

1 **Supporting Information**

2 **An agar-polyvinyl alcohol hydrogel loaded with tannic acid**
3 **with efficient hemostatic and antibacterial capacity for**
4 **wound dressing**

5 Can Cheng^a, Xu Peng^{a,b}, Linjie Xi^c, Chang Wan^a, Shubin Shi^a, Yuhang Wang^a, and
6 Xixun Yu^{a*}

7 a. College of Polymer Science and Engineering, Sichuan University, Chengdu 610065,
8 P.R. China. E-mail: yuxixun@163.com

9 b. Experimental and Research Animal Institute, Sichuan University, Chengdu 610065,
10 P.R. China.

11 c. Western Theater Command Air Force Hospital, Department of Oncology
12 Hematology, No. 137 Jiuyanqiao shunjiang Road, Chengdu, Sichuan province, 610021,
13 P.R. China.

14

15 **Pages:6**

16 **Experimental methods:5**

17 **Figures:2**

18 ***Xixun Yu (Corresponding author)**

19 College of Polymer Science and Engineering, Sichuan University,
20 No.24 South Section 1, Yihuan Road, Chengdu, China, 610065, E-mail:
21 yuxixun@163.com

22

23 **Materials and methods**

24 **Degradation ratio**

25 The degradation test of all hydrogel specimens was carried out in vitro. Briefly,
26 the hydrogel-samples were soaked in PBS until the swelling equilibrium was reached,
27 and after recording the initial weight, they were incubated in a shaker at 37 °C for a
28 specified time (1 d, 3 d, 6 d, 9 d, 14 d), weighed and recorded again, and the relative
29 degradation ratio of the hydrogels were calculated as follows:

$$30 \text{ Degradation ratio (\%)} = \frac{m_0 - m_1}{m_0} \times 100\%$$

31 Where m_0 is the initial weight of hydrogel, m_1 represents the weight of the
32 corresponding hydrogel being degraded. Data from each specimen was calculated using
33 triplicate measurement.

34

35 **Biomechanical performance**

36 The tensile strength of the hydrogel specimens was tested according to the method
37 of Huang. Briefly, each sample from each group was trimmed as a test strap of 4 mm ×
38 20 mm in size. Five tissue strips in each group were extended on an Instron material
39 testing machine (Instron Co. USA) from 0 g load until the tissue strip ruptured at a
40 constant speed of 10 mm min⁻¹. After measurement, the ultimate tensile stress and the
41 ultimate tensile strain were recorded before failure.

42 The compression strength was determined by a similar method. Briefly, the
43 hydrogels with a height of 10 mm and a diameter of 18 mm were prepared for the
44 compression test. The displacement rate was set as 5 mm min⁻¹. The stress, strain, and
45 compression modulus were recorded and calculated until the sample broke.

46

47 **Cytotoxicity assay**

48 L929 mouse fibroblast cells were seeded in DMEM with 10% FBS and antibiotics
49 (1% penicillin-streptomycin). The cells were incubated at 37 °C in a humidified
50 incubator with 5% CO₂. For sub-cultivation, 0.25% trypsin was used to detach cells
51 from culture plate.

52 All specimens were sterilized by γ-rays for 15 min with an irradiation
53 measurement of 25 KGy. Then, the sterilized samples were placed in 24-well plates and
54 soaked overnight in DMEM medium without serum.

55 CCK-8 array was adopted to measure the cytotoxicity of AGAR@PVA-TA
56 hydrogels. CCK-8 can be reduced to yellow formazan product by dehydrogenase in

57 cells. The quantity of formazan produced was directly proportional to the number of
58 living cells. 200 μ l P3 generation of L929 cells (1×10^5 cells/ml) were slowly dropped
59 onto the surface of the hydrogels. After incubation for 3 h, 800 μ l serum-containing
60 medium was added to each well. These plates were incubated in the same environment
61 as above, and the medium was changed every other day. CCK-8 was used to evaluate
62 the cell proliferation after 1, 3 and 5 days. Results were the average of three independent
63 measurements.

64

65 **Hemolysis test**

66 4 ml of rabbit whole blood (containing 3.8 wt% sodium citrate) was dispensed in
67 1.5 ml centrifuge tubes and centrifuge at 1500 rpm for 15 min at 4 °C. The erythrocyte
68 solution was obtained by diluting the lower red blood cells (RBCs) after centrifugation
69 with isotonic PBS solution at a ratio of 1:7. About 1.6 ml PBS and 0.4 ml RBCs solution
70 were added to the hydrogels in a 24-well plate, and all specimens were incubated at 37
71 °C for 3 h. Meanwhile, we dispersed the RBCs in isotonic PBS buffer as a negative
72 control and dispersed the RBCs in distilled water as a positive control. After incubating
73 for 3 h, all samples were centrifuged at 3000 rpm for 4 min, the 100 μ l of corresponding
74 samples supernatant was transferred to a 96-well plate, and the absorbance of their
75 released hemoglobin was measured using a spectrophotometer at 570 nm. All
76 experiments were performed in triplicate. The hemolysis rate of different hydrogels was
77 calculated as follows:

$$78 \text{ Hemolysis rate (\%)} = \frac{\text{Suspensions}_{abs} - \text{Negative control}_{abs}}{\text{Positive control}_{abs} - \text{Negative control}_{abs}} \times 100\%$$

79 The hydrogel specimens were removed from the above hemolysis rate
80 determination experiment. Samples were gently washed in PBS solution to remove the
81 unadhesive RBCs, and immersed in 2.5% glutaraldehyde solution and fixed at 4 °C for
82 24 h. The hydrogels were then gradient-dehydrated by ethanol (30%, 50%, 70%, 90%,
83 95%, 98% and 100%) and underwent critical point drying. Finally, the adhesion of red
84 blood cells on the specimen surface was observed by SEM.

85

86 **Antibacterial studies**

87 The antibacterial ability of AGAR@PVA-TA hydrogels was determined by plate
88 count method and agar disc diffusion test, and Staphylococcus aureus and Escherichia
89 coli were used as model bacteria.

90 For plate count method, the bacteria were first incubated in Nutrient Broth (NB)

91 at 37 °C until the exponential growth phase. The bacterial broth was then diluted with
92 saline and a concentration of 1×10^7 colony forming units (CFU)/ml was used for
93 subsequent experiments. Each hydrogel specimen was made into a disk of 1 cm
94 diameter and 4 mm thickness, sterilized and placed in a 12-well plate. 30 μ l of the above
95 bacterial suspension and 270 μ l of saline were added to the surface of each hydrogel
96 and co-cultivated for 3 h at 37 °C, the blank well was considered as a control group.
97 Subsequently, the above co-cultured bacterial suspension was diluted about 1000 times
98 and inoculated with 100 μ l of this dilution on NB agar plates and incubated at 37 °C for
99 24h. the reduction rate of bacteria was calculated by counting the numbers of CFUs on
100 the agar plate. The bacterial reduction rate of hydrogels was calculated as follows:

$$101 \quad \text{Reduction rate of bacteria (\%)} = \frac{q_{control} - q_{sample}}{q_{control}} \times 100\%$$

102 Where q_{sample} and $q_{control}$ were the number of CFUs on the agar plate for the hydrogel
103 sample group and the control group. Data from each sample was calculated using
104 triplicate measurement.

105 In the agar disc diffusion test, the above bacterial solution was diluted 10 times
106 and inoculated on NB agar plates, and the solution was spread evenly on the agar plates
107 with an applicator, then the hydrogel was placed on the agar plates and the inhibition
108 area was measured after incubation at 37 °C for 24 h. All experiments were performed
109 in triplicate.

110

111 **Results and discussions**

112 **Degradation ratio**

113 It could be seen from Figure S1 that the degradation ratio of all hydrogel-samples
114 was low at 14 days, and only the degradation ratio of blank group (AGAR@PVA
115 hydrogel) exceeded 10% (11.04%). This indicated that all hydrogel-samples had good
116 stability, and the stability increased with the increase of TA content. This was because
117 after being subjected to freeze-thaw cycle, the agar and PVA in hydrogel had formed a
118 large number of hydrogen bonds, which endowed the hydrogels with good stability,
119 and TA could further increase the density of hydrogen bonds, making the stability of
120 hydrogels further improved.

121

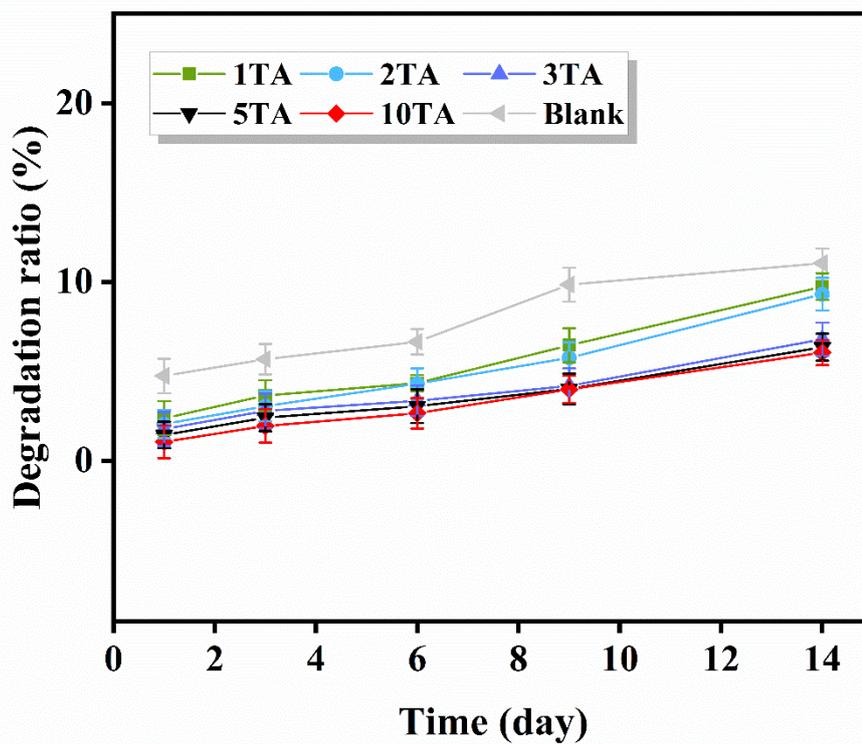


Figure S1. The degradation ratio of hydrogels with different TA concentrations.

122

123

124

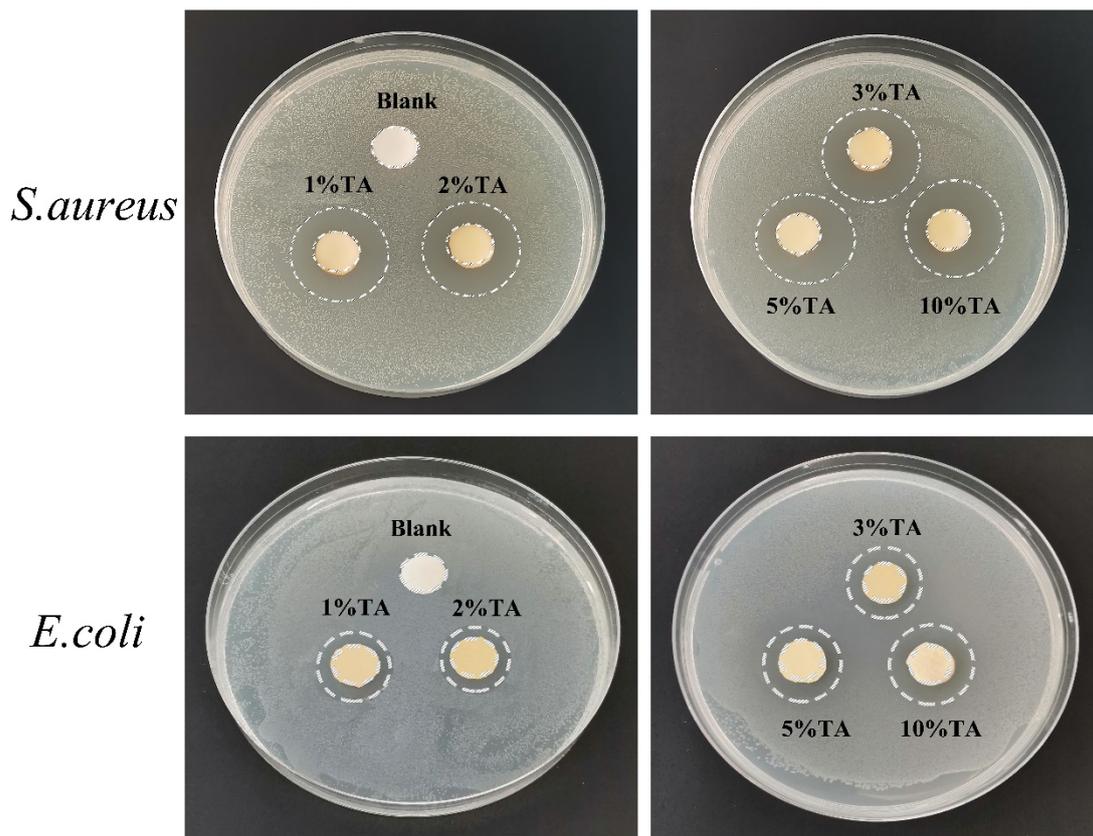
125

126 **Agar disc diffusion test**

127 The antibacterial effect of the hydrogel specimen was also confirmed using the

128 agar disc diffusion test. The areas of inhibitory zone of specimens were shown in Figure

129 S2.



130

131 Figure. S2. Areas of inhibitory zones of different hydrogels against *E. coli* and *S. aureus*.

132

133 As can be seen from the figure, AGAR@PVA hydrogel has no antibacterial
 134 activity, but with the increased of TA concentration in hydrogel, the antibacterial ability
 135 of AGAR@PVA-TA hydrogels increased and showed better antibacterial effect against
 136 *S. aureus* and *E. coli*.

137