

Supporting information

**Title:**

NIR-light-trigger delivery of Doxorubicin-loaded PLGA nanoparticles for synergistic cancer therapy on DMBA/TPA induced tumor mice

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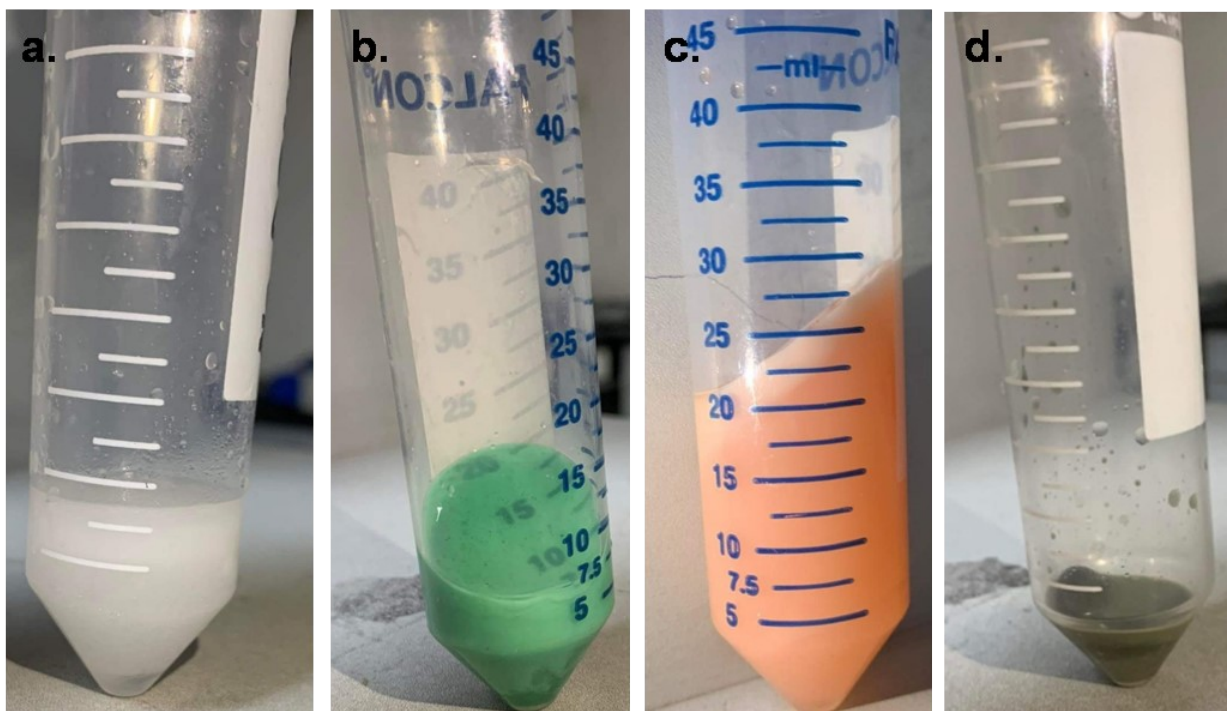
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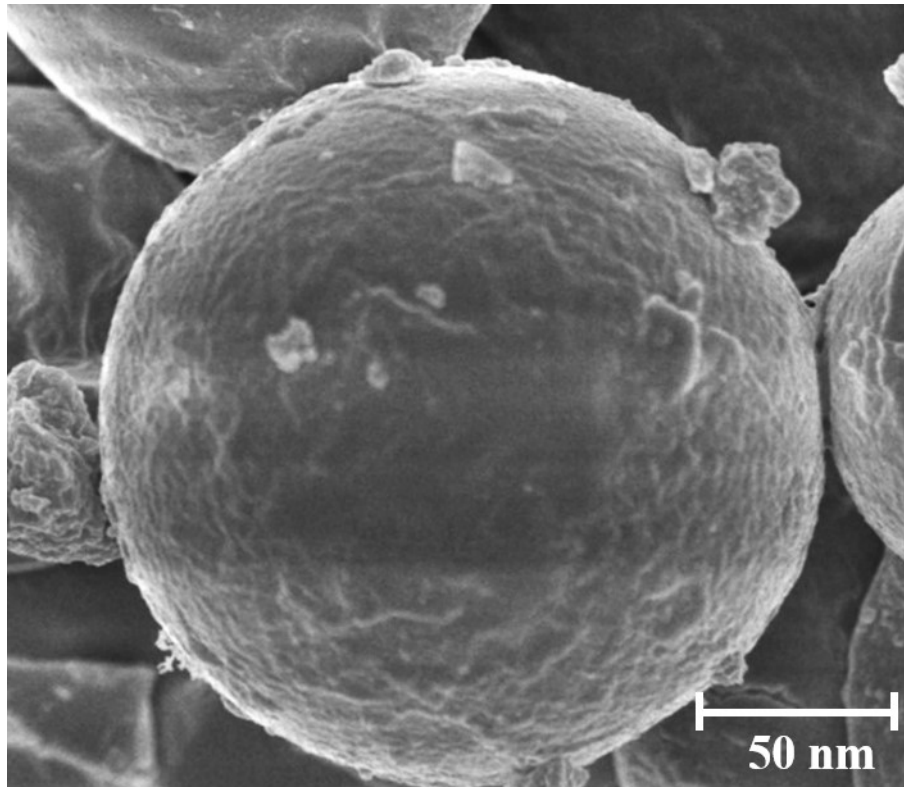
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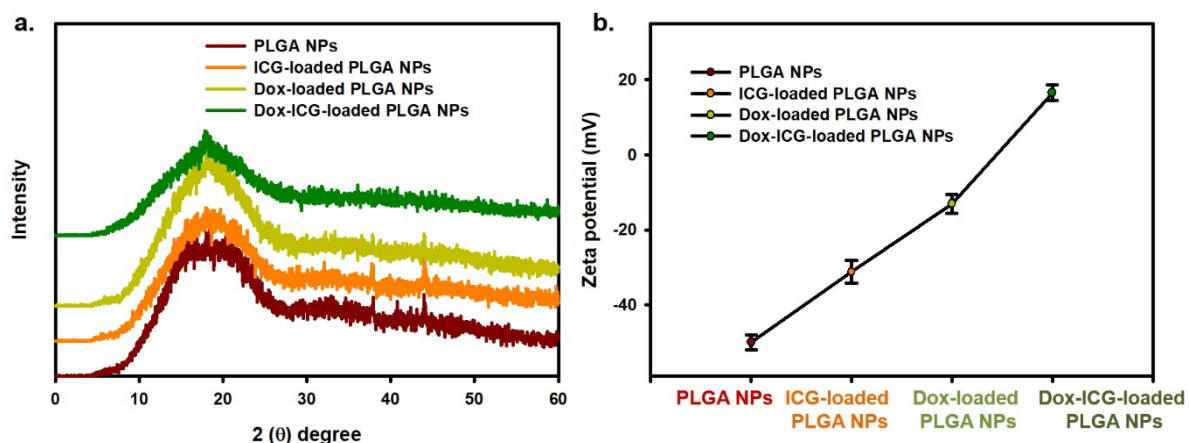
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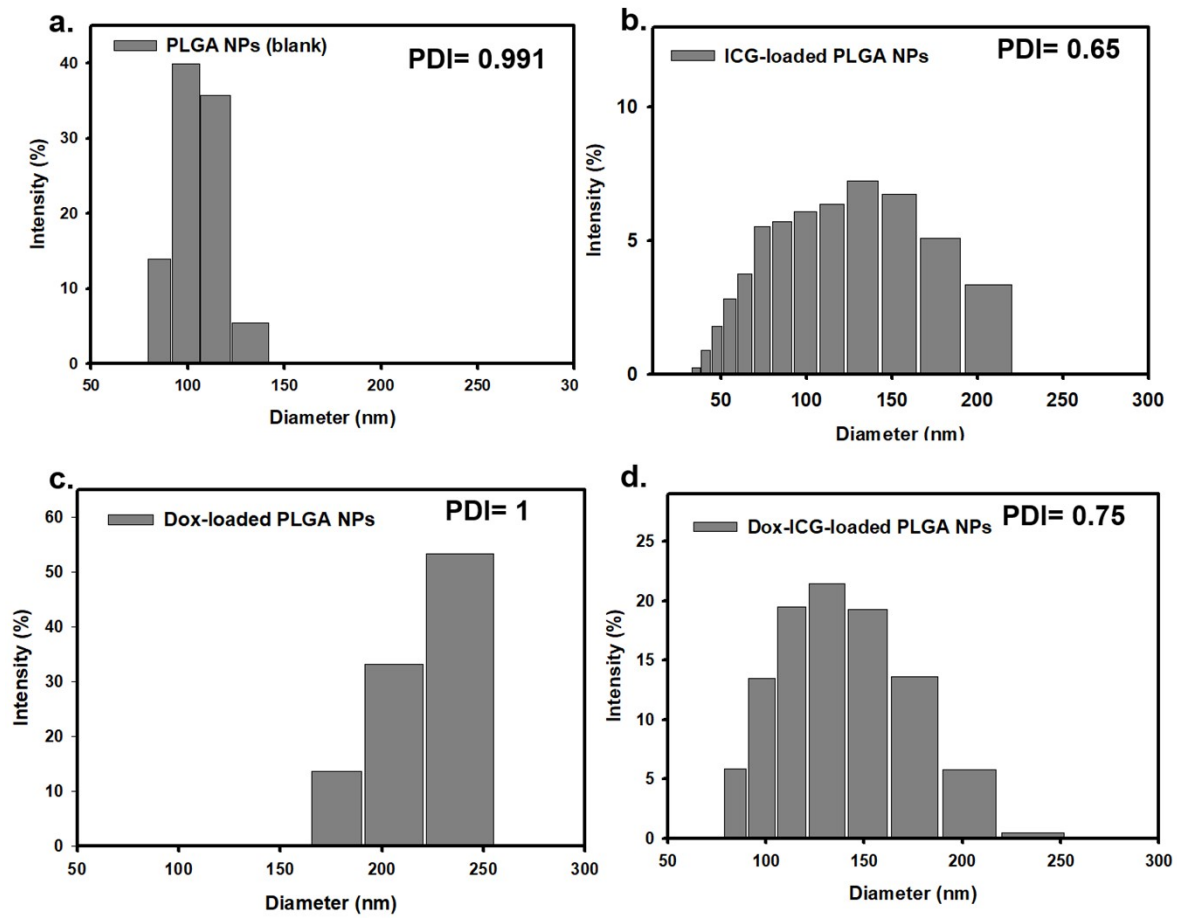
**Figure S1.** The photo images (a) PLGA NPs (blank), (b) ICG-loaded PLGA NPs, (c) Dox-loaded PLGA NPs and (d) Dox-ICG-loaded PLGA NPs during nanoparticles synthesis.



**Figure S2.** The magnified scanning electron microscopic (SEM) image (scale bar 50 nm) of Dox-ICG loaded PLGA NPs.



**Figure S3.** (a) The X-ray diffraction (XRD) pattern blank PLGA NPs, ICG-loaded PLGA NPs, Dox-loaded PLGA NPs and Dox-ICG-loaded PLGA NPs. (b) The zeta potential (mV) for the surface charge of PLGA NPs, ICG-loaded PLGA NPs, Dox-loaded PLGA NPs and (d) Dox-ICG-loaded PLGA NPs.

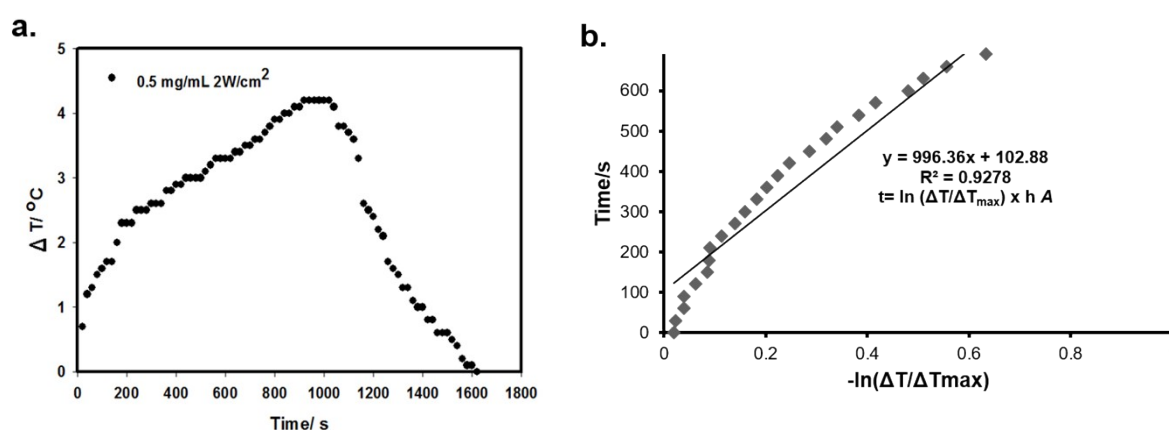


**Figure S4.** The dynamic light scattering (DLS) based hydrodynamic size (diameter) range and polydispersity index (PDI) analysis of (a) PLGA NPs, (b) ICG-loaded PLGA NPs, (c) Dox-loaded PLGA NPs and (d) Dox-ICG-loaded PLGA NPs.

The photothermal conversion efficiency was measured by using following equation:

$$\eta = \frac{hA\Delta T_{\max} - Q_s}{I(1 - 10^{-A\lambda})}$$

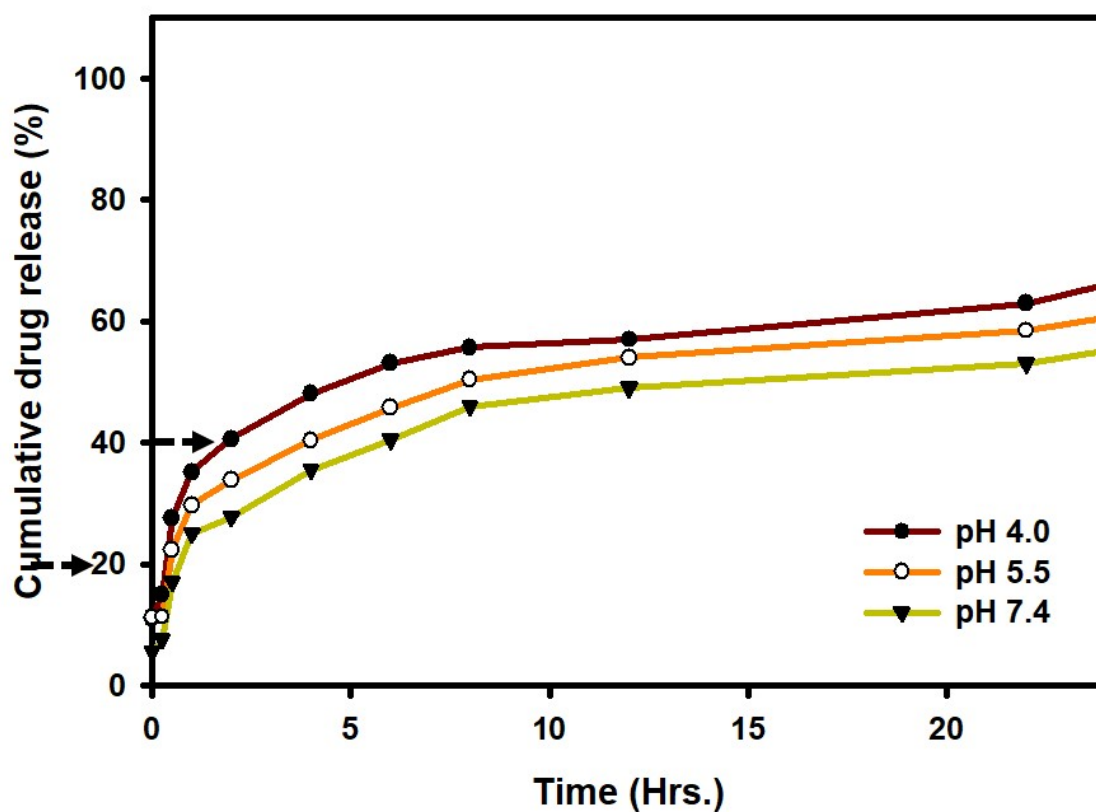
Where  $h$  is the heat transfer coefficient,  $A$  is the surface area of the container,  $\Delta T_{\max}$  is the temperature change of the Dox-ICG-loaded PLGA NPs solution at the maximum steady-state temperature,  $I$  is the laser power,  $A\lambda$  is the Dox-ICG-loaded PLGA NPs at 808 nm,  $Q_s$  is the heat associated with the light absorbance of the solvent, and  $\eta$  is the photothermal conversion efficiency. [1], [2]



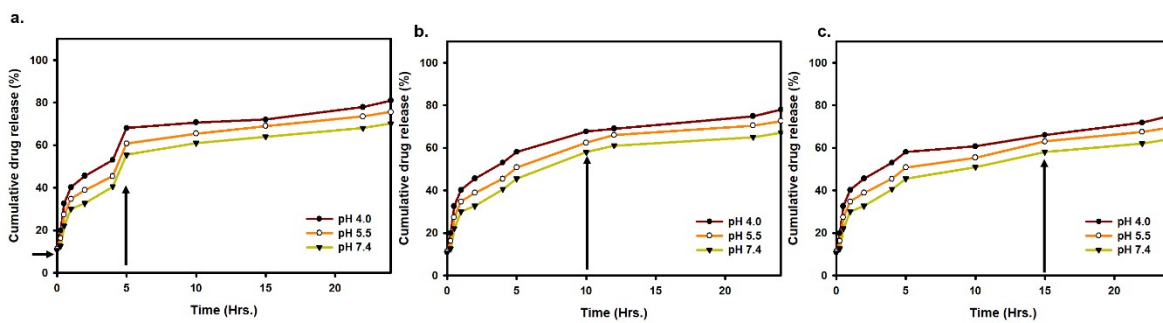
**Figure S5.** (Left) Temperature profile ( $\Delta T = T_n - T_0$ ) of a solution of Dox-ICG-loaded PLGA NPs in water at 0.5 mg/mL when illuminated with a 808 nm laser (2 W/cm<sup>2</sup>) during 15 min and after turning off the laser during 15 min; (Right) time constant for heat transfer is determined by applying the linear time from the cooling period (from 900 to 1600 s) versus negative natural logarithm of the driving force temperature.

#### References:

1. K. Mebrouk, F. Chotard, C. L. Goff-Gaillard, Y. Arlot-Bonnemains, M. Fourmigué, F. Camerel, Water-soluble nickel-bis(dithiolene) complexes as photothermal agents. *Chem. Commun.*, 2015, **51**, 5268-5270.
2. Sharker SM, Kim SM, Lee JE, Choi KH, Shin G, Lee S, Lee KD, Jeong JH, Lee H, Park SY. Functionalized biocompatible WO<sub>3</sub> nanoparticles for triggered and targeted in vitro and in vivo photothermal therapy, *Journal of Controlled Release*, 2015, **217**, 211-220.

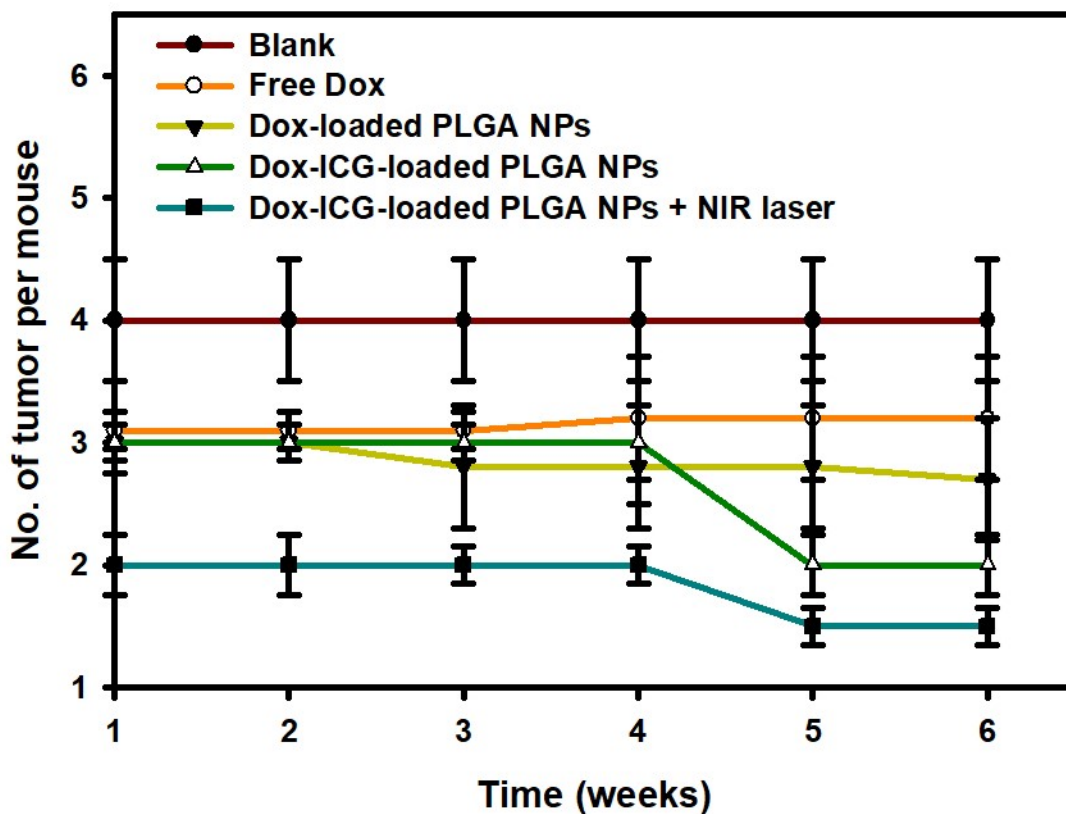


**Figure S6.** The pH-responsive in vitro (%) ICG release from Dox-ICG-loaded PLGA NPs. The release medium was pH 7.4, 5.5, and 4.0 with temperature 36°C. To determine the amount of ICG released, a 3 mL solution was taken from the outside released medium, and 3 ml of the solution was replaced by new-release media. The absorbances were measured at 810 nm using UV-visible spectroscopy; the amount (%) of the drug released was then calculated.

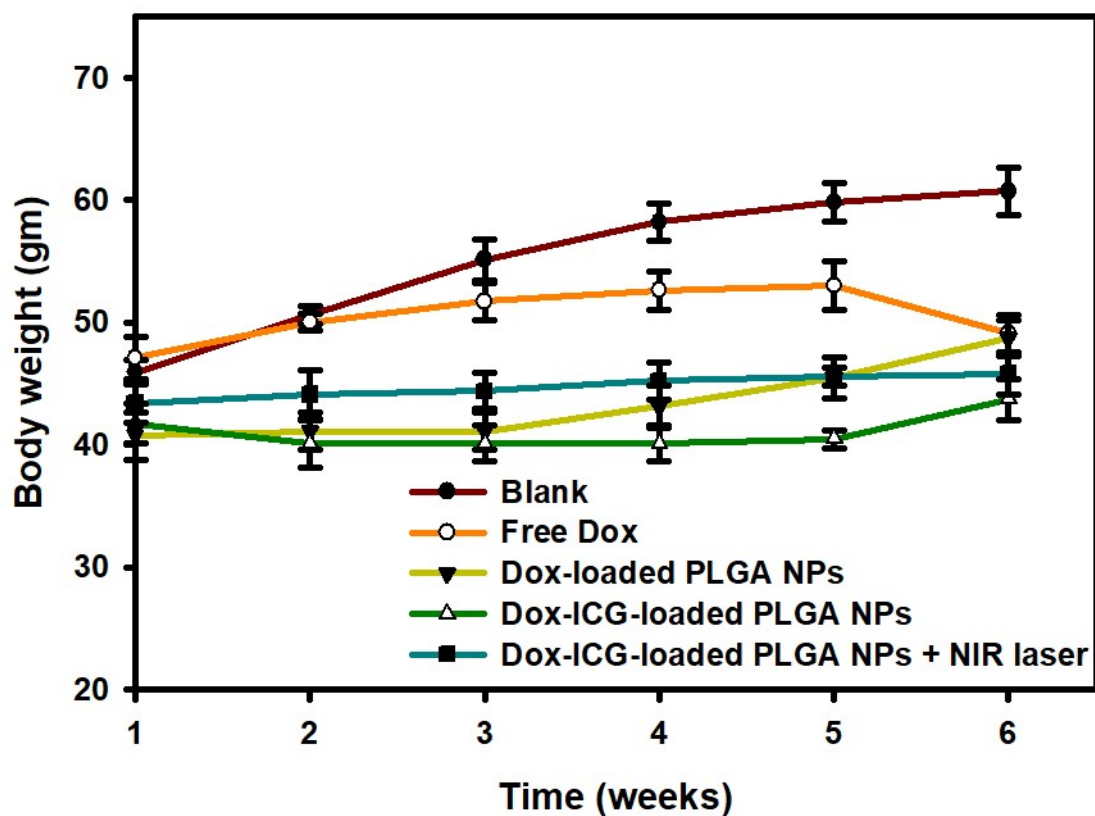


**Figure S7.** The heat-responsive *in vitro* drug release in response to 5 min NIR irradiation (808 nm laser, 2 W/cm<sup>2</sup>). The NIR light was used at the 5 h, (b) 10 h, (c) 15 h of drug release study.





**Figure S8.** The *in vivo* anticancer activity by observing tumor number after administration of blank (control), free Dox, Dox-loaded PLGA NPs, Dox-ICG-loaded PLGA NPs and Dox-ICG-loaded PLGA NPs with 5 min NIR laser irradiation (mean  $\pm$ SD, n = 5).



**Figure S9.** (a) The body (average) weight of the treated mice during in vivo anticancer activity of blank (control), free Dox, Dox-loaded PLGA NPs, Dox-ICG-loaded PLGA NPs and Dox-ICG-loaded-PLGA NPs with 5 min NIR laser irradiation (mean  $\pm$ SD, n = 5).