

1 **Supporting information**

2 **Hyaluronic acid-based Fabric with Blood induced Network**

3 **Densification and Tissue Adhesion for Bleeding Control**

4 Zhibo Xu,^{a,#} Linyu Wang,^{a,#} Xinwei Zheng,^a Ziying Wang,^a Yunxiang Weng,^a Qinhui

5 Chen,^a Haiqing Liu,^{a*} and Yan Fang^{a*}

6 ^a Fujian Key Laboratory of Polymer Materials, College of Chemistry and Materials
7 Science, Fujian Normal University, Fujian 350007, China

8 # Zhibo Xu and Linyu Wang contributed equally.

9 *Correspondence to: Haiqing Liu (E-mail: haiqingliu@fjnu.edu.cn)

10 Yan Fang (E-mail: fangyan_YWJ@fjnu.edu.cn)

11

12

13

14

15

16

17

18

19

20

21

22

23 **Experimental section**

24 ***Ex vivo* blood clotting index**

25 Fresh anticoagulated rat blood (50 μ L) was added dropwise onto material samples
26 ($10 \times 10 \text{ mm}^2$) and incubated at 37°C for 5 minutes. After gentle rinsing with 10 mL PBS
27 to remove unclotted components, 200 μ L supernatant was transferred to a 96-well plate.
28 Absorbance at 540 nm was measured using a microplate reader. A mixture of 200 μ L
29 of anticoagulated blood with 10 ml of PBS was used as a negative control. The BCI
30 was calculated as follows:

31
$$\text{BCI (\%)} = A_s/A_b \times 100\%$$

32 where A_s is the absorbance of the supernatant of the mixture of the material and
33 blood, and A_b is the absorbance of a mixture of 50 μ L rat blood and 10 mL PBS.

34 **Erythrocytes and platelets adhesion**

35 For adhesion of erythrocyte, samples ($10 \times 10 \text{ mm}^2$) in 5 mL tubes were incubated
36 with 2 mL diluted blood (37°C, 1 hours), washed with PBS, then fixed in 2.5%
37 glutaraldehyde for 4 hours. For adhesion of platelet, platelet-rich plasma (PRP) was
38 obtained by centrifuging whole blood (1200 rpm, 10 minutes). Samples were incubated
39 with 2 mL PRP (37°C, 1 hours). Following the incubation period, each sample was
40 rinsed thrice using PBS and then immersed in a 2.5% glutaraldehyde fixative for 1.5
41 hours. Erythrocytes and platelets were then dehydrated through a gradient ethanol (0%
42 to 100% in 10% increments, with two final steps at absolute ethanol), spending 10
43 minutes at each concentration. Following dehydration, samples were dried at 37°C for
44 48 hours and subsequently examined using SEM.

45 ***Ex vivo* blood coagulation time test**

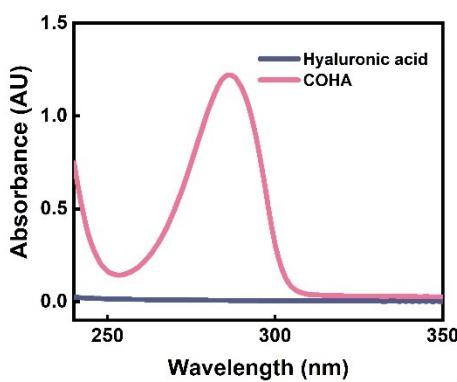
46 The 10×10 mm square samples were placed separately in individual wells of a 24-well cell culture plate, with 20 μ L of anticoagulated whole blood added to each well.

47 At predetermined time points, PBS was added to each well for washing to remove

48 unbound blood components. The coagulation endpoint of each sample was recorded

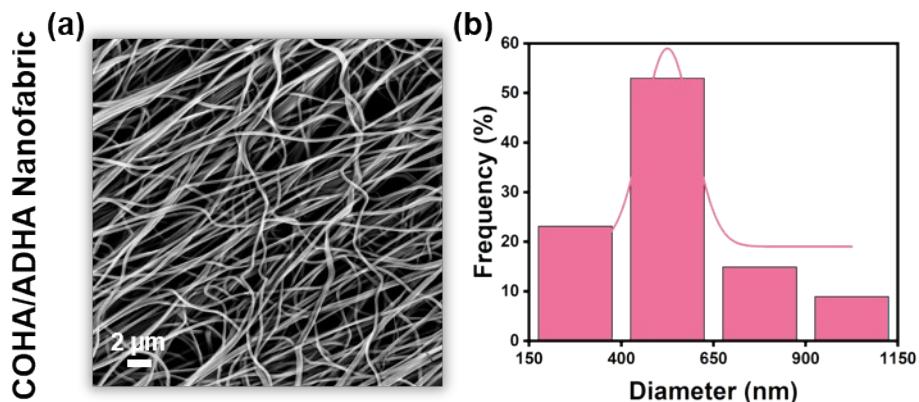
49 when the eluent became colorless and transparent.

50



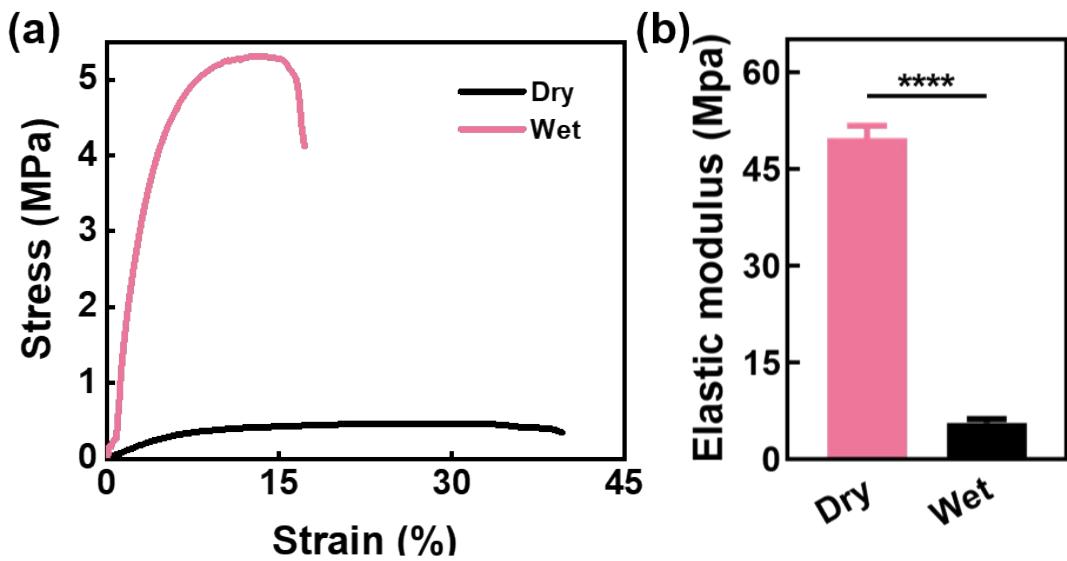
51

52 Figure S1 UV-vis spectra of hyaluronic acid and COHA.



53

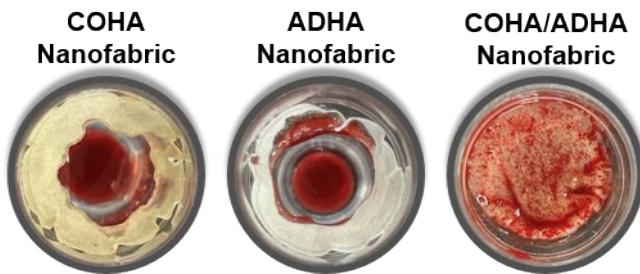
54 Figure S2 SEM images of COHA/ADHA nanofabric and histogram of diameter distribution of COHA/AHDA nanofabric.



56

57 Figure S3 Mechanical properties of COHA/ADHA nanofabric before and blood

58 contact. (a) Tensile stress-strain curves; (b) Bar charts of elastic modulus.

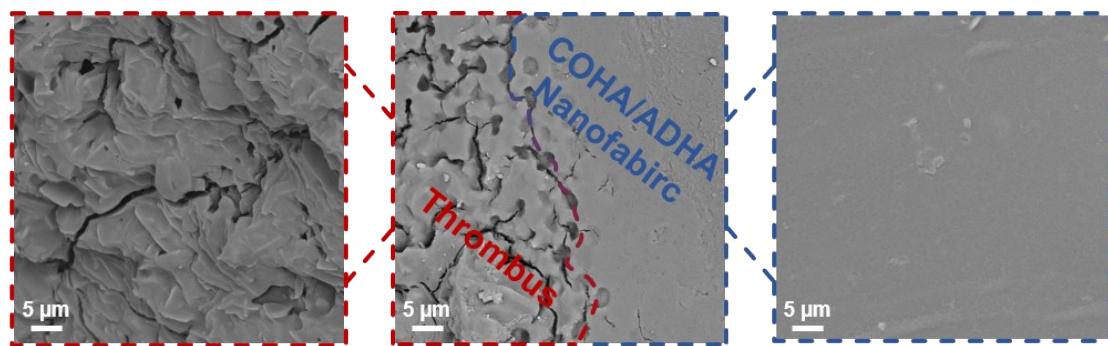


59

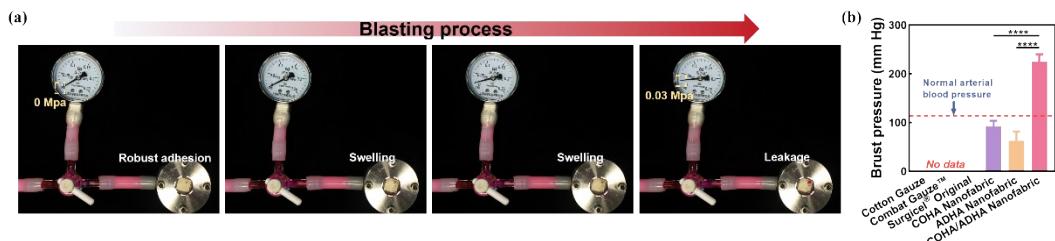
60 Figure S4 The photographs of COHA nanofabric, ADHA nanofabric, COHA/ADHA

61 nanofabric after the experiment of the blood blocking.

62



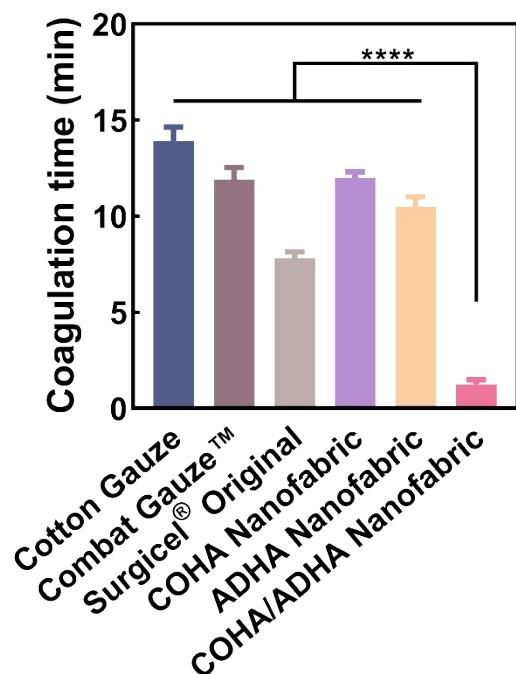
63 Figure S5 Post-blood contact SEM images of COHA/ADHA nanofabric.



64

65 Figure S6 (a) The images of the bursting pressure test of COHA/ADHA nanofabric; (b)

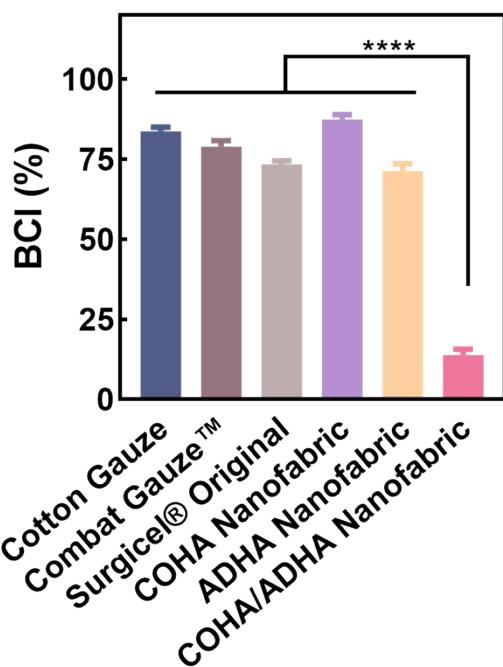
66 Bursting pressure of COHA nanofabric, ADHA nanofabric, COHA/ADHA nanofabric.



67

68 Figure S8 Coagulation time of cotton gauze, Combat Gauze™, Surgicel® Original,

69 COHA nanofabric, ADHA nanofabric, and COHA/ADHA nanofabric.



70

71 Figure S8 BCI values of cotton gauze, Combat GauzeTM, Surgicel® Original, COHA
72 nanofabric, ADHA nanofabric, and COHA/ADHA nanofabric.

73 Supplementary Table 1: Comparison of hemostatic performance between the present
74 COHA/ADHA nanofabric and representative nanofibrous materials from the literature.

Material Composition	Key Hemostatic Metrics	
	(<i>Ex vivo</i>)	(<i>In vivo</i>)
Chitosan, PEO, and Kaolin ¹	Clotting time: ca. 43 seconds SEM: Adhesion and activation of erythrocytes and platelets observed on CPK10 surface.	Hemostasis time: ca. 57.3 seconds; Blood loss: ca. 0.131 g. Notes: Relies on kaolin's pro-coagulant activity; the non-degradable component may

		raise considerations for long-term implantation.
κ -Carrageenan, CMCS, PVA and Tranexamic Acid ²	Clotting time: ca. 429 seconds SEM: Formation of a “fiber-clot” hybrid structure promoting erythrocyte adhesion; TXA loading enhanced platelet adhesion.	Hemostasis time: ca. 38.4 seconds; Significant reduction in blood loss. Notes: Functions primarily via drug release (“chemical intervention”); may have limited active tissue adhesion, posing potential interface bleeding risk.
Chitosan, N-alkylated Chitosan and PEO ³	Clotting time: ca. 58.8 seconds SEM: Extensive adhesion of erythrocytes and platelets, attributed to electrostatic interaction and platelet activation.	Hemostasis time: ca. 87 seconds; Blood loss: ca. 0.087 g. Notes: Mechanism is coagulation-pathway independent; may require secondary removal, adding procedural complexity.
Gelatin, Polycaprolacton	Clotting time: ca. 526 seconds SEM: Hydrophilic layer captures	Hemostasis time: ca. 59 seconds; Blood loss: ca. 0.18

e, Zeolite and Dopamine ⁴	blood cells; PCL layer acts as a penetration barrier.	g. Notes: Dual-layer design physically manages blood absorption and penetration; may rely more on physical sealing than active coagulation activation.
This Work: COHA, ADHA and PEO	Extremely short clotting time: ca. 60 seconds SEM: High adhesion ratios for erythrocytes (77%) and Platelets (82%). Mechanism: Catechol groups enhance platelet binding and erythrocyte aggregation; cross-linked network via Schiff base reaction effectively entraps blood cells.	Immediate physical sealing. Blood loss: 0.044 g. Notes: Synergistic mechanism: rapid hydrophilic absorption, protein interaction, fibrin-mimetic cross-linking, and dual-adhesive barriers. Fully degradable, eliminating secondary removal.

75 (1) Liu, T.; Zhang, Z.; Liu, J.; Dong, P.; Tian, F.; Li, F.; Meng, X. Electrospun kaolin-

76 loaded chitosan/PEO nanofibers for rapid hemostasis and accelerated wound healing.

77 *Int. J. Biol. Macromol.* **2022**, *217*, 998-1011.

78 (2) Salmasi, S. S.; Ehsani, M.; Zandi, M.; Saeed, M.; Sabeti, M. Polysaccharide-based

79 (kappa carrageenan/carboxymethyl chitosan) nanofibrous membrane loaded with

80 antifibrinolytic drug for rapid hemostasis- in vitro and in vivo evaluation. *Int. J. Biol.*
81 *Macromol.* **2023**, 247, 125786.

82 (3) Liu, T.; Liu, S.; Shi, Y.; Zhang, Z.; Ding, S.; Hou, K.; Zhang, W.; Meng, X.; Li, F.

83 Electrospun nanofiber membranes for rapid liver hemostasis via N-alkylated chitosan

84 doped chitosan/PEO. *Int. J. Biol. Macromol.* **2023**, 258, 128948.

85 (4) Song, Y.; Zhu, Y.; Wang, Q.; Chen, X.; Chen, Y.; Han, G.; Lu, W.; Guo, Y. One-

86 step Preparation of Antibacterial Gelatin/Polycaprolactone Nanofibrous Janus

87 Membranes for Efficient Hemostasis. *ACS Appl. Polym. Mater.* **2023**, 5, 7364–7374.

88