

Selective Detection of Membrane-Bound Amyloid- β Oligomers Using SERS “Hot-Spots”: Toward Early
Diagnostics of Alzheimer’s Disease

Supporting Information

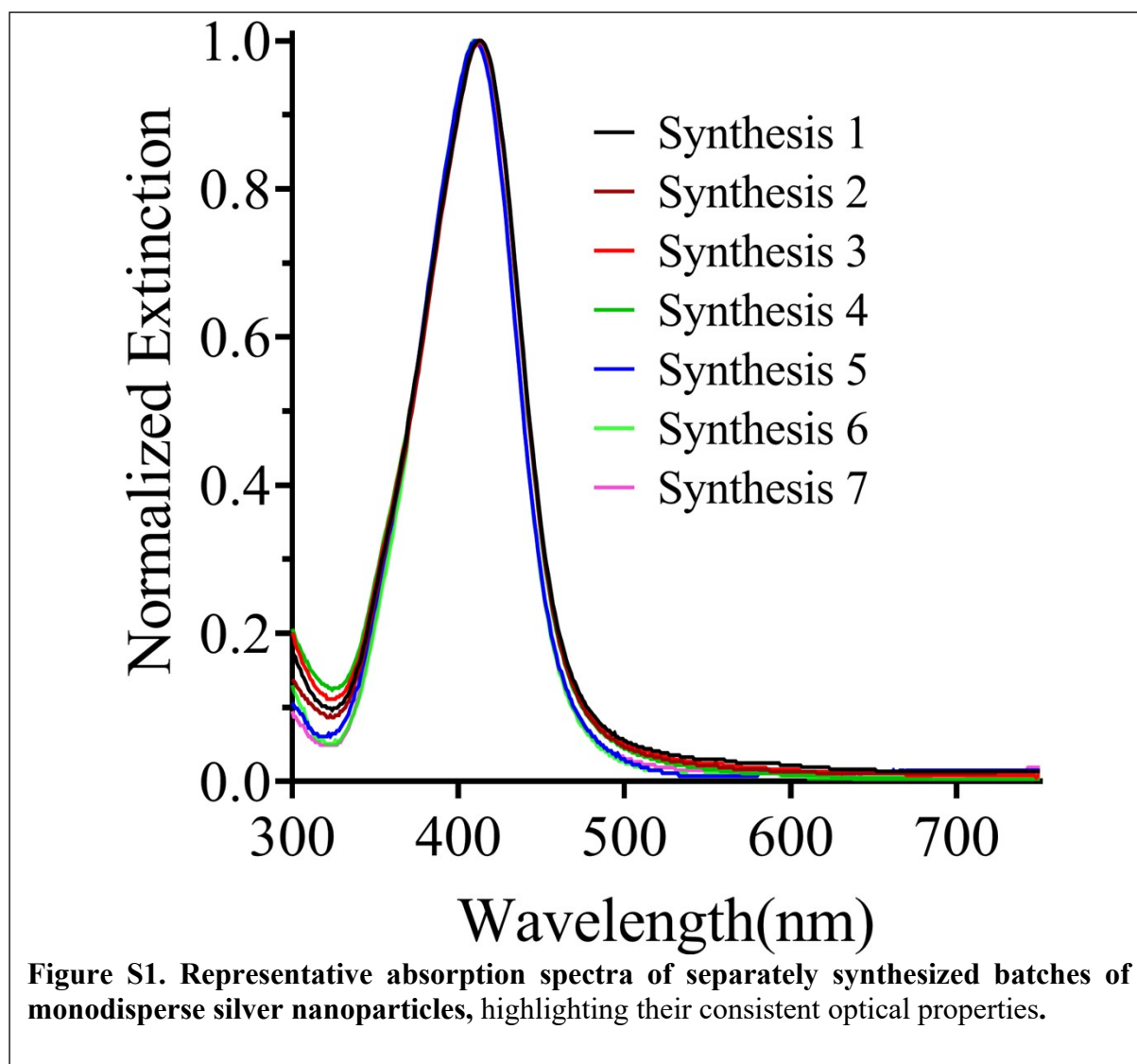
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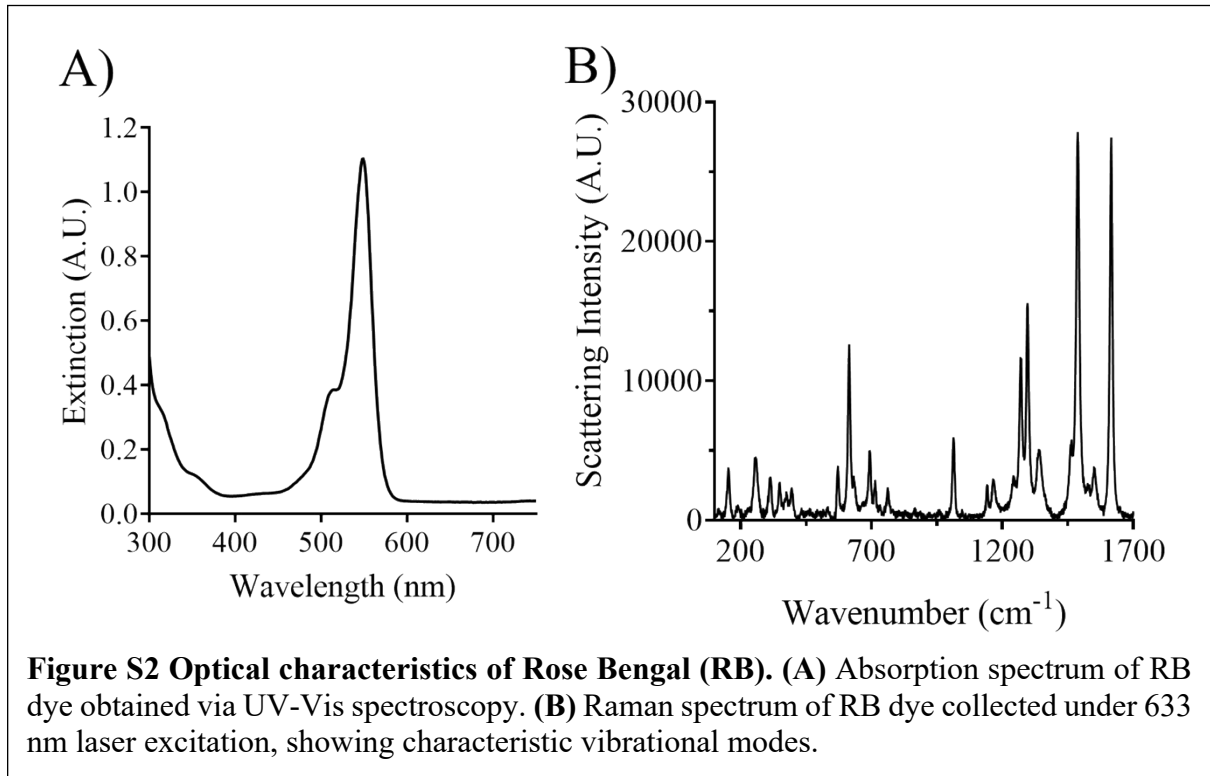
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Loading of Rose Bengal dye on AgNP-construct

In the absorbance spectra of the RB-nanoconstructs, a prominent peak was observed at 550 nm across different activation times. Using Beer-Lambert's Law $A = \epsilon Cl$, where A is absorbance (a unitless measure of light absorbed), ϵ is the molar absorptivity or extinction coefficient, l is the path length or thickness of the absorbing medium in centimeters, and C is the molar dye concentration; the concentrations of RB were calculated. The resulting concentrations were 314 nM, 68 nM, and 41 nM for constructs activated for 5, 10, and 15 minutes, respectively.

$$C \text{ (5minutes activation)} = \frac{A}{\epsilon l} = \frac{0.030798}{98,000} = 314 \text{ nM}$$

$$C \text{ (10minutes activation)} = \frac{A}{\epsilon l} = \frac{0.006657}{98,000} = 68 \text{ nM}$$

$$C \text{ (15 minutes activation)} = \frac{A}{\epsilon l} = \frac{0.004031}{98,000} = 41 \text{ nM}$$

Using the same Beer-Lambert equation, the concentration of the RB-nanoconstructs was also calculated to be 0.12 nM = 120 pM.

$$\text{Number of RB molecules per AgNP} = \frac{\text{Concentration of RB dye on the construct}}{\text{Concentration of RB - nanoconstruct}},$$

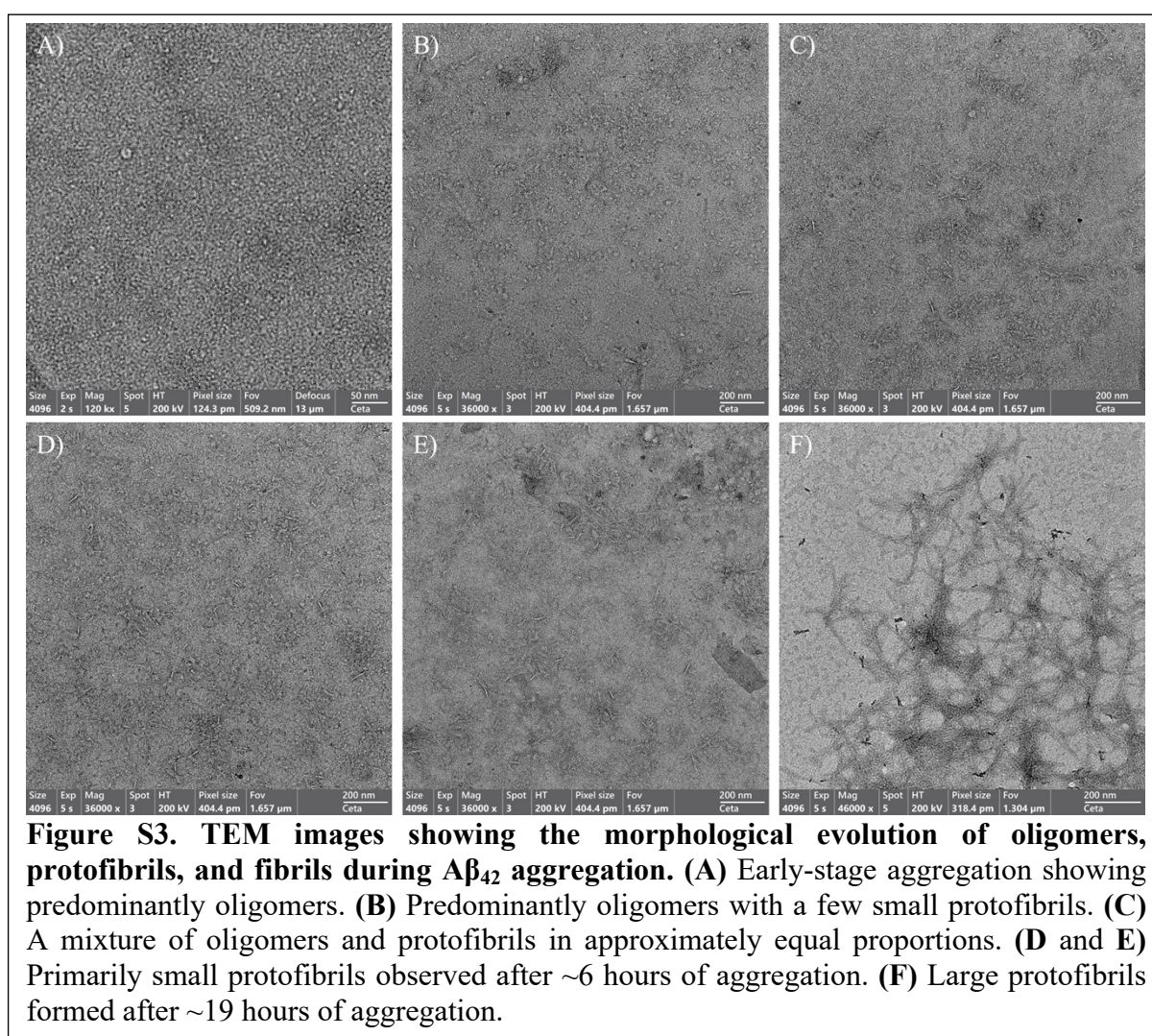
$$\text{RB molecules per AgNP (5 minute activation)} = \frac{314 \text{ nM}}{0.12 \text{ nM}} = 2617$$

$$\text{RB molecules per AgNP (10 minute activation)} = \frac{68 \text{ nM}}{0.12 \text{ nM}} = 567$$

$$RB \text{ molecules per AgNP (15 minute activation)} = \frac{41 \text{ nM}}{0.12 \text{ nM}} = 342$$

Table S1: Calculation of loading of Rose Bengal dye molecules on RB-nanoconstruct.

Activation time	Concentration of RB per 120 pM AgNP	Number of RB per nanoparticle
5 minutes	314 nM	2617
10 minutes	68 nM	567
15 minutes	41 nM	342



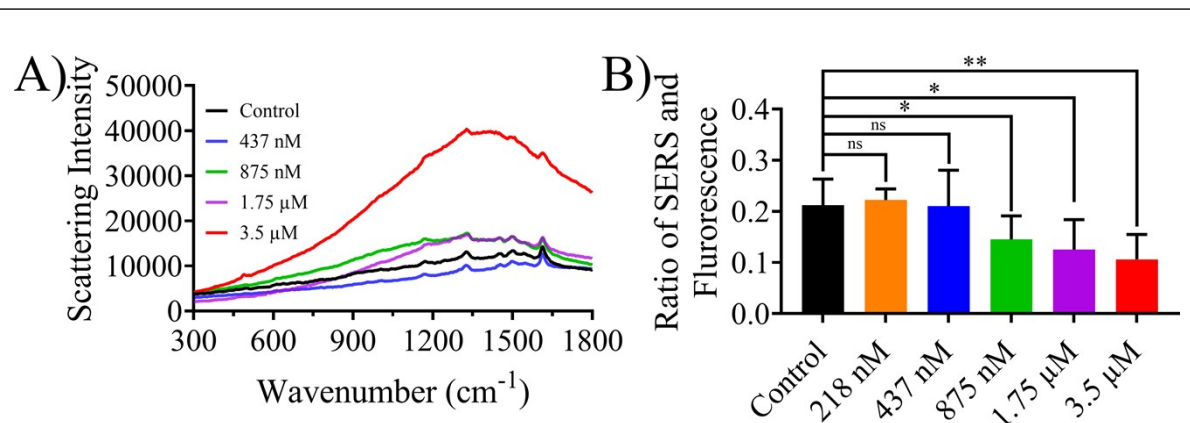
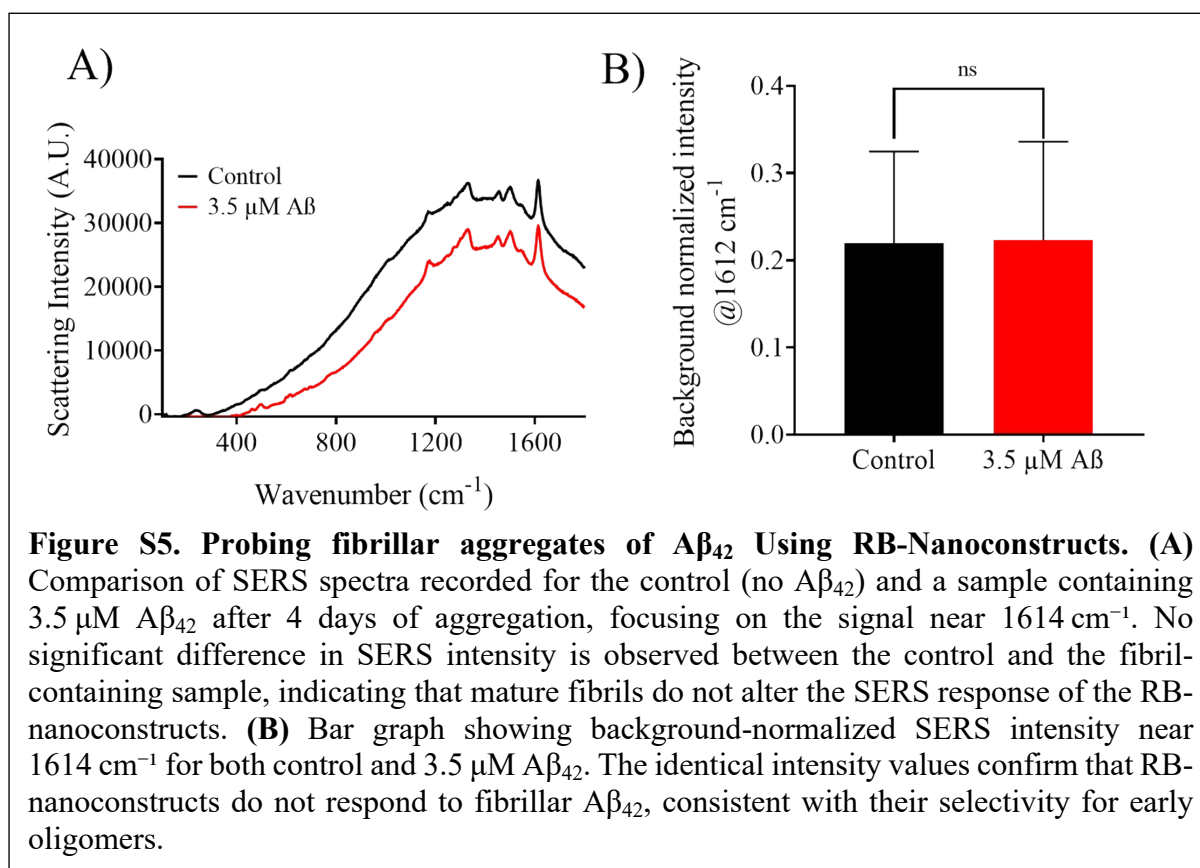


Figure S4. Probing Small Oligomers of Aβ₄₂ Using RB-Nanoconstructs. (A) Representative spectra illustrating the variation in SERS intensity at ~1614 cm⁻¹ with different concentrations of Aβ₄₂ oligomers. As the concentration of Aβ₄₂ decreased from 3.5 μM to 437 nM, the SERS signal at ~1614 cm⁻¹ increased, while the fluorescence background decreased, indicating reduced interaction between oligomers and the RB-nanoconstructs. (B) Bar graph quantifying the ratio of SERS intensity to fluorescence at ~1614 cm⁻¹ for varying oligomer concentrations, measured after 1 hour of peptide aggregation. A clear increase in the SERS-to-fluorescence ratio is observed as the concentration of soluble oligomers decreases, consistent with reduced RB displacement from the nanoparticle surface.



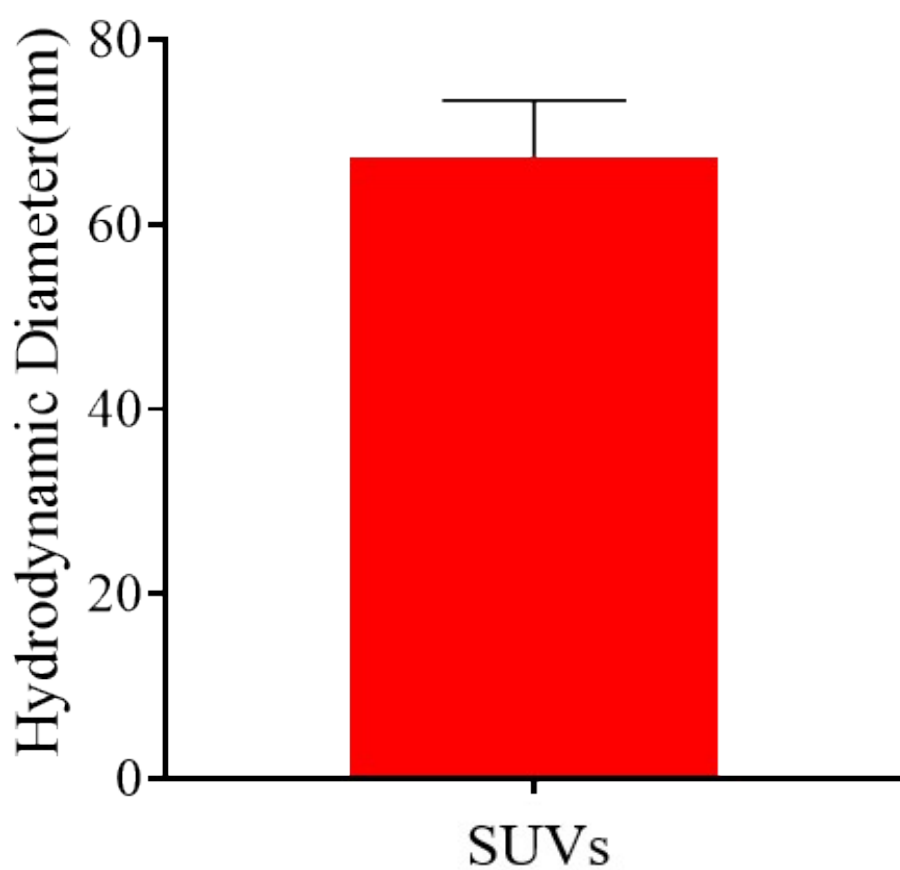
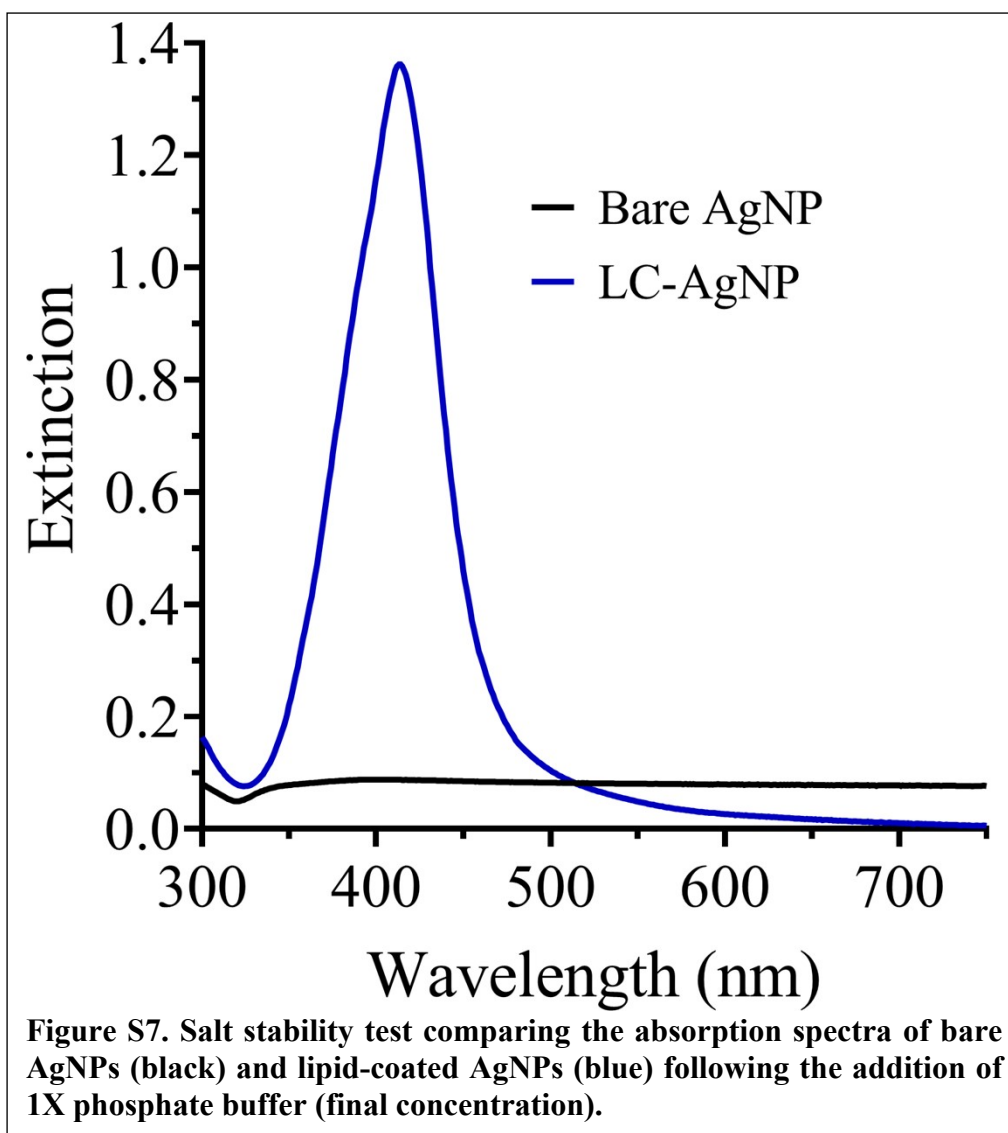


Figure S6. Hydrodynamic diameter of SUVs (67 ± 6 nm) measured using Dynamic Light Scattering.



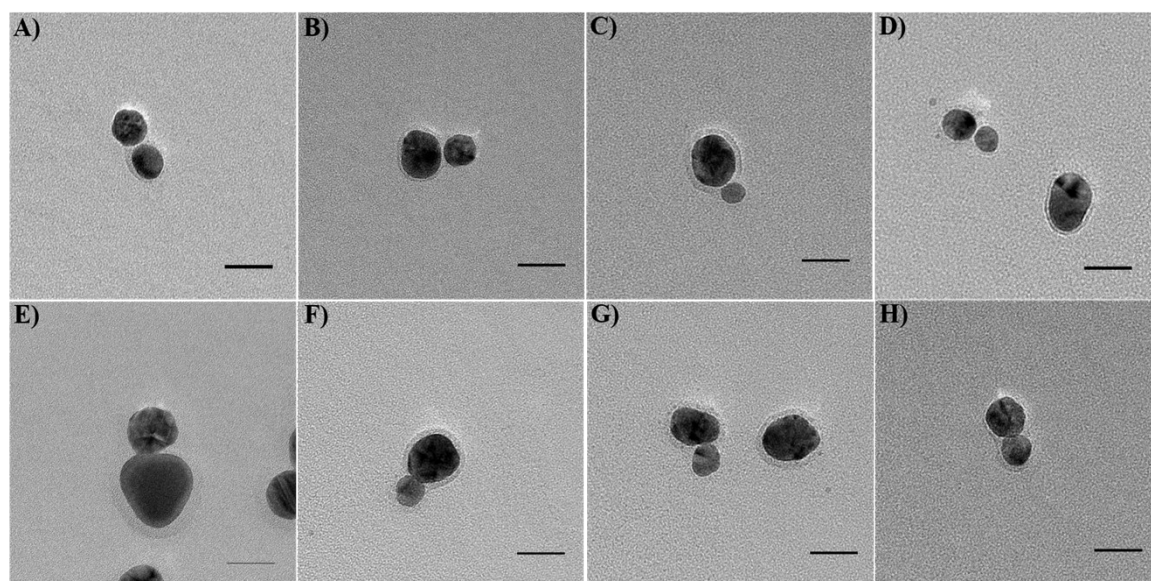


Figure S8. TEM images showing the formation of SERS “hot spots” during interactions between A β -loaded lipid-coated AgNPs (LC-AgNPs) and Rose Bengal-functionalized silver nanoparticles (RB-AgNPs). Two distinct interaction patterns were observed: separated configurations with a visible interparticle gap (panels A–D) and overlapping configurations (panels E–H). The transparent layer surrounding the AgNPs in the LC-AgNPs (but absent in RB-AgNPs) indicates the presence of a lipid bilayer. Scale bar: 25 nm.

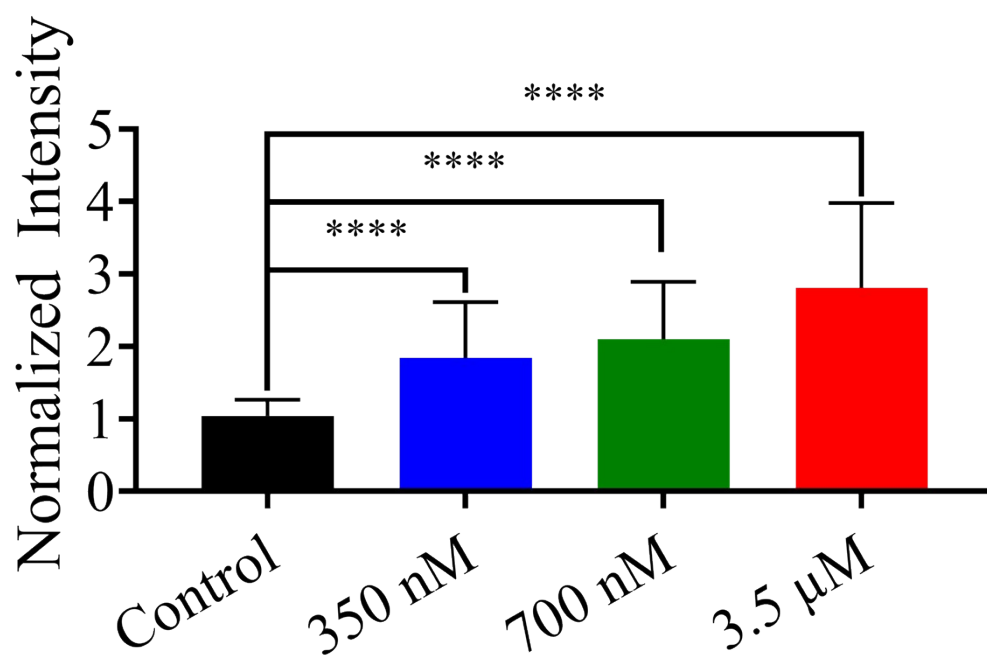


Figure S9. Increase in the RB-SERS with increasing loading of Aβ₄₂ oligomers on LC-AgNP. Bar graph quantifying the normalized SERS intensity of RB for lower concentrations (3.5 μM, 700 nM, 350 nM) of Aβ₄₂ oligomer at ~1614 cm⁻¹.

Calculation for the number of A β ₄₂ being detected:

The prolate-shaped diffraction-limited spot in our experimental setup has a radius along the z-axis:

$$R_z = \frac{2n\lambda}{N_A^2} = \frac{2 \times 1.33 \times 532}{0.5^2} = 5660 \text{ nm}$$

The radius along the lateral (short) axes is:

$$R_{xy} = \frac{0.61 \times \lambda}{N_A} = \frac{0.61 \times 532 \text{ nm}}{0.5} = 649 \text{ nm}$$

The volume of this diffraction-limited focal region is:

$$V = \frac{4}{3}\pi \times a \times b \times c = \frac{4}{3}\pi \times 649 \times 649 \times 5660 \text{ nm}^3 = 9986066046 \text{ nm}^3$$

$$\text{Now, } 1 \text{ nm}^3 = 10^{-24} \text{ liters} = 10^{-9} \text{ fL}$$

and,

$$V = 9.986 \text{ fL}$$

Estimating the Number of Particles in the Focal Volume

For a concentration of **0.3 nM**, the number of particles within this 9.986 fL Volume is calculated as follows:

$$\text{Concentration } C = 0.3 \text{ nM} = 0.3 \times 10^{-9} \text{ mol/L}$$

$$\text{Volume } V = 9.986 \text{ fL} = 9.986 \times 10^{-15} \text{ L}$$

$$\text{Avogadro's number } N_A = 6.022 \times 10^{23} \text{ particles/mol}$$

$$\text{Moles} = C \times V = (0.3 \times 10^{-9}) \times (9.986 \times 10^{-15}) = 2.996 \times 10^{-24} \text{ mol}$$

$$\text{Number of particles} = \text{moles} \times N_A = 2.996 \times 10^{-24} \times 6.022 \times 10^{23} = 18.04 \times 10^{-1} = 1.8$$

Therefore, during a 10-second data acquisition, on average, 1.8 LC-AgNP particles are present in the focal volume. This is equivalent to acquiring data from 1 particle over 18 seconds, assuming linear scaling.

Diffusion Characteristics of LC-AgNPs

The diffusion constant D is given by the Stokes-Einstein equation:

$$D = \frac{k_B T}{6\pi\eta r}$$

Where k_B is the Boltzmann constant = $1.380649 \times 10^{-23} \text{ J/K}$, T is the absolute temperature (in Kelvin), η is the dynamic viscosity of the fluid (in Pa·s), r is the radius of the particle (in meters).

$$D = \frac{1.380649 \times 10^{-23} \text{ J K}^{-1} \times 297.15 \text{ K}}{6 \times \pi \times 0.0009107 \text{ Pa.s} \times 23 \times 10^{-9} \text{ m}} = 1.04 \times 10^{-11} \text{ m}^2 \text{ s}^{-1}$$

Diffusion Time Through Focal Volume

Using the relation $\langle r^2 \rangle = 4 \times D \times \tau_D$, and the lateral radius $r = 649 \text{ nm}$:

$$\tau_D = \frac{\langle r^2 \rangle}{4D} = \frac{(649 \times 10^{-9})^2 \text{ m}^2}{4 \times 1.04 \times 10^{-11} \text{ m}^2 \text{ s}^{-1}} = \frac{1.012 \times 10^{-13}}{10^{-11}} \text{ s} = 10.13 \text{ msec}$$

Assuming each LC-AgNP leaves the focal volume after this diffusion time and does not return within the 18-second data acquisition period, the maximum number of distinct LC-AgNPs detected in this time is:

$$\frac{18 \text{ sec}}{10.13 \text{ msec}} = 1777 \text{ particles.}$$

Signal Scaling with A β ₄₂ Concentration

Therefore, at a sample concentration of 3.5 μM $\text{A}\beta_{42}$, the data could include signals from up to 1777 $\text{A}\beta_{42}$ -loaded LC-AgNPs. Therefore, at the detection limit of 218 nM $\text{A}\beta_{42}$, the number of detected $\text{A}\beta_{42}$ -loaded LC-AgNPs is: $(1777 \times 218 \text{ nM} \div 3500 \text{ nM}) = 110$.

Thus, at our detection limit, an average of 110 $\text{A}\beta_{42}$ -loaded LC-AgNPs contributes to the measured signal during each 10-second.

Table S2: Comparison of the our SERS-based detection platform with other reported methods for detecting lipophilic- $\text{A}\beta_{42}$ oligomers.

Sl. No.	Reference	Method of Detection	Target Species	Detection Limit	Specificity towards lipophilic/ vesicle associated oligomers
1	High performance plasma amyloid- β biomarkers for Alzheimer's disease. <i>Nakamura et al., 2018, Nature, 554, 249-254.</i>	Immunoprecipitation-mass spectrometry	$\text{A}\beta_{42}$, $\text{A}\beta_{40}$, $\text{APP}_{669-711}$ (ratios)	Lower limit based on standard curves ($\sim 40 - 160$ pM range, depending on peptide).	No: Targets primarily soluble peptides; no focus explicitly on oligomeric or membrane-bound forms.
2	New ELISAs with high specificity for soluble oligomers of amyloid β -protein detect natural $\text{A}\beta$ oligomers in human brain but not CSF. <i>Yang et al., Alzheimer's & Dementia, 2013, 9, 99-112.</i>	Sandwich ELISA	Soluble $\text{A}\beta$ oligomers	~ 39 pg/ml (using synthetic $\text{A}\beta$ dimer standards)	No: Explicitly targets soluble oligomers in brain extracts; no mention of membrane-associated forms.
3	Subtyping of circulating exosome-bound amyloid β reflects brain plaque deposition. <i>Lim et al., Nature Communication, 2019, 10, 1144.</i>	Amplified plasmonic exosome platform (with SPR)	Exosome-carrying prefibrillar $\text{A}\beta_{42}$ aggregates ($\text{A}\beta_{42}^+$ and CD63^+ exosomes).	~ 200 exosomes (10^5 -fold improvement over Western blot; 10^3 -fold over standard ELISA).	Yes: Targets $\text{A}\beta$ oligomers bound to exosomes (smallest of the extra-cellular vesicles); distinct from free soluble oligomers.
4	Bifunctional Fluorescent/ Raman Nanoprobe for the Early Detection of Amyloid. <i>Xia et al., Nature Scientific Report, 2019, 9, 8497.</i>	Surface-enhanced Raman scattering and fluorescence.	$\text{A}\beta_{42}$ aggregates/ peptides.	Not explicitly stated; linear detection range $1-2$ μM (saturation > 2 μM).	No: No explicit distinction or preference for lipophilic forms.
5	Our method	Surface-enhanced Raman scattering	Lipophilic, membrane-bound small oligomers	~ 110 $\text{A}\beta_{42}$ -loaded-Lipid-bilayer coated AgNPs.	Yes: Specifically designed to detect lipophilic membrane associated $\text{A}\beta$

			of A β_{42}		oligomers.
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