Supplementary Materials

Selection of healthy sperm based on positive rheotaxis using a microfluidic device

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1. Supplementary Videos

Video S1 (A, B & C): Videos represent the sperm track used to analyze various velocities from stock, no-flow (control), and with-flow group.

Video S2 (A, B & C): Videos illustrating the extent of difficulty faced by sperm cells while entering channel "b" at $2 \mu L/min$, $1 \mu L/min$ and $0.5 \mu L/min$ respectively.

Video S3 (A): Video representing 0.5 $\mu L/min$ is an optimal rate where the sperm cells were seen actively swimming against the flow in channel "b".

Video S3 (B): Video representing at 10.5 $\mu L/min$ induced high force in channel "b", due to which the sperm cells were unable to enter the channel "b" thereby avoiding contamination.

Video S4: Video showing sperm cells facing hindrance due to a high flow rate because of reduced width in channel "a".

Video S5: Videos illustrating no-flow conditions inside the chip after semen loading.

2. Supplementary Table

Supplementary Table 1: Comparison of the data obtained from the existing microfluidic sperm sorting chips in terms of motility, sperm DNA fragmentation (SDF), morphology analysis and recovery rate, along with their limitations.

			Morpholog	Recovery	
Devices/Studies	Motility	SDF	y analysis	rate	Limitations
		2.6±1.04 %			
With-flow (from	99.47±	(84%	61.56	1.38 ±	
this paper)	0.62%	improvement)	±1.93%	0.97%	
No-flow		3.9±0.33 %			Dead and immotile
(control) (from		(74%	44.65±		sperm cells in the
this paper)	81±04%	improvement)	2.41%	1.46 ± 1%	collected sample
					Inconvenient sample
	100%				collection with flow
1			NA	NA	on and off process.
					Sorted sperm sample
2	NA	NA	NA	NA	was not collected
	99.46				
3	(±0.92)	$6\pm0.45\%$	48%	28%	
					Sorted sperm sample
4	NA	NA	NA	NA	was not collected
					Sorted sperm sample
5	NA	NA	NA	NA	was not collected
					1) Sorted sperm
					sample was not
					collected
					for a brief time frame
				1.94 ±	
6	100%	NA	NA	0.32%	
					Non-motile and dead
	82.9			18.26	cells in the collected
7	±15.06%	NA	NA	±10.31%	sample

					Sorted sperm sample
8	NA	NA	NA	NA	was not collected
					1) Flow turned off
					and then reversed to
					direct the cells
	The				towards collecting
	standard				chamber.
	deviation				2) Sample is
	between				collected using
	inlet and				CryoTip
	collection				3) Only 5 sperm cells
	chamber				are trapped at one
9	is ±7%	NA	NA	NA	time
					1) Require multiple
					equipments for the
					device function.
					2) Non-motile sperm
					cells in the collected
					sample
10	32.58%	NA	NA	NA	
					Sorted sperm sample
11	82.24%	NA	NA	NA	was not collected
					Sorted sperm sample
12	NA	NA	NA	NA	was not collected

					The collected sample
					contained some non-
13	$\begin{array}{c} 70.9\pm4.5\\\%\end{array}$	NA	$77.5 \pm 6.4\%$	NA	viable cells
					Sorted sperm sample
14	90%	NA	NA	NA	was not collected
					Low motility or dead
					sperm cells in the
15	93%	NA	NA	NA	outlet.
					1) Use of resistive
					pulse measurement is
					is necessary for the
					small aperture
					2) The aperture gets
	Motility				clogged due to debris
16	index 148, 15 & 0	NA	NA	NA	from the reservoir
					Preprocessing of the
					semen sample is
					required using 20
17					μm pore size filter
					before loading onto
	95.4 ± 3 %	$0.8\pm1.9~\%$	NA	$3.6\pm4\%$	the chip.
18					Complicated chip
		2 (0/			assembly
	<90%	3-070	~56%		Compliants 1 strin
				80%	Complicated chip
				improveme	assembly
19	NA	NA	NA	nt	
					Lose some good- quality sperm cells.
20	95.7%	NA	NA	NA	-1
	93.6±1.6				The collected sample
21	% viability	1.63±0.79	NA	NA	viable cells

3. Microfluidic chip image



Fig. S1: The 3D image of the microfluidic chip designed in COMSOL

4. Morphology assessment images



Fig. S2 (A): Brightfield images of the sperm cells (from stock) obtained with 40X objective. The sperm cells encircled with black are morphologically normal, and others are morphologically abnormal with principal piece coiled, pyriform head, tapered head, small tail or bent neck.



Fig. S2 (B): 40X objective brightfield images of the sperm cells isolated from the collection chamber of the chip with the no-flow (control) condition. The sperm cells encircled with black are morphologically normal, and others are morphologically abnormal with principal piece coiled, pyriform head, tapered head, small tail or bent neck.



Fig. S2 (C): 40X objective brightfield images of the sperm cells isolated from the collection chamber of the chip with-flow $(0.5 \ \mu l/min$ rate) conditions. The sperm cells encircled with black are morphologically normal, and others are morphologically abnormal with principal piece coiled, pyriform head, tapered head, small tail or bent neck.

5. DNA fragmentation assessment images



Fig. S3 (A): Brightfield images of the sperm cells (from stock) obtained with 40X objective. Sperm cells showing big and medium halo have non-fragmented DNA. Sperm cells showing no halo have fragmented DNA.



Fig. S3 (B): 40X objective brightfield images of the sperm cells isolated from the collection chamber of the chip with no-flow (control) condition. Sperm cells showing big and medium halo have non-fragmented DNA. Sperm cells showing no halo have fragmented DNA.



Fig. S3 (C): 40X objective brightfield images of the sperm cells isolated from the collection chamber of the with-flow $(0.5 \ \mu l/min)$ chip settings. Sperm cells showing big and medium halo have non-fragmented DNA. Sperm cells showing no halo have fragmented DNA.

6. Isolation efficiency plot



Fig. S4: Isolation efficiency comparison between the different flow rates to examine the optimal flow rate for sperm cell selection on the microfluidic chip.

7. COMSOL results



Fig. S5 (A): Slice log velocity magnitude (a.u.) of the collection sample inlet and waste collection chambers. (B): the log velocity profile (slice & volume) simulation of the microfluidic chip representing the inside view of channel "b" showing the velocity is higher in the center and lower against the walls. (C): volume log shear stress profile (a.u.) of the microfluidic chip. (D): volume log shear stress profile of the channel "b" showing shear stress is higher against the walls and lower in the center. In reality, the outlet of channel "b" is connected to the inlet chamber of the chip.

Computational results:

The slice log velocity profile of the microfluidic chip in COMSOL demonstrated that chambers have different velocity sketches. As the volume of the chambers is larger, the velocity of the fluid inside the chambers is very low. However, the velocity at the end and beginning of the channels is higher (**Fig. S5 A**). The log volume and slice velocity profile of channel b (inside view) showed higher velocity in the center than in the walls (**Fig. S5 B**). The results of the volume log shear stress profile of the microfluidic chip revealed high shear stress in the channels and low in the chambers (**Fig. S5 C**). The volume log shear stress profile of channel b (inside view) showed high shear stress against the walls of channel "b" and low in the center (**Fig. S5 D**).

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