

1 **Supporting Information**

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3 **Asymmetric fabrication and in-vivo evaluation of wound healing potency**
4 **of electrospun biomimetic nanofibrous scaffold based on collagen**
5 **crosslinked modified-chitosan and graphene oxide quantum dot**
6 **nanocomposites.**

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8 Koushik Dutta ^a, Kunal Sarkar ^c, Srikanta Karmakar ^a, Bhuman Gangopadhyay ^a, Arijita Basu ^a,
9 Sarbashri Bank ^c, Sriparna De ^b, Beauty Das ^{*a}, Madhusudan Das ^{*c}, Dipankar Chattopadhyay ^{*a}

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11 ^a Department of Polymer Science and Technology, University of Calcutta, 92 A.P.C. Road,
12 Kolkata 700009, India.

13 e-mail: dipankar.chattopadhyay@gmail.com

14 ^b Department of Allied Health Sciences, Brainware University, Kolkata-700129, India.

15 ^c Department of Zoology, University of Calcutta, 35, Ballygunge circular road, Kolkata 700019,
16 India

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24 **1. EXPERIMENTAL SECTION**

25 **1.1. Materials**

26 Potassium permanganate (KMnO₄, ACS grade), sulphuric acid (98% H₂SO₄, GR grade),
27 sodium nitrate (NaNO₂, extra pure), hydrogen peroxide (30% H₂O₂), acetic acid (CH₃COOH,
28 glacial 100%), formic acid (HCOOH, 98-100% pure) were purchased from Merck Specialties
29 Private Ltd., India. Chloroform (CHCl₃, anhydrous), phosphate buffered saline (PBS), methanol
30 (CH₃OH, anhydrous), 2,2,2-trifluoroethanol (TFE), trichloroacetic acid (TCA), thiobarbituric
31 acid (TBA), nitro blue tetrazolium chloride (NBT) and riboflavin were procured from Sisco
32 Research Laboratories Pvt. Ltd. (India). Glutaraldehyde (25% in water) and N, N-
33 dimethylformamide (DMF, anhydrous) were purchased from Spectrochem Pvt. Ltd. (Mumbai,
34 India). Phthalic anhydride and decanoyl chloride were purchased from TCI Chemical Pvt. Ltd.,
35 Japan. L929 fibroblast cell was purchased from the National Centre for Cell Science (NCCS,
36 Pune, India). Chitosan, polycaprolactone (Mn 80000, PCL), nylon syringe filter (0.2 μm pore
37 size), dialysis tubing (molecular weight cut-off 2000 Da), collagen (type I), 1-ethyl-3-(3-
38 (dimethylamino)-propyl) carbodiimide (EDC), fluorescein diacetate (FDA) and 2,2-diphenyl-1-
39 picrylhydrazyl were obtained from Sigma-Aldrich, Germany. Dulbecco's modified eagle
40 medium (DMEM), fetal bovine serum, MTT reagent, tetramethylethylenediamine (TEMED),
41 penicillin, and streptomycin were procured from HiMedia, Mumbai, India.

42 **1.2. Characterization**

43 Fourier transform infrared (FTIR) spectroscopy was performed using Perkin-Elmer
44 spectrum Two FT-IR spectrometer over wave number 400-4000 cm⁻¹. The surface morphology
45 and the fiber dimension were elucidated by the scanning electron microscope (ZEISS EVO-
46 MA10, Germany) and transmission electron microscopy (HRTEM, JEOLJEM 2100) operated at

47 200 kV acceleration voltage. The particle and fiber size distribution were displayed by Image J
48 (1.51K) software. The X-ray diffraction (XRD) analysis was carried out between $2\theta = 3$ and 40°
49 by employing an X-PERT-PRO Panalytical diffractometer with $\text{CuK}\alpha$ (40 kV/30 mA) as the X-
50 ray source comprising a wavelength of approximately 1.4506 nm. UV-visible spectroscopy was
51 recorded by a Perkin-Elmer UV-vis Spectrophotometer Lambda 25. X-ray photoelectron
52 spectroscopy (XPS) study was characterized by a Thermo-VG Scientific ESCA Lab250
53 microprobe equipped with $\text{AlK}\alpha$ monochromatic source comprising 1486.6 eV photons
54 operating at 14 kV and 20 mA. ^{13}C solid state nuclear magnetic resonance (NMR) spectroscopy
55 was carried out using AV 500S Bruker 500 MHz instrument. ^1H solution NMR spectroscopy was
56 done with the employment of a 400 MHz Bruker instrument. NMR grade trifluoroacetic acid
57 (5% v/v) incorporated D_2O was taken as a solvent for all the compounds. The mechanical
58 properties were estimated according to the ASTM method D882-95a with the assistance of the
59 Zwick Roell (ZO10) instrument. The water contact angle measurements of all the scaffolds were
60 evaluated using an Apex ACAM-D2 contact angle system.

61 **1.3. Porosity measurement**

62 The liquid displacing method was utilized to estimate the porosity of the scaffolds.
63 Briefly, the scaffold (weighing W_i) was immersed in a tube containing absolute ethanol. The
64 total volume (V_1) of the ethanol with the scaffold was recorded. The scaffold was kept immersed
65 in ethanol until saturation. The ethanol-saturated scaffold was taken out and the remaining
66 volume (V_2) of the ethanol left was noted. The weight (W_f) of the ethanol-soaked scaffold was
67 also recorded. The recorded data were employed in equation 1 to calculate the porosity of the
68 scaffold. The data sets were calculated thrice experimentally and the average value was taken.

69 Porosity = $\frac{W_f/\rho - W_i/\rho}{V_1 - V_2}$ (1) ρ = density of ethanol

70 **1.4. Water vapor transmission rate (WVTR)**

71 The WVTR of the scaffolds was determined by pouring 20 mL of phosphate buffer saline
 72 (PBS) into a 50 mL centrifuge tube with an open area of S cm². The centrifuge tube was covered
 73 with a piece of a scaffold, and the total weight was recorded (W₁). The scaffold covered tube was
 74 incubated at 37 °C for about 24 hours and subsequently, the total weight was again recorded
 75 (W₂). Equation 2 was employed to evaluate the WVTR of the scaffolds in 24 hours. After three
 76 times of experiments, the average values were taken.

77 WVTR = $\frac{W_1 - W_2}{S}$ (2)

78 **1.5. Catalase-Like activity**

79 The catalase-like activity assay was estimated by the addition of 10 (M) H₂O₂ in 100 µg
 80 mL⁻¹ scaffolds. After 10 min, the evolution of gas bubbles was seen. The catalase-like activity of
 81 the scaffolds was also detected by analysing the reduction rate of H₂O₂ levels. The standard
 82 initial concentration of H₂O₂ was 25 mmol L⁻¹, and the final concentration of H₂O₂ after the
 83 incubation with the scaffold was evaluated spectrophotometrically with regard to the absorbance
 84 peak of H₂O₂ at 230 nm.

85 **1.6. Antimicrobial activities assay**

86 The antimicrobial activity of the scaffolds was assessed with the help of the plate
 87 counting method. Both *Escherichia coli* (*E. coli*) and *Staphylococcus aureus* (*S. aureus*) bacteria

88 were cultured in Luria-Bertani (LB) medium over a period of 16 hours at 37 °C with continuous
89 shaking, followed by washing with fresh sterile 0.9% saline thrice. The cultures were then
90 diluted in sterile 0.9% saline solution to $\sim 10^7$ colony-forming units per milliliter (CFU mL⁻¹). To
91 expose the active surface of the bacteria, all the scaffolds with an area of 2 cm² were placed in a
92 plastic holder. Bacterial suspensions (0.5 mL per cm²) were subjected to contact with the
93 scaffold surface over a period of 60 min at 37 °C temperature. With the discarding of excess
94 bacterial suspension, the scaffolds were washed thoroughly with sterile 0.9% saline. After
95 thorough washing, scaffolds were put into a 50 mL tube containing 10 mL of sterile 0.9% saline
96 and subjected to vortex for 8 min to remove the bacterial cells from the scaffold's surface.
97 Finally, the collected bacteria cells were put on LB agar plates and incubated for a period of 16
98 hours at 37 °C.

99 To get the SEM image of bacteria, the bacterial suspensions (*S. aureus*) were exposed to
100 the surface of the scaffold by the method mentioned above, followed by a thorough washing of
101 the scaffold with sterile 0.9% saline solution and fixed with Karnovsky's fixative (2.5 wt%
102 glutaraldehyde in 0.2 M PBS buffer) for 3 hours. The dehydration step of the samples was
103 carried out by sequential immersion in water/ethanol (30, 50, 60, 70, 80, 90, 100%), and kept in a
104 desiccator (below 30 °C) for 12 hours to dry. Finally, the samples were sputter-coated with
105 platinum and were imaged by SEM.

106 **1.7. *In vitro* blood coagulation test**

107 According to reported literature¹, the nanofiber scaffolds and medical gauze (served as a control)
108 were cut into a circular pattern (approximately 20 mm in diameter). The experimental part was
109 initiated with the casting of 100 μ L of blood (comprising 10% sodium citrate by volume) onto
110 the upper surface of individual samples and subjected to incubation at 37 °C for 5 min. The

111 samples were mildly rinsed in 50 mL of distilled water to separate uncoagulated red blood cells.
112 Drabkin's reagents (D5941 Sigma-Aldrich) were employed for quantitative estimation of blood
113 coagulations on each scaffold in compliance with the manufacturer's guidelines of the same. The
114 absorbance values of individual samples were measured at a wavelength of 540 nm in a UV
115 spectrophotometer. Other than that, the assessment of blood clotting time was done in
116 accordance with the previously reported study¹. The medical gauze and the scaffolds with
117 coagulated blood was air dried for 4 hours at 37 °C. Then the samples were fixed in 0.25%
118 glutaraldehyde for 45 minutes. After fixation the samples were subjected to alcohol gradation
119 (50%, 70%, 90% and 100%) for 10 minutes at each step. Finally, the samples were air dried and
120 studied by SEM imaging.

121 **1.8. Cell culture**

122 Under an atmospheric condition of 5% CO₂ and a temperature of 37 °C, a mouse
123 fibroblast cell line L929 was cultured in Dulbeccos modified eagle medium (DMEM) with the
124 subsequent addition of 10 wt% fetal bovine serum and 1wt% antibiotic. Coverslips were coated
125 by scaffold and stationed onto 24 well cell culture plates. The cells in the culture flask were
126 disengaged by trypsin-EDTA and subsequently seeded on the scaffold at a density of 1.5×10^4
127 cells per well.

128 **1.9. *In vitro* biocompatibility, cell adhesion, and proliferation studies**

129 An MTT assay (3-[4,5-dimethylthiazol-2-yl]-2,5-diphenyl tetrazolium bromide) was
130 engaged to estimate the biocompatibility of the scaffold at different culture duration up to 72
131 hours for three times. MTT solution was subsequently added to each well and was subjected to
132 incubation for 3 hours. The optical density of the formazan complex dissolved in dimethyl
133 sulfoxide was evaluated with a microplate reader at the wavelength of 570 nm. The percentage of
134 cell viability was determined by investigating the optical density of the control and samples.

135 The adhesion and proliferation of L929 fibroblast cells were assessed at regular time
136 intervals (day 1, 3, and 5) through fluorescein diacetate staining. First, the scaffolds with cells
137 were removed from the culture medium and washed with PBS. The cells, after thorough
138 washing, were incubated with FDA solution (10 µg/mL) for 30 min and again washed with PBS.
139 Finally, the obtained cells were viewed with a Leica fluorescence microscope.

140 For SEM analysis, the scaffolds with cells were removed from the culture medium and
141 washed with PBS, followed by incubation with 4% paraformaldehyde for 30 min. The scaffolds
142 were dehydrated in a graded series of ethanol solutions and dried overnight. The dehydrated
143 scaffolds were examined under SEM at 5 kV accelerating voltage.

144 **1.10. *In vivo* wound healing experiments**

145 For excisional wound healing investigation, healthy male Wistar rats of weight 200–230
146 g were chosen. All the experimental procedures were done before the approval of the
147 Institutional Animal Ethical Committee (Department of Zoology, University of Calcutta, India,
148 885/GO/RE/S/05/CPCSEA). An intraperitoneal administration of ketamine (35 mg/kg) and
149 xylazine (5 mg/kg) was done to anesthetize individual animals. A complete thickness excision
150 wound was made by excising the dorsal skin of rats after shaving the dorsal surface and
151 disinfecting it with 70% ethanol. 18 Wister rats were subdivided into three groups (six rats per
152 group). Group 1 (control) rats were tended with gauze, while group 2 and 3 were tended with
153 scaffold 1 and 3 respectively. In order to keep the healing material on the incised area, scaffolds
154 were additionally enveloped with gauze and fixed with a bandage. Photographs of wounds were
155 taken on days 3,7 and 10 after the wound incision. Wound size was traced with the equipment of
156 a transparent sheet, followed by a new dressing. The wound closure percentage was determined
157 by the following formula.

$$C_n = \frac{(S_0 - S_n)}{S_0} \times 100 \dots\dots\dots (3)$$

158

159 Where C_n is the percentage of wound size reduction on days 3, 7, and 10 post-wounding, S_0 is
160 the initial wound area, and S_n is the wound area on days 3, 7, and 10 post-wounding.

161 **1.11. Histological analysis**

162 On day 3, 7, and 12 after surgery, a full-thickness skin biopsy was taken from the center
163 of wounds with surrounding tissues. Tissue samples were fixed in 10% formalin for histological
164 analysis of tissue samples, and these were embedded in paraffin wax after dehydration using a
165 series of graded alcohol. The tissues were sectioned at 5 μm for hematoxylin and eosin (H&E)
166 and Masson–Goldner trichrome (MGT) staining.

167 **1.12. Biochemical Assays**

168 Malondialdehyde (MDA) levels in the tissue were determined by mixing 0.5 mL of
169 homogenate with 2.5 mL of trichloroacetic acid (20%) and 1.0 mL of thiobarbituric acid (0.6%).
170 The mixture was heated for 30 min in a boiling water bath, cooled, and centrifuged at 3000 g for
171 10 min. The absorbance was measured at 535 nm².

172 Superoxide dismutase activity was determined by method according to literature³. The
173 reaction mixture composed of 80 mM Tris (pH 8.9), 0.12 mM EDTA, 10.8 mM TEMED,
174 0.003% BSA, 30 μM riboflavin in 5 mM KOH, 300 μM NBT (SRL, 11207), 50 μL supernatant
175 was added. It was kept under light (150 W) for 2 min, and the absorbance was taken at 560 nm.
176 A blank without enzyme and light showed NBT present in the reaction mixture. Unit SOD was
177 calculated as U/mg protein.

178 The rate of decomposition of hydrogen peroxide (H₂O₂) at 240 nm absorbance over 1 min
179 was used to assess catalase activity in the wound tissue biopsy samples according to the
180 literature⁴. Catalase activity was expressed as U/g protein.

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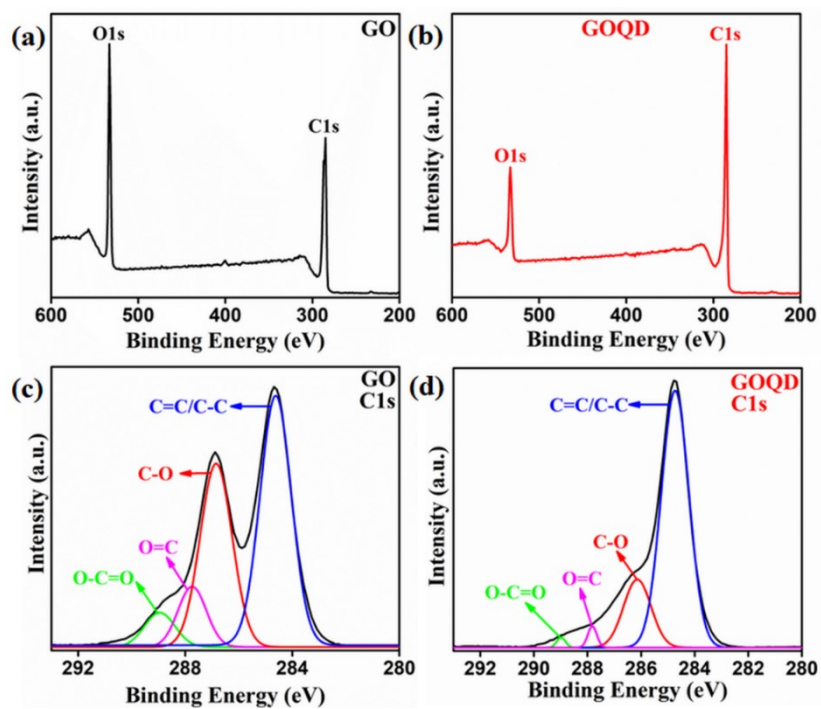
183 **1.13. ELISA**

184 Proteins were isolated from wound tissue biopsy samples in RIPA buffer. Then levels of
185 inflammatory cytokines IL-6, TNF- α , and IL-1 β were measured by using ELISA using a
186 commercial kit from Sigma.

187 **2.20. Statistical Analysis**

188 Each and every experimental sets were conducted thrice with data written in the form of average
189 \pm standard deviation. Statistical analysis was executed by one-way ANOVA with Tukey's post
190 hoc test by employing Origin Pro 8.0. P values < 0.05 were assessed to be statistically
191 noteworthy.

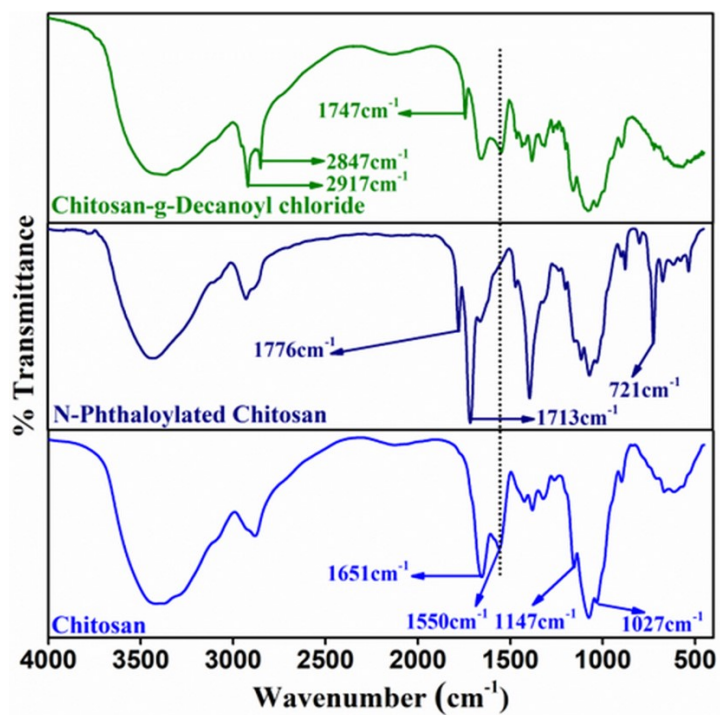
192 **Supplementary Figures**



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194 **Figure S1.** XPS survey spectra of GO (a) and GOQD (b). High-resolution C1s peaks of GO (c)

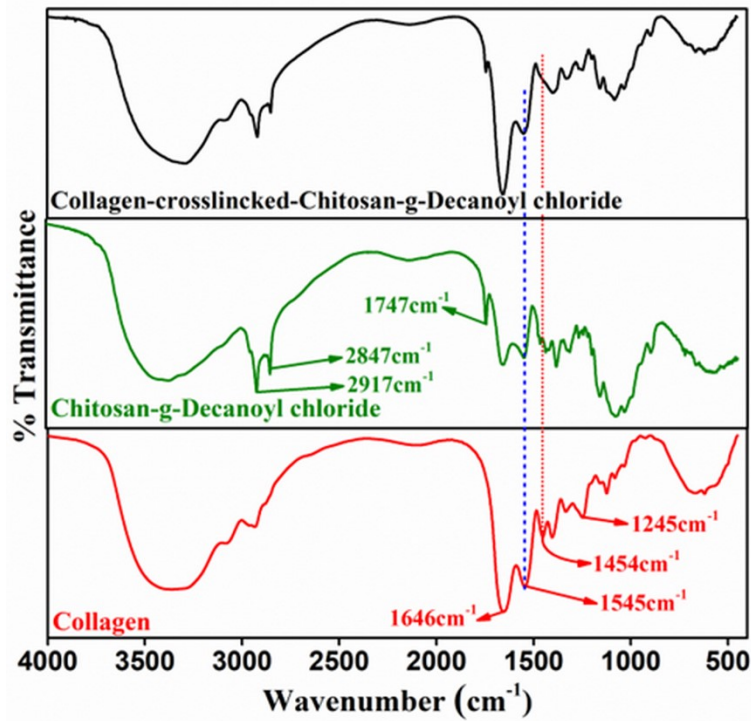
195 and GOQD (d).



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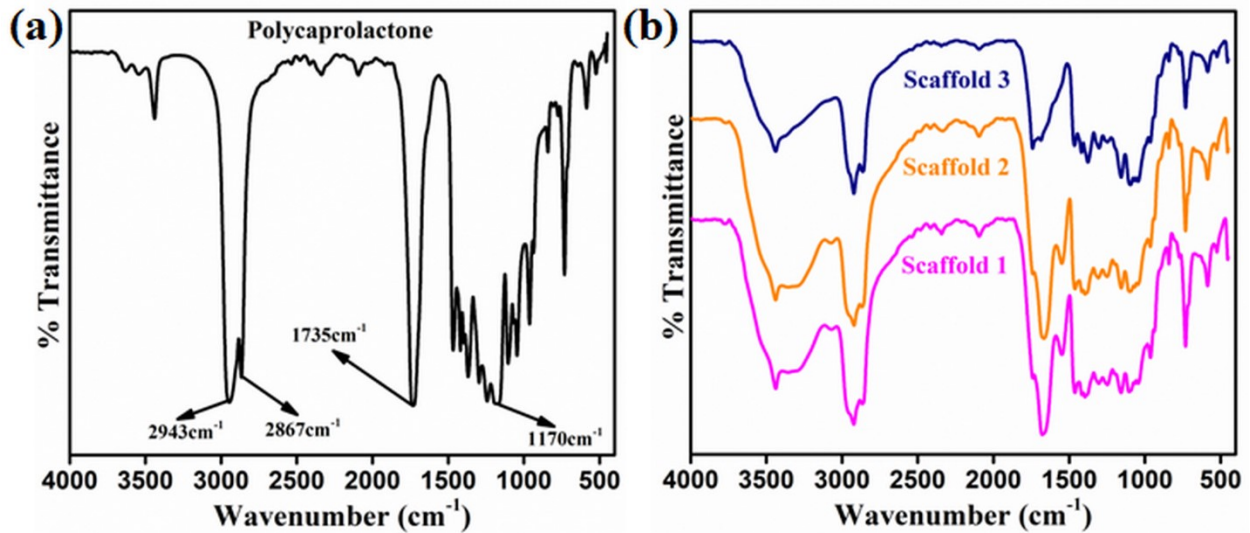
Figure S2. FTIR spectroscopy of chitosan, N-phthaloylated chitosan, and CS-g-Dc.



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Figure S3. FTIR spectroscopy of collagen, CS-g-Dc, and CG-cross-CS-g-Dc.



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Figure S4. FTIR spectroscopy of polycaprolactone (a) and scaffold 1, 2, and 3 (b).

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