

## Supplementary Material

### **Spatially-extended 3D Magnetic DNA Nanodevice-Based Split-Type photoelectrochemical Strategy for Sensitive and Reliable MiRNA**

#### **Detection in Cancer Cells**

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## **Experimental section**

### **Chemicals**

Methylene blue (MB), Deoxynucleotide triphosphates (dNTPs) and all the HPLC-purified oligonucleotide sequences were obtained from Sangon Biotech Co., Ltd. (Shanghai, China). DNA oligonucleotide sequences were shown in **Table S1**. T4 DNA ligase, phi 29 DNA polymerase, rNTP Mix and RNase inhibitor were purchased from New England Biolabs, Ltd (Beijing, China). Streptavidin-magnetic nanobeads (streptavidin-MBs, the mean diameter is 300 nm) were purchased from Biomag Biotechnology Co., Ltd (Wuxi, China). All other reagents were of analytical grade. All aqueous solutions were prepared using ultra-pure water ( $\geq 18 \text{ M}\Omega \text{ cm}^{-1}$ ) and treated with DEPC.

### **Apparatus**

Agarose gel electrophoresis analysis was performed on an electrophoresis analyzer and gel imaging was accomplished on a Molecular Imager® GelDoc™ XR+ imaging system (Bio-Rad, USA). All photoelectrochemical tests were measured on ZAHNER-PP21 (Zana, Germany). The UV-vis absorption spectra were collected on a UH-4150 spectrophotometer (Hitachi, Japan). AFM were collected on Bruker Multimode 8 (USA). Isothermal titration calorimetry (ITC) experiments were carried out using a MicroCal ITC200 titration calorimeter (GE Healthcare, USA).

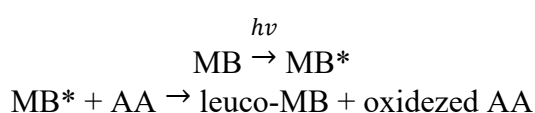
### **Preparation and of space-expanded 3D magnetic DNA nanodevice**

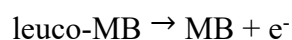
The first stage of space-expanded 3D magnetic DNA nanodevice involves the target recognition and RCA amplification reaction process, which was performed in a homogeneous solution as follows: target miR-21 and padlock probe were mixed in 1×T4 DNA ligase buffer (40 mM Tris-HCl, 10 mM MgCl<sub>2</sub>, 10 mM DTT, 0.5 mM ATP, pH 7.80). The mixture was heated to 90 °C for 5 min and then slowly cooled to room temperature, yielding circular DNA with a nick. Subsequently, the nicked

circular DNA was connected by incubation with T4 DNA ligase in 10×T4 DNA ligase buffer overnight ligation reaction followed by 65 °C for 10 min. Second, the RCA reaction occurred at 37 °C for 2 h with the addition of 10× phi 29 DNA polymerase buffer, phi 29 DNA polymerase and dNTP followed by 65 °C for 10 min. The mixture for the resulting DNA strands and three primers (biotin-P1, P2 and P3) were incubated in TAE/Mg<sup>2+</sup> buffer (20 mM Tris, 10 mM acetic acid, 1 mM EDTA and 6.25 mM magnesium acetate, pH 7.60) solution, which was heated to 90 °C for 5 min and then slowly cooled to room temperature, folding into predetermined high-order DNA scaffolds. Finally, streptavidin-modified MB was added to the above solution, and high-order DNA scaffolds were anchored to magnetic particles through avidin-biotin to form 3D magnetic DNA nanodevices.

### **Construction of Split-type “turn-off” PEC biosensor**

In order to obtain the negatively charged FTO electrode surface for PEC measurement, the processing involved was shown in Supplementary Material (part I). The as-mentioned magnetic DNA nanodevices were transferred the into 30 µL (1mg/ml) MB solution (containing 0.1 M Ascorbic Acid (AA) and 0.2 M Na<sub>2</sub>SO<sub>4</sub>, pH 7.80) and was incubated at 37 ° C for 2 h. The visible light source ( $\lambda=629$  nm) is used to 15 s (**Fig.S2**). After magnetically separated of the bound MB with the as-designed magnetic DNA nanodevice, the photocurrent signal for the rest of the MB solution was measured towards bare FTO electrode. The bare FTO electrodes with surface area 2.5 cm × 3 cm were ultrasonically cleaned for 1 h in 1 M NaOH, water/ethanol (1:1, V/V), acetone and ultra-pure water, followed by blown dry with nitrogen gas, respectively. Upon visible light illumination (**Fig. S2**), the MB can transform to leuco-MB, and the subsequent current generation occurs in the presence of strong reducing agents AA as illustrated below.





### **Agarose gel electrophoresis analysis**

For agarose gel electrophoresis analysis, the RCA amplification products and the resulting high-order folded DNA nanostructure were run on 2% agarose gel electrophoresis in 1×TAE buffer for 45 min with a constant voltage of 90 V at 0 ° C, followed by the EB staining and visualization in gel imaging system (Molecular Imager® GelDoc™ XR+)

### **Isothermal titration calorimetry**

All ITC experiments were conducted using MicroCal ITC200 titration calorimeter using protocols developed in our laboratory. For all ITC measurements, the reference power and stirring speed were set at 5  $\mu\text{cal}\cdot\text{s}^{-1}$  and 750 rpm, respectively. The calorimetric experiments were run at 310.15 K. The sample cell was filled with 4  $\mu\text{M}$  high-order DNA scaffolds solution. In each titration experiment, 20 injections of 2  $\mu\text{L}$  500  $\mu\text{M}$  MB solution (with an initial injection of 0.4  $\mu\text{L}$ ) were titrated into the sample cell. All the data were analyzed and plotted using Origin 7.0 software provided by the ITC200 calorimeter.

### **Cell lines and cell culture**

A human cervical cancer cell line (HeLa), a human lung cancer cell line (A549) and a hepatocellular carcinoma cell line (HepG2) were cultured in cell culture medium mixed with 10% FBS and 1% penicillin streptomycin. All cells were first incubated at 37 °C in a humidified atmosphere of 5%  $\text{CO}_2$ .

**Table S1. Sequences of oligonucleotides used in this study**

<b>Name</b>	<b>Sequence (5'-3')</b>
<b>Padlock</b>	<u>P-CTG ATA AGC TAT AAG ATG AAG ATA GCG CAC AAT GGT CGG</u> <u>ATT CTC AAC TCG TAT TCT CAA CTC GTA TTC TCA ACT CGT TCA</u> <u>ACA TCA GT</u>
<b>Short chain 1</b>	Biotin-CCC TGA CTC <u>ACA ATG GTC GGA TTC</u> CGT CTC TG
<b>Short chain 2</b>	CAG CCC TGT <u>AAG ATG AAG ATA GCG</u> TCT ATG CC
<b>Short chain 3</b>	<u>TCT CAA CTT CAA CTC GTA TTC TCA ACT</u> CGT AT
<b>miR-21</b>	<u>UAG CUU AUC AGA CUG AUG UUG A</u>
<b>Let-7a</b>	UGA GGU AGU AGG UUG UAU AGU U
<b>miR-141</b>	UAA CAC UGU CUG GUA AAG AUG G
<b>miR-155</b>	UUA AUG CUA AUC GUG AUA GGG GU

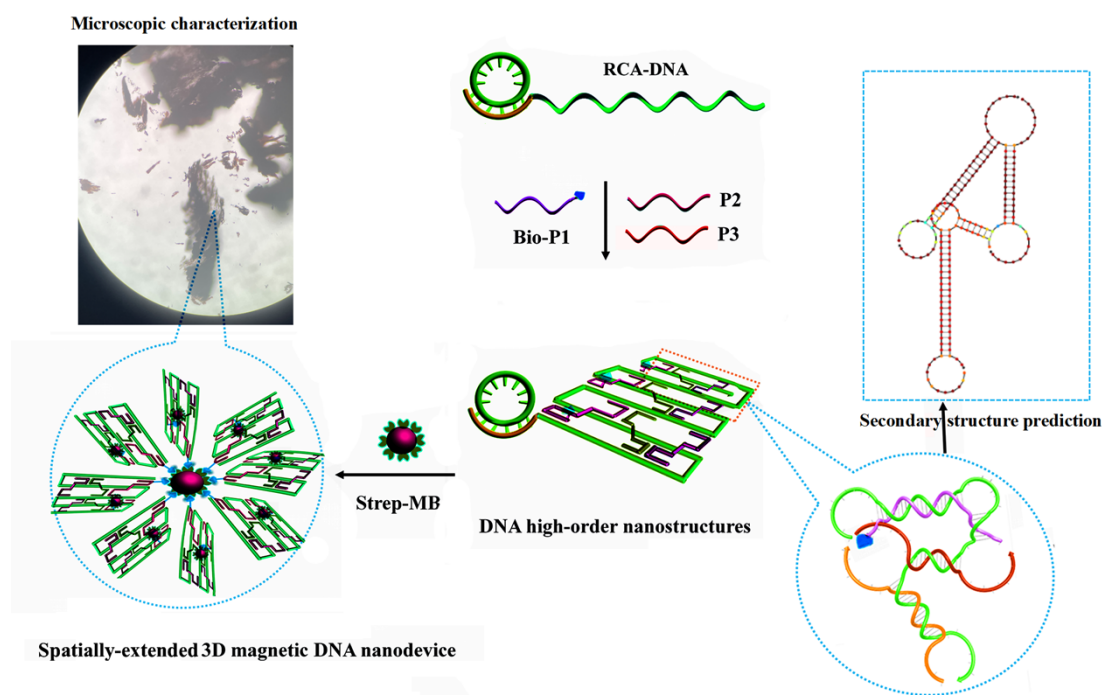
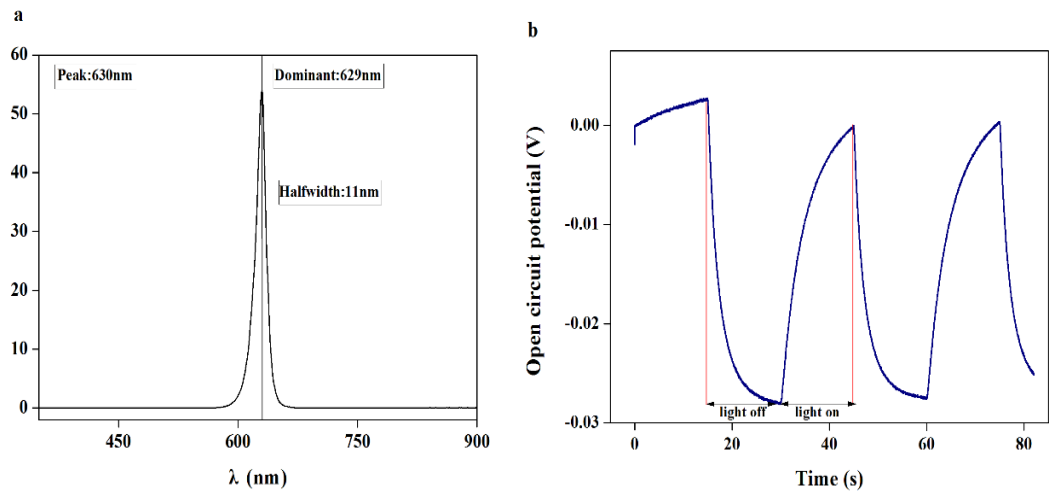
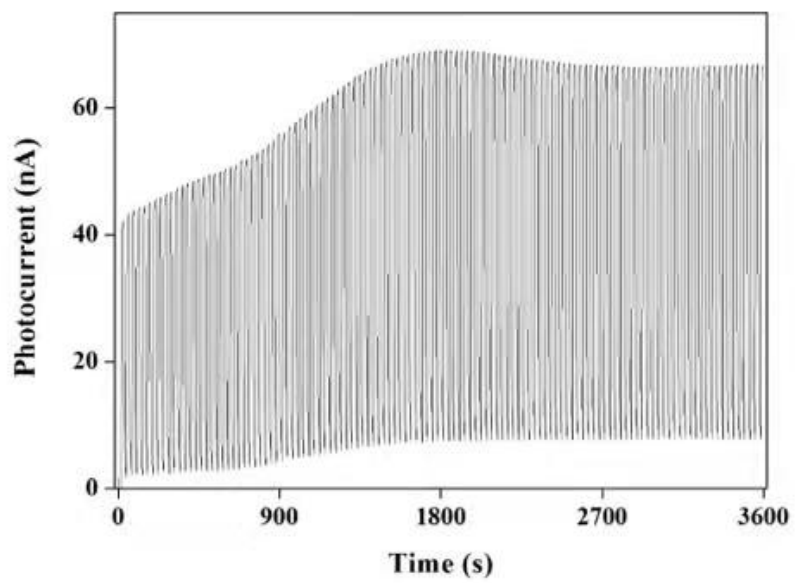


Fig. S1. The second structure of high folded DNA scaffolds unit and the microscopic characterization of the 3D magnetic DNA nanodevices



**Fig. S2.** The selection of light source wavelength (a) and switching time interval (b)



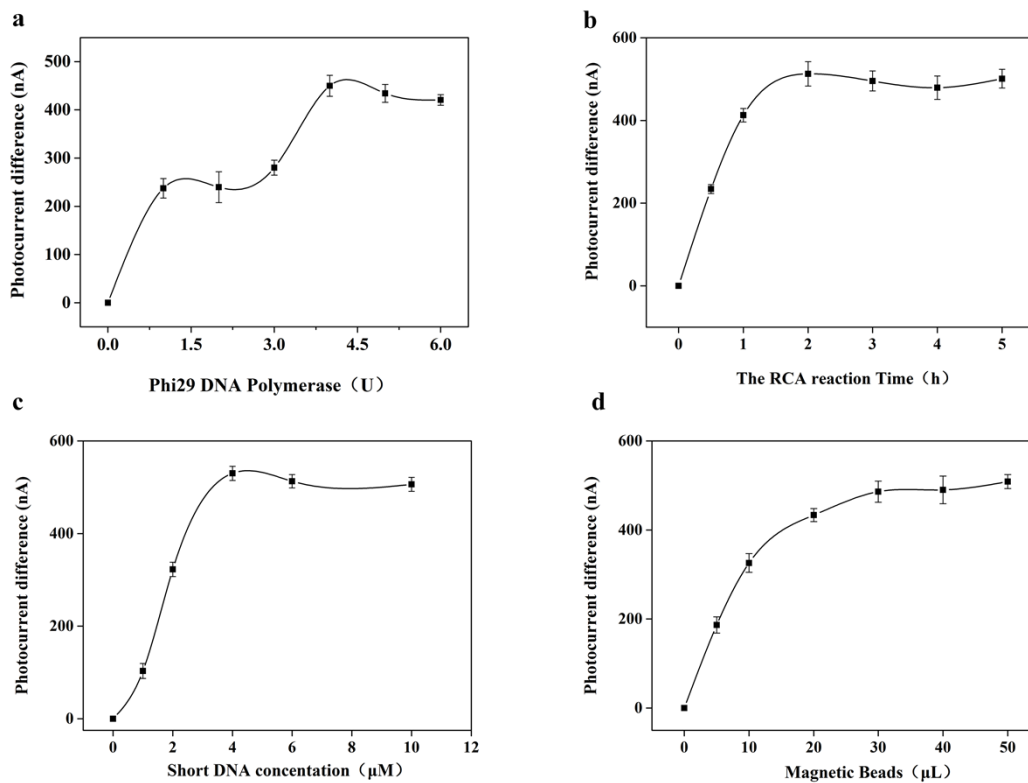


**Fig. S3.** The real-time monitoring of photoelectric response the coexistence system of MB and MB/high-order DNA scaffolds complex.

## Results and discussion

### Optimization of experimental conditions

To improve the operation performance of the as-proposed split-type PEC assay, the experimental conditions should be carefully optimized. First, both the padlock probe was hybridized with miR-21 and the resulting DNA-RNA duplex triggers the RCA polymerization was performed in homogeneous solution. The RCA reaction conditions including the amount of phi29 DNA polymerase, and the reaction time of RCA (**Fig. S4**) were optimized. The value of photocurrent change ( $\Delta I = I - I_0$ ) was adopted to appraise the performance of the PEC sensor, where  $I$  and  $I_0$  were photocurrents signal responses of this PEC sensor in the presence and absence of the target miR-21, respectively. As indicated in **Fig. S4A**, the photocurrent change ( $\Delta I$ ) increased with the increasing amount of phi29 DNA polymerase, and then increased to a maximum value at 4 U, indicating a saturated amplification. For the polymerization time of RCA (**Fig. S4B**), from 0.5 h to 5 h, the photocurrent change ( $\Delta I$ ) increases rapidly with the increase of polymerization time and reaches a plateau at 2 h. Therefore, the optimized phi29 DNA polymerase dosages of 4 U and the optimized polymerization time of 2 h were employed in the following experiments. Additionally, the amount of three short stable strands (biton-P1, P2, P3) plays an important role in formation of high-order DNA scaffolds. As shown in **Fig. S4C**, the concentration of 4  $\mu\text{M}$  biton-P1, P2, P3 was found to give the best PEC response, indicating that it was sufficient for forming well-defined DNA scaffolds. Finally, in order to full removal of the target miR-21-triggered MB/DNA scaffold complex from the free MB solution, the amount of streptavidin magnetic nanobeads (strep-MB) was carefully optimized. As indicated in **Fig. S4D**, the photocurrent change ( $\Delta I$ ) increased with the increasing amount of strep-MB, and then increased to a maximum value at 30  $\mu\text{L}$ , indicating a saturated probe load and being selected.



**Fig. S4.** Effect of the concentration of phi29 DNA polymerase (a), RCA time (b); the concentration of short DNA (c); and the concentration of magnetic beads (d) on the PEC response of sensing system.

**Table S2. Comparison of different methods for miR-21 detection**

<b>method</b>	<b>Linear range</b>	<b>Detection limit (fM)</b>	<b>ref</b>
Electrochemistry	10 fM - 5 nM	2.36	1
Electrochemistry	10 fM - 1.0 nM	10	2
Electrochemistry	2 fM - 1 nM	2	3
ECL	1pM - 10 nM	300	4
ECL	2.34 fM -100 pM	0.721	5
Fluorescence	0.01 nM - 200 nM	10 <sup>4</sup>	6
Fluorescence	0.2 nM - 20 nM	9.8*10 <sup>4</sup>	7
Fluorescence	100 fM - 50 pM	67.3	8
SERS	1.0 fM - 10 nM	0.34	9
SERS	10 fM - 100 nM	2.88	10
Photoelectrochemistry	1 fM - 1 nM	0.37	11
Photoelectrochemistry	10 fM - 1 μM	3.25	12
Photoelectrochemistry	1 pM - 100 nM	310	13
Photoelectrochemistry	10 fM - 100 nM	3.4	14
Photoelectrochemistry	<b>10 fM - 1 μM</b>	<b>2.443</b>	In this work

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