## **Supporting Information**

## A PDA-DTC/Cu-MnO<sub>2</sub> Nanoplatform for MR Imaging and Multi-Therapy of Triple-Negative Breast Cancer

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## **Experimental Section**

**Materials:** Dopamine hydrochloride was purchased from sigma. Copper (II) chloride dihydrate (CuCl<sub>2</sub>·2H<sub>2</sub>O), diethyldithiocarbamate (DTC), 5,5'-Dithiobis-(2-nitrobenzoic acid) (DTNB), methylene blue (MB) and Rhodamine (RhB) were purchased from Aladdin. Fetal bovine serium (FBS), phosphate-buffered saline (PBS), Dulbecco's modified Eagle medium (DMEM), penicillin streptomycin (PS), Cell counting Kit-8 (CCK-8) and trypsin were ordered from KeyGEN BioTECH. The used antibodies were purchased from Servicebio. Unless otherwise noted, all chemicals were used without further purification. MDA-MB-231 human breast cancer cells were cultured from cells originally purchased from Chinese Academy of Sciences Cell Library. Female BALB/c nude mice were purchased from Slac Experimental Animal Centre (Shanghai, China). All experiments in vivo were conducted in compliance with the guidelines for the Care and Use of Laboratory Animals of Tongji University Experimental Animal Center and the ethical approval number was TJBB00721102.

**Characterizations:** TEM images were obtained with a TEOL JEM-2100 transmission electron microscope. Zeta-potential measurements were conducted on a Malvern Zetasizer Nano ZS instrument. Confocal fluorescence imaging was performed on a laser confocal scanning microscope (Leica TCS SP5). 808 nm NIR lasers (Changchun Laser) were used to carry out the PTT study. The camera (DALI TECHNOLOGY) was utilized to monitor the photothermal conversion.

**Synthesis of PDA-DTC/Cu-MnO<sub>2</sub>:** PDA NPs were synthesized by a reported method.<sup>1</sup> Typically, 50 mg of dopamine hydrochloride was dissolved in 100 mL Tris-HCl buffer (10mM, pH=10.5). 20 mg DTC was added to the as-synthesized PDA colloid formed after 5 h of polymerization. After 20 h incubation at room temperature, the DTC- loaded PDA NPs were washed with water for several times to remove the unloaded DTC. 20 mg CuCl<sub>2</sub> was added in 20 mL of a DTC-loaded PDA NPs dispersion (1 mg/mL) under sonication, after that, the mixture solution was kept for further 2 h under drastic agitation. Thereafter, PDA-DTC-Cu NPs were collected by centrifugation and washed with water for three times. 12.5 mL of KMnO<sub>4</sub> (0.2 mg/mL) was dropwise added into 5 mL of PDA-DTC/Cu suspension (1 mg/mL) under sonication. And then, after stirring for 5 min, the PDA-DTC/Cu-MnO<sub>2</sub> was obtained by centrifugation. S, Cu and Mn elements were quantified by ICP-OES.

According to reported method,<sup>2, 3</sup> RhB labeled PDA-DTC/Cu-MnO<sub>2</sub> was obtained for cellular uptake and biodistribution studies in vitro and in vivo. In brief, 1 mL PDA-DTC/Cu-MnO<sub>2</sub> solution (2 mg/mL) and 1 mg RhB were stirred overnight. Then, the precipitate was collected by centrifugation (10000 rpm, 10 min), and washed with water to remove the excess dye. The release process of RhB was monitored using UV-vis absorbance measurements. In the presence of GSH (10 mM), the release of GSH percent sharply increased to 44% within 4 h and reached 83% at 24 h (Figure S7), which could be attributed to the biodegradation of MnO<sub>2</sub> by reacting with GSH.<sup>4</sup>

**DTC release profiles from PDA-DTC/Cu-MnO<sub>2</sub>:** Briefly, 2 mg lyophilized NPs were put in a centrifuge tube and redispersed in 2 mL phosphate buffer solution (PBS, pH 7.4, containing 0.1% w/v Tween 80, with or without 10 mM H<sub>2</sub>O<sub>2</sub>). The tube was put into a shaker and vibrated at 200 rpm at 37 °C. At designated time intervals, the tube was taken out and centrifuged at 10000 rpm for 5 min. Then, the supernatant was transferred into a test tube and dealt with aqua regia for ICP analysis. The pellet was resuspended in 2 mL fresh PBS solution and put back into the shaker for subsequent measurement. The cumulative release of DTC from NPs was plotted against time.

•OH generation by  $Mn^{2+}$ -mediated Fenton-like reaction: In vitro •OH generation measurement was carried out using methylene blue as an indicator.<sup>5</sup> 25 mM NaCO<sub>3</sub>/5% CO<sub>2</sub> buffer solution containing 10 µg/mL MB, 8 mM H<sub>2</sub>O<sub>2</sub>, and 0.5 mM MnCl<sub>2</sub> was allowed to incubate at 37 °C for 30 min. The •OH-induced MB degradation was measured by the absorbance change at 665 nm.

Scavenging effect of GSH on ·OH: 25 mM NaCO<sub>3</sub>/5% CO<sub>2</sub> buffer solution containing 10  $\mu$ g/mL MB, 8 mM H<sub>2</sub>O<sub>2</sub>, 10 mM GSH and 0.5 mM MnCl<sub>2</sub> or PDA-DTC/Cu-MnO<sub>2</sub> (0.5 mM by Mn) was allowed to incubate at 37 °C for 30 min. The ·OH-induced MB degradation was measured by the absorbance change at 665 nm.

**GSH depletion measurements:** 5,5'-Dithiobis (2-nitrobenzoic acid) (DTNB) was used to detect GSH consumption of PDA-DTC/Cu-MnO<sub>2</sub>.<sup>6</sup> 1 mg PDA-DTC/Cu-MnO<sub>2</sub> was dispersed in 10 mL of GSH solution (1 mM) at room temperature. After determined time (10 min, 1 h, 2 h, 3 h), the supernatant was collected. Then, DTNB solution was added into supernatant, and the mixture contained for another 10 min before UV-vis measurement. PBS and pure PDA were used as the control.

In vitro photothermal performance: In vitro photothermal performance of PDA-DTC/Cu-MnO<sub>2</sub> was investigated by measuring the temperature changes of its suspensions with the concentrations ranged from 0 to 400  $\mu$ g/mL upon 808 nm laser illumination for 5 min. The changed temperature was recorded and imaged simultaneously with an infrared thermal imaging camera.

**Cell lines:** MDA-MB-231 human breast cancer cells were cultured in DMEM supplemented with 10% FBS and 1% PS solution at 37 °C in an incubator containing 5% carbon dioxide.

**Cytotoxicity assessment:** MDA-MB-231 Cells were seeded into 96-well plates at a density of  $7 \times 10^3$  cells with 100 µL of DMEM per well. After incubation for 24 h, the cells were treated by different concentrations of PDA-DTC/Cu-MnO<sub>2</sub> (0, 2.5, 5, 10, 20 µg/mL) for 24 h. For PTT groups, MDA-MB-231 cells were irradiated under 808 nm laser for 5 min.

**Detection of intracellular GSH:** For in vitro GSH detection, MDA-MB -231 cells were seeded into culture plates and treated with (a) PBS as a control; (b) PDA; (c) PDA-DTC/Cu; (d) PDA-DTC-MnO<sub>2</sub> and (e) PDA-DTC/Cu-MnO<sub>2</sub> for 6 h, respectively. The intracellular GSH content was confirmed by GSH assay kits (Beyotime) according to the manufacturer's instructions.

**Detection of insoluble fraction NPL4:** According to the reported method,<sup>7</sup> immobilization of endogenous NPL4 was detected by western blot. Briefly, for in vitro insoluble fraction detection, MDA-MB -231 cells were seeded into culture plates at a density of  $5 \times 10^6$  cells per dish and treated with (a) PBS as a control; (b) PDA; (c) PDA-MnO<sub>2</sub>; (d) DTC/Cu and (e) PDA-DTC/Cu-MnO<sub>2</sub> for 4 h, respectively. Cells were washed with cold PBS, and lysis buffer (50 mM HEPES pH 7.4, 150 mM NaCl, 2 mM MgCl<sub>2</sub>, 10% glycerol,

0.5% Triton X-100, protease inhibitor cocktail by Servicebio) was added, and the plate was agitated gently for 10 min at 4 °C. Then, cells were scraped into tubes and insoluble fraction was extracted. Protein concentration was determined by the bicinchoninic acid (BCA) method. Protein of different groups were added into the sodium dodecyl sulfate (SDS)-polyacrylamide gels, and transferred to polyvinylidene fluoride (PVDF) membrane. The PVDF membrane was proved with anti-NPL4 (1:1,000; Abcam, ab224435), followed by HRP-conjugated secondary antibody. The protein bands of different groups were detected by the ECL kit.

**Cellular uptake measured by confocal microscopy:** To investigate the cellular internalization of PDA-DTC-MnO<sub>2</sub>, MDA-MB-231 cells ( $1 \times 10^5$  cells per well) were cultured in confocal dishes with DMEM for 24 h. For the confocal imaging, after incubating for 24 h, the cells were treated with RhB labelled PDA-DTC-MnO<sub>2</sub> (10, 20, 40 µg/mL) for another 6 h. The cells were then washed three times with ice-cold PBS and visualized immediately by using a confocal microscope with a 63 × oil-immersion objective lens.

In vivo photothermal/fluorescence/MR imaging: All experiments in vivo were conducted in compliance with the guidelines of the Laboratory Animal Center of Tongji University (Shanghai, China). Tumor xenograft model was established by breast fat pad orthotopic transplantation on the BALB/c nude mice (5-6 weeks old, female, ~20g).  $5 \times 10^5$  MDA-MB- 231 cells were injected into the right mammary fat pad for each mouse. After tumor volume reached 200-300 mm<sup>3</sup>, the fluorescent imaging was performed by NightOWL LB 983 IN VIVO imaging system. Mice injected with RhB or PDA-DTC/Cu-MnO<sub>2</sub>-RhB were observed at 1 h, 3 h, 6 h and 24 h, respectively. Finally, all mice were sacrificed to excise main organs (heart, lung, liver, spleen and kidney) and the tumors for further observation.

For in vivo photothermal effect evaluation, tumor-bearing mice were administrated with 100  $\mu$ L of 5 mg/mL PDA-DTC/Cu-MnO<sub>2</sub> suspension and PBS respectively, and then irradiated with 808 nm NIR laser at the power density of 1 W/cm<sup>2</sup> for 10 min at 24 h post intravenous injection. The tumor temperatures of mice were also recorded with the IR camera thermographic system.

T1 relaxivity of PDA-DTC/Cu-MnO<sub>2</sub> suspension with different concentration was assessed via 1.5 T medical superconducting MR T1-weighted MRI system (Bruker, USA). Before scanning, concentration of Mn<sup>2+</sup> was determined by ICP-OES. In vivo T1-weighted MR imaging dynamic evaluations was performed by a 3.0 T clinical MRI scanner (GE 750plus 3.0 T system, USA). The images of tumor-bearing mice were collected at 3 h and 6 h post intravenous injection of PDA-DTC/Cu-MnO<sub>2</sub> and Mn<sup>2+</sup> (concentration of Mn<sup>2+</sup>: 0.5 mM) with a rat coil (50 × 41 × 26 cm). The parameters of MRI scanner are as follows: field of view (FOV) = 90 × 60 mm<sup>2</sup>; matrix = 256 × 256; repetition time (TR) = 500 ms; echo time (TE) = 20 ms; slice thickness = 4 mm; slices = 15; spacing = 0.5 mm.

In vivo antitumor efficiency evaluation: When the average tumor volume approached 100 mm<sup>3</sup>, the tumor-bearing mice were randomly divided into 7 groups (n = 5): PBS, PDA-MnO<sub>2</sub>, DTC/Cu, PDA + 808 nm laser, PDA-DTC/Cu, PDA-DTC/Cu-MnO<sub>2</sub>, PDA-DTC/Cu-MnO<sub>2</sub> + 808 nm laser. Intravenous injection of PDA-DTC/Cu-MnO<sub>2</sub> suspension was conducted at a 3-day interval. The tumor sites were illuminated with 808 nm laser post injection for 24 h (1 W/cm<sup>2</sup>, 10 min). Tumor sizes and mice body weight were recorded every 2 days. Tumor weight was measured after all mice were sacrificed at day 14. Tumor volume was calculated using the following formula:

## Tumor volume = $0.5 \times \text{length} \times \text{width}^2$

Statistical analysis: One-way single factorial of variance (ANOVA) was performed for all data analysis and values were presented as means  $\pm$  standard deviation. P < 0.05 (\*), P < 0.01 (\*\*) and P < 0.001(\*\*\*) mean significant difference. All the data was analysed by SPSS 20.0.



**Figure S1.** The energy variation of DTC and PDA before combination and after combination. The DFT calculation was carried out by Gaussian 09 with D3-b3lyp/6-31g\* (PCM) method.



Figure S2. (a) Hydrodynamic diameters and (b) PDI of nanoparticles. (c) TEM-elemental mapping of PDA-DTC/Cu-MnO<sub>2</sub>.



Figure S3. (a) XPS spectrum of PDA- DTC/Cu-MnO<sub>2</sub>. (b) The XPS high-resolution scans of Mn 2p peaks.

Mn	Cu	S
32.5 ppm	11.2 ppm	10.4 ppm

Table S1. Mn, Cu and S elements were quantified by ICP-OES.



**Figure S4.** The infrared temperature (IRT) images of PDA-DTC/Cu-MnO<sub>2</sub> NPs with different concentration under 808 nm laser irradiation.



**Figure S5.** (a) Temperature variation of PDA-DTC/Cu-MnO<sub>2</sub> dispersion (400  $\mu$ g/mL) with 808 nm laser on and off for five cycles. The absorption spectra of pure MnO<sub>2</sub> (b) and PDA-DTC/Cu-MnO<sub>2</sub> (c) treated with different concentrations of GSH. The absorbance (d) and photographs (e) of MB treated with Mn<sup>2+</sup> with different concentrations of H<sub>2</sub>O<sub>2</sub>. (f) The MB degradation by Mn<sup>2+</sup>-based Fenton-like reaction in the presence of GSH (10 mM).



Figure S6. TEM of the degradation of PDA-DTC/Cu-MnO<sub>2</sub> at different time in Simulated Body Fluid (SBF) with H<sub>2</sub>O<sub>2</sub>.



Figure S7. (a) Vis spectra of RhB at various concentrations. (b) Calibration curve of RhB at 553 nm. (c) The release of RhB

from the PDA-DTC/Cu-MnO<sub>2</sub>-RhB in the presence of GSH.



**Figure S8.** (a) Relative protein level of NPL4 after different nanoparticles treatment. (b) Histopathological examination of tumor tissues by H&E staining and apoptosis-related protein caspase-3 expression by IHC staining.



Figure S9. H&E staining of main organs isolated from nude mice after different treatments on day 14. Scale bar = 100 µm.

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