

Supplementary Figures and Tables

Article Title:

Multiparameter mobile blood analysis for complete blood count utilizing contrast-enhanced defocusing imaging and machine vision

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Supplementary Figures

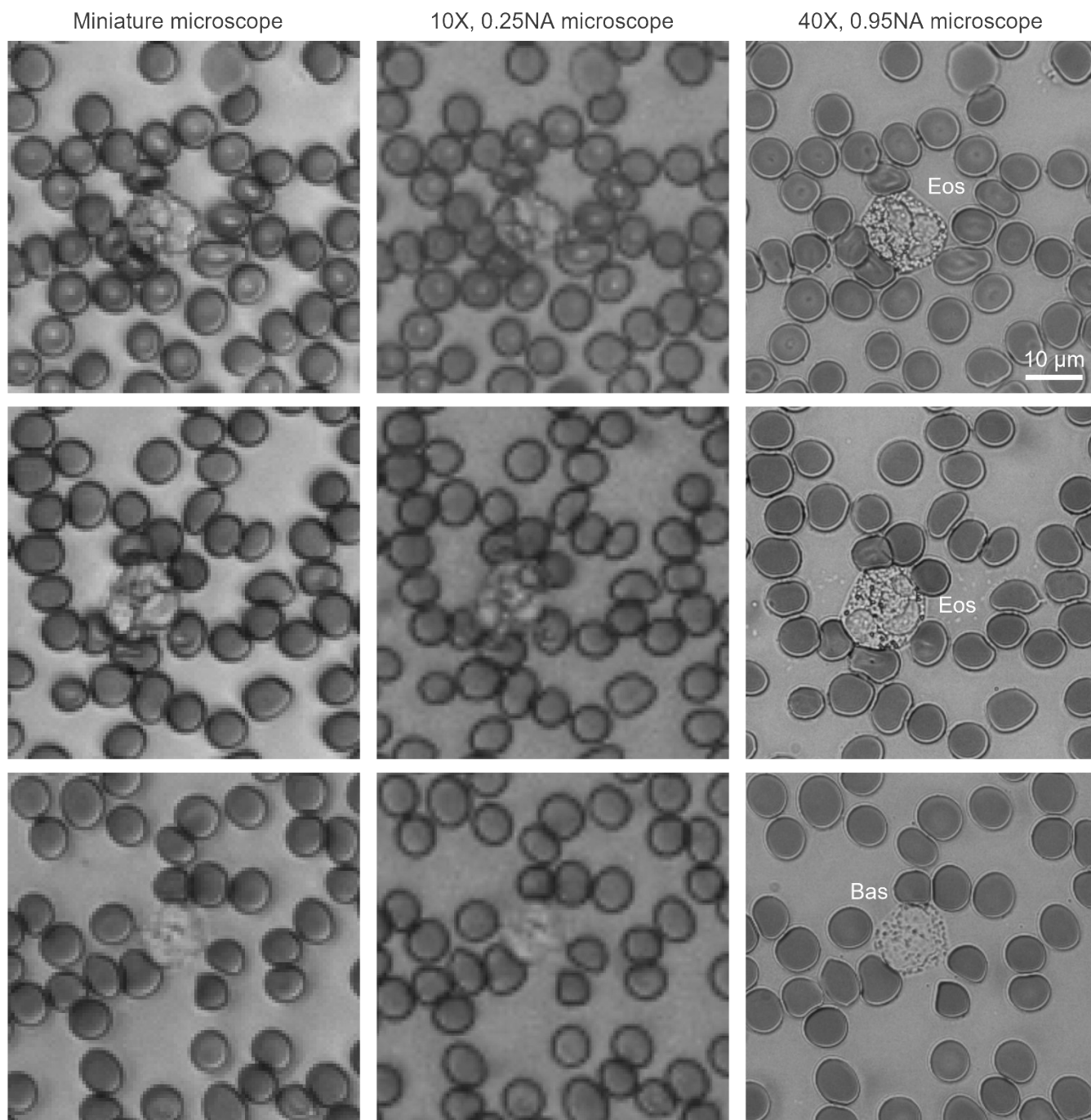


Fig. 1 CEDI images, without up-sampling, captured by the miniature microscope, 10X, 0.25NA microscope, and the 40X, 0.95NA microscope, respectively. Eos: eosinophil; Bas: basophil.

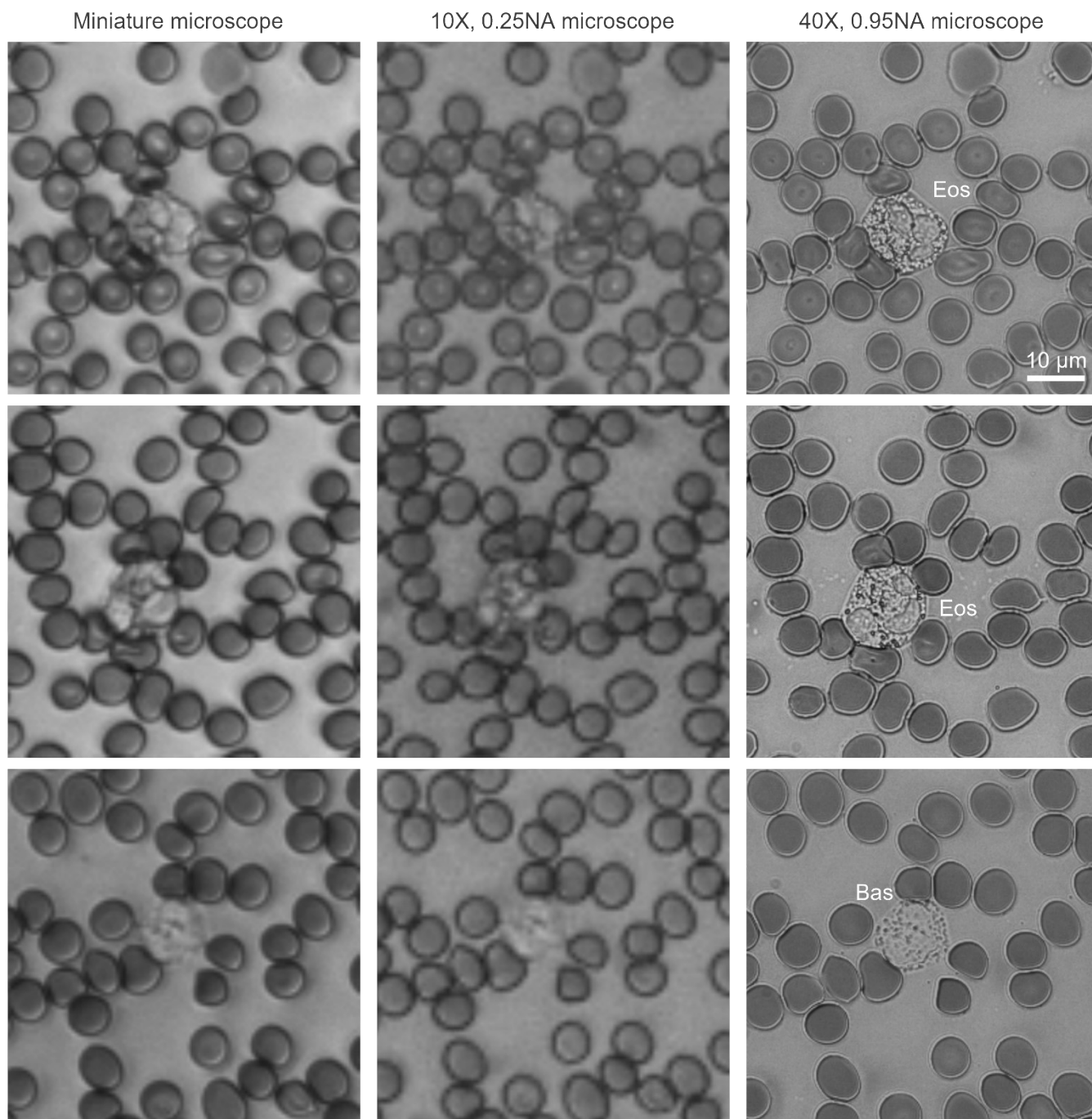


Fig. 2 CEDI images, with up-sampling, captured by the miniature microscope, 10X, 0.25NA microscope, and the 40X, 0.95NA microscope, respectively. Eos: eosinophil; Bas: basophil.

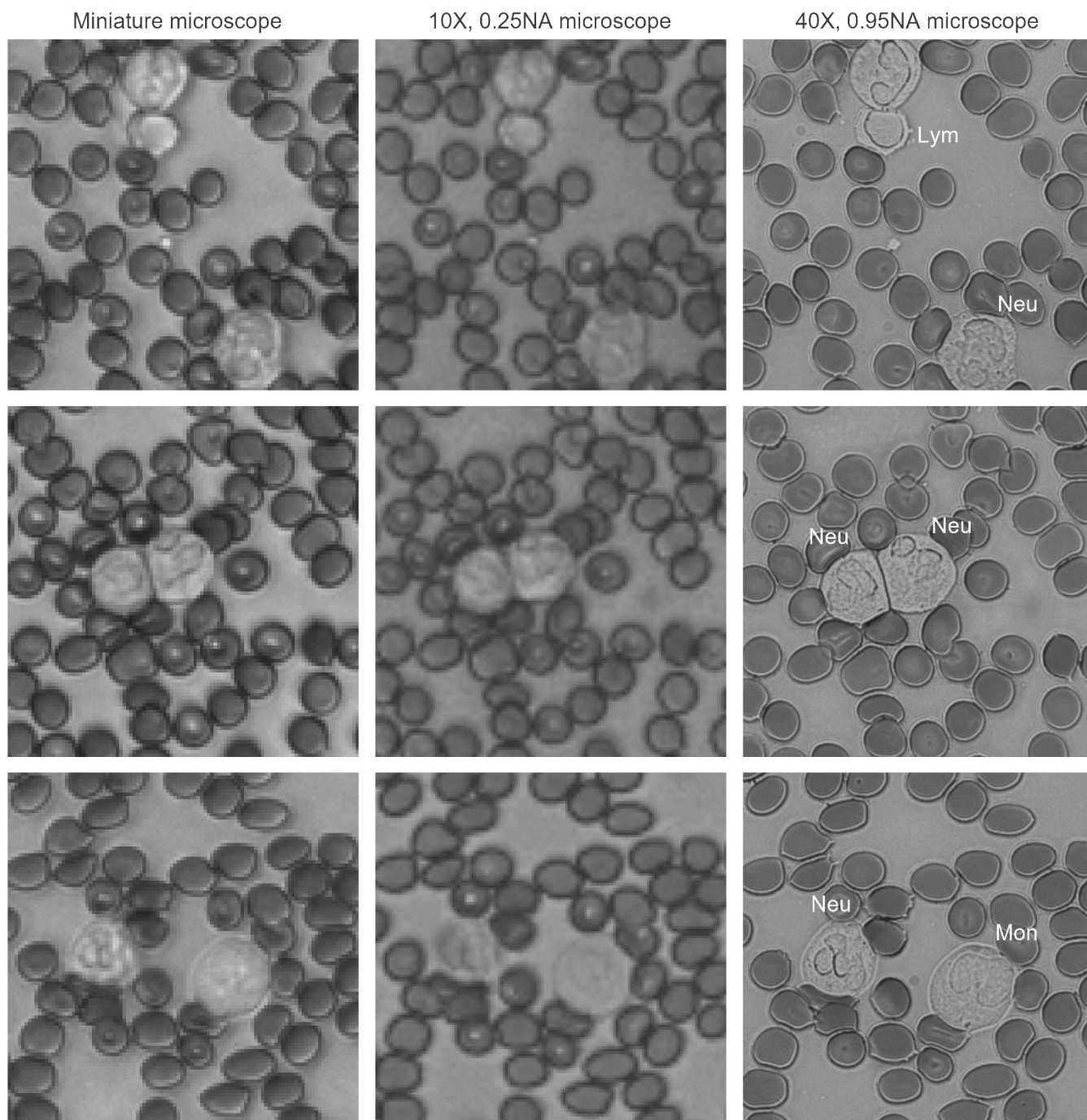


Fig. 3 CEDI images, without up-sampling, captured by the miniature microscope, 10X, 0.25NA microscope, and the 40X, 0.95NA microscope, respectively. Neu: neutrophil; Lym: lymphocyte; Mon: monocyte.

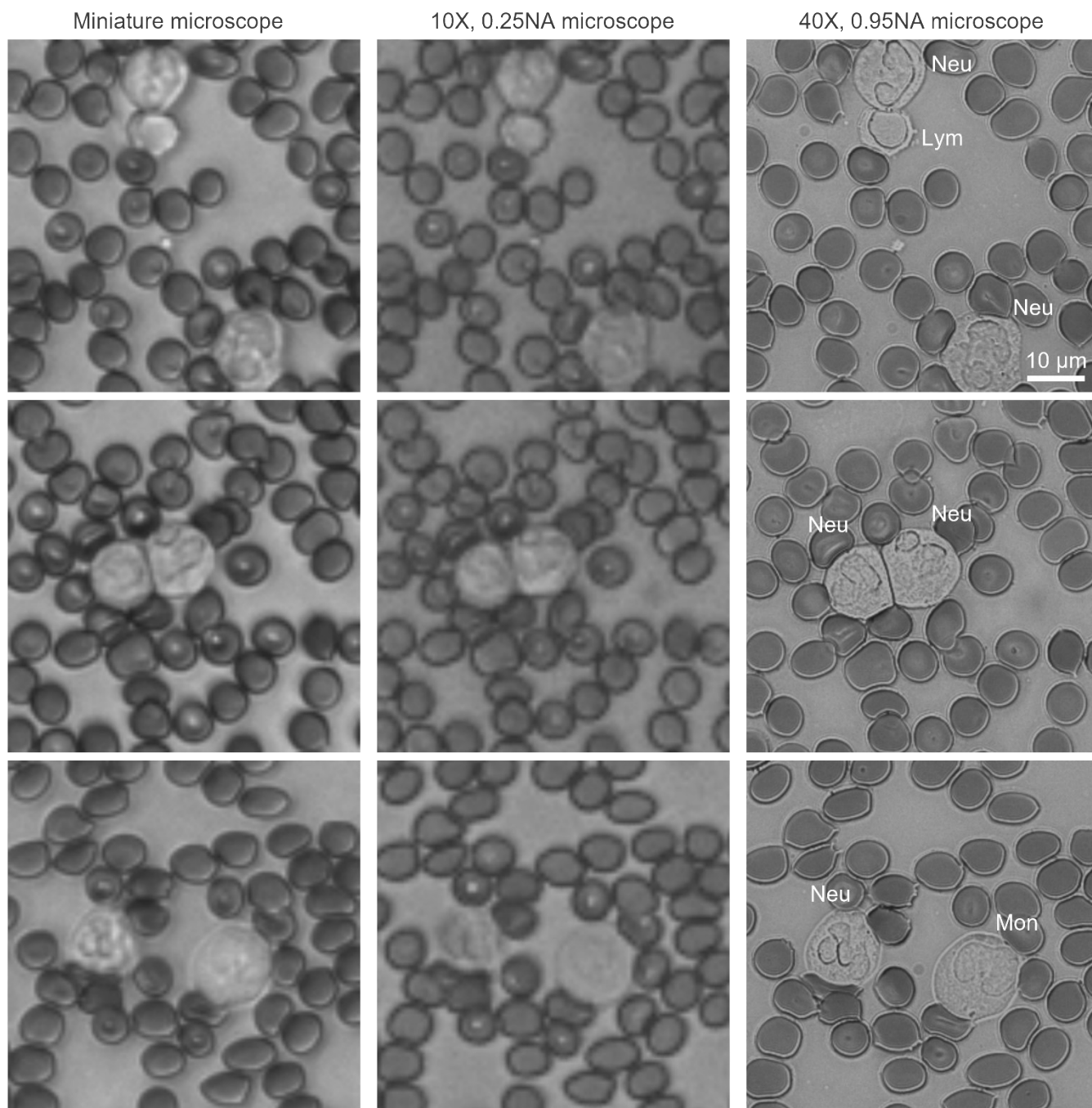


Fig. 4 CEDI images, with up-sampling, captured by the miniature microscope, 10X, 0.25NA microscope, and the 40X, 0.95NA microscope, respectively. Neu: neutrophil; Lym: lymphocyte; Mon: monocyte.

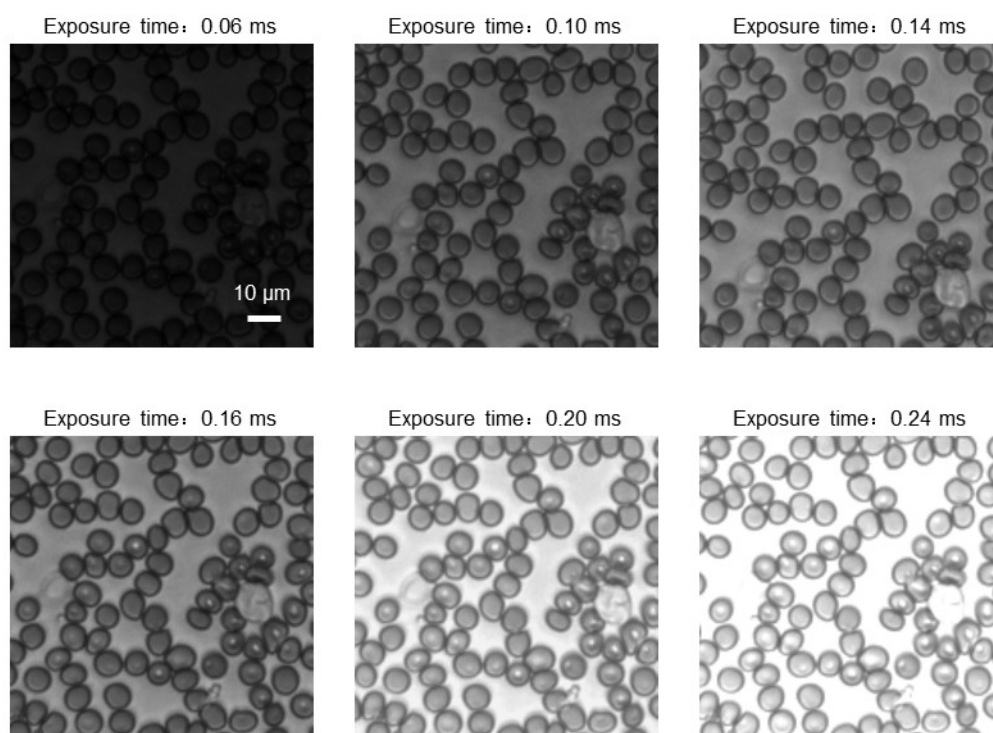


Fig. 5 Some CEDI images with different exposure times.

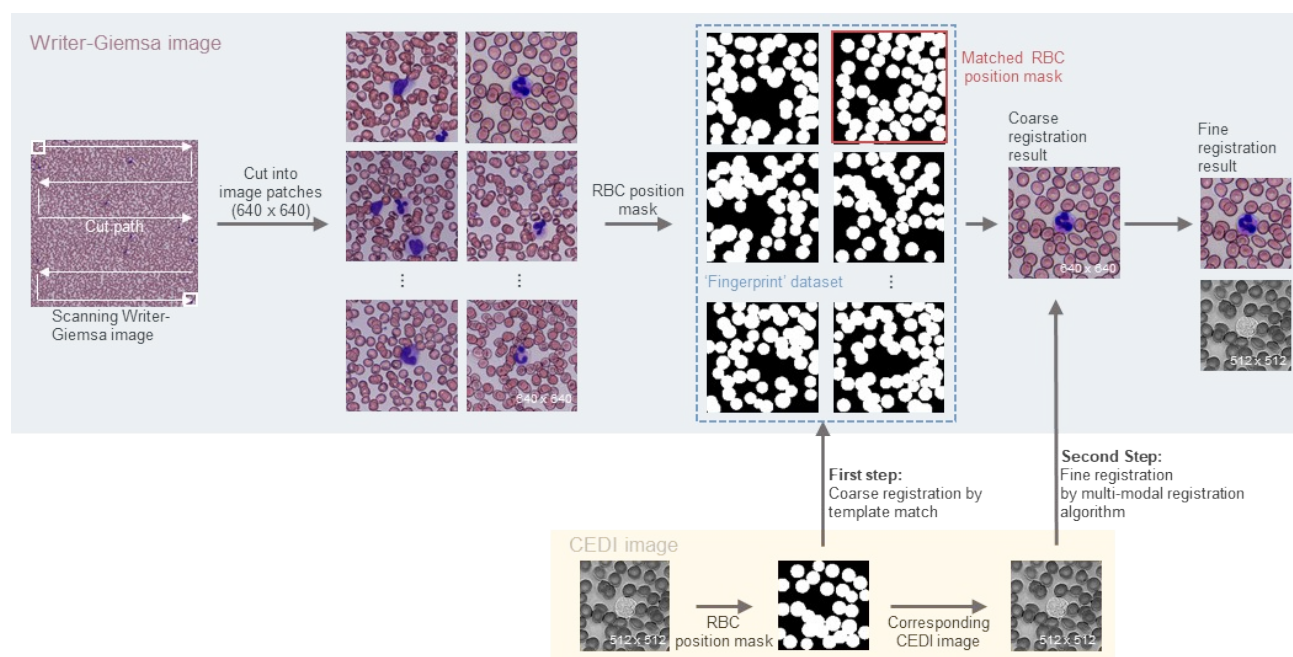


Fig. 6 The two-step image registration algorithm for the CEDI images by the miniature microscope and the Wright-Giemsa images. The RBC position mask images (binary images generated after performing the RBC segmentation algorithm) were adopted as the 'fingerprint' characteristics of the CEDI images and the Wright-Giemsa images. In the image preprocessing stage, the Wright-Giemsa images were cut into small image patches with image sizes of 640 x 640, following a cut path of the 'z' shape. Then the RBC segmentation algorithm introduced in the main text was performed to obtain the RBC position mask images of all the image patches ('fingerprint' dataset of the Wright-Giemsa images). The RBC position mask of the input CEDI image (image size of 512 x 512) would also be obtained by the RBC segmentation algorithm. After the image preprocessing, the two-step registration algorithm containing coarse and fine registration steps would be performed. The matched RBC position mask from the 'fingerprint' dataset for the RBC position mask image of the input CEDI image was searched by the coarse registration algorithm based on template matching, with a similarity criterion of minimum absolute difference (MAD). The fine registration algorithm based on the multimodal registration from MATLAB was used to correct the affine transformation between the Wright-Giemsa image (coarse registration result according to the matched RBC position mask) and the magnified CEDI image. Finally, the matched Wright-Giemsa and CEDI images with image sizes of 512x512 were obtained.

Confusion matrix

Predicting label	NEU	LYM	EOS	BAS	MON	BG
NEU	862	0	1	1	0	4
LYM	3	187	0	0	1	0
EOS	1	0	16	0	0	0
BAS	1	0	0	23	0	1
MON	1	0	0	0	74	1
BG	2	0	0	0	0	0
Actual label						

Fig. 7 Confusion matrix. The horizontal axis presents the actual number of instances, and the vertical axis shows the predicted number of instances from the trained network. NEU: Neutrophil, LYM: Lymphocyte, EOS: Eosinophil, BAS: Basophil, MON: Monocyte, BG: Background.

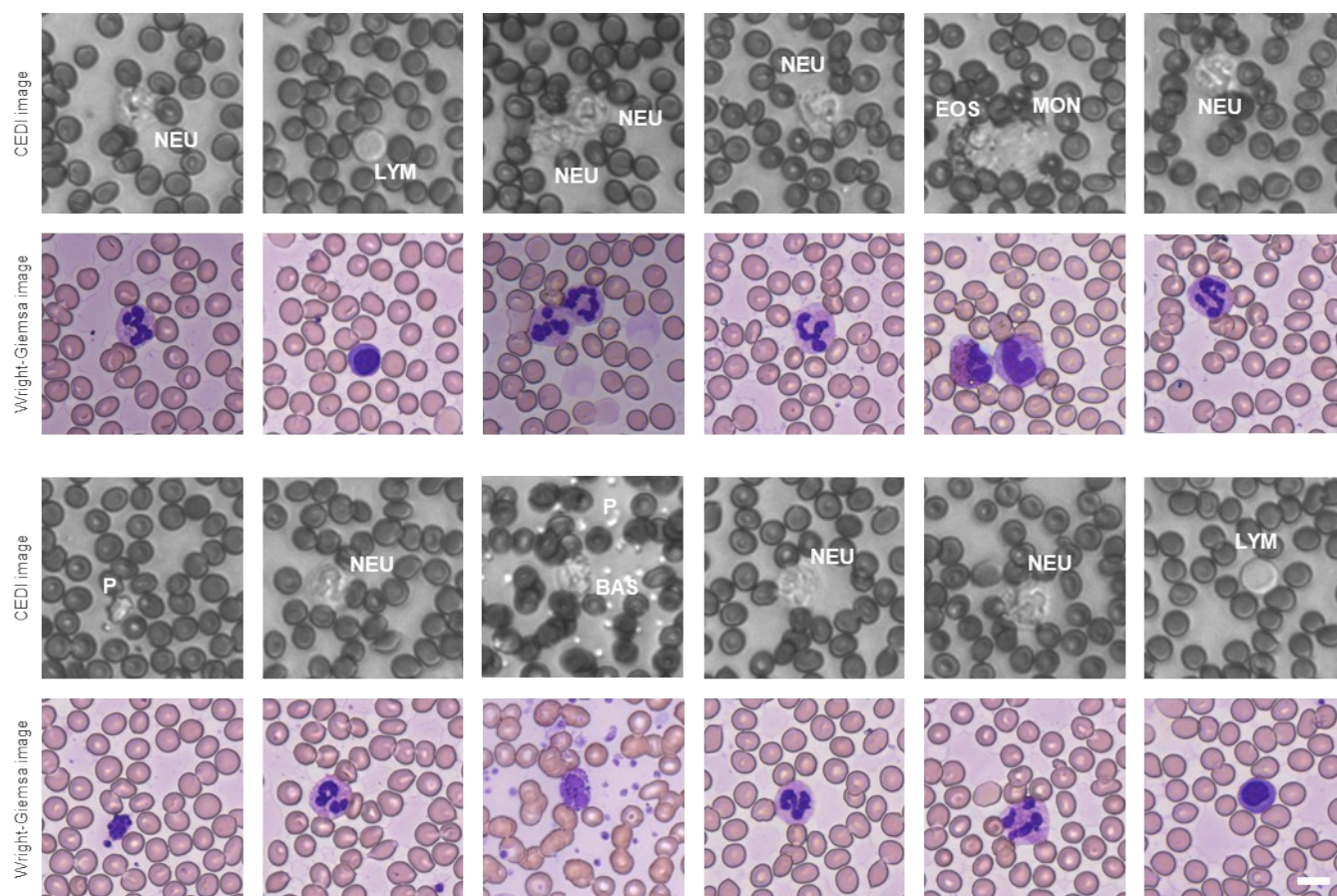


Fig. 8 Image pair of the CEDI images from the mobile blood analyzer and the Wright-Giemsa images from the conventional bright-field microscope (40X, 0.95 NA). The blood cell types for the cell presented in the image centers were marked. P: platelet, NEU: neutrophil, EOS: eosinophil, BAS: basophil, MON: monocyte, LYM: Lymphocyte. Scale bar: 10 μ m.

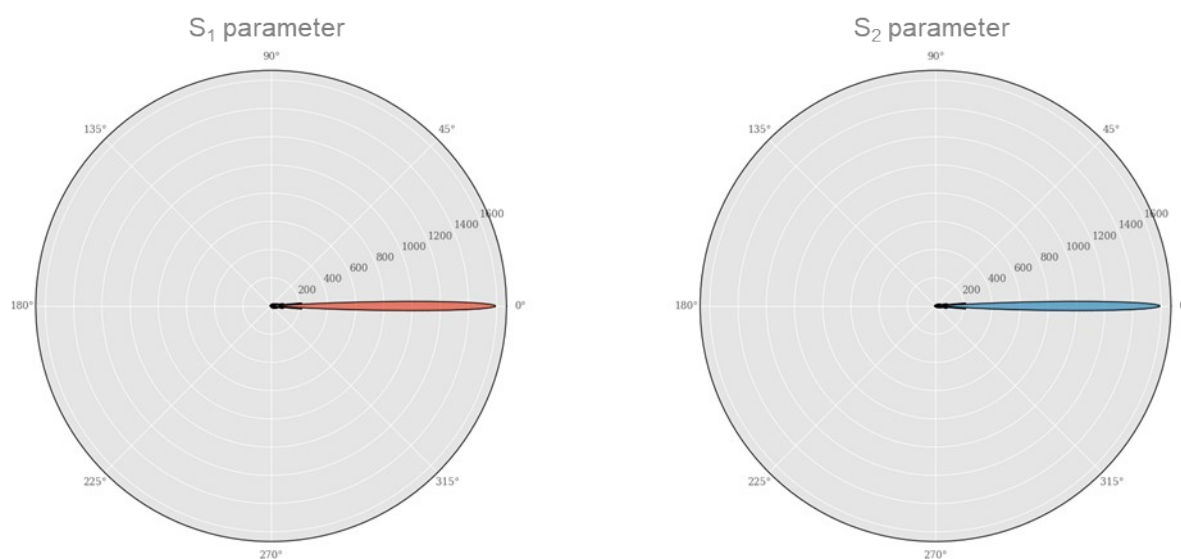


Fig. 9 Scattering amplitude maps S_1 (parallel to the scattering plane) and S_2 (perpendicular to the scattering plane) at scattering angle intervals of $[0^\circ, 360^\circ]$ according to the Mie scattering theory. In the simulation, the light source is set as a plane wave with $0.415 \mu\text{m}$ light, the RBC diameter is set as $7.2 \mu\text{m}$ (the average RBC diameter for blood smears), the media refractive index is set as 1.0 (air refractive index); The RBC refractive index is calculated as¹:

$n = n_1 + in_2$. Here, n_1 and n_2 , related to the hemoglobin concentration, are the real and imaginary parts of the complex refractive index, respectively. And $n_1 = n_0 + \alpha c$, n_0 presents the refractive index in the absence of hemoglobin and α presents the refractive index increment of hemoglobin under specific

illumination wavelength λ , and c presents the hemoglobin concentration;
$$n_2 = \frac{\ln 10 \lambda \epsilon_{\mu M} c}{4\pi M}$$
, with $\epsilon_{\mu M}$ presents the micromolar extinction coefficient of the hemoglobin at wavelength λ , M presents the molar mass of hemoglobin. Under $0.415 \mu\text{m}$ light illumination, the n_0 approximates to 1.345 and α approximates to 0.0017 (dl/g) according to the study by O. Zhernovaya et al.². Besides, the $\epsilon_{\mu M} = 363848 \times 10^{-3} \text{cm}^2/\mu\text{mol}$, $M = 64500 \text{g/mol}$, $c = 34 \text{g/dl}$ (the normal physical intraerythrocytic hemoglobin concentration¹). According to the results, the scattering lights are highly concentrated within small forward-angle intervals, with up to 70% of S_1 's scattering energies lie in an angle interval of $[-6.45^\circ, 6.45^\circ]$ and up to 70% of S_2 's scattering energies lie in an angle interval of $[-11.56^\circ, 11.56^\circ]$. Additionally, the reported miniature microscope's numerical aperture can achieve 0.25 from the resolution test results. The aperture angle of the miniature microscope is at least 14.5° [aperture angle = $\arcsin(0.25)$]. Hence, the microscope can collect most of the scattering light of a single RBC. And the light attenuation when the lights go through a single RBC mainly contributes to light absorption rather than light scattering.

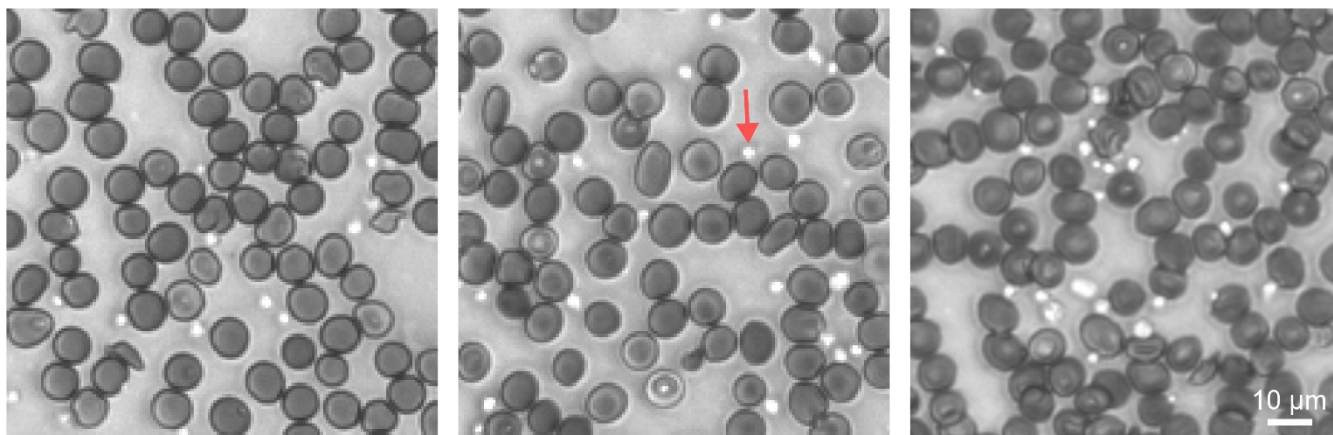


Fig. 10 CEDI images, captured by the miniature microscope, from a sample with increased platelet count. One of the platelet examples is indicated by the red arrow.

Supplementary Tables

Table 1 Performance indexes for FWD testing.

	Neutrophil	Eosinophil	Basophil	Lymphocyte	Monocyte	Average
Precision	0.993	0.941	0.920	0.979	0.974	0.961
Recall	0.991	0.941	0.958	1.000	0.987	0.975
F1 Score	0.992	0.941	0.939	0.989	0.980	0.968

Table 2 Sample amount for FWD (n = 30)

Sample	Image	Total WBC	Neutrophil	Eosinophil	Basophil	Lymphocyte	Monocyte
1	145	326	273	1	8	28	16
2	150	242	133	5	2	91	11
3	160	207	109	60	1	34	3
4	178	341	287	2	1	43	9
5	87	118	78	4	0	25	10
6	164	245	133	2	3	82	25
7	118	848	825	1	1	12	9
8	189	290	202	5	1	65	17
9	174	293	159	4	2	108	20
10	149	237	167	1	0	65	4
11	141	210	130	2	0	75	3
12	147	189	122	2	2	61	2
13	163	263	178	2	1	79	3
14	180	290	244	9	2	27	8
15	89	191	92	10	1	73	15
16	119	328	180	10	5	67	66
17	85	184	144	0	0	34	6
18	131	235	196	1	2	34	2
19	68	104	75	14	0	12	1
20	94	190	135	3	0	44	8
21	154	258	101	11	2	143	2
22	30	187	181	0	0	3	2
23	45	330	323	0	0	3	4
24	50	343	335	1	0	3	4
25	90	184	155	1	2	23	5
26	50	92	79	1	1	11	1
27	90	147	120	6	1	14	6
28	100	166	137	7	1	18	4
29	70	152	129	0	6	10	7
30	90	202	174	1	4	16	7

Table 3 Statistics of the image gradient for the five WBC populations and the granulocyte.

	Median	Interquartile Range	95% Confidence Interval	
			Lower Limit	Upper Limit
Neutrophil	121.513	21.213	118.680	133.800
Eosinophil	133.608	29.919	125.617	149.171
Basophil	106.214	18.540	103.043	114.253
Lymphocyte	81.885	13.192	77.739	86.032
Monocyte	134.037	21.810	125.968	142.106
Granulocyte	126.240	21.213	118.679	133.780

Table 4 Statistics of the image area for the lymphocyte, monocyte, and granulocyte.

	Median	Interquartile Range	95% Confidence Interval	
			Lower Limit	Upper Limit
Lymphocyte	6391.450	1329	5782.540	7000.360
Monocyte	13778.700	1382	13034.410	14522.990
Granulocyte	10773.100	1584	10014.690	11531.510

Table 5 Statistics of the image mean intensity for the three granulocyte populations.

	Median	Interquartile Range	95% Confidence Interval	
			Lower Limit	Upper Limit
Neutrophil	166.245	12.177	162.822	170.693
Eosinophil	150.308	10.721	144.177	152.438
Basophil	168.606	7.125	165.406	170.369

Table 6 Independence sample t-test for equality of image area, mean intensity, and gradient

Image feature		T-value	Degrees of freedom	P-value	Mean difference	Std. error difference	95% Confidence interval of the difference	
							Lower	Upper
Image area	Gran Vs. Lym	7.954	77	1.248x10 ⁻¹¹	4225.821	531.291	3167.887	5283.756
	Gran Vs. Mon	-5.810	77	1.335x10 ⁻⁷	-3161.430	544.139	-4244.950	-2077.910
	Lym Vs. Mon	-16.079	38	1.529x10 ⁻¹⁸	-7387.250	459.448	-8317.85	-6457.150
Image mean intensity	Eos Vs. Bas	-8.505	31.135	2.513x10 ⁻¹⁰	-19.580	2.302	-24.274	-14.885
	Eos Vs. Neu	6.698	36.978	7.193x10 ⁻⁸	18.670	2.7887	13.023	24.319
Image gradient	Lym Vs. Mon	-12.032	38	1.574x10 ⁻¹⁴	-52.151	4.334	-60.926	-43.377
	Bas Vs. Neu	3.717	37	0.665x10 ⁻³	17.018	4.579	7.741	26.295

Table 7 Independence sample t-test for equality of RBC hemoglobin means (anemia versus health).

T-value	Degrees of freedom	P-value	Mean difference	Std. error difference	95% Confidence interval of the difference	
					Lower	Upper
-58.625	1259.401	0.000	-11.289	0.193	-11.667	-10.911

Table 8 Independence sample t-test for equality of RBC area means (anemia versus health).

T-value	Degrees of freedom	P-value	Mean difference	Std. error difference	95% Confidence interval of the difference	
					Lower	Upper
-17.764		9.996 x 10 ⁻⁶²	-17.764	-6.912	-7.675	-6.148

Table 9 Statistic data of the RBC hemoglobin and area for the anemia sample.

	Median	Interquartile Range	95% Confidence Interval	
			Lower	Upper
Hemoglobin	21.509	5.370	21.269	21.913
Area	48.254	11.356	47.196	48.593

Table 10 Statistic data of the RBC hemoglobin and area for the health sample.

	Median	Interquartile Range	95% Confidence Interval	
			Lower	Upper
Hemoglobin	33.064	4.813	32.683	33.078
Area	55.037	7.776	54.482	55.121

References

- 1 J. Gienger, H. Groß, J. Neukammer and M. Bär, Determining the refractive index of human hemoglobin solutions by Kramers–Kronig relations with an improved absorption model, *Appl. Opt.*, 2016, **55**, 8951.
- 2 O. Zhernovaya, O. Sydoruk, V. Tuchin and A. Douplik, The refractive index of human hemoglobin in the visible range, *Phys. Med. Biol.*, 2011, **56**, 4013–4021.