Electronic Supplementary Information (ESI) for:

Injectable zwitterionic thermosensitive hydrogels with low-protein adsorption and combined effect of photothermal-chemotherapy[†]

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Fig. S1 (a) FT-IR spectrum and (b) ¹H NMR spectrum of PNS nanogels.

The copolymerization of SBMA, NIPAM and MBA was confirmed by FTIR and ¹H NMR spectrum. In Fig. S1a, the peak at 2924 cm⁻¹ (peak a) is assigned to C–H stretching vibrations of methyl or methylene in polymer. The peak at 1649 cm⁻¹ (peak b) is assigned to C=O stretching of amide and 1462 cm⁻¹ (peak c) is assigned to C–N bond of amine. The stretching bands of S=O in SBMA appears at 1044 cm⁻¹ (peak e). ¹H NMR spectrum was shown in Fig. S1b. The peaks at δ =1.48~1.60 (a) and δ =1.91~2.01 (b) were assigned to methylene (a) and methylidyne (b) produced from the polymerization of carbon-carbon double bonds, respectively. The others are assigned as follows: δ =1.1 (g, CH(CH₃)₂), 2.2 (m, CH₂CH₂SO₃⁻), 2.89 (n, CH₂CH₂SO₃⁻), 3.16 (k, N⁺(CH₃)₂), 3.52 (l, N⁺CH₂CH₂CH₂SO₃⁻), 3.71 (j, COOCH₂CH₂), 3.79 (f, CH(CH₃)₂), 4.41 (i, COOCH₂; h, CONHCH₂NHCO).



Fig. S2 Diameters of PNA nanogels versus temperature.



Fig. S3 (a) FT-IR spectra of PDA NPs. (b) Hydrodynamic diameter of PDA NPs and its distribution measured by DLS. (c) TEM image of PDA NPs and (d) UV-Vis-NIR spectra of PDA NPs aqueous suspension and DA aqueous solution (both the concentration of DA and PDA NPs were 200 µg/mL).



Fig. S4 (a) Photographs and (b) rheology behavior of the sol-gel transition of PNS dispersion (25 wt%).

Photothermal conversion efficiency of PDA NPs



Fig. S5 (a) Temperature change curve of PDA NPs dispersion (200 μ g/mL) under NIR laser irradiation (808 nm, 1.0 W/cm²) for 15 min and then shutting off the laser, and (b) linear relationship of time *versus* – *lnθ* obtained from the cooling curve in (a).

The photothermal conversion efficiency (η) of PDA NPs can be calculated according to Eq. S1 as reported ^{1,2} and the experimental data.

$$\eta = \frac{hA\Delta T_{\text{max}} - Q_s}{I(1 - 10^{-A_s})}$$
 (Eq. S1)

Wherein *h* is the heat transfer coefficient, *A* is the surface area of the container, ΔT_{max} is the maximum temperature change of PDA NPs suspension at the steady-state temperature, *I* is the laser power density used, A_{λ} is the absorbance of the PDA NPs suspension at 808 nm, and *Qs* is the heat of the solvent (water) produced by the laser irradiation.

In this system, ΔT_{max} was 38.0 °C (Fig. S5a), A_{λ} was 0.237 (Fig. S3d, l=1 cm) and I was 1.0 W/cm². Q_s could be calculated from $Q_s = C_{\text{water}} m\Delta T/t = 4.2 \text{ J/(g·°C)} \times 0.30 \text{ g} \times 5.8 \text{ °C/900 s} = 8.12 \text{ mW}$. hA was obtained by applying the linear time data from the cooling period $vs -ln\theta$ (Fig. S5b) and Eq. S2. Herein, θ is defined in Eq. S3, m and Cp are the mass (0.30 g) and heat capacity of water (4.2 J/(g·°C)).

$$\tau_s = \frac{\sum_i m_i c_{p,i}}{hA}$$
(Eq. S2)

$$\theta = \frac{\Delta T}{\Delta T_{\text{max}}} = \frac{T - T_{surr}}{T_{\text{max}} - T_{surr}}$$
(Eq. S3)

According to the data in Fig. S5a and Eq. 3, $-ln\theta$ at different time could be calculated out. In addition, the slope of the fitted line in Fig. S5b was the time constant τ_s (281.01). Therefore, *hA* equaled to 4.48 mW/°C according to Eq. S2 and η was 38.5% based on Eq. S1.



Fig. S6 *In vitro* DOX release profiles of D/PNS and D/PNA hydrogels. (a) Without and (b) with FBS adsorbed on the DOX-loaded hydrogel (n=3). Note: ** P<0.01, with significant difference.



Fig. S7 Body weight of mice versus time.



Fig. S8 *In vivo* anti-tumor effect. (a) Tumour volumes change of D/PNS compared with D/PNA versus time. (b) Tumour volumes change of D-PDA/PNS compared with D-PDA/PNA *versus* time and (c) the corresponding photographs of the peeled tumours after intratumoral injection for 14 days. (d) Fluorescence

images of tumour tissue slice stained by Tunel. **P<0.01, *P<0.05.

References

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- 2 Y. L. Liu, K. L. Ai, J. H. Liu, M. Deng, Y. Y. He and L. H. Lu, Adv. Mater., 2013, 25, 1353–1359.