

Selective Detection of Membrane-Bound Amyloid- $\beta$  Oligomers Using SERS “Hot-Spots”: Toward Early  
Diagnostics of Alzheimer’s Disease

Supporting Information

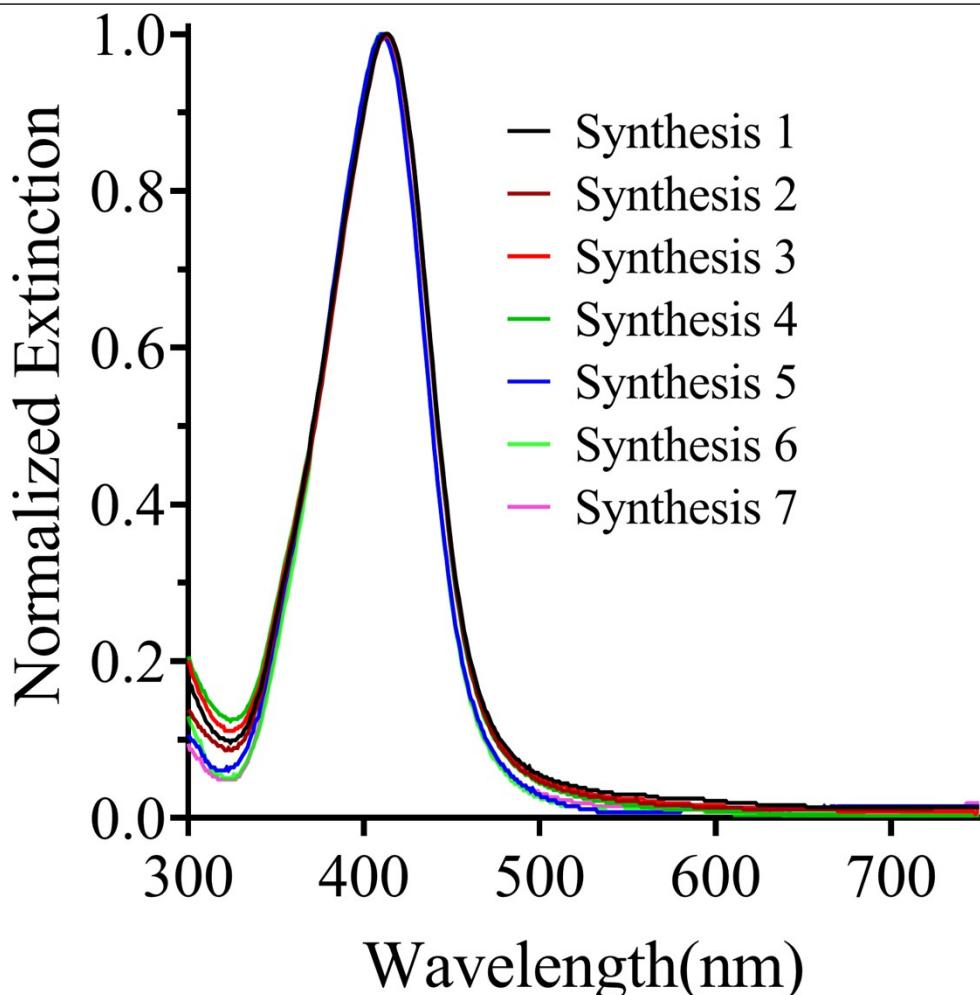
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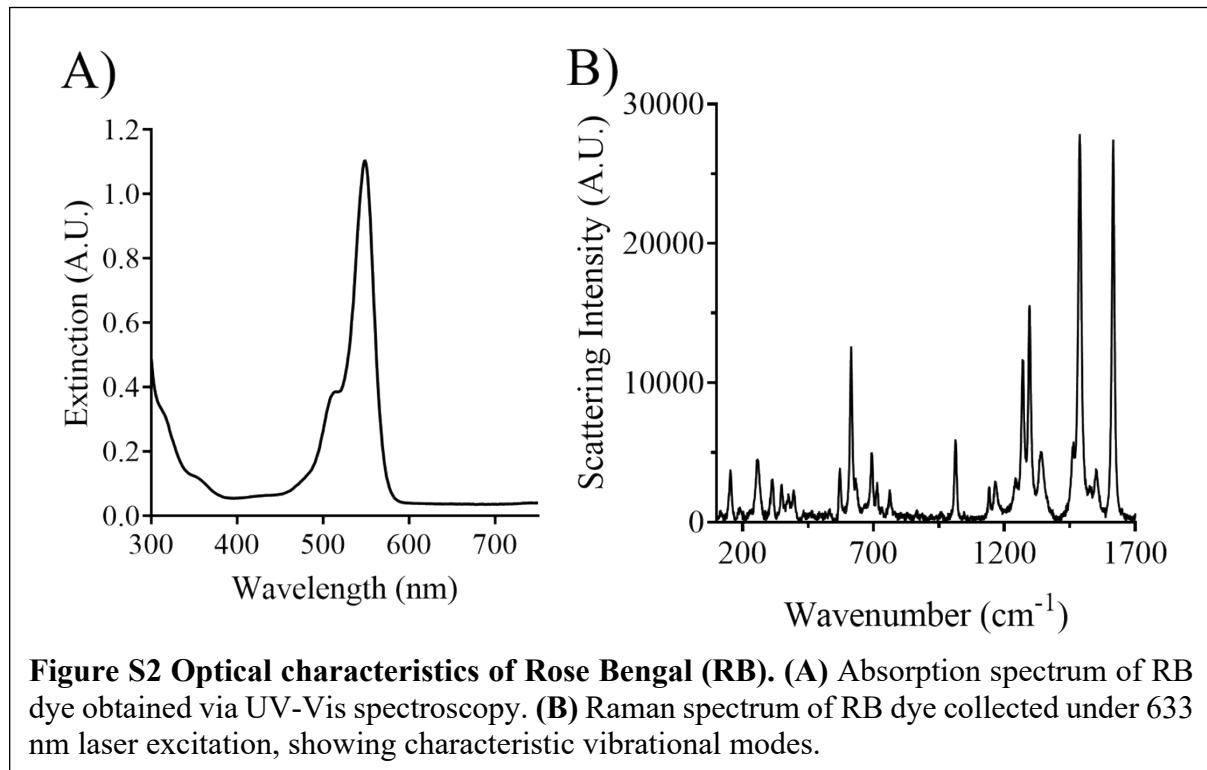
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**Figure S1.** Representative absorption spectra of separately synthesized batches of monodisperse silver nanoparticles, highlighting their consistent optical properties.



**Figure S2 Optical characteristics of Rose Bengal (RB).** **(A)** Absorption spectrum of RB dye obtained via UV-Vis spectroscopy. **(B)** Raman spectrum of RB dye collected under 633 nm laser excitation, showing characteristic vibrational modes.

#### Loading of Rose Bengal dye on AgNP-construct

In the absorbance spectra of the RB-nanoconstructs, a prominent peak was observed at 550 nm across different activation times. Using Beer-Lambert's Law  $A = \epsilon Cl$ , where A is absorbance (a unitless measure of light absorbed),  $\epsilon$  is the molar absorptivity or extinction coefficient,  $l$  is the path length or thickness of the absorbing medium in centimeters, and C is the molar dye concentration; the concentrations of RB were calculated. The resulting concentrations were 314 nM, 68 nM, and 41 nM for constructs activated for 5, 10, and 15 minutes, respectively.

$$C \text{ (5minutes activation)} = \frac{A}{\epsilon l} = \frac{0.030798}{98,000} = 314 \text{ nM}$$

$$C \text{ (10minutes activation)} = \frac{A}{\epsilon l} = \frac{0.006657}{98,000} = 68 \text{ nM}$$

$$C \text{ (15 minutes activation)} = \frac{A}{\epsilon l} = \frac{0.004031}{98,000} = 41 \text{ nM}$$

Using the same Beer-Lambert equation, the concentration of the RB-nanoconstructs was also calculated to be 0.12 nM = 120 pM.

$$\text{Number of RB molecules per AgNP} = \frac{\text{Concentration of RB dye on the construct}}{\text{Concentration of RB - nanoconstruct}},$$

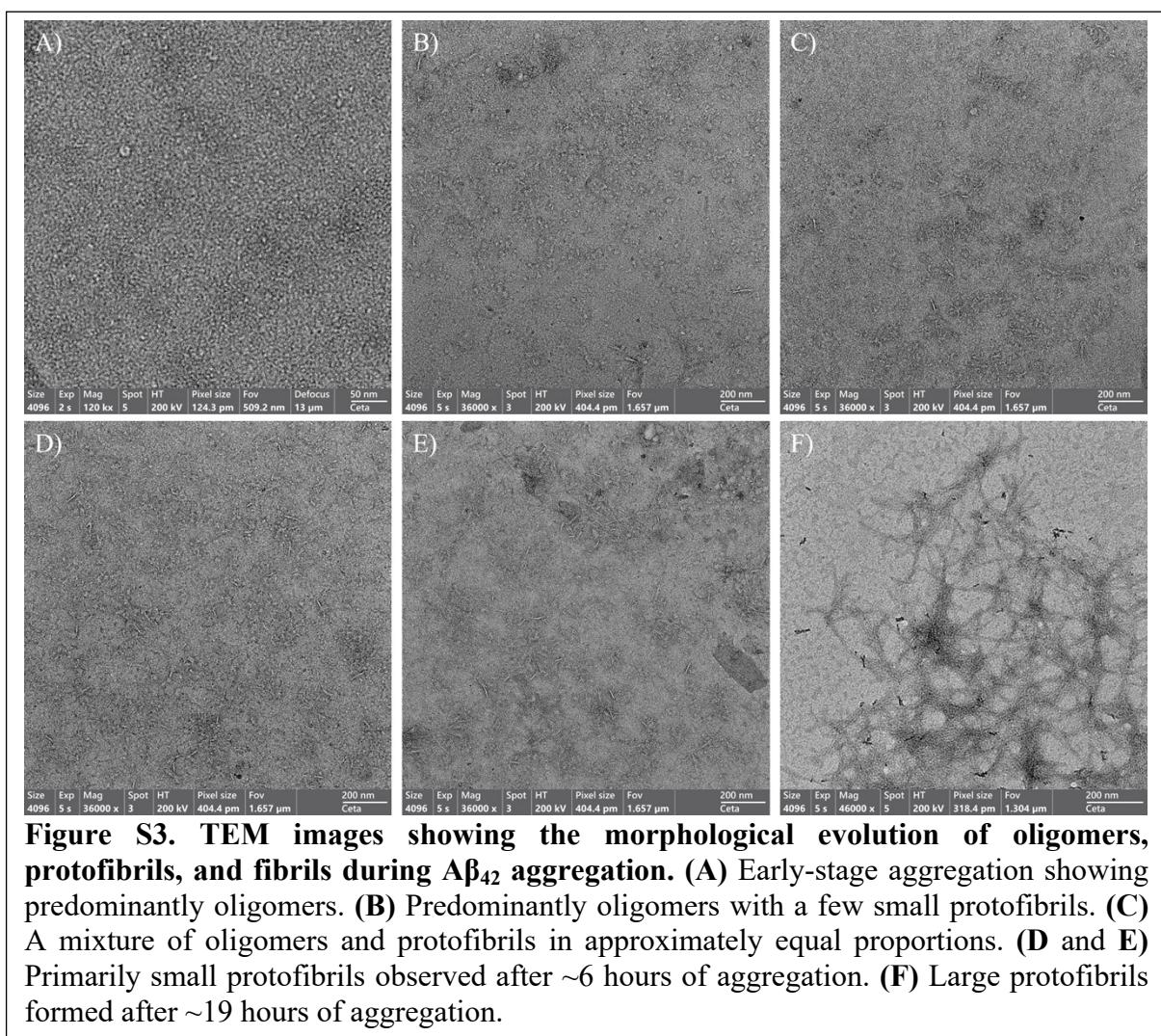
$$\text{RB molecules per AgNP (5 minute activation)} = \frac{314 \text{ nM}}{0.12 \text{ nM}} = 2617$$

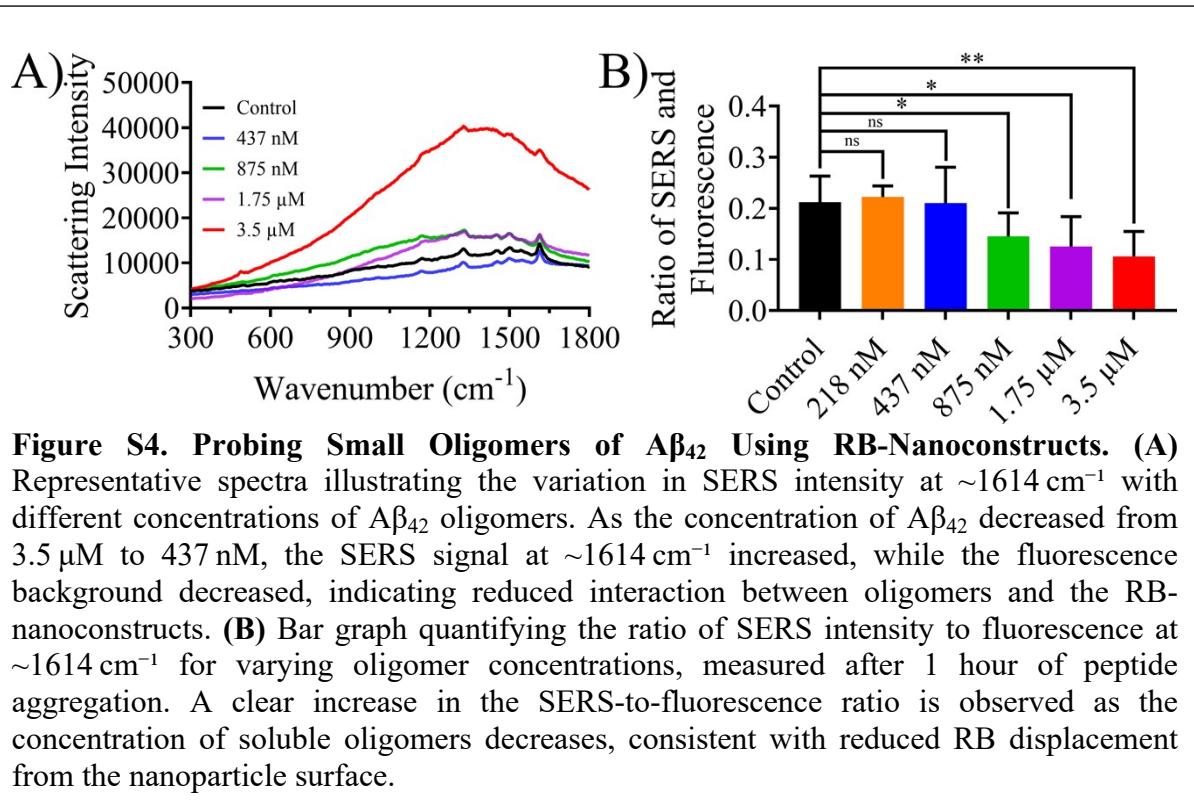
$$\text{RB molecules per AgNP (10 minute activation)} = \frac{68 \text{ nM}}{0.12 \text{ nM}} = 567$$

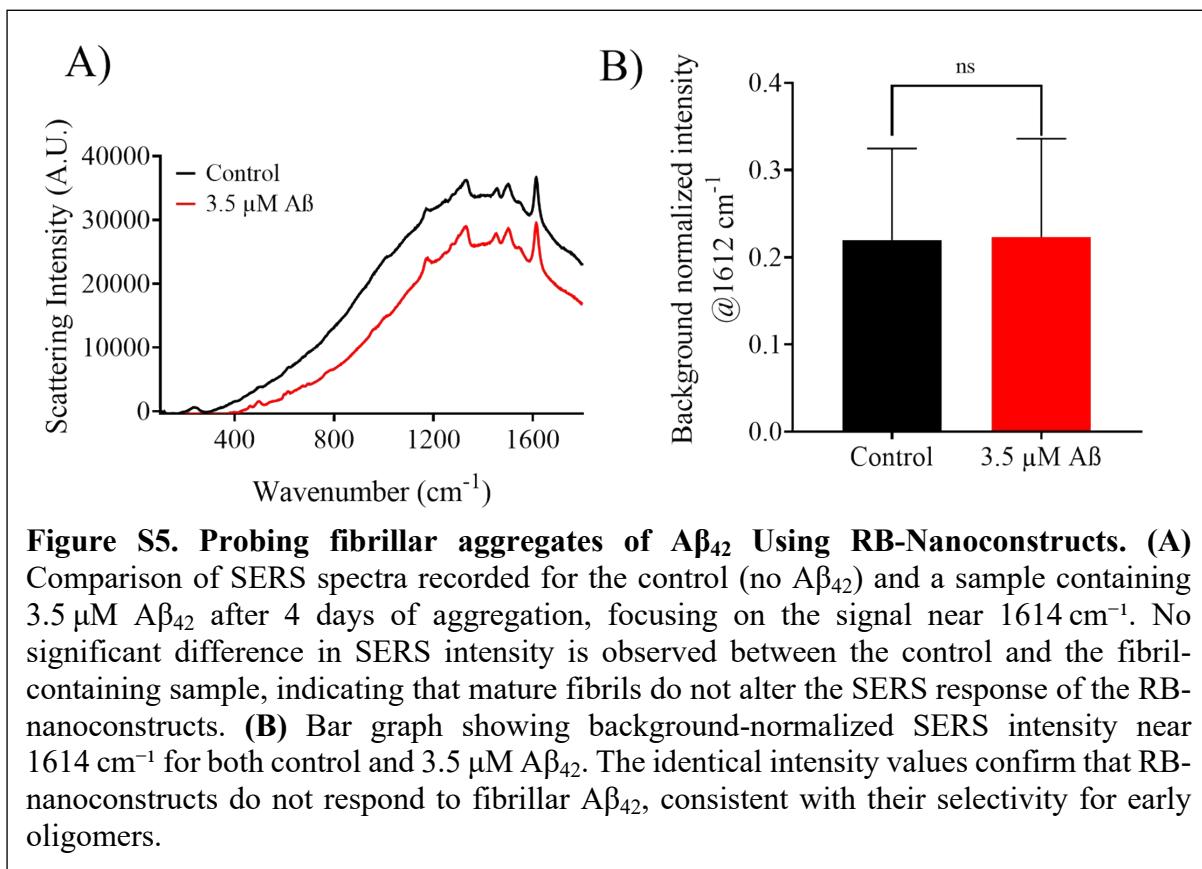
$$RB \text{ molecules per AgNP (15 minute activation)} = \frac{41 \text{ nM}}{0.12 \text{ nM}} = 342$$

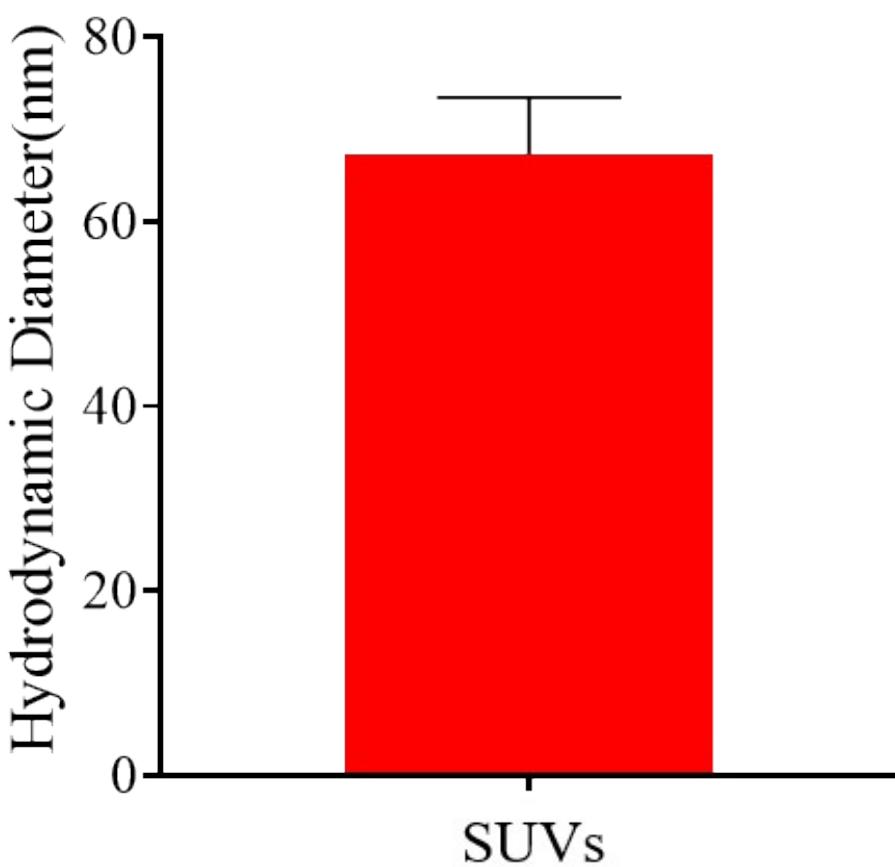
**Table S1:** Calculation of loading of Rose Bengal dye molecules on RB-nanoconstruct.

Activation time	Concentration of RB per 120 pM AgNP	Number of RB per nanoparticle
5 minutes	314 nM	2617
10 minutes	68 nM	567
15 minutes	41 nM	342

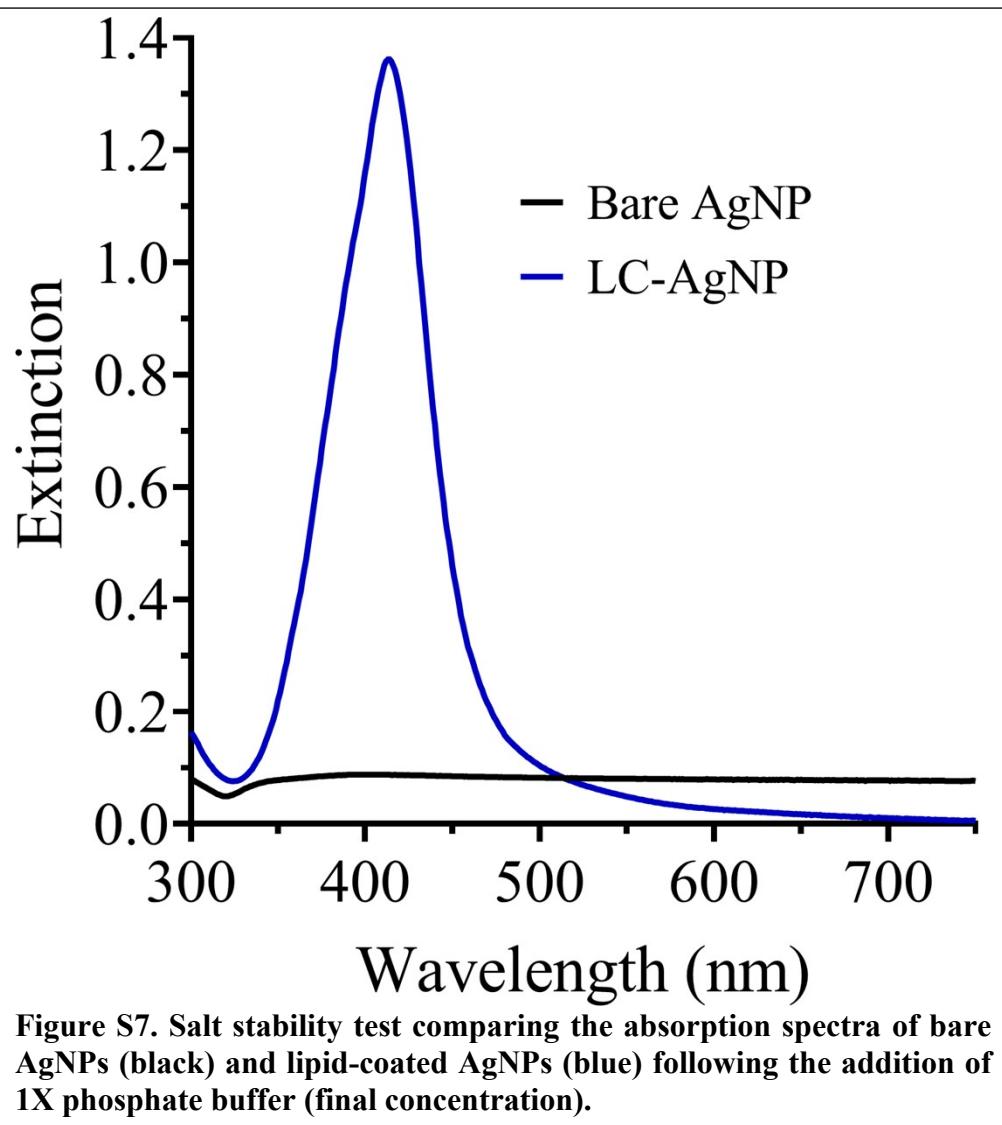


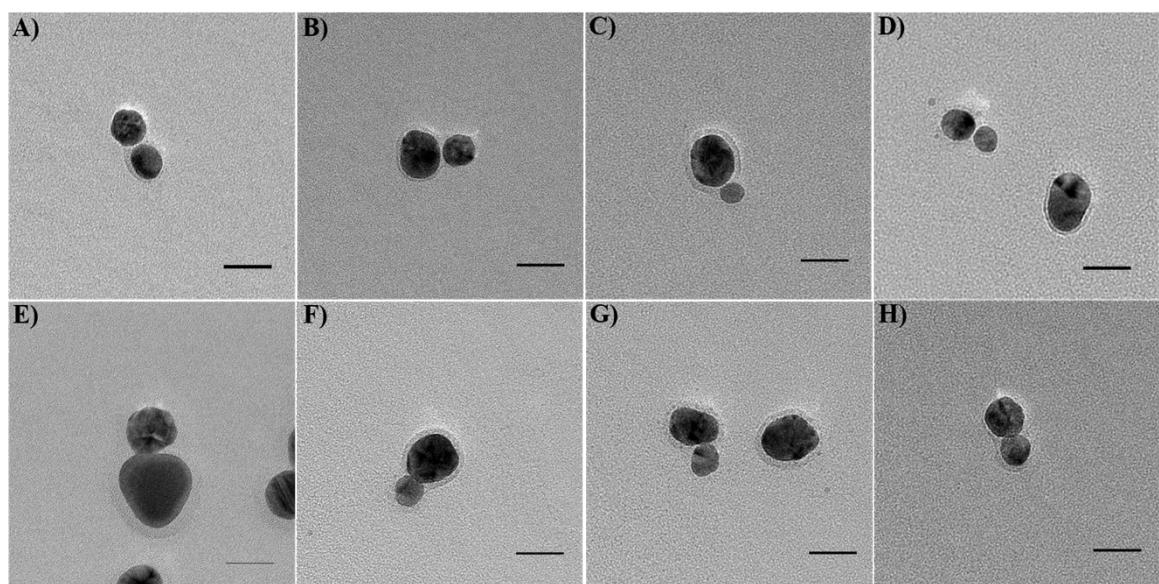




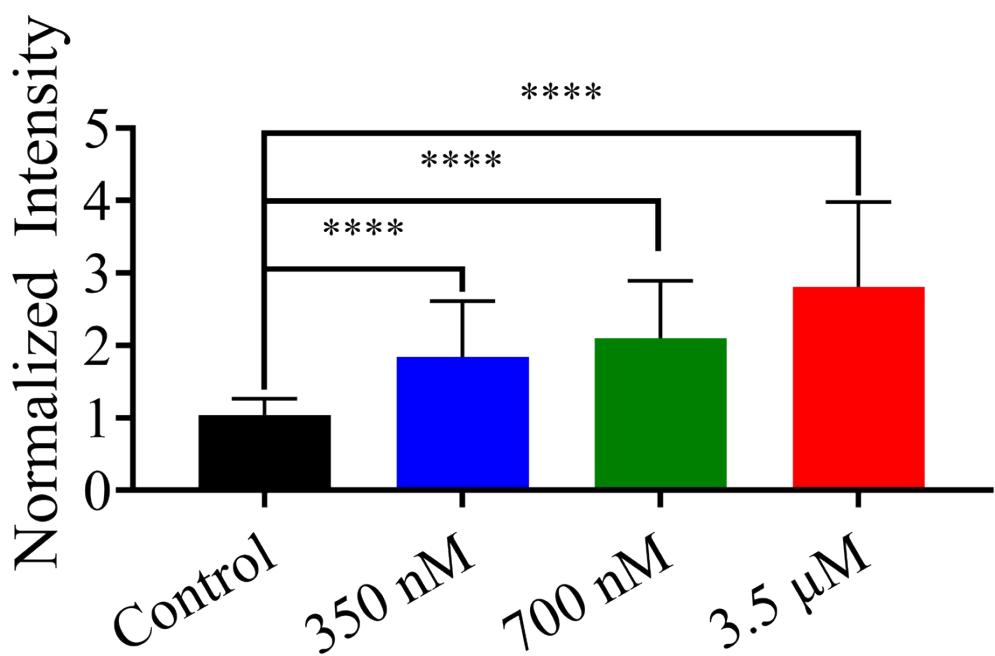


**Figure S6. Hydrodynamic diameter of SUVs ( $67 \pm 6$  nm) measured using Dynamic Light Scattering.**





**Figure S8.** TEM images showing the formation of SERS “hot spots” during interactions between  $\text{A}\beta$ -loaded lipid-coated AgNPs (LC-AgNPs) and Rose Bengal-functionalized silver nanoparticles (RB-AgNPs). Two distinct interaction patterns were observed: separated configurations with a visible interparticle gap (panels A–D) and overlapping configurations (panels E–H). The transparent layer surrounding the AgNPs in the LC-AgNPs (but absent in RB-AgNPs) indicates the presence of a lipid bilayer. Scale bar: 25 nm.



**Figure S9. Increase in the RB-SERS with increasing loading of A $\beta$ <sub>42</sub> oligomers on LC-AgNP.** Bar graph quantifying the normalized SERS intensity of RB for lower concentrations (3.5  $\mu$ M, 700 nM, 350 nM) of A $\beta$ <sub>42</sub> oligomer at  $\sim$ 1614  $\text{cm}^{-1}$ .

### Calculation for the number of A $\beta$ <sub>42</sub> being detected:

The prolate-shaped diffraction-limited spot in our experimental setup has a radius along the z-axis:

$$R_z = \frac{2n\lambda}{N_A^2} = \frac{2 \times 1.33 \times 532}{0.5^2} = 5660 \text{ nm}$$

The radius along the lateral (short) axes is:

$$R_{xy} = \frac{0.61 \times \lambda}{N_A} = \frac{0.61 \times 532 \text{ nm}}{0.5} = 649 \text{ nm}$$

The volume of this diffraction-limited focal region is:

$$V = \frac{4}{3}\pi \times a \times b \times c = \frac{4}{3}\pi \times 649 \times 649 \times 5660 \text{ nm}^3 = 9986066046 \text{ nm}^3$$

Now, 1 nm<sup>3</sup> = 10<sup>-24</sup> liters = 10<sup>-9</sup>fL

and,

$$V = 9.986 \text{ fL}$$

### Estimating the Number of Particles in the Focal Volume

For a concentration of 0.3 nM, the number of particles within this 9.986 fL Volume is calculated as follows:

$$\text{Concentration } C = 0.3 \text{ nM} = 0.3 \times 10^{-9} \text{ mol/L}$$

$$\text{Volume } V = 9.986 \text{ fL} = 9.986 \times 10^{-15} \text{ L}$$

$$\text{Avogadro's number } N_A = 6.022 \times 10^{23} \text{ particles/mol}$$

$$\text{Moles} = C \times V = (0.3 \times 10^{-9}) \times (9.986 \times 10^{-15}) = 2.996 \times 10^{-24} \text{ mol}$$

$$\text{Number of particles} = \text{moles} \times N_A = 2.996 \times 10^{-24} \times 6.022 \times 10^{23} = 18.04 \times 10^{-1} = 1.8$$

Therefore, during a 10-second data acquisition, on average, 1.8 LC-AgNP particles are present in the focal volume. This is equivalent to acquiring data from 1 particle over 18 seconds, assuming linear scaling.

### Diffusion Characteristics of LC-AgNPs

The diffusion constant D is given by the Stokes-Einstein equation:

$$D = \frac{k_B T}{6\pi\eta r}$$

Where  $k_B$  is the Boltzmann constant = 1.380649 × 10<sup>-23</sup> J/K, T is the absolute temperature (in Kelvin),  $\eta$  is the dynamic viscosity of the fluid (in Pa·s), r is the radius of the particle (in meters).

$$D = \frac{1.380649 \times 10^{-23} \text{ JK}^{-1} \times 297.15 \text{ K}}{6 \times \pi \times 0.0009107 \text{ Pa.S} \times 23 \times 10^{-9} \text{ m}} = 1.04 \times 10^{-11} \text{ m}^2 \text{ s}^{-1}$$

### Diffusion Time Through Focal Volume

Using the relation  $\langle r^2 \rangle = 4 \times D \times \tau_D$ , and the lateral radius  $r = 649 \text{ nm}$ :

$$\tau_D = \frac{\langle r^2 \rangle}{4D} = \frac{(649 \times 10^{-9})^2 \text{ m}^2}{4 \times 1.04 \times 10^{-11} \text{ m}^2 \text{ s}^{-1}} = \frac{1.012 \times 10^{-13}}{10^{-11}} \text{ s} = 10.13 \text{ msec}$$

Assuming each LC-AgNP leaves the focal volume after this diffusion time and does not return within the 18-second data acquisition period, the maximum number of distinct LC-AgNPs detected in this time is:

$$\frac{18 \text{ sec}}{10.13 \text{ msec}} = 1777 \text{ particles.}$$

### Signal Scaling with A $\beta$ <sub>42</sub> Concentration

Therefore, at a sample concentration of 3.5  $\mu\text{M}$   $\text{A}\beta_{42}$ , the data could include signals from up to 1777  $\text{A}\beta_{42}$ -loaded LC-AgNPs. Therefore, at the detection limit of 218 nM  $\text{A}\beta_{42}$ , the number of detected  $\text{A}\beta_{42}$ -loaded LC-AgNPs is:  $(1777 \times 218 \text{ nM} \div 3500 \text{ nM}) = 110$ .

Thus, at our detection limit, an average of 110  $\text{A}\beta_{42}$ -loaded LC-AgNPs contributes to the measured signal during each 10-second.

**Table S2:** Comparison of the our SERS-based detection platform with other reported methods for detecting lipophilic- $\text{A}\beta_{42}$  oligomers.

Sl. No .	Reference	Method of Detection	Target Species	Detection Limit	Specificity towards lipophilic/ vesicle associated oligomers
1	High performance plasma amyloid- $\beta$ biomarkers for Alzheimer's disease. <i>Nakamura et al.</i> , 2018, <i>Nature</i> , 554, 249-254.	Immunoprecipitation-mass spectrometry	$\text{A}\beta_{42}$ , $\text{A}\beta_{40}$ , $\text{APP}_{669-711}$ (ratios)	Lower limit based on standard curves ( $\sim 40 - 160 \text{ pM}$ range, depending on peptide).	<b>No:</b> Targets primarily soluble peptides; no focus explicitly on oligomeric or membrane-bound forms.
2	New ELISAs with high specificity for soluble oligomers of amyloid $\beta$ -protein detect natural $\text{A}\beta$ oligomers in human brain but not CSF. <i>Yang et al.</i> , <i>Alzheimer's &amp; Dementia</i> , 2013, 9, 99–112.	Sandwich ELISA	Soluble $\text{A}\beta$ oligomers	$\sim 39 \text{ pg/ml}$ (using synthetic $\text{A}\beta$ dimer standards)	<b>No:</b> Explicitly targets soluble oligomers in brain extracts; no mention of membrane-associated forms.
3	Subtyping of circulating exosome-bound amyloid $\beta$ reflects brain plaque deposition. <i>Lim et al.</i> , <i>Nature Communication</i> , 2019, 10, 1144.	Amplified plasmonic exosome platform (with SPR)	Exosome-carrying prefibrillar $\text{A}\beta_{42}$ aggregates ( $\text{A}\beta_{42}^+$ and $\text{CD63}^+$ exosomes).	$\sim 200$ exosomes ( $10^5$ -fold improvement over Western blot; $10^3$ -fold over standard ELISA).	<b>Yes:</b> Targets $\text{A}\beta$ oligomers bound to exosomes (smallest of the extra-cellular vesicles); distinct from free soluble oligomers.
4	Bifunctional Fluorescent/ Raman Nanoprobe for the Early Detection of Amyloid. <i>Xia et al.</i> , <i>Nature Scientific Report</i> , 2019, 9, 8497.	Surface-enhanced Raman scattering and fluorescence.	$\text{A}\beta_{42}$ aggregates/ peptides.	Not explicitly stated; linear detection range $1-2 \text{ }\mu\text{M}$ (saturation $>2 \text{ }\mu\text{M}$ ).	<b>No:</b> No explicit distinction or preference for lipophilic forms.
5	Our method	Surface-enhanced Raman scattering	Lipophilic, membrane-bound small oligomers	$\sim 110 \text{ A}\beta_{42}$ -loaded-Lipid-bilayer coated AgNPs.	<b>Yes:</b> Specifically designed to detect lipophilic membrane associated $\text{A}\beta$

of A $\beta$ <sub>42</sub>

oligomers.