#### Electronic Supplementary Material (ESI) for Nanoscale Horizons. Historian Supplementary Material (ESI) for Nanoscale Horizons. This journal is © The Royal Society of Chemistry 2022 This journal is © The Royal Society of Chemistry 2021

1 **Electronic Supporting Information** 2 3 A tumor microenvironment dual responsive contrast agent for contrary contrastmagnetic resonance imaging and specific chemotherapy of tumors 4 5 Yudie Lu,<sup>a+</sup> Jie Feng,<sup>b+</sup> Zhiyu Liang,<sup>b</sup> Xuanyi Lu,<sup>a</sup> Shuai Guo,<sup>a</sup> Lin Huang,<sup>a</sup> Wei Xiong,<sup>b</sup> Sijin 6 7 Chen,<sup>b</sup> Huimin Zhou,<sup>c</sup> Xuehua Ma,<sup>d</sup> Yikai Xu,<sup>b</sup> Xiaozhong Qiu,<sup>c</sup> Aiguo Wu,<sup>d</sup> Xiaoyuan Chen,<sup>e,f,g</sup> Zheyu Shen<sup>a,b,c</sup>\* 8 9 <sup>a</sup> School of Biomedical Engineering, Southern Medical University, 1023 Shatai South Road, 10 Guangzhou, Guangdong 510515, China 11 <sup>b</sup> Medical Imaging Center, Nanfang Hospital, Southern Medical University, 1023 Shatai South 12 Road, Guangzhou, Guangdong 510515, China 13 <sup>c</sup> Guangdong Provincial Key Laboratory of Construction and Detection in Tissue Engineering, 14 School of Basic Medical Sciences, Southern Medical University, 1023 Shatai South Road, 15 Guangzhou, Guangdong 510515, China 16 <sup>d</sup> Cixi Institute of Biomedical Engineering, CAS Key Laboratory of Magnetic Materials and 17 Devices, Ningbo Institute of Materials Technology and Engineering, Chinese Academy of 18 Sciences, 1219 Zhongguan West Road, Ningbo, Zhejiang 315201, China 19 <sup>e</sup> Departments of Diagnostic Radiology, Surgery, Chemical and Biomolecular Engineering, and 20 Biomedical Engineering, Yong Loo Lin School of Medicine and Faculty of Engineering, 21 National University of Singapore, Singapore, 119074, Singapore 22 <sup>f</sup> Clinical Imaging Research Centre, Centre for Translational Medicine, Yong Loo Lin School 23 of Medicine, National University of Singapore, Singapore 117599, Singapore 24 <sup>g</sup> Nanomedicine Translational Research Program, NUS Center for Nanomedicine, Yong Loo 25 Lin School of Medicine, National University of Singapore, Singapore 117597, Singapore 26 27 **Corresponding Author** 

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## 29

# 30 Author Contributions

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### 32 Experimental Methods

Synthesis of FeGdNP Nanoparticles: 160 mL of PAA (Mw = 1800) solution (4.0 mg/mL) 33 was first purged with nitrogen ( $\geq 1.0$  h) to remove oxygen. The polymer solution was then 34 35 heated to reflux (100 °C). After that, 3.2 mL of mixture of iron precursors (500 mM FeCl<sub>3</sub> plus 250 mM FeSO<sub>4</sub>) was quickly injected into the heated polymer solution, followed by addition 36 37 of 48 mL of ammonia solution (28 %). The reaction was kept at 100 °C under magnetic stirring. After 30 min, 3.2 mL of Gd(NO<sub>3</sub>)<sub>3</sub> (500 mM) and 24 mL of ammonia solution (28 %) were 38 added into the reaction system. The reaction was continued for 60 min under magnetic stirring 39 at 100 °C to obtain the FeGdNP. Finally, the solutions were cooled down to room temperature. 40 The obtained FeGdNP nanoparticles were purified by membrane dialysis (Mw cut-off 6-8 kDa) 41 42 against Milli-Q water for 5 days with a daily change of the water. The purified FeGdNP was 43 concentrated by centrifugal ultrafiltration (Millipore, molecular size cutoff of 10 kDa). The Fe and Gd concentrations of the solutions were measured by inductively coupled plasma optical 44 emission spectrometry (ICP-OES). 45

Synthesis of mPEG-FBA: Methoxy poly(ethylene glycol) (mPEG, Mw = 2000) was dissolved 46 in dichloromethane with a concentration of 50 mg/mL. To 160 mL of the mPEG solution (8.0 47 g, 4.0 mmol), 4-Formylbenzoic acid (FBA, 1.8 g, 12 mmol), dimethylformamide (DMF, 20 48 mL), Dicyclohexylcarbodiimide (DCC, 2.48 g, 12 mmol), and 4-(Dimethylamino)pyridine 49 (DMAP, 732 mg, 6.0 mmol) were added. The solution was stirred at room temperature for 24 50 h, and then filtered thrice to discard the precipitate dicyclohexylurea (DCU). After that, 51 52 dichloromethane of the filtrate was evaporated via N2 bubbling, and the product was dispersed in MilliQ water (50 mL). The resulting mPEG-FBA was collected by freeze-drying. The 53 obtained white powder of mPEG-FBA was stored at room temperature for further use. 54

*Influence of Solvents on the Reaction between FBA and CA*: 0.3 mL of cystamine
dihydrochloride (CA) in methanol (20 mg/mL) was mixed with 37.1 μL of triethylamine (TEA).
After that, 0.80 mL of FBA (5.0 mg/mL in DMF, DMSO, THF, or ethanol) was added into the

58 above-mentioned mixture. After vortexing for 30 s, the mixtures were kept shaking in an 59 incubator at 37 °C for 72 h. The obtained auto-fluorescent FBA-CA1-4 were measured by a 60 fluorescence spectrophotometer.

Synthesis of mPEG-FBA-CA: 3.0 mL of cystamine dihydrochloride (CA) in methanol (20
mg/mL) and 371 μL of triethylamine (TEA) were respectively added into 8.0 mL of methanol.
28.4 mL of mPEG-FBA in THF (20 mg/mL) were then mixed with the above-mentioned
solution. After vortexing for 30 s, the mixture was kept shaking in an incubator at 45 °C for 72
h. The obtained mPEG-FBA-CA was stored for further use.

Synthesis of FeGdNP@mPEG: 0.5 mL of FeGdNP nanoparticles in pure water (Gd = 22.2 66 mM, Fe = 45.3 mM) was added into 3.624, 4.062, 4.281, 4.390, and 4.445 mL of DMF 67 respectively. After that, 0.876, 0.438, 0.219, 0.110 and 0.055 mL of the above-obtained mPEG-68 69 FBA-CA (15.94 mg/mL) (mPEG-FBA-CA/Gd mass ratio = 8.0, 4.0, 2.0, 1.0 and 0.5) were respectively charged into the above-mentioned solutions with following addition of 10 µL of 70 N-(3-Dimethylaminopropyl)-N'-ethylcarbodiimide (EDC). Although the reaction between -71 COOH and -NH<sub>2</sub> is faster in mild acid solutions than in neutral or alkaline solutions, EDC (but 72 not EDC.HCl) was used in this study because the benzoic imine in mPEG-FBA-CA is an acid 73 labile linker. The total volume of the five reaction solutions was all 5.0 mL. The obtained 74 75 FeGdNP@mPEG1-5 nanoparticles (in organic solvents, i.e., DMF, THF, and methanol) were then obtained after reaction under magnetic stirring at room temperature for 16 h. 76

*Synthesis of self-assembled FeGdNP@mPEG (SA-FeGdNP@mPEG)*: Milli-Q water was dropwise added into the above obtained FeGdNP@mPEG1-5 nanoparticles (volume ratio of water to nanoparticle solution = 9 : 1) under magnetic stirring. After that, the nanoparticle solutions were subjected to 3 days of dialysis (Mw cut-off 12-14 kDa) against Milli-Q water to remove the organic solvents (i.e., DMF, THF, and methanol) and un-conjugated organic molecules (i.e., mPEG-FBA, CA, TEA, mPEG-FBA-CA, and (mPEG-FBA)2-CA). After the 83 dialysis, the FeGdNP@mPEG1-5 nanoparticles were purified and self-assembled forming SA84 FeGdNP@mPEG1-5.

Synthesis of FeGdNP-DOX@mPEG and SA-FeGdNP-DOX@mPEG: 0.5 mL of FeGdNP 85 86 nanoparticles in pure water (Gd = 22.2 mM, Fe = 45.3 mM) was added into 1.269, 2.666, 3.364,3.713, and 3.887 mL of DMF, respectively. After that, 0.438 mL of the mPEG-FBA-CA (15.94 87 mg/mL) (mPEG-FBA-CA/Gd mass ratio = 4.0) were charged into the above-mentioned 88 solutions with following addition of EDC (10 µL). Five batches of FeGdNP@mPEG2 89 nanoparticles were then obtained after reaction under magnetic stirring at room temperature for 90 16 h. 1.0 mg/mL of DOX in DMF ranging from 2.793 to 0.175 mL (DOX/Gd mass ratio = 1.6, 91 92 0.8, 0.4, 0.2, or 0.1) was then added into the obtained FeGdNP@mPEG2 nanoparticles. The 93 total volume of the five reaction solutions was all 5.0 mL. After 4.0 h of reaction under magnetic 94 stirring at room temperature, FeGdNP-DOX1-5@mPEG2 nanoparticles in organic solvents were obtained. The SA-FeGdNP-DOX1-5@mPEG2 were finally prepared utilizing similar 95 procedures as the above-mentioned SA-FeGdNP@mPEG. 96

97 *Disassembling of the SA-FeGdNP-DOX2@mPEG2 nanoparticles*: 1.0 mL of SA-FeGdNP-98 DOX2@mPEG2 nanoparticles ( $C_{Gd} = 2.0 \text{ mM}$ ,  $C_{DOX} = 139 \text{ µg/mL}$ ) were mixed with 1.0 mL 99 of PBS (pH 7.4 or pH 6.8) with or without GSH (20 mM). The solutions were kept in a shaking 100 incubator at 37 °C for 24 h, and then taken for TEM observation and MRI measurement.

101 *Release Behavior of DOX from SA-FeGdNP-DOX2@mPEG2*: The release behavior of DOX from SA-FeGdNP-DOX2@mPEG2 nanoparticles at pH 7.4 without GSH or at pH 6.8 with 10 102 103 mM of GSH was determined by a fluorescence spectrophotometer. Typically, 1.0 mL of SA-FeGdNP-DOX2@mPEG2 nanoparticles ( $C_{Gd} = 2.0 \text{ mM}$ ,  $C_{DOX} = 139 \mu \text{g/mL}$ ) were mixed with 104 1.0 mL of PBS (pH 7.4 or pH 6.8) with or without GSH (20 mM). The solutions were kept in a 105 106 shaking incubator at 37 °C. At predetermined time intervals, 0.2 mL of the solution was taken 107 and centrifuged at  $15,000 \times g$  for 20 min. The supernatants were then measured by a fluorescence spectrophotometer (Ex: 480 nm) and the fluorescence intensity at 593 nm was 108

109 converted into the DOX concentration using a calibration curve constructed with standard DOX 110 solutions. The DOX release behavior at different conditions was monitored *via* plot of the 111 cumulative released DOX content (*i.e.*, the mass percentage of the released DOX to the total 112 amount of DOX in the nanoparticles) as a function of incubation time.

113 *Cell culture*: U-87 MG (human glioblastoma cell line), and HepG2 (human hepatoma cell 114 line) cells were cultured in the DMEM medium supplemented with 10 wt% of fetal bovine 115 serum (FBS), 100 units/mL of penicillin and 100  $\mu$ g/mL of streptomycin. All of the cells were 116 incubated at 37 °C in a humidified atmosphere containing 5 % of CO<sub>2</sub>.

117 Cellular uptake by laser scanning confocal microscopy (LSCM): Uptake of the nanoparticles by U-87 MG, or HepG2 cells was studied using LSCM. Typically, 0.5 mL of U-87 MG, or 118 119 HepG2 cells in growth medium were seeded into each well of Falcon<sup>®</sup> Culture Slide (8 Well, Corning) at a density of 5.0×10<sup>5</sup> cells/mL and allowed to adhere at 37 °C for 24 h. The growth 120 121 medium was replaced with a fresh one (0.5 mL, without FBS) containing SA-FeGdNP-DOX2@mPEG2 nanoparticles ( $C_{Gd} = 140 \mu M$ ). Herein, before dispersing in DMEM medium 122 (without FBS), the SA-FeGdNP-DOX2@mPEG2 nanoparticles were incubated at 37 °C for 24 123 h at pH 7.4 without GSH, or at pH 6.8 with 10 mM of GSH. After further 2 h incubation, the 124 cells were washed twice with PBS. The cells were then fixed with aqueous buffered zinc 125 126 formalin fixative (Z-FIX) for 30 min, permeabilized with 0.1 % Triton X-100 for 5 min, blocked with 1.0 % BSA for 30 min and treated with the mixture of Phalloidin-FITC (0.5 µg/mL) and 127 Hoechst (5  $\mu$ g/mL) for 30 min at room temperature. A small drop volume (~ 20  $\mu$ L) of the 128 129 antifade mounting medium (Vectashield, H-1000) was added onto each cell specimen, which was then covered using cover slips. The cover slips were then fixed onto the slides by nail 130 131 polish. After that, the LSCM images of the samples were observed on a LSCM imaging system. 132 *Cell Viability Assay:* The cytotoxicity and therapeutic efficacy of the nanoparticles was assessed with U-87 MG, or HepG2 cells by using the MTT method. Typically, 100 µL of U-87 133 134 MG or HepG2 cells in complete DMEM medium were seeded into each well of a 96-well plate

at a concentration of  $5 \times 10^4$  cells/mL and allowed to adhere overnight. The growth medium was 135 replaced with a fresh one (without FBS) containing various concentrations of free DOX, SA-136 FeGdNP@mPEG2, or SA-FeGdNP-DOX2@mPEG2 nanoparticles. Herein, before dispersing 137 in DMEM medium (without FBS), the SA-FeGdNP@mPEG2, and SA-FeGdNP-138 DOX2@mPEG2 nanoparticles were incubated at 37 °C for 24 h at pH 7.4 without GSH, or at 139 pH 6.8 with 10 mM of GSH. After charging the fresh growth medium without FBS containing 140 nanoparticles or free DOX, the cells were incubated for 4 h at 37 °C. After that, the growth 141 medium containing nanoparticles or DOX was replaced with complete DMEM medium. After 142 further incubation for 44 h, 10 µL of MTT (5.0 mg/mL in PBS) was added to each well of the 143 144 96-well plate. After an additional 4.0 h of incubation, the growth medium was removed and the 145 resulted formazan crystals in each well were dissolved with 100 µL of dimethyl sulfoxide (DMSO). The absorbance was recorded at a wavelength of 570 nm using a multi-mode 146 microplate reader. 147

148 Tumor Model: All animal procedures were performed in accordance with the Guidelines for Care and Use of Laboratory Animals of Southern Medical University and approved by the 149 Animal Ethics Committee of Southern Medical University. The U-87 MG tumor-bearing nude 150 mice were prepared by inoculating U-87 MG cells (4  $\times$  10<sup>6</sup> cells in 100 µL PBS) into the right 151 152 shoulder of each mouse (female, 5 weeks) under anesthesia. The tumor size was measured via a caliper at predetermined times. The tumor volume was calculated through  $ab^{2}/2$ , where a and 153 b are respectively the length and width of a tumor. The relative tumor volume  $(V/V_0)$  was the 154 155 ratio of tumor volume after treatment (V) to that before treatment ( $V_0$ ).

156 *CC-MRI of tumors*: The U-87 MG tumor-bearing nude mice were anaesthetized by isoflurane 157 (1.0-2.0%) in oxygen, and placed in an animal-specific body coil for MRI data acquisition. 158 Mice were kept warm by circulating warm water (37 °C), and were placed in a stretched prone 159 position with a respiratory sensor during the experiments.  $T_1$ -weighted images were acquired at 160 pre-injection and post injection (intravenously) of commercial Dotarem<sup>®</sup> ( $C_{Gd} = 5.0 \text{ mg} / \text{kg}$ ), 161 or SA-FeGdNP-DOX2@mPEG2 nanoparticles ( $C_{Gd} = 5.0 \text{ mg} / \text{kg}$ ). Multi-slice multi-echo 162 sequence was employed to acquire images using parameters as follows: repetition time (TR) = 163 1000 ms, echo time (TE) = 30 ms, flip angle = 180°, matrix size = 256 × 256, field of view = 164 40 × 40 mm<sup>2</sup>, slices = 16, slice thickness = 1 mm. MR images were analyzed by measuring 165 signal intensity with the software Image J. The signal-to-noise ratio (SNR) and SNR ratio (*i.e.*, 166 signal enhancement) were calculated according to the following equations (1) and (2).

167 
$$SNR = SI_{mean} / SD_{noise}$$
 (1)

168  $\Delta$ SNR = (SNR<sub>post</sub> - SNR<sub>pre</sub>) / SNR<sub>pre</sub> × 100 % (2)

169 *High-performance chemotherapy*: When the tumor volume was around 150 mm<sup>3</sup>, 100  $\mu$ L of 170 saline, SA-FeGdNP@mPEG2, free DOX, SA-FeGdNP-DOX2@mPEG2 were injected 171 intravenously into the mice under anesthesia (n = 5/group). The DOX dosage was 5 mg/kg or 172 10 mg/kg. After injection, dimensions of the tumors and body weights of the mice were 173 monitored every other day.

174Statistical analysis: Statistical significance was determined by applying Student's *t*-test or175by a one-way ANOVA followed by Student-Newman-Keuls test using Sigma Stat version 3.5.176The significance level was fixed as P < 0.05.

Sample Nomenclature	FeGdNP <sup>a)</sup> (mL)	mPEG-FBA-CA <sup>b)</sup> (mL)	mPEG-FBA-CA/Gd Mass Ratio <sup>c)</sup>	EDC (µL)	DMF (mL)	Gd Recovery <sup>d)</sup> (%)
SA-FeGdNP@mPEG1	0.5	0.876	8.0	10	3.624	83
SA-FeGdNP@mPEG2	0.5	0.438	4.0	10	4.062	84
SA-FeGdNP@mPEG3	0.5	0.219	2.0	10	4.281	82
SA-FeGdNP@mPEG4	0.5	0.110	1.0	10	4.390	78
SA-FeGdNP@mPEG5	0.5	0.055	0.5	10	4.445	76

178 Table S1. Synthesis conditions and characterization results of SA-FeGdNP@mPEG.

179 <sup>a)</sup> The feeding FeGdNP was dispersed in pure water with 22.2 mM of  $C_{Gd}$  and 45.3 mM of  $C_{Fe}$ . 180 <sup>b)</sup> The concentration of feeding mPEG-FBA-CA is 15.94 mg/mL.

181 <sup>c)</sup> Calculated from the mass ratio of feeding mPEG-FBA-CA to Gd in FeGdNP.

182 <sup>d)</sup> Calculated from the molar ratio of Gd in SA-FeGdNP@mPEG to that in the feeding FeGdNP.

185 Table S2. Synthesis conditions and characterization results of SA-FeGdNP-DOX@mPEG.

Sample Nomenclature	FeGdNP <sup>a)</sup> (mL)	mPEG- FBA-CA <sup>b)</sup> (mL)	DOX/Gd Mass Ratio <sup>c)</sup>	DOX (mL)	EDC (µL)	DMF (mL)	DOX Loading Efficiency <sup>d)</sup> (%)	DOX Loading Content <sup>e)</sup> (%)	r <sub>1</sub> <sup>f)</sup> (mM <sup>-1</sup> s <sup>-1</sup> )	<i>r</i> ₂ <sup>f)</sup> (mM⁻¹ s⁻¹)	<b>r</b> <sub>2</sub> /r <sub>1</sub>
SA-FeGdNP- DOX1@mPEG2	0.5	0.438	1.6	2.793	10	1.269	28.8	21.4	-	-	-
SA-FeGdNP- DOX2@mPEG2	0.5	0.438	0.8	1.396	10	2.666	55.4	20.6	18.37±0.35	336.9±7.5	18.4±0.7
SA-FeGdNP- DOX3@mPEG2	0.5	0.438	0.4	0.698	10	3.364	71.2	13.2	18.82	303.3	16.1
SA-FeGdNP- DOX4@mPEG2	0.5	0.438	0.2	0.349	10	3.713	76.0	7.1	18.78	280.2	14.9
SA-FeGdNP- DOX5@mPEG2	0.5	0.438	0.1	0.175	10	3.887	76.5	3.6	20.06	258.8	12.9
FeGdNP	-	-	-		-	-	-		20.32	146.9	7.2

<sup>a)</sup> The feeding FeGdNP was dispersed in pure water with 22.2 mM of  $C_{Gd}$  and 45.3 mM of  $C_{Fe}$ .

187 <sup>b)</sup> The concentration of feeding mPEG-FBA-CA is 15.94 mg/mL.

188 <sup>c)</sup> Calculated from the mass ratio of feeding DOX to Gd in FeGdNP.

189 <sup>d)</sup> Calculated from the mass percentage of loaded DOX to the feeding DOX.

190 <sup>e)</sup> Calculated from the mass percentage of loaded DOX to the SA-FeGdNP-DOX@mPEG 191 nanoparticles.

<sup>192</sup> <sup>f)</sup> The  $r_1$  and  $r_2$  were measured on a MRI scanner system (7.0 T, Bruker, B-C 70/16 US) (mean

193 ± SD, n = 3).



196 Fig. S1. Schematic illustration for the synthesis of mPEG-FBA.





199 Fig. S2. Influence of formylbenzoic acid (FBA) solvents (DMF, DMSO, THF, and ethanol) on 200 the reaction between FBA and cystamine dihydrochloride (CA) in the presence of triethylamine 201 (TEA). CA solvent is methanol. Reaction temperature: 37 °C. Reaction time: 72 h. (a): Photo of the resulting FBA-CA1-4 solutions reacted in DMF, DMSO, THF, or ethanol. Yellow color 202 of FBA-CA3 solution indicates much higher recovery in THF than other solvents. (b, c): 203 204 Fluorescence spectra of the auto-fluorescent FBA-CA1-4. (b): Emission curves at the excitation 205 of 405 nm. (c): Excitation curves at the emission of 510 nm. The maximum excitation, and 206 emission of FBA-CA3 is respectively measured to be 412, and 492 nm.

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- 208





210 Fig. S3. The <sup>1</sup>H NMR spectrum of mPEG-FBA-CA.



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Fig. S4. (a): Molecular structures of the compounds. (b): FT-IR spectra of mPEG, FBA, and 213 214 mPEG-FBA. (c): FT-IR spectra of CA, mPEG-FBA-CA, and FeGdNP@mPEG2. FBA has a characteristic peak at 1690 cm<sup>-1</sup> (C=O stretching vibration in carboxyl group). mPEG has a 215 characteristic peak at 1470 cm<sup>-1</sup> (C-H stretching vibration in methylene). Both the characteristic 216 peak at 1700 cm<sup>-1</sup> (C=O stretching vibration in ester) and that at 1470 cm<sup>-1</sup> demonstrate the 217 successful synthesis of mPEG-FBA. In addition, CA has a characteristic peak at 3430 cm<sup>-1</sup> 218 219 (N-H stretching vibration in primary amine). Both the characteristic peak at 3430 cm<sup>-1</sup> and that 220 at 1650 cm<sup>-1</sup> (C=N stretching vibration) demonstrate the successful formation of mPEG-FBA-CA. The peaks at 1650 cm<sup>-1</sup> (C=N stretching vibration) and 3400 cm<sup>-1</sup> (O-H stretching vibration 221 222 in carboxyl group) indicate the conjugation of mPEG-FBA-CA on the surface of FeGdNP generating FeGdNP@mPEG2. 223



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226 Fig. S5. Fluorescence spectra and standard curve of SA-FeGdNP@mPEG2 nanoparticles. (a):

227 Fluorescence spectrum of SA-FeGdNP@mPEG2 (Em = 650 nm). (b): Fluorescence spectra of

228 SA-FeGdNP@mPEG2 (Ex = 425 nm) with various Gd concentrations from 3.63 to 116  $\mu$ M.

- 229 (c): Plot of fluorescence intensity at 646 nm (Ex = 425 nm) as a function of  $C_{\text{Gd}}$  ( $\mu$ M) or  $C_{\text{mPEG}}$ .
- 230  $_{FBA-CA}$  (µg/mL).



Fig. S6. Size distribution of SA-FeGdNP-DOX2-4@mPEG2 measured from the TEM images.
The average particle sizes were respectively measured to be 77.8, 71.3, and 66.6 for SAFeGdNP-DOX2-4@mPEG2.



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**Fig. S7.**  $T_1$  relaxation rate  $(1/T_1)$  (a) or  $T_2$  relaxation rate  $(1/T_2)$  (b) plotted as a function of  $C_{Gd}$ for SA-FeGdNP-DOX1-5@mPEG2. For  $T_1$  relaxation rates: TE = 10 ms, TR = 100 ~ 4000 ms. For  $T_2$  relaxation rates: TR = 2000 ms, TE = 10 ~160 ms. SA-FeGdNP-DOX2-1@mPEG2, SA-FeGdNP-DOX2-2@mPEG2, and SA-FeGdNP-DOX2-3@mPEG2 were synthesized from 3 different batches at same conditions. There is no linear relationship between  $1/T_2$  and  $C_{Gd}$  for SA-FeGdNP-DOX1@mPEG2 (R<sup>2</sup> = 0.932) because 1.6 of DOX/Gd mass ratio is too high resulting in unstable aggregates.



247 Fig. S8. Release behaviors of DOX from SA-FeGdNP-DOX2@mPEG2 nanoparticles at pH

248 7.4 without GSH or at pH 6.8 with 10 mM of GSH. \*\*\* P < 0.001.



Fig. S9. LSCM images of U-87 MG cells incubated with SA-FeGdNP-DOX2@mPEG2 251 252 nanoparticles. Before incubation with cells, the nanoparticles were incubated at 37 °C for 24 h 253 at pH 6.8 with 10 mM of GSH, or at pH 7.4 without GSH. The cells untreated with nanoparticles are used as the control. DOX is red. The cytoskeleton stained with phalloidin-FITC is green. 254 255 The nucleus stained with Hoechst 33258 is blue.



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Fig. S10. LSCM images of HepG2 cells incubated with SA-FeGdNP-DOX2@mPEG2 nanoparticles. Before incubation with cells, the nanoparticles were incubated at 37 °C for 24 h at pH 6.8 with 10 mM of GSH, or at pH 7.4 without GSH. The cells untreated with nanoparticles are used as the control. DOX is red. The cytoskeleton stained with phalloidin-FITC is green. The nucleus stained with Hoechst 33258 is blue.



Fig. S11. LSCM images of U-87 MG cells incubated with SA-FeGdNP-DOX2@mPEG2 nanoparticles. Before incubation with cells, the nanoparticles were incubated at 37 °C for 24 h at pH 6.8 with 10 mM of GSH. The nucleus stained with Hoechst 33258 is blue (a, d). The DOX is red (b, d). The endosome and lysosome stained with LysoTracker<sup>TM</sup> is green (c, d). The red signal overlaps with green and blue, which demonstrates that the nanoparticles were internalized into endosomes *via* endocytosis mechanism, and some of them escaped from the endosome and lysosome and entered into the nucleus.





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Fig. S13. Histological analyses (H&E staining) of main organs and tumors from the subcutaneous U-87 MG tumor-bearing nude mice at day 2 post-injection of saline, SA-FeGdNP@mPEG2 or SA-FeGdNP-DOX2@mPEG2 nanoparticle.