

## Supplementary Information

### A simple microfluidic dispenser for single-microparticle and cell samples.

A. Kasukurti, C.D. Eggleton, S.A.Desai, D.I. Disharoon, D.W.M. Marr\*

#### Section 1

##### Derivation of probability of doublets

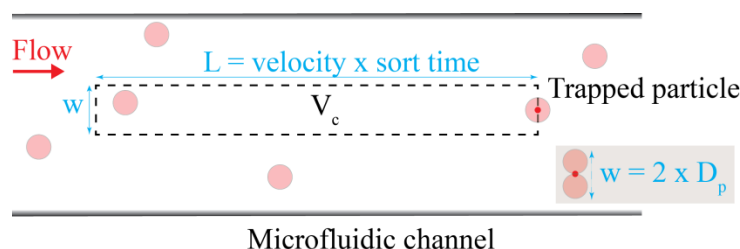


Figure S1: Schematic identifying the unit volume  $V_c$  encapsulating fluid volume flowing past the optical trap during the sorting. Here, width of the control volume  $w$  is the capture range of the optical trap and is approximately twice the particle diameter (inset image) and  $L$ , length of the control volume is the length of the column of fluid that will flow past the optical trap during the sorting. Marked in red is the optical trap and the pink circles represent microparticles or cells.

Doublets arise primarily due to optical trapping and isolation of multiple particles at once, which happens when a second particle flows into the trap after it has already trapped a sorting target. To identify the appropriate system parameters that influence doublet formation, we quantify the probability of a second particle in the fluid plug flowing into the optical trap during the time the detection system requires to identify and translate a trapped particle away from the particle streamlines. This fluid plug has unit volume  $V_c$ , of length  $L$ , width  $w$  and height  $h$  as illustrated in Figure S1. The total time the optical trap requires to detect and translate a particle or cell out of the path of this fluid plug is defined as  $\tau$  and with the average flow velocity  $v$ ,  $L = v\tau$ . We define a normalized concentration  $\varphi$  as the number of particles per defined unit volume  $V_c$  in the bulk sample at particle concentration  $C \mu\text{m}^{-3}$  and  $\varphi = CV_c = CLwh = Cv\tau wh$ . The probability of a unit volume having  $x$  number of particles is governed by a Poisson distribution  $P(x) = e^{-\varphi}(\varphi^x/x!)!$ . With this, the doublet probability becomes,

$$P_{\text{doublet}}(\varphi) = P(x > 0) = 1 - P(x = 0) = 1 - e^{-\varphi}$$

For our microparticle system,  $C = 3 \times 10^{-5} \mu\text{m}^{-3}$ ,  $v = 60 \mu\text{m s}^{-1}$ ,  $\tau = 1.2 \text{ s}$ ,  $w = 10 \mu\text{m}$ ,  $h = 10 \mu\text{m}$ ,  $\varphi = Cv\tau wh = 0.216$  and  $P_{\text{doublet}}(\varphi) = 19.42\%$ .

## Section 2

### Derivation of back force oscillation

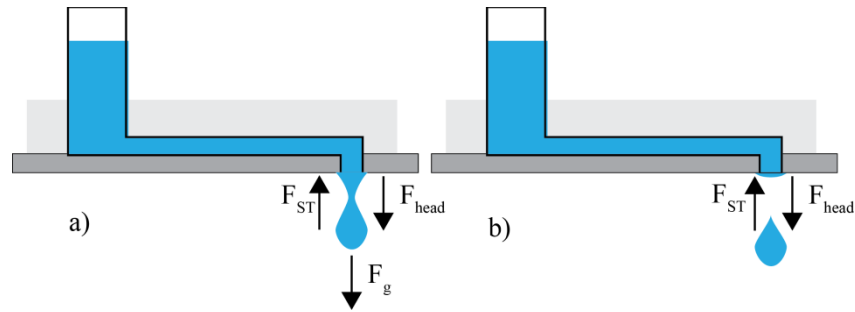


Figure S2: Illustration of the forces involved in droplet formation.  $F_{ST}$  is the force caused by surface tension,  $F_g$  is the gravitational force and  $F_{head}$  is due to the pressure head a) During droplet formation, surface tension forces pull the fluid up while pressure head and droplet mass pull the droplet down. b) Immediately after a droplet falls, there is no gravitational force due to the mass of the droplet opposing the surface tension force causing a sudden change in the force balance at the exit induces a back pressure wave proportional to the falling droplet weight.

The net force on the droplet while it is forming is,

$$F_b = \text{force due to pressure head} + \text{gravitational force} - \text{surface tension force}$$

, where surface tension forces arise due to the water-air hydrophobic glass interface and gravitational force due to the mass of the droplet being formed. Assuming pressure head and surface tension force are constant the droplet formation, oscillations in back force are approximately  $\Delta F_b = \Delta(\text{gravitational force}) = \Delta mg$ . With the droplet mass  $m$  of  $\sim 55$  mg, we expect oscillations in back force of  $\sim 550$  mN oscillations.

## Section 3

### Final Design parameters

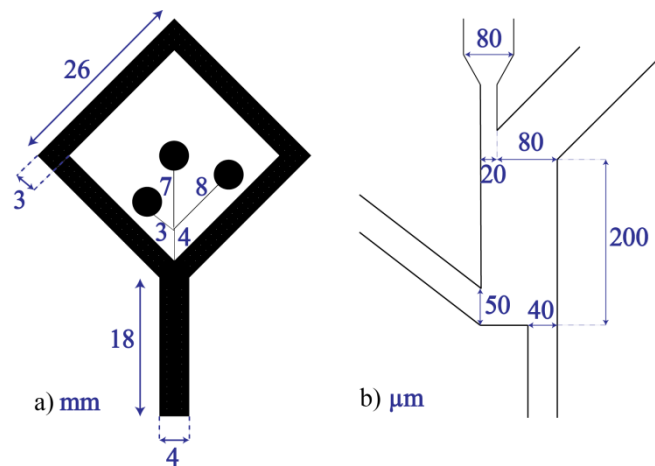


Figure S3: Device dimensions. a) Supply channels (mm). b) Particle isolation section ( $\mu\text{m}$ ). (see Figure 2 for location of each)

## References

S1. L. Mazutis, J. Gilbert, W. L. Ung, D. A. Weitz, A. D. Griffiths, and J. A. Heyman, *Nat. Protoc.*, 2013, **8**, 870–891.