

1 **Supplementary Data**

2 **For**

3 **A metronidazole-probe sensor based on imprinted biocompatible**
4 **nanofilm for rapid and sensitive detection of anaerobic protozoan**

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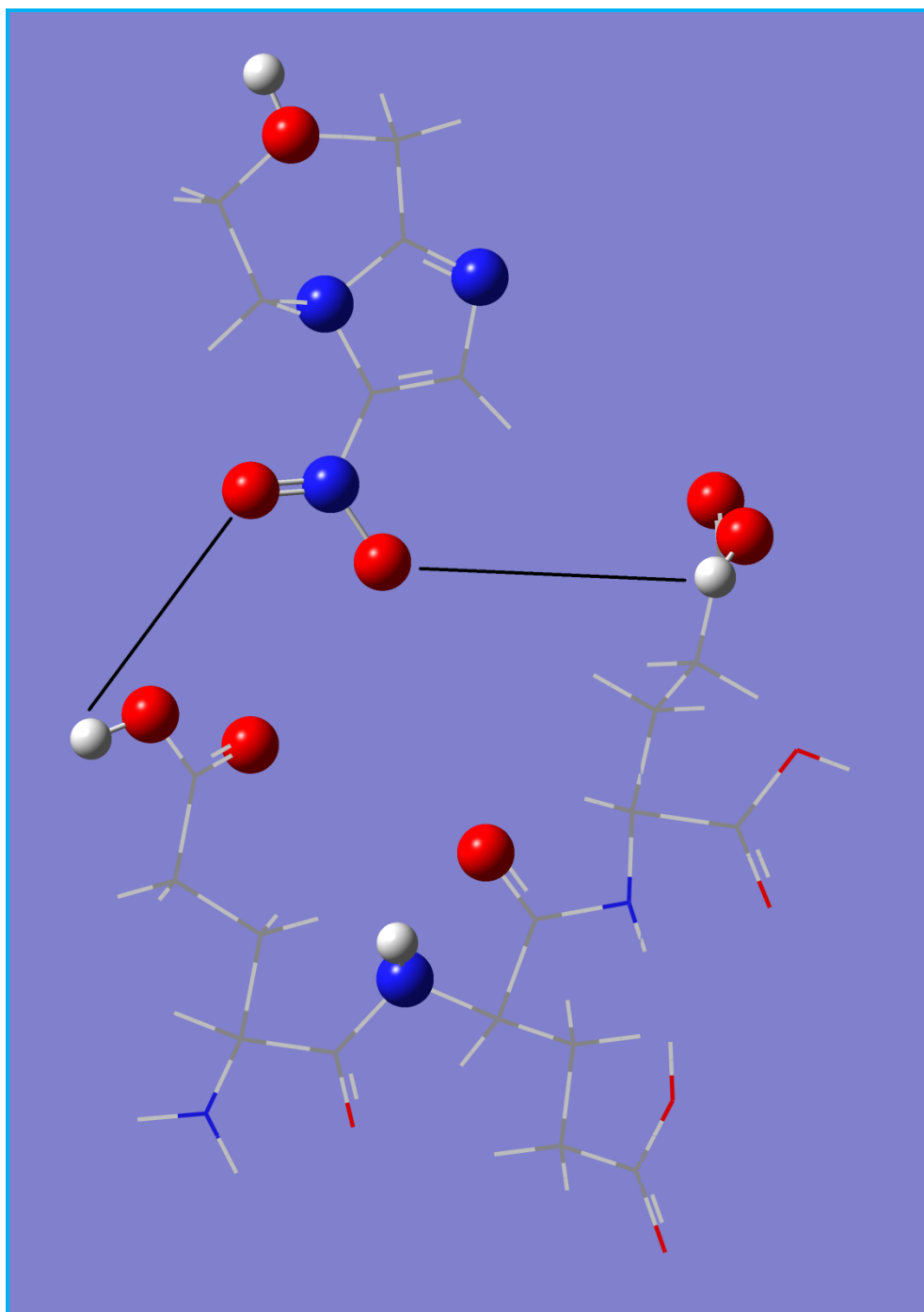
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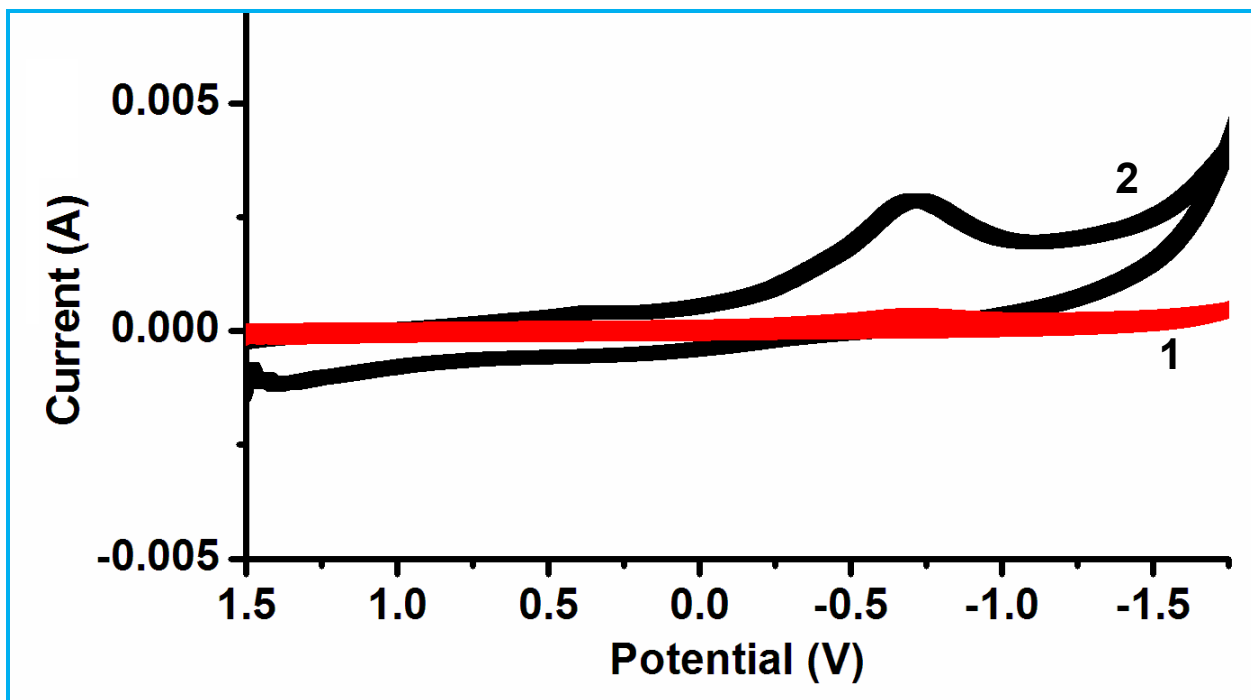
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16 **Figure S1:** Optimized conformation of the one sided complex of MDZ-PGA by multilayer
17 ONIOM method.



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20 **Figure S2:** Template rebinding study on MDZ-imprinted (run 1) and non-imprinted (run 2)
 21 polymer modified PGEs.

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25 **Table S1:** Comparative studies of surface roughness factor on modified and bare electrodes.

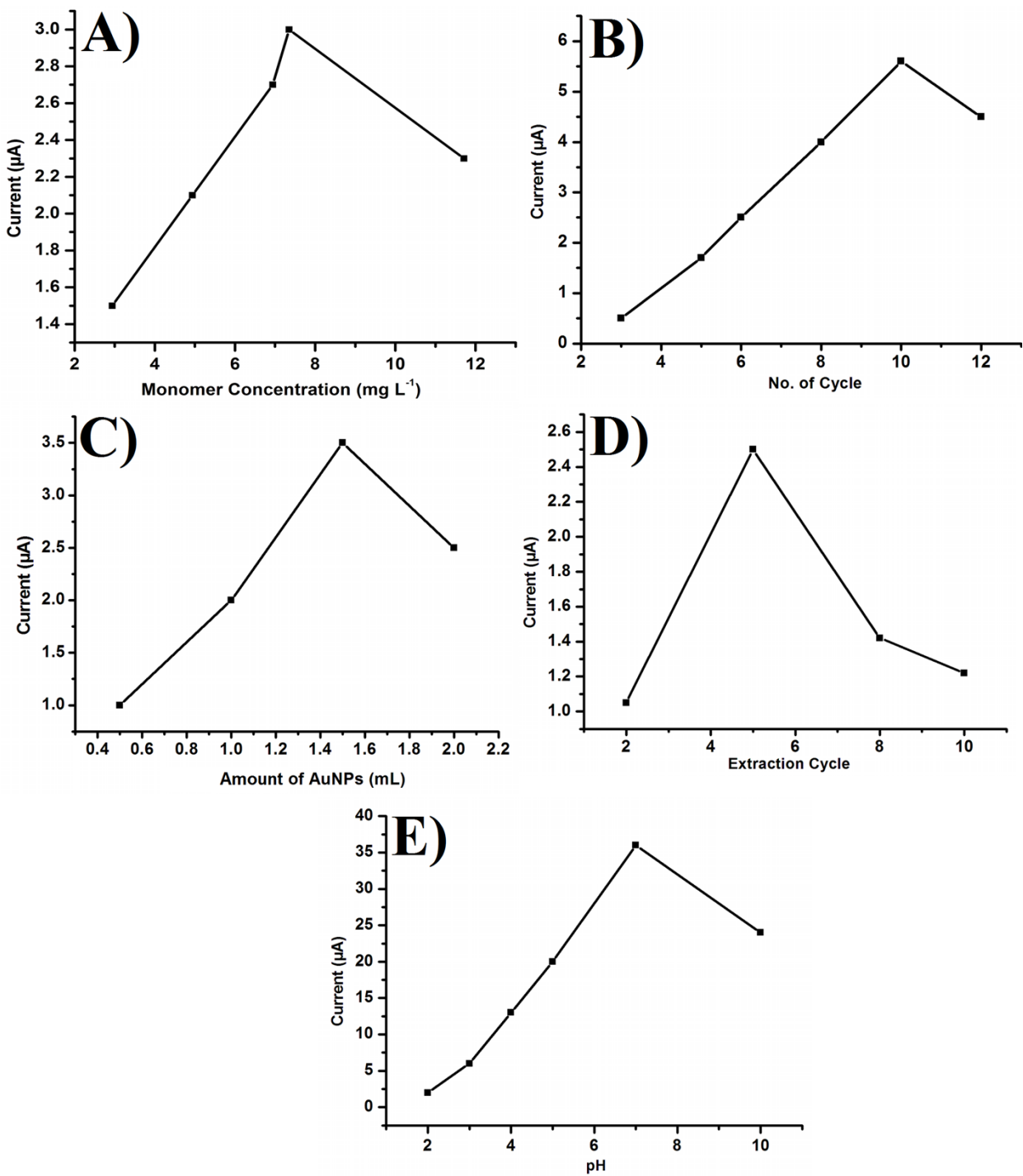
S.N.	Types of electrode	I_p (μA)	A (cm^2)	A_{geom} (cm^2)	$R_f = A / A_{\text{geom}}$
1.	Bare PGE	203	0.061	0.094	0.648
2.	PGA modified PGE	167	0.046	0.094	0.489
3.	AuNPs/PGA modified PGE	298	0.074	0.094	0.797

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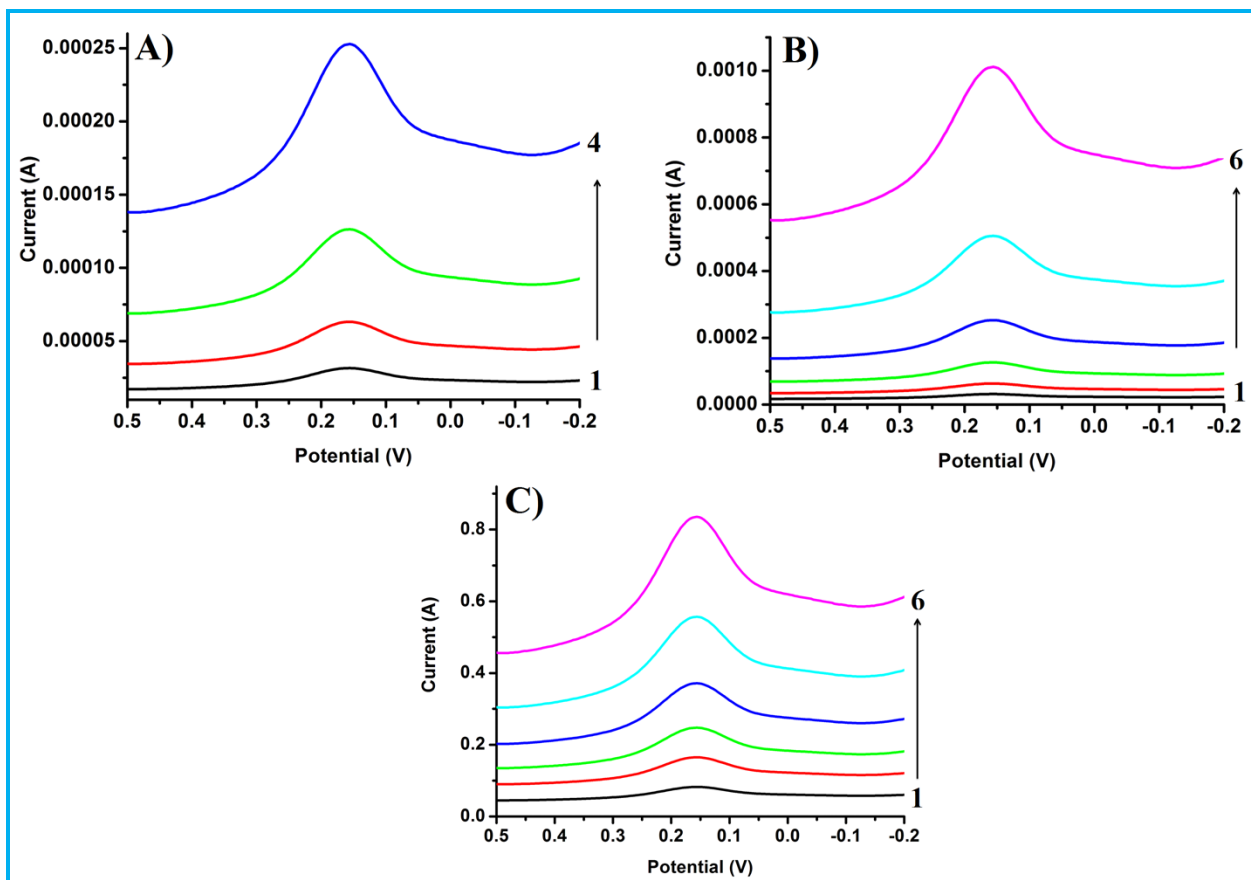
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31 **Figure S3:** Optimization of different parameters affecting sensor development: (A) monomer
 32 concentration, (B) number of cycle for electro-polymerization of glutamic acid, (C) amount of
 33 AuNPs, (D) number of cycle for MDZ extraction, and E) pH of supporting electrolyte.



35

36 **Figure S4:** DPSV runs for different concentration of MDZ in a potential range between +0.5 to
 37 -0.2 V in optimized condition (with 50mV modulation amplitude, 50ms pulse width and 5mV
 38 step potential): (A) 0.098 to 0.98 mg L⁻¹, (B) 1.0 to 12.0 mg L⁻¹, and (C) 30 to 130.0mg L⁻¹.

40 **S1. Optimization of deposition potential and deposition time**

41 Deposition potential and deposition time are very important parameters in the
42 electrochemical analysis. Herein, optimization of deposition potential and deposition time is also
43 performed. The DPSV current for 0.1 mgL⁻¹MDZ was found to be increasing with the increase
44 of deposition time up to 60s and then became constant. This indicated that the uptake of MDZ at
45 MIP electrode surface was quite facile, and the saturation occurred very fast. For the DPSV
46 measurements, accumulation potential was optimized to be -0.5 V, any value higher or lower
47 than this potential cause reduction in peak current.

48

49 **S2. Adsorption study of MDZ**

50 On the surface of PGE, chronocoulometry technique was applied to calculate the surface
51 coverage (Γ^0) and diffusion coefficient (D) of the MDZ. According to the integrated Cottrell
52 equation, the relation between charges (Q) vs. square root of time ($t^{1/2}$) can be described as
53 follows [S1]:

54
$$Q = 2nFAC(Dt)^{1/2}\pi^{-1/2} + Q_{ads} + Q_{dl} \quad (1)$$

55
$$Q_{ads} = nFA\tau^0 \quad (2)$$

56
$$I_p = \frac{n^2 F^2 I^0 A \vartheta}{4RT} \quad (3)$$

57 Where, A is the geometrical area of electrode that is ($9.4 \times 10^{-2} \text{cm}^2$), C is the concentration
58 ($14.2 \mu\text{M}$) of MDZ, Q_{dl} is the double layer charge, Q_{ads} is the Faradaic oxidative charge and other
59 symbols have their usual meanings. Q_{dl} is assumed not changed in the presence and absence of
60 MDZ in our total experiments. For MDZ-MIP, Q_{dl} and total charge ($Q_{dl} + Q_{ads}$) is evaluated
61 from the respective intercepts of the Anson plots (Q vs. $t^{1/2}$) in the absence and presence of
62 MDZ. The values of n and Γ^0 can be obtained as 4.0 and $1.06 \times 10^{-9} \text{mol cm}^{-2}$, respectively using
63 equations 1-3. In the present instance, Γ^0 reflects the total surface coverage of MDZ analyte
64 ($1.05 \times 10^{-10} \text{mol}$ or 6.05×10^{13} molecules) specifically bound to MIP cavities (each molecule per
65 cavity). From the slope of the Anson plot 'D' values can be calculated for MDZ is found to be
66 $2.47 \times 10^{-3} \text{cm}^2 \text{s}^{-1}$ for MDZ-MIP. The higher 'D' values may be explaining the surface
67 diffusivity of the template on the different modified electrodes.

68

69

70 **S3. Kinetic study of MDZ**

71 According to the Butler-Volmer model of electrode kinetics, the values of rate constant
72 (k_s) indicates that the rate of kinetics, required time for equilibrium and electron transfer
73 coefficient (α) is used to describe the symmetry between the reverse electron transfer steps.
74 Under investigation, potential shifting with scan rate supports the irreversibility of the
75 electrochemical reaction. Peak potential of an irreversible process obeys the following equations
76 [S2]:

$$\alpha n = \frac{1.857RT}{F(E_p - E_p)} \quad (4)$$

77

$$E_p = E_p - b(0.52 - 0.51 \log_b d - \log k_s + 0.5 \log v) \quad (5)$$

78

$$b = \frac{2.303RT}{\alpha nF} \quad (6)$$

79

80

81 Where, $b = 2.303RT/\alpha nF$, α = electron transfer co-efficient, n = no. of electron, E_p = peak
82 potential, D = diffusion co-efficient, v = scan rate.

83 Let us think in terms of energy barriers between the oxidized form and the reduced form as $Ox +$
84 $e^- = Red$, the free energy of the reactants can be changed by increasing or decreasing the potential
85 applied to the electrode. The extent to which the free energy changes contributes to a change in
86 the activation energy is dependent on the magnitude of α , which ranges from 0 to 1. Herein, the
87 estimated values of α and k_s , for the reduction of MDZ at MIP-modified PGE were found to be
88 0.1986 and 0.232 $cm s^{-1}$, respectively using above equations (4-6). Therefore, the lower value of
89 α (<0.5) suggests the irreversibility of the process, whereas the higher value of k_s indicates a fast
90 kinetics due to the role of MIP-cavities present at the electrode surface.

91

92 **Reference:**

93 S1. A. Bard, L.R. Faulkner, *Electrochemical Methods Fundamentals and Application*, second
94 ed., John Wiley and Sons, New York, 1980.

95 S2. E. Laviron, General expression of the linear potential sweep voltammogram in the case of
96 diffusion less electrochemical system, J. Electroanal. chem. 101 (1979)19-28.