCo bimetal-organic framework nanosheets for nonenzymatic glucose biosensing, *Sens. Actuators B Chem.*, 2019, 281, 652-658.