

Supporting information

Strontium vanadate-supported graphitic carbon nitride nanocomposite for simultaneous voltammetric determination of acetaminophen and levofloxacin in complex biological samples

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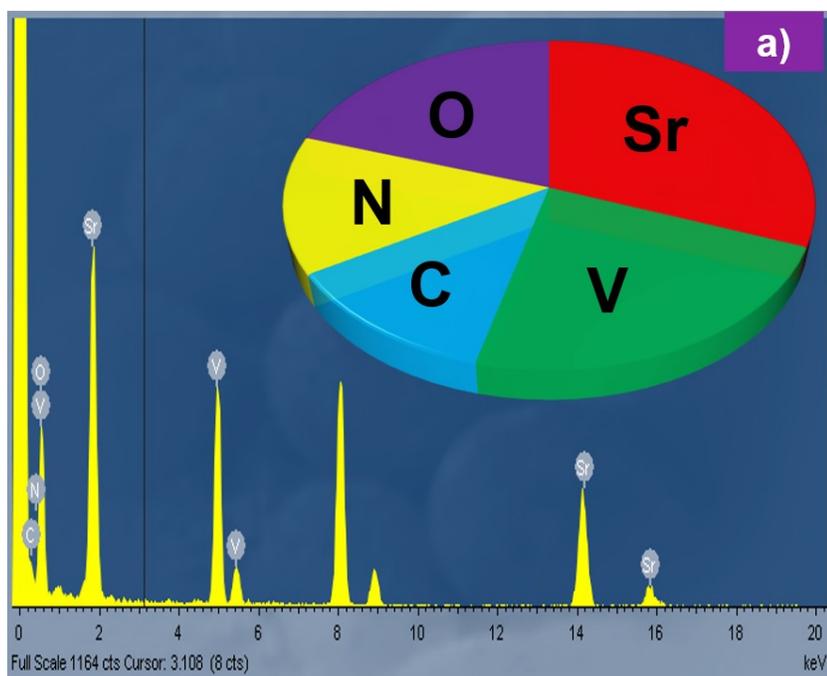


Fig S1. Fig S1. EDAX elemental analysis spectrum of SrV/GCN nanocomposite sample showing the peaks of Sr, V, O, C, and N respectively.

Table S1. Comparison of the EIS parameters of the electrodes.

Materials	R_s (Ω)	C_{dl} (nF)	R_{ct} (Ω)	Z_w (DW)
Bare GCE	40.4	339	328	294
SrV/GCE	36	344	266	248
GCN/GCE	37.9	386	129	316
SrV/GCN/GCE	37.4	450	83	250

S1. Optimization of SrV/GCN/GCE

To optimize the loading amount, the electrochemical activity was studied by varying the amount of SrV/GCN nanocomposite on the GCE surface from 1 to 12 mg/mL. The maximum current response was observed when the GC-electrode was modified with 6 mg of SrV/GCN (**Fig. S2 a**). Moreover, the concentration of SrV/GCN dispersion solution used to deposit over GCE was also optimized by varying the suspension volume from 1 to 10 μ L. The modified GC electrode with a concentration of 6 μ L SrV/GCN suspension exhibited a higher electrochemical response in comparison with the other studied concentrations (**Fig.**

S2 b). Therefore, the 6 μL (6.0 mg/mL) of SrV/GCN suspension was used for electrochemical detection studies.

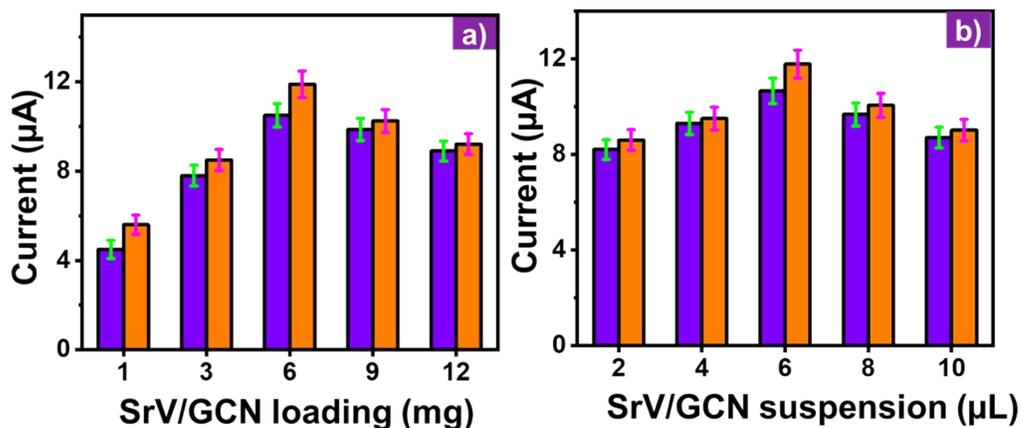


Fig S2. Bar chart diagram showing the electrooxidation peak current response of **a)** varying the amount of SrV/GCN (mg) deposited over GCE, **b)** The amount of SrV/GCN solution (6 μL) utilized to drop-cast onto GCE surface to fabricate SrV/GCN/GCE.

S2. Optimization of electrochemical sensing performance of SrV/GCN in different electrode surface and buffer solutions.

The sensing performance of the SrV/GCN nanocomposite was systematically optimized in two different buffer electrolyte solutions and supporting SrV/GCN over GCE and screen-printed carbon electrode (SPCE) working electrodes. As shown in **Fig S3a**, the CV profiles of the 100 μM of ACAMP and 100 μM of LEV at SrV/GCN/GCE recorded in phosphate buffer solution (PBS, 0.1 M), and acetate buffer solution (ABS, 0.1 M) at a scan rate of 50 mVs^{-1} . The SrV/GCN/GCE exhibited a well-defined redox peak with higher oxidation peak current response along with low ΔE as noticed in 0.1 M PBS in comparison with the ABS electrolyte solution, suggesting the SrV/GCN/GCE exhibit efficient electrocatalytic activity toward detection of ACAMP and LEV in 0.1 M PBS (**Fig S3a**). In addition, the sensing response of the SrV/GCN was also studied by modifying SrV/GCN over different electrode surfaces such as GCE and screen-printed carbon electrode (SPCE) and CV curves were recorded in 0.1 M PBS (pH=7.0) at a scan rate of 50 mV s^{-1} (**Fig S3 b**). Therefore, the GCE was utilized to modify the as-prepared SrV/GCN nanocomposite and implemented for electrochemical sensing.

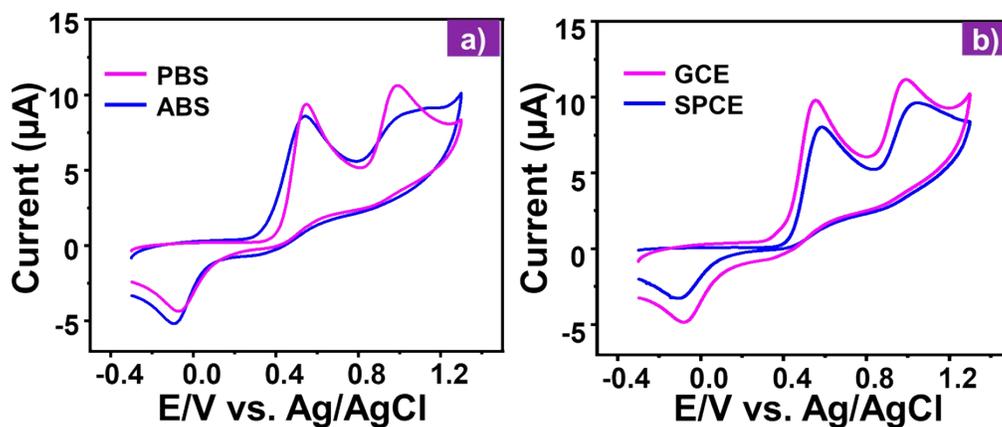


Fig S3. CV plots of **a)** SrV/GCN/GCE in the presence of 0.1 M of phosphate buffer solution (PBS) and acetate buffer solution (ABS) at scan rate 50 mVs^{-1} with $100 \mu\text{M}$ addition of ACAMP and LEV. **b)** SrV/GCN modified over GCE and SPCE in the presence of 0.1 M of PBS at 50 mVs^{-1} of scan rate with $100 \mu\text{M}$ addition of ACAMP and LEV, respectively.

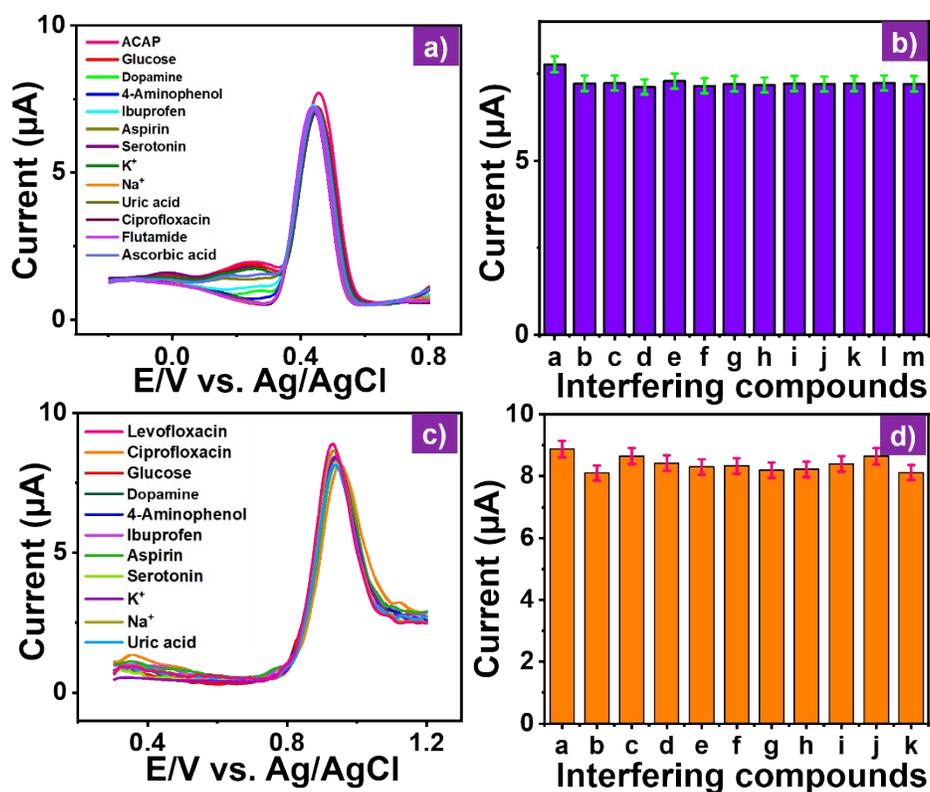


Fig S4. Selectivity performance of the SrV/GCN/GCE in the presence of various interference compounds. a, c) DPV curves of the 100 μ M ACAMP and LEV in the presence of various interference compounds at SrV/GCN/GCE in 0.1M PBS. b, d) corresponding bar diagram of ACAMP and LEV against various interference compounds.

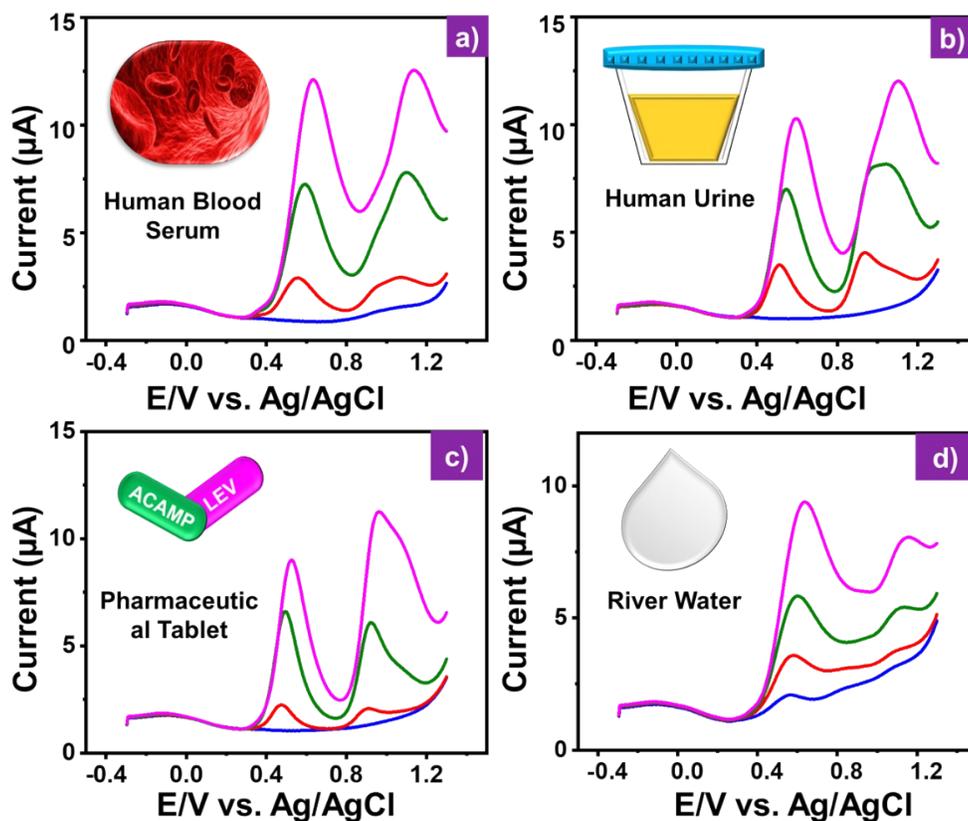


Fig S5. DPV response curves of SrV/GCN/GCE obtained in the presence of ACAMP and LEV in 0.1 M PBS containing a) human blood serum, b) human urine, c) commercial pharmaceutical tablet, and d) river water.

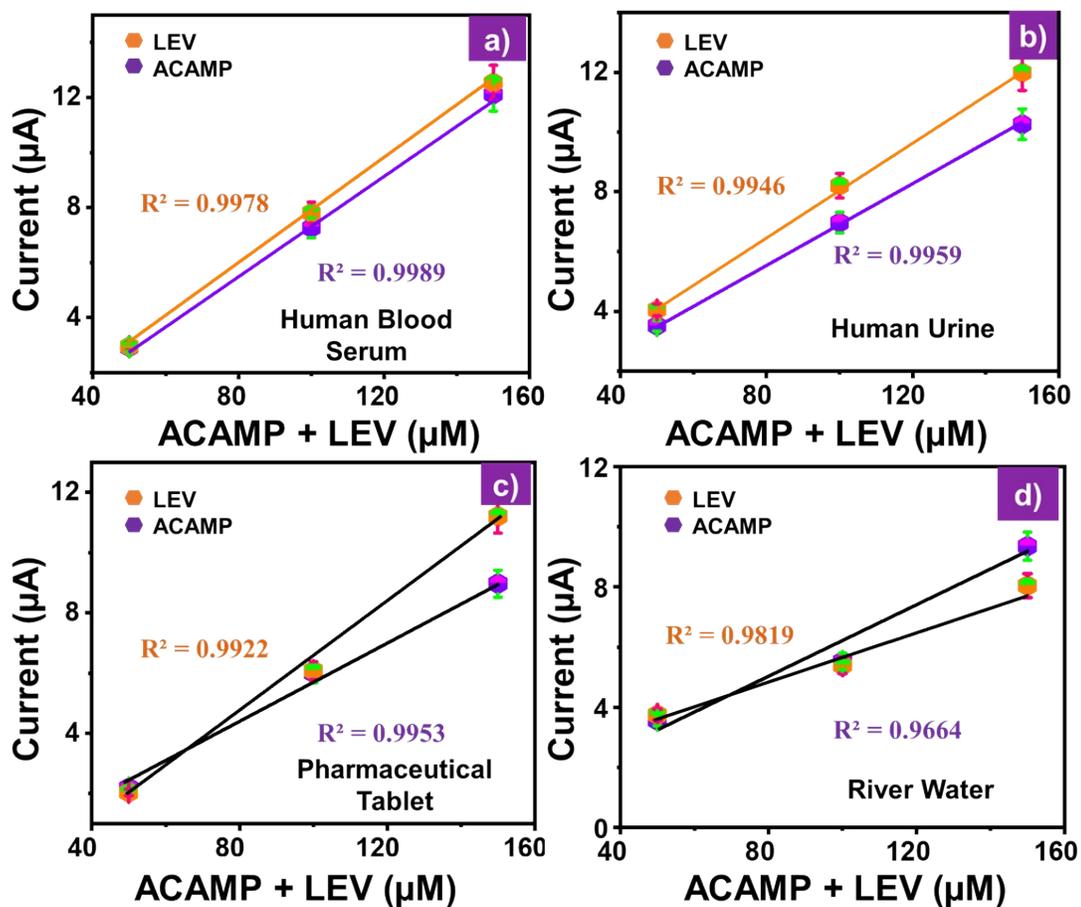


Fig S6. Linearity plot of current response vs. concentration of ACAMP and LEV at SrV/GCN/GCE in **a)** human blood serum, **b)** human urine, **c)** commercial pharmaceutical tablet, and **d)** river water.