

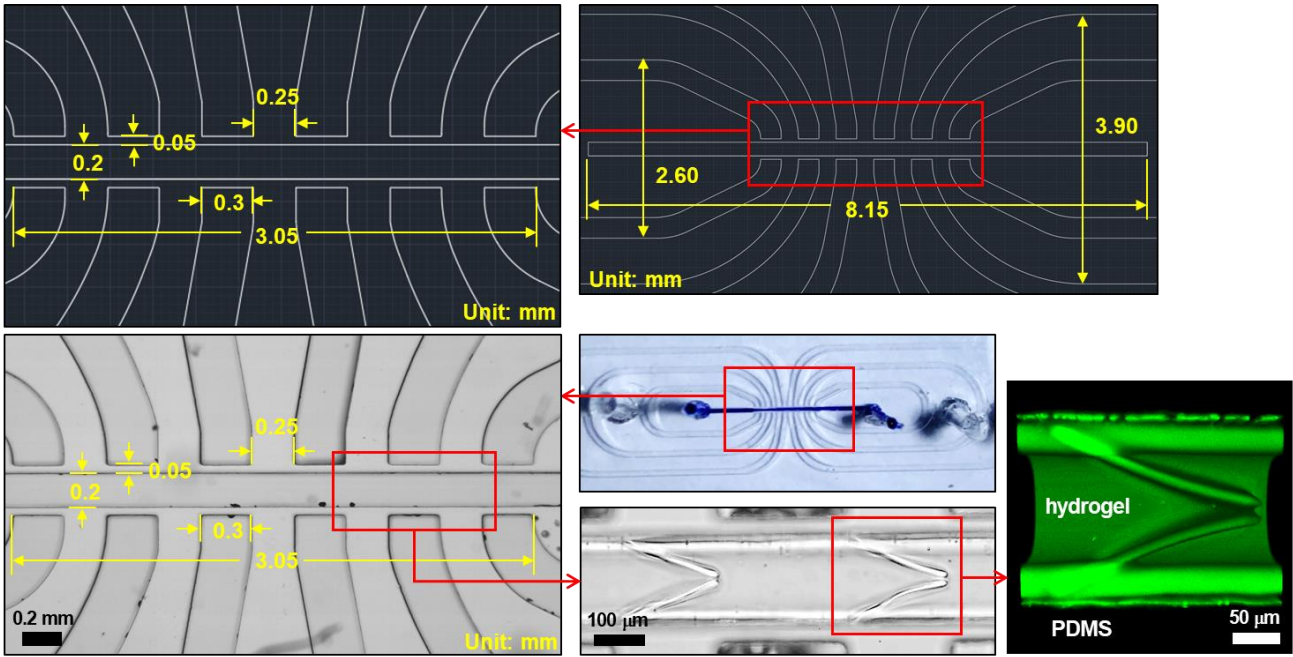
Electronic Supplementary Information (ESI) for

## **Microfluidic valvular chip and numerical lymphatic vessel model for study of lymph transport characteristics**

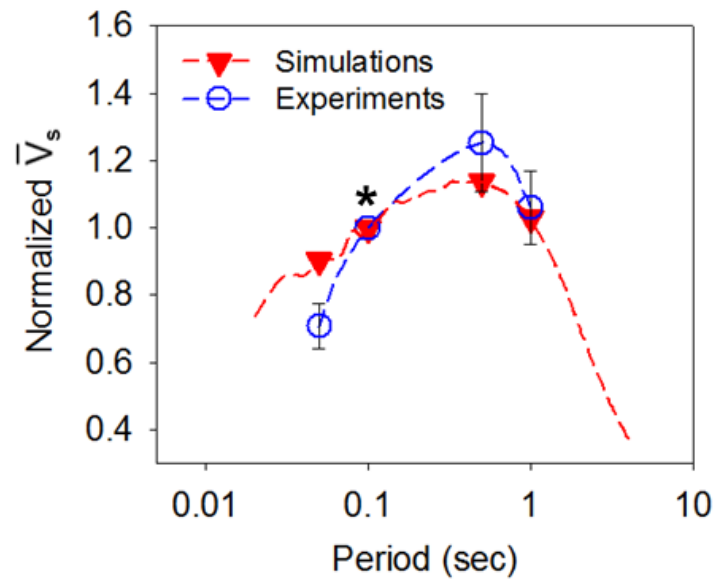
Jaemin In, Jihye Ryu, Hyeonji Yu, Dongwon Kang, Taeyoung Kim, and Jungwook Kim\*

Department of Chemical and Biomolecular Engineering, Sogang University, Seoul, South Korea.

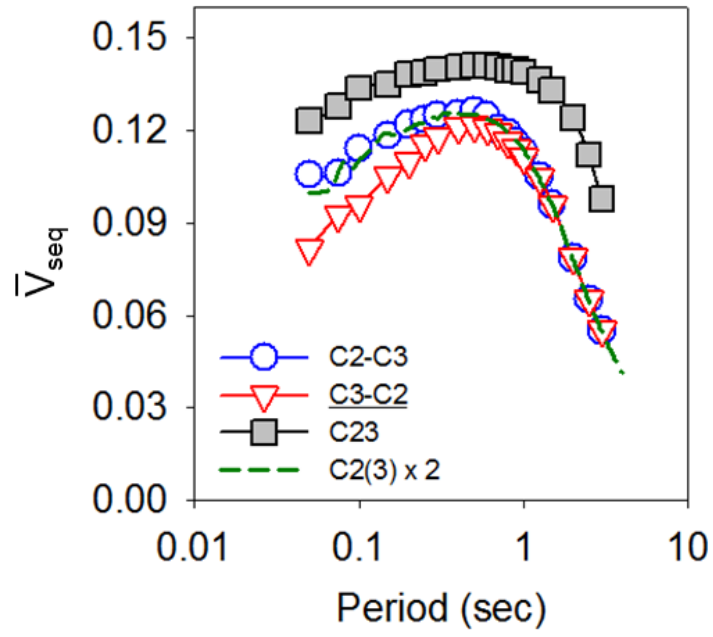
Correspondence to: [jungwkim@sogang.ac.kr](mailto:jungwkim@sogang.ac.kr)



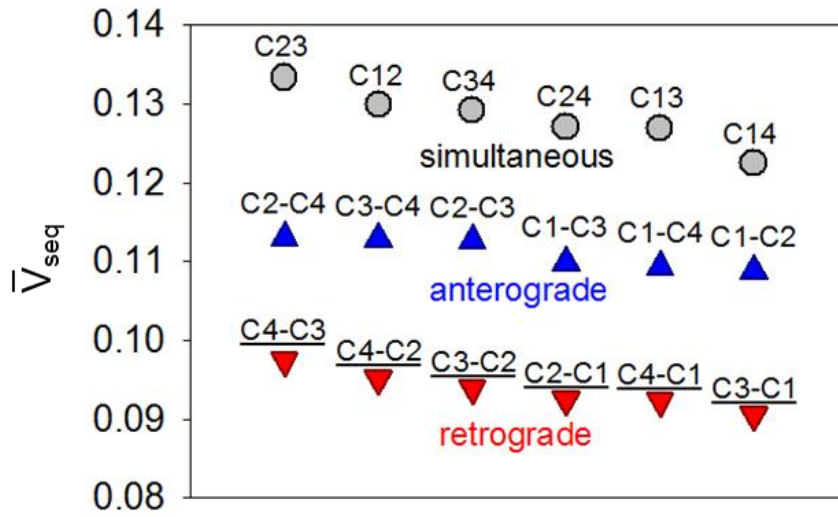
**Figure S1.** Details of the geometry and dimensions of the PDMS microfluidic device and hydrogel luminal structure with the bicuspid valve leaflets. Top images correspond to the CAD design.



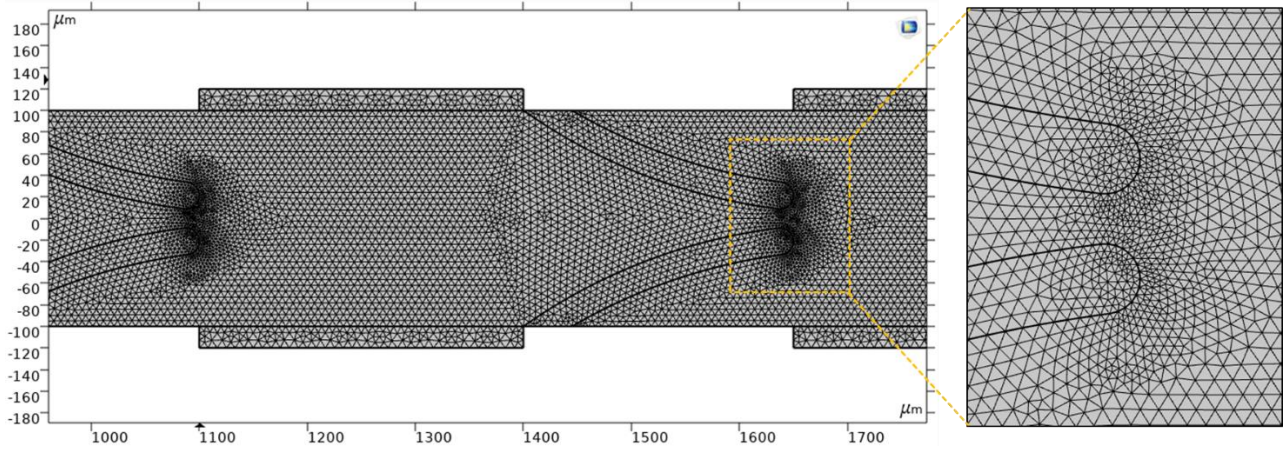
**Figure S2.** The simulation results for the dependency of  $\bar{V}_s$  on the compression period was reproduced experimentally using the microfluidic valvular chip. An asterisk indicates the data points used for normalization of experimental and numerical results.



**Figure S3.** The dependency of  $\bar{V}_{seq}$  on the compression period for varying sequences. The optimum periods corresponding to the maximum  $\bar{V}_{seq}$  are 0.6, 0.5, 0.4, and 0.5 s for C23, C2-C3, C2(3), and C3-C2, respectively. The phase delay is 1.0, and the contraction fraction is 6 %.



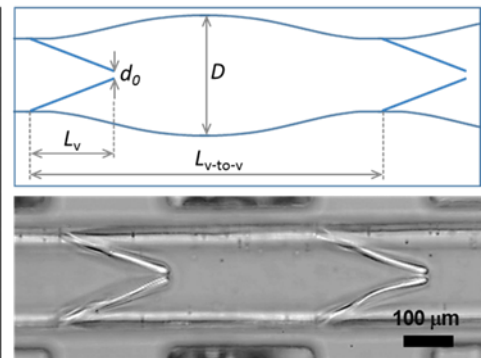
**Figure S4.**  $\bar{V}_{seq}$  calculated for various sequences of compressing two chambers, which are indicated above each data point. The contraction fraction is 6 %, and the period is 0.1 sec. The phase delay for the anterograde and retrograde sequences is 1.0.



**Figure S5.** The numerical lymphatic vessel model constructed in the Fluid-Structure Interaction interface using COMSOL. 56,498 elements were used to mesh the model, where the fluid mesh was refined in regions between the valve leaflets (right).

**Table S1.** Comparisons in geometry and mechanical properties between the rat mesenteric lymphatic vessel and our systems.

		Rat mesenteric lymphatic vessel	Our systems		Ref.
			Microfluidic chip	Numerical model	
Geometry	$L_{v-to-v}$	400-500 $\mu\text{m}$	550 $\mu\text{m}$	550 $\mu\text{m}$	6
	$L_v$	120-140 $\mu\text{m}$	210 $\mu\text{m}$	250 $\mu\text{m}$	6
	$D$	100-300 $\mu\text{m}$	125 $\mu\text{m}$	200 $\mu\text{m}$	6
	$d_0$	2 $\mu\text{m}^*$	5-10 $\mu\text{m}$	20 $\mu\text{m}$	6
Valve leaflet	Young's modulus	58 kPa <sup>#</sup>	40 kPa	Soft: 40 kPa Rigid: 4 MPa	11
	Poisson's ratio	0.45 <sup>*</sup>	Not measured	0.49	11
Lymph	Viscosity	1.08-1.36 mPa·sec	1/3-3 mPa·sec	0.89 mPa·sec (water)	2
	Density	1.005-1.016 g/ml	1.00 g/ml (water)	1.00 g/ml (water)	2
Active pumping	Contraction fraction	5-50 %	0-20 %	0-22 %	18
	Period	~0.5-3 sec	0.05-1 sec	0.01-5 sec	19-21
	Phase delay	0-0.5 <sup>*</sup>	0-2	0-3	3, 8
	Sequence	Antero- and retro-grade, simultaneous	Antero- and retro-grade, simultaneous	Antero- and retro-grade, simultaneous	3
	Pressure difference	$\pm 20 \text{ mmH}_2\text{O}^*$	Not applied	$\pm 8 \text{ mmH}_2\text{O}$	7



\* These are values used in the existing analytical or numerical studies based on the in vivo or ex vivo measurements.

# Shear modulus of 20 kPa was converted to Young's modulus assuming isotropic and homogeneous materials with Poisson's ratio of 0.45.

**Table S2.** Sequences of compression of four adjacent chambers classified based on  $N_s$  and  $N_r$ . Number in parentheses indicates total number of sequences in each classification.

$N_r \backslash N_s$	1	2	3	4
0	(1) 1-2-3-4	(3) 12-3-4 1-23-4 1-2-34	(2) 1-234 123-4	(1) 1234
1	(11) 1-2-4-3 1-3-2-4 1-3-4-2 1-4-2-3 2-1-3-4 2-3-1-4 2-3-4-1 2-4-1-3 3-1-2-4 3-4-1-2 4-1-2-3	(22) 12-4-3 1-24-3 13-2-4 1-3-24 13-4-2 1-34-2 14-2-3 1-4-23 2-13-4 2-1-34 23-1-4 2-3-14 23-4-1 2-34-1 24-1-3 2-4-13 3-12-4 3-1-24 34-1-2 3-4-12 4-12-3 4-1-23	(6) 124-3 134-2 2-134 234-1 3-124 4-123	Not available
2	(11) 1-4-3-2 2-1-4-3 2-4-3-1 3-1-4-2 3-2-1-4 3-2-4-1 3-4-2-1 4-1-3-2 4-2-1-3 4-2-3-1 4-3-1-2	(11) 14-3-2 2-14-3 24-3-1 3-14-2 3-2-14 3-24-1 34-2-1 4-13-2 4-2-13 4-23-1 4-3-12	Not available	Not available
3	(1) 4-3-2-1	Not available	Not available	Not available